

The Application of Interferometry to Magnetic Resonance Imaging

BASP Frontiers 2011.09.07

Ken Johnson

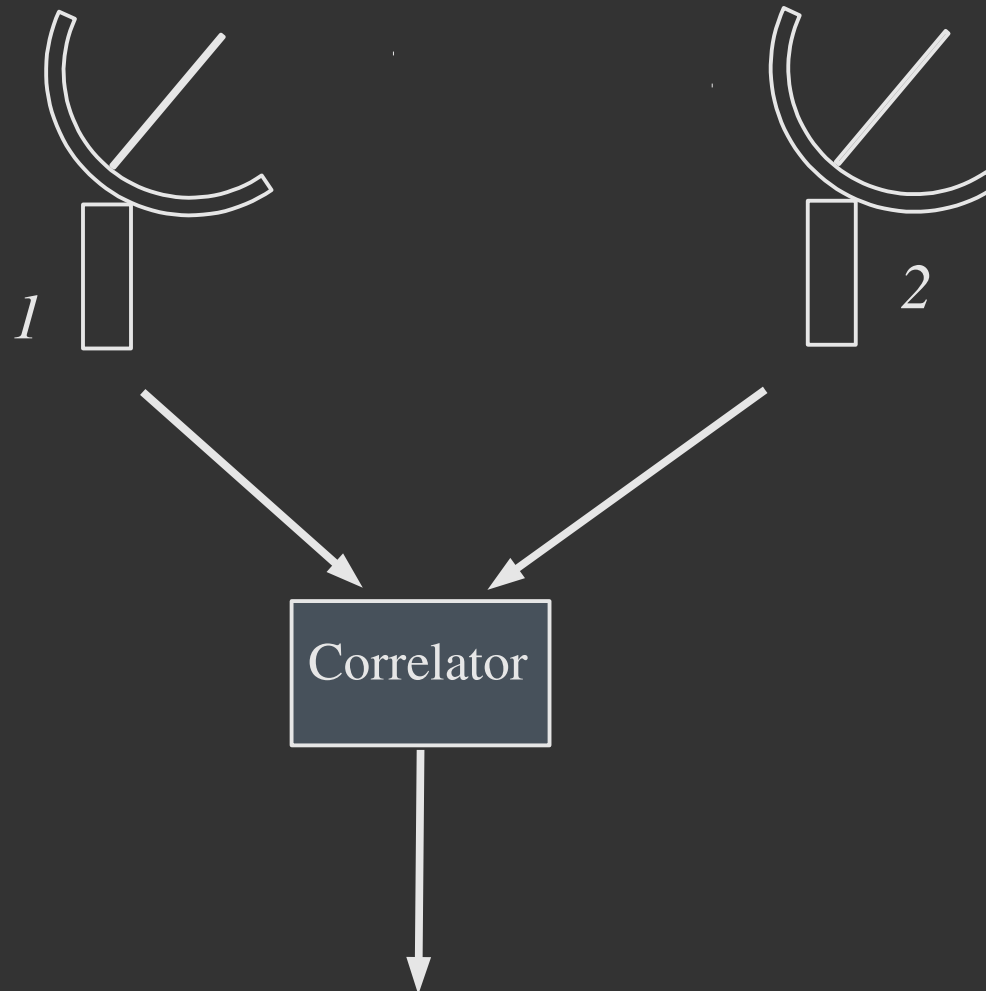
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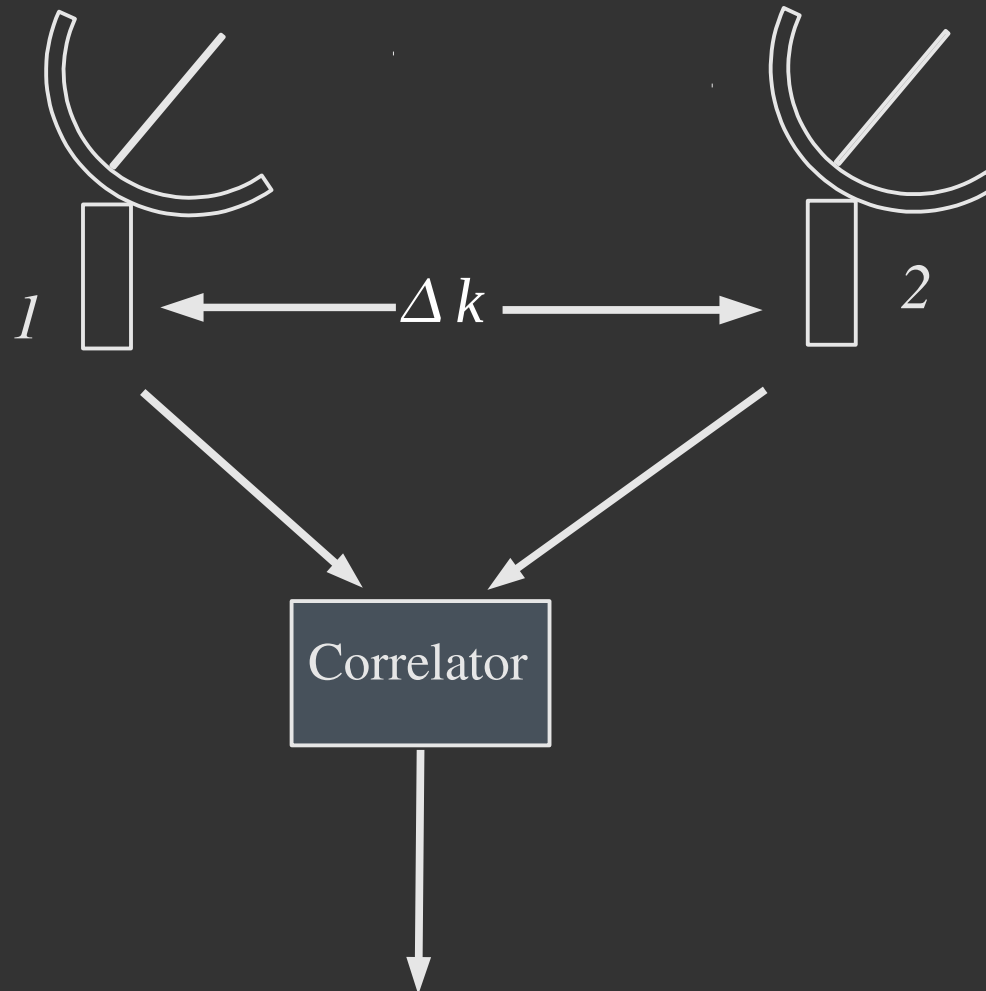
Introduction

- Interferometry is a powerful imaging technique
 - Radio Astronomy
 - Satellite Geography
 - Optical Coherence Tomography (OCT)
- Application of interferometry to MR
 - enhanced resolution
 - reduction in scan time
- Results for 1-D and 2-D (+time) MR Spectroscopic Imaging

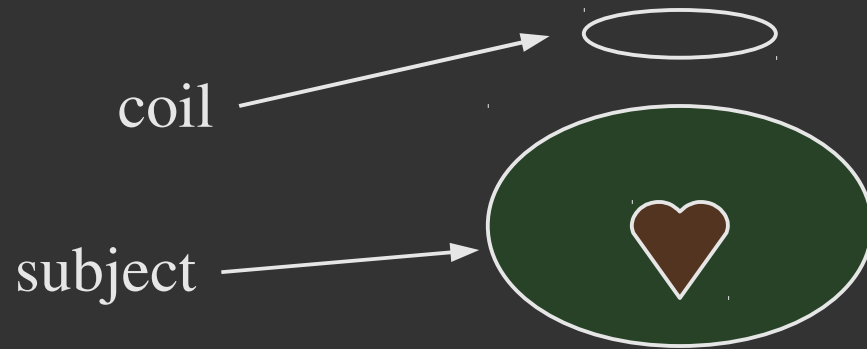
Interferometry in Radio Astronomy



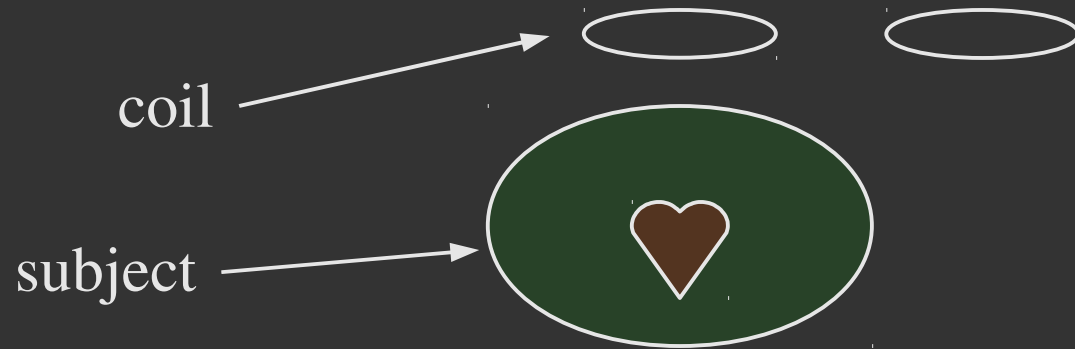
Interferometry in Radio Astronomy



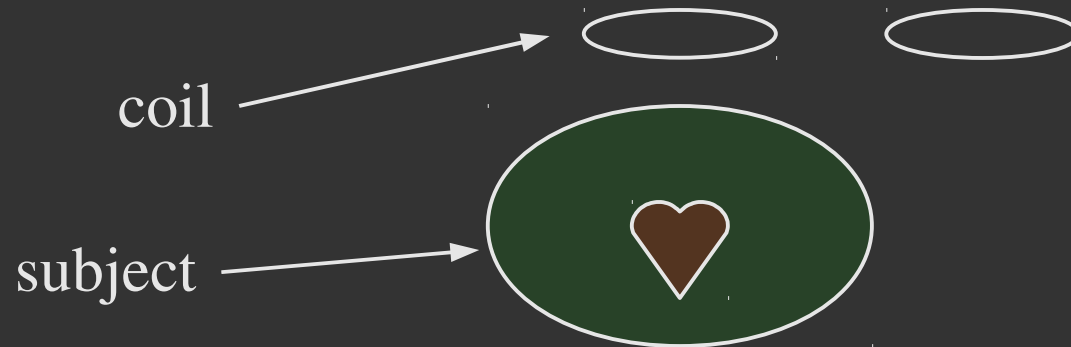
Interferometry to MR



Interferometry to MR

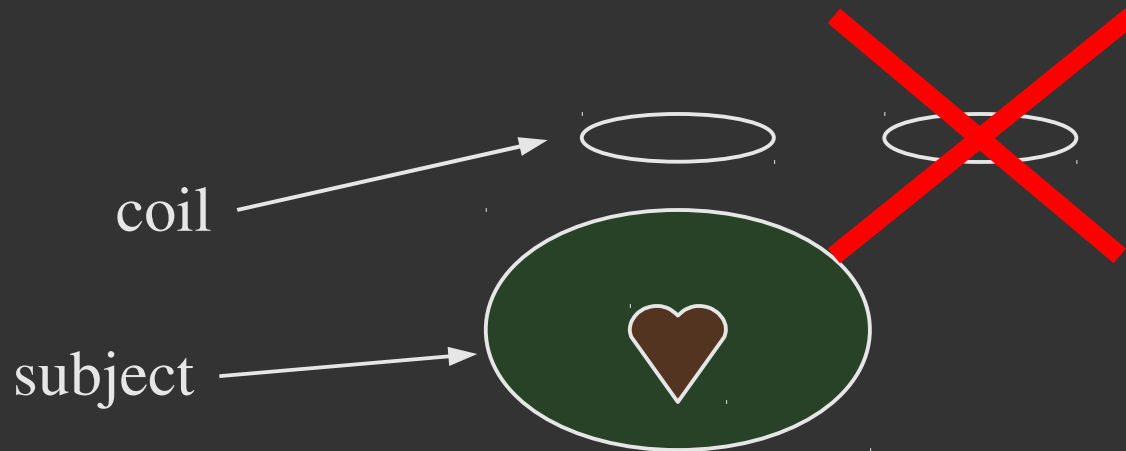


Interferometry to MR



- Direct application: Coils need to be 3×10^8 m apart

Interferometry to MR



- Direct application: Coils need to be 3×10^8 m apart
- Correlate signals from a single coil

Interferometry

$$s(r, f) \underset{FT}{\Leftrightarrow} S(k, t)$$

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$$\Gamma(k_1, k_2, \tau) = \int S(k_1, t) S^*(k_2, t - \tau) dt$$

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- With incoherence

$$|s(r, f)|^2 \underset{FT}{\Leftrightarrow} \Gamma(\Delta k, \tau) \quad \Delta k = k_1 - k_2$$

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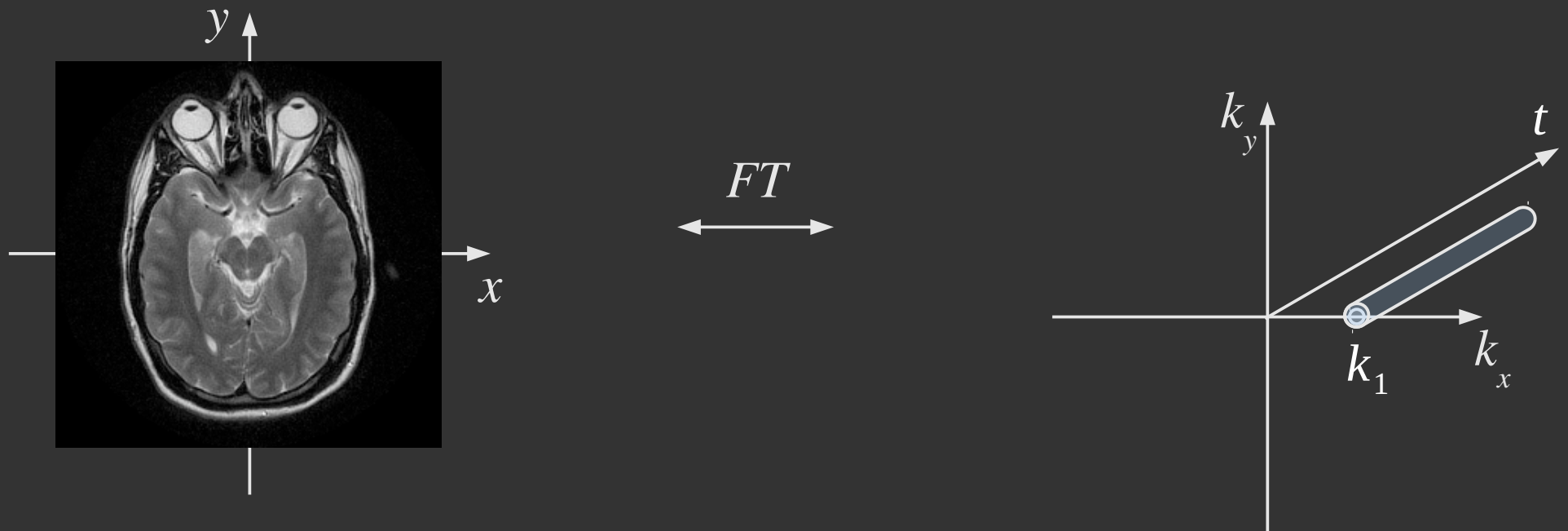
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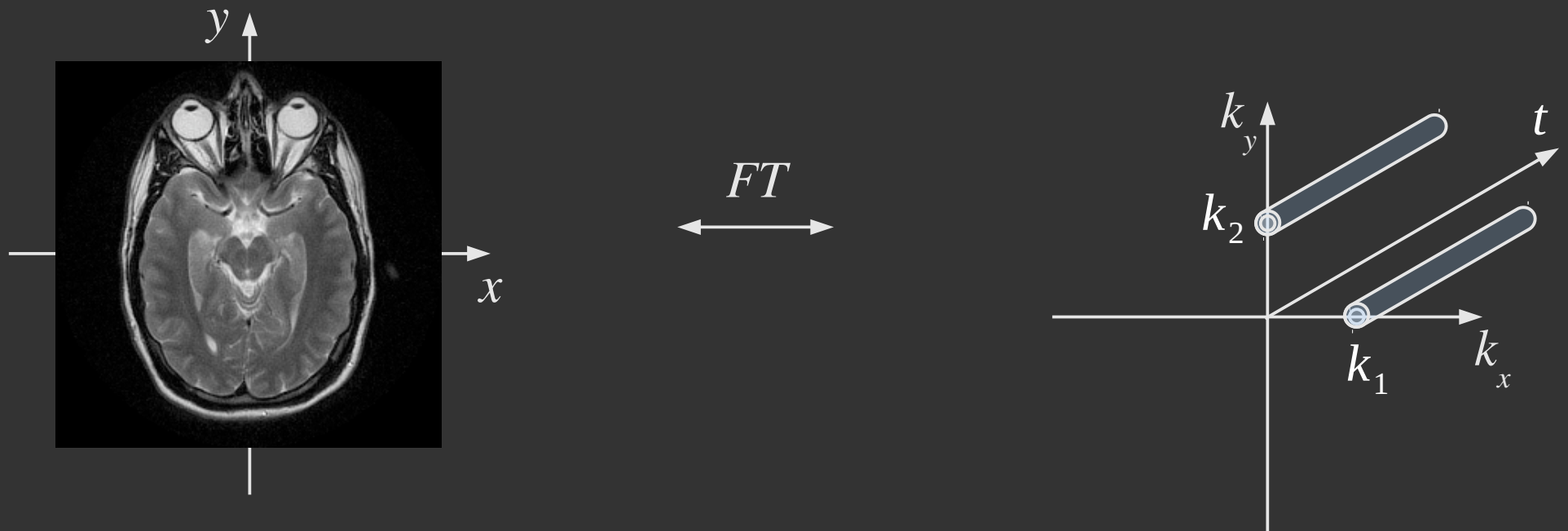
$$|s(r, f)|^2 \underset{FT}{\Leftrightarrow} \Gamma(\Delta k, \tau) \quad \Delta k = k_1 - k_2$$

- For N positions of k , there are at most $N(N-1)$ positions of Δk

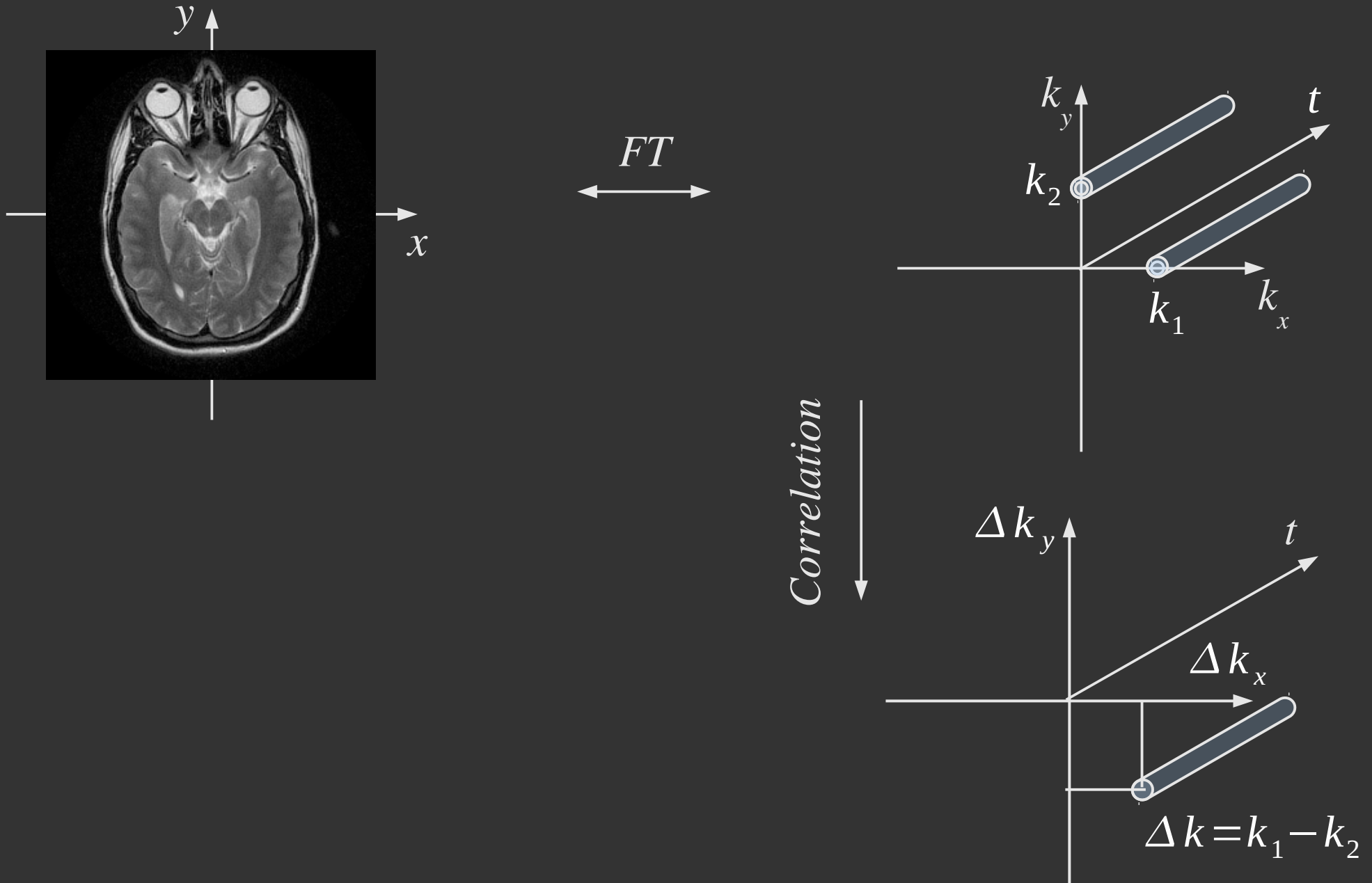
MR Interferometry



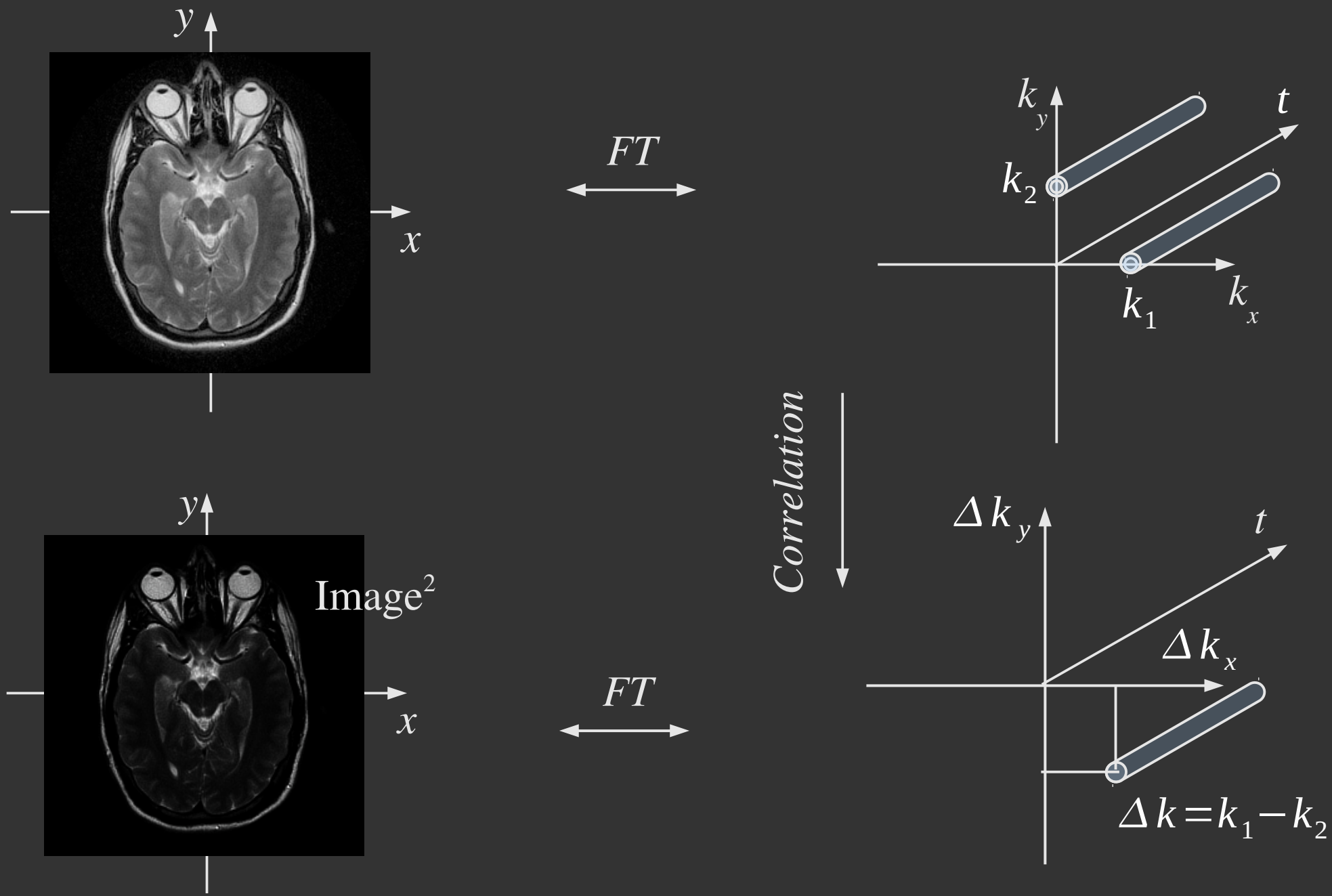
MR Interferometry



MR Interferometry



MR Interferometry



Proof of Concept

12x12x2080

Spectroscopic
Image

$$\sum_f |s(\vec{r}, f)|$$

Standard



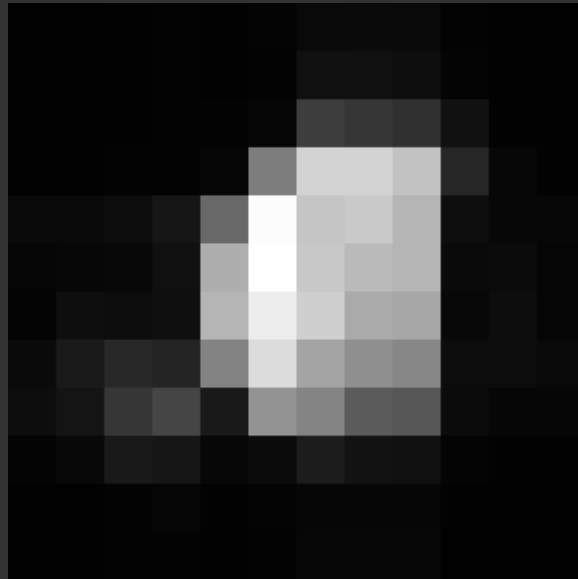
Proof of Concept

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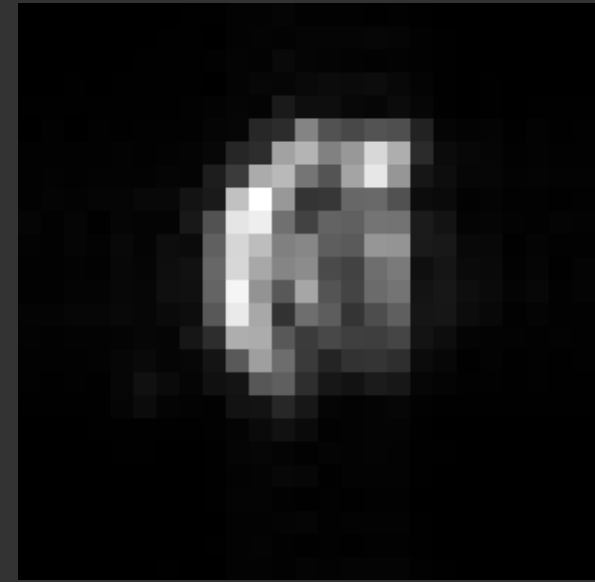
Spectroscopic
Image

$$\sum_f |s(\vec{r}, f)|$$

Standard



Interferometry



$$\sum_f |s(\vec{r}, f)|^2$$

Proof of Concept

12x12x2080

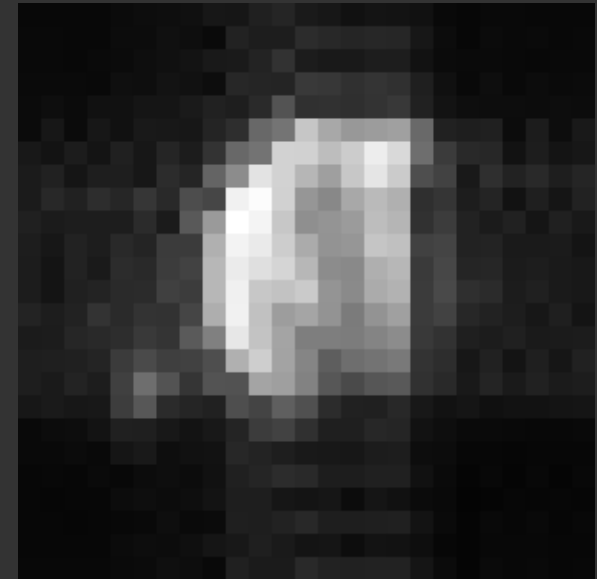
Spectroscopic
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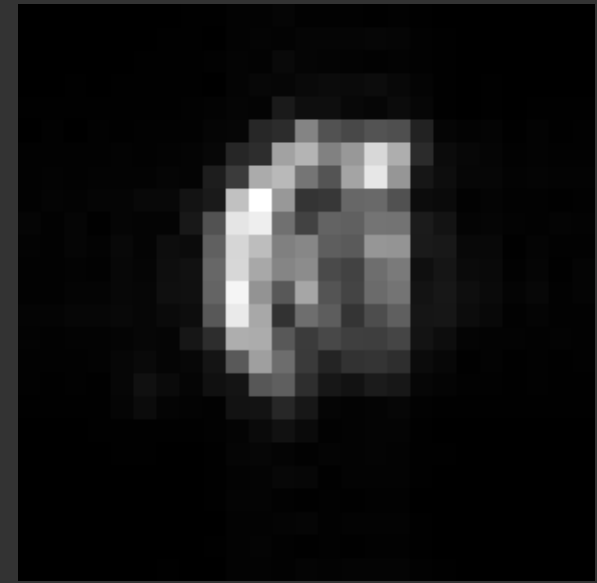
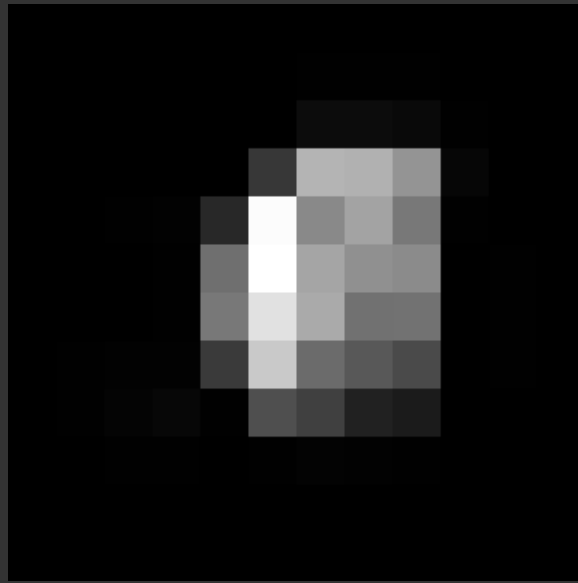
Standard



Interferometry



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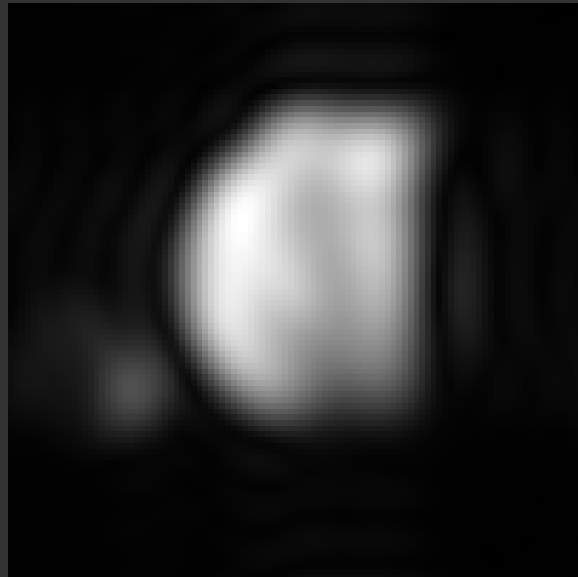
Proof of Concept

12x12x2080

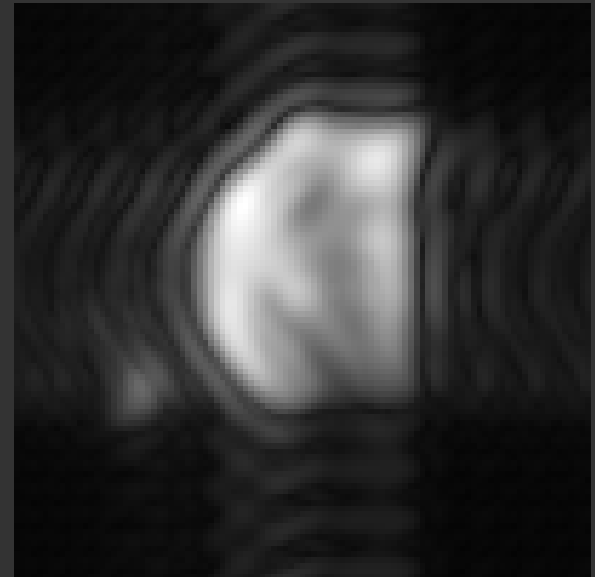
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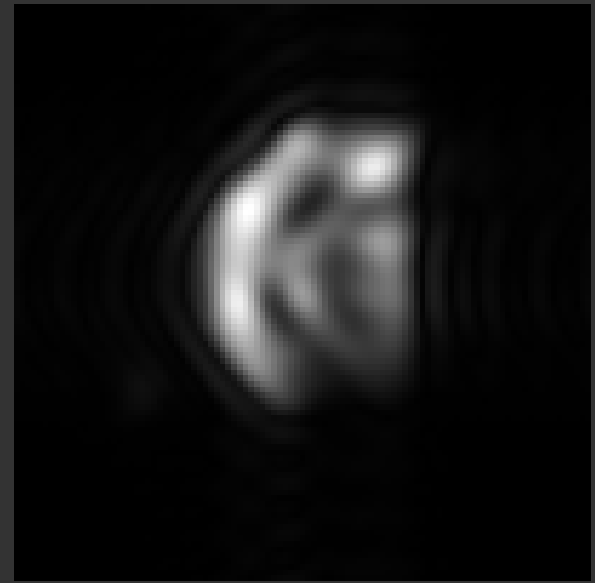
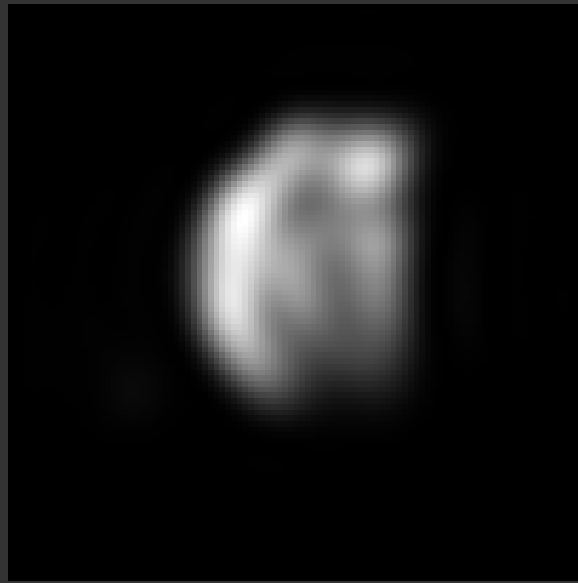
Standard



Interferometry



$$\sum_f |s(\vec{r}, f)|^2$$

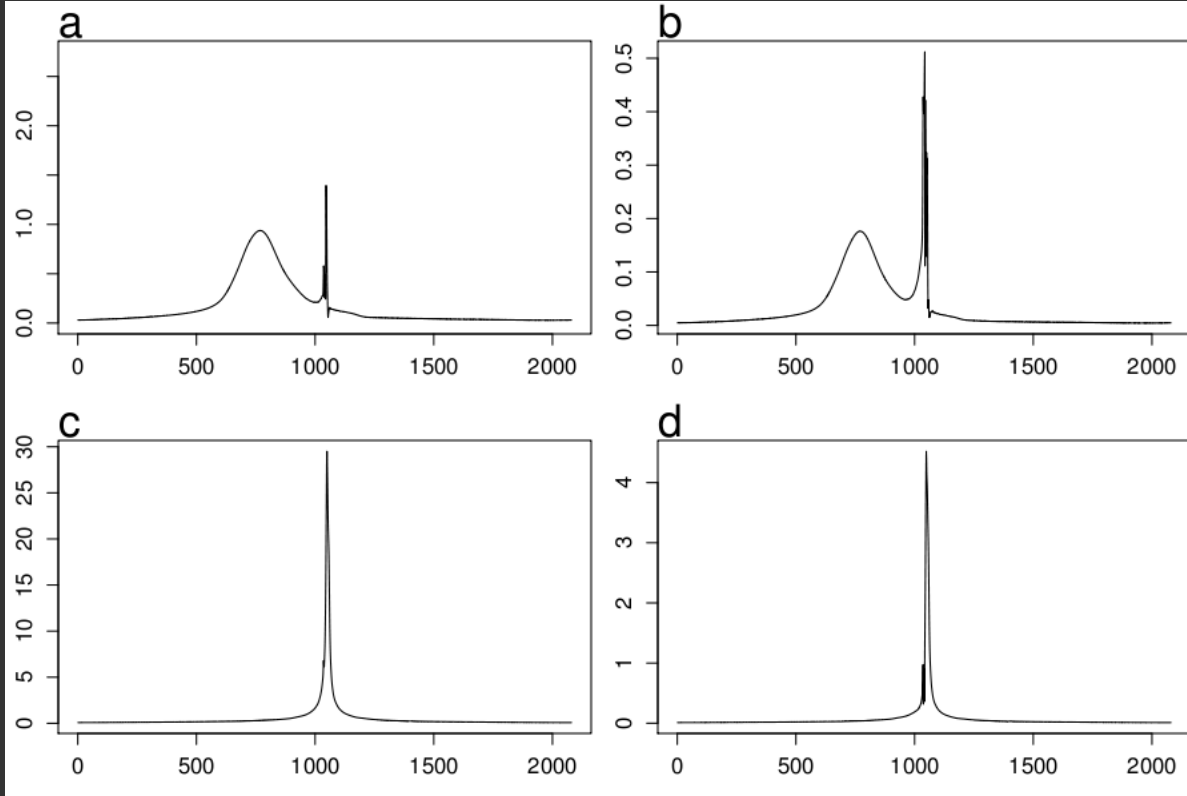


Proof of Concept

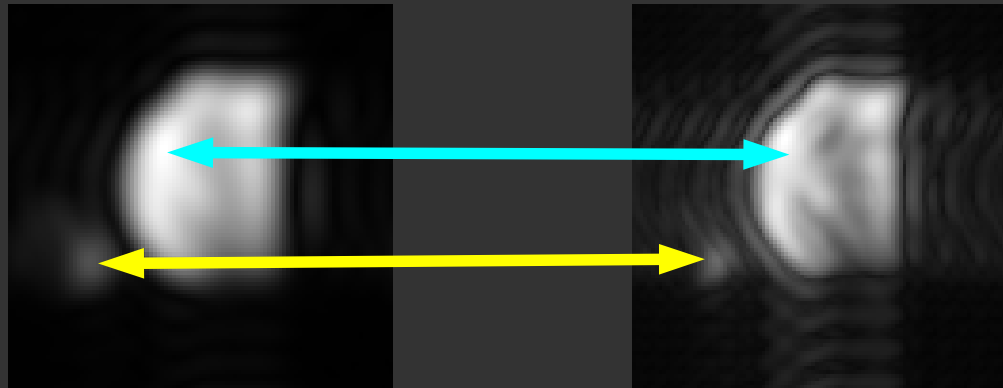
Standard

Interferometry

Lipid



Water



Complication: Coherence

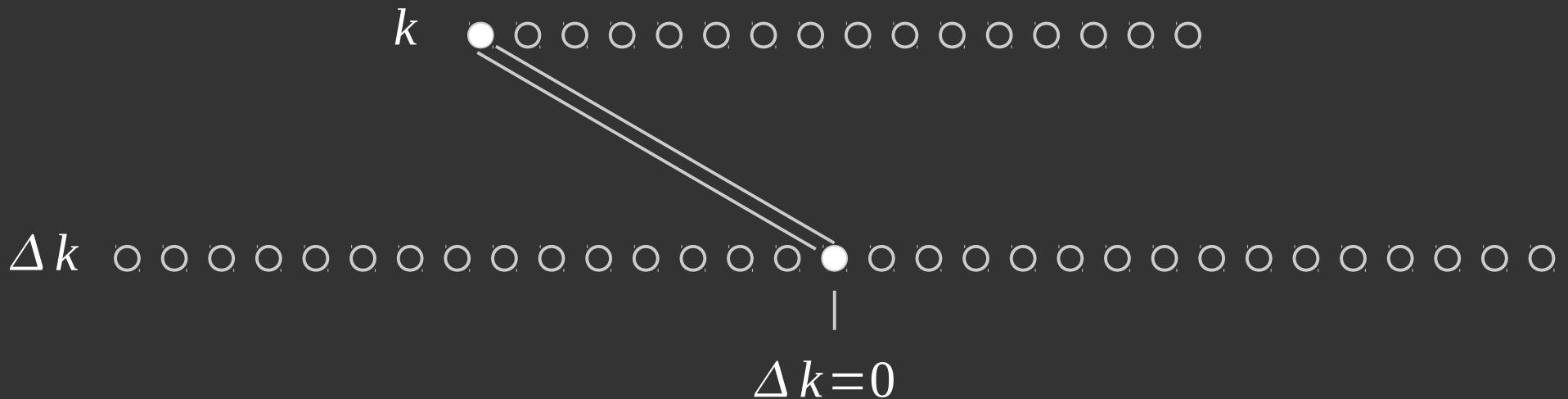
- Voxels will confound with other voxels that oscillate at the same frequency

Complication: Coherence

- Voxels will confound with other voxels that oscillate at the same frequency
- A gradient during readout will avoid coherence for a 1-D image

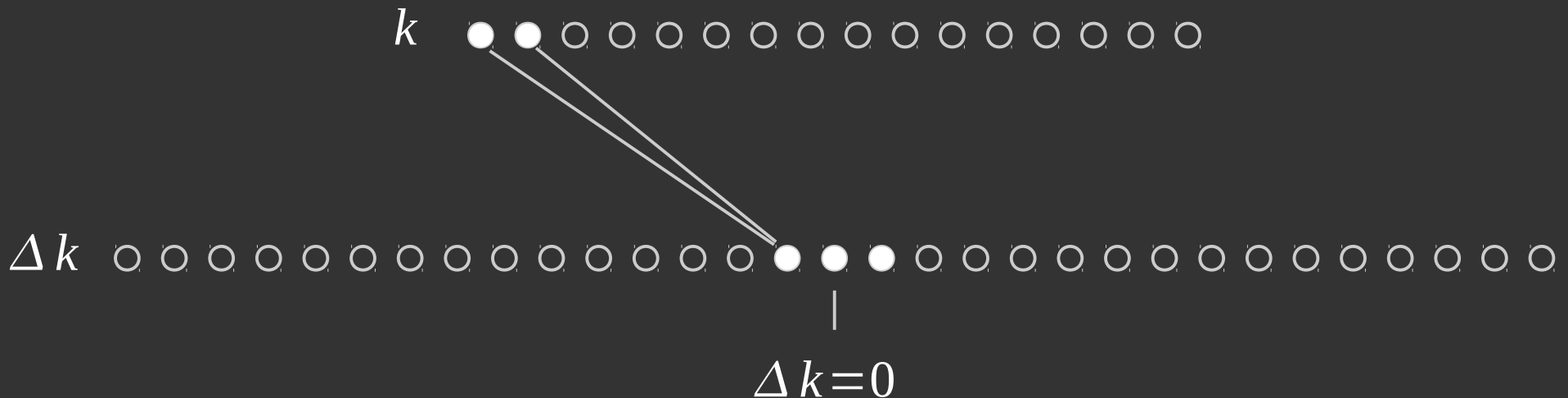
1-D Incoherent Image

- Subset of k -space locations will fully map new domain



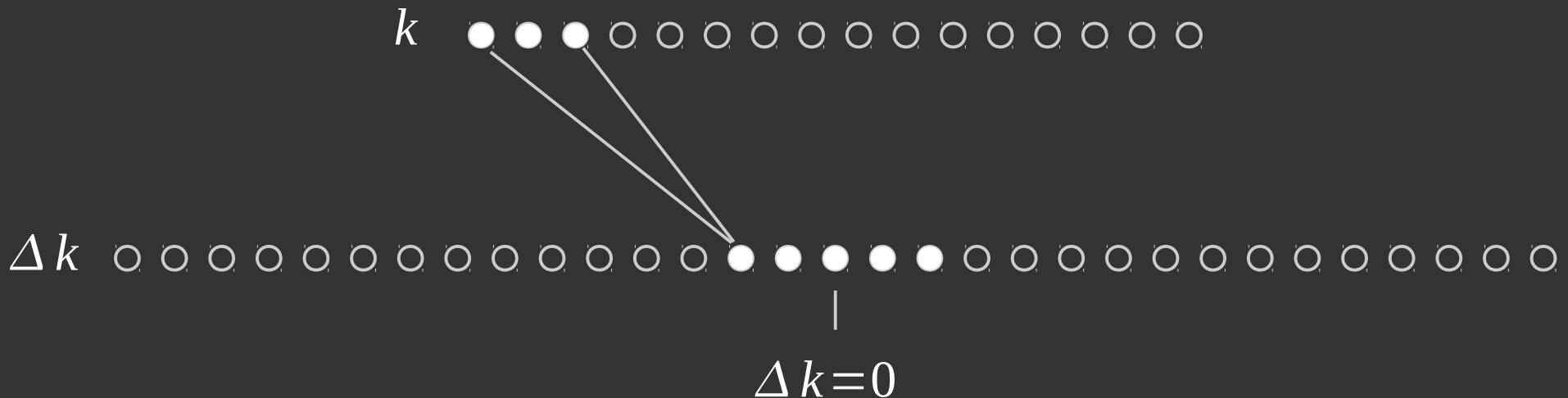
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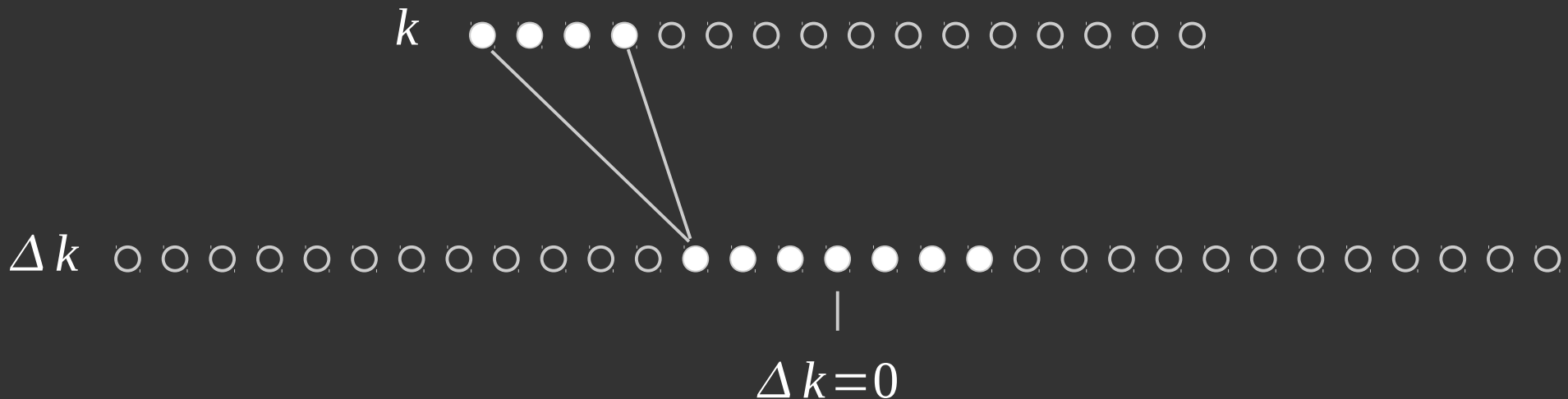
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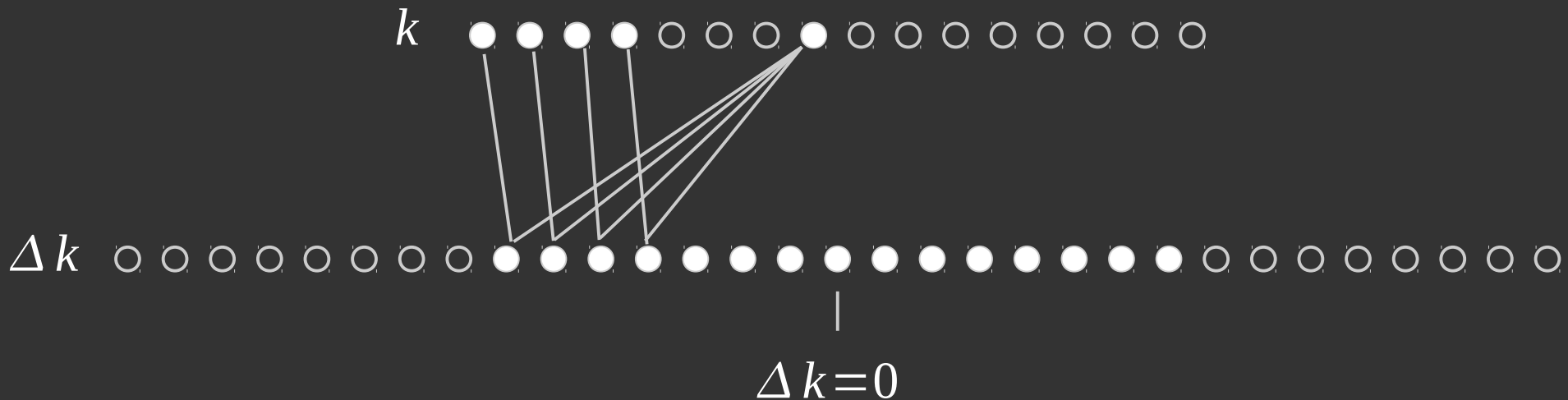
1-D Incoherent Image

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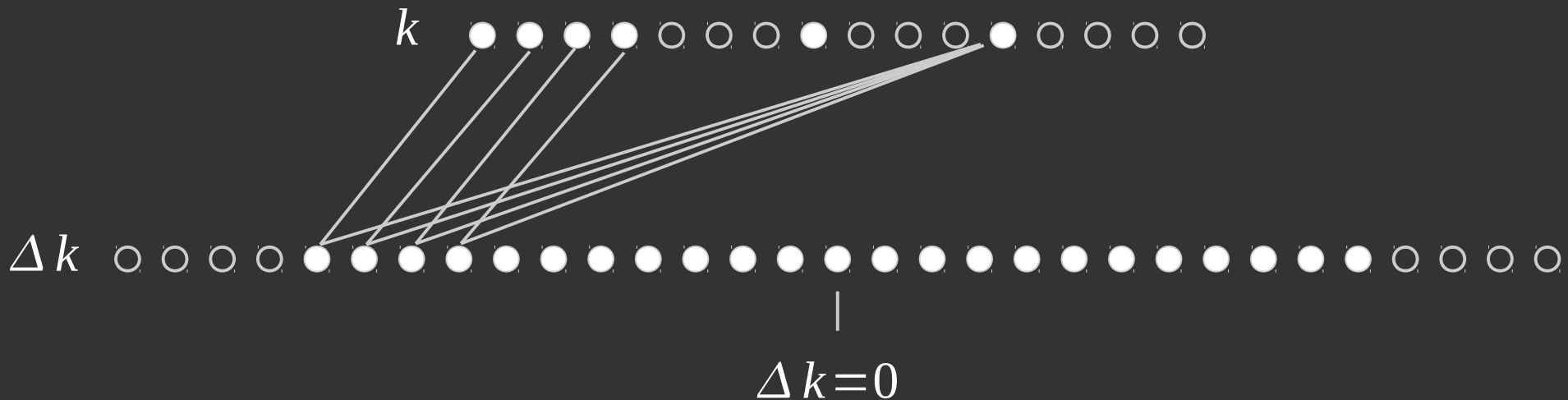
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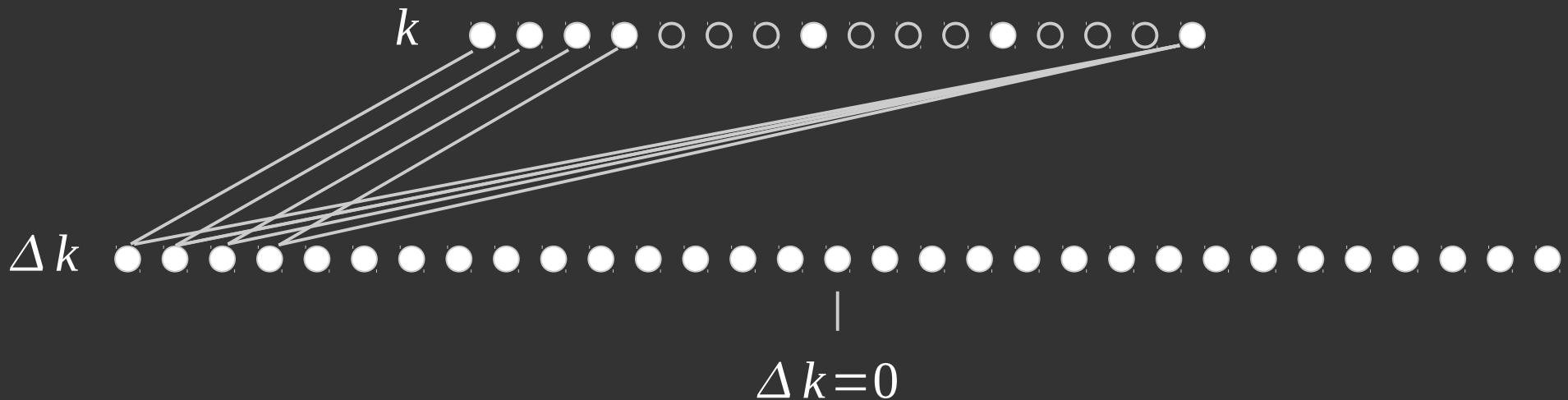
1-D Incoherent Image

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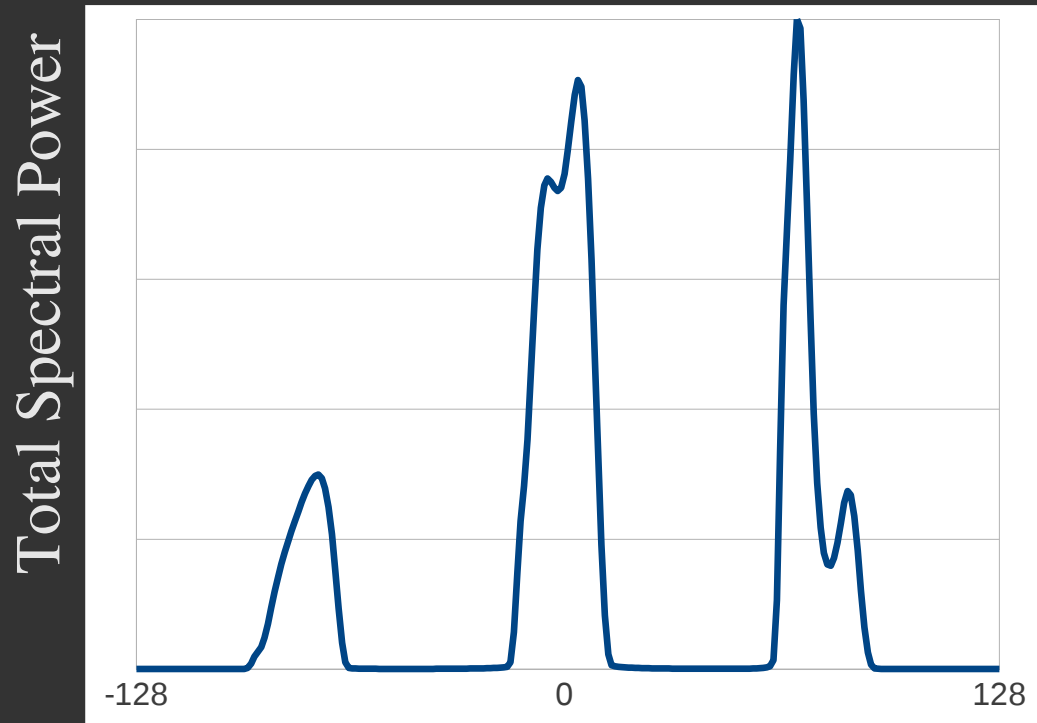


1-D Incoherent Image

- Subset of k -space locations will fully map new domain



1-D Spectroscopic Imaging



← x →

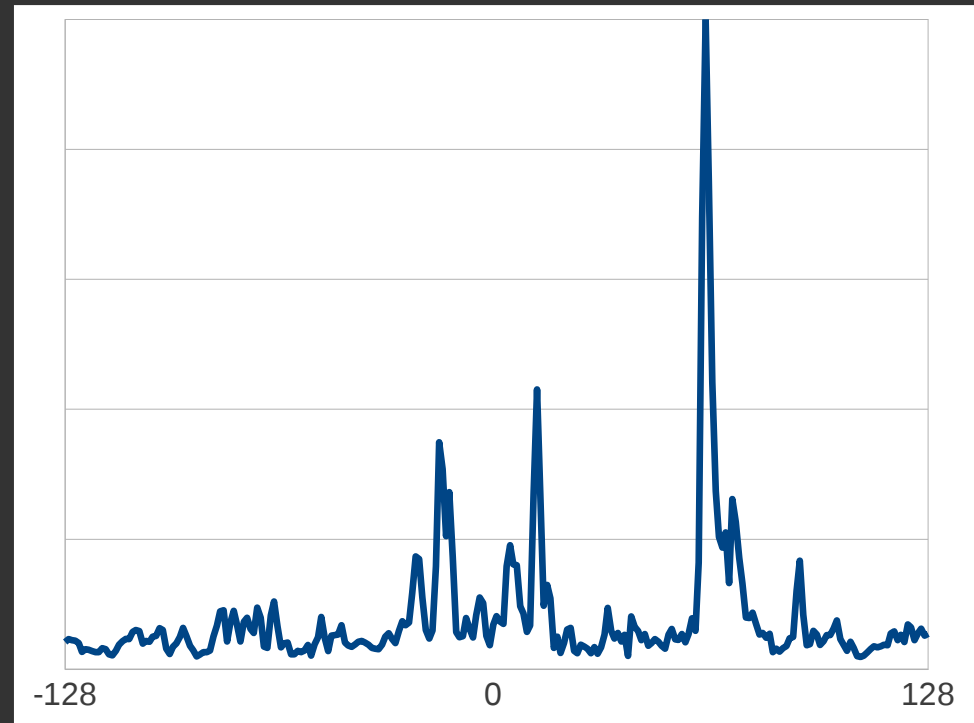
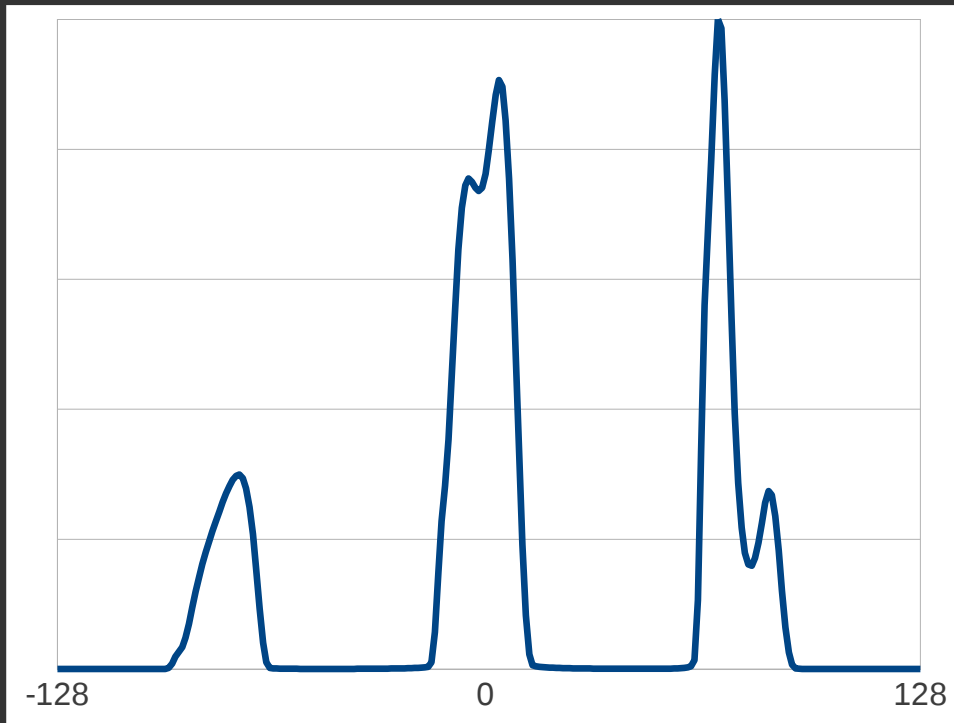
Standard

(257 phase encodes)

1-D Spectroscopic Imaging

Coherent (no readout gradient)

Total Spectral Power



← x →

Standard

(257 phase encodes)

← x →

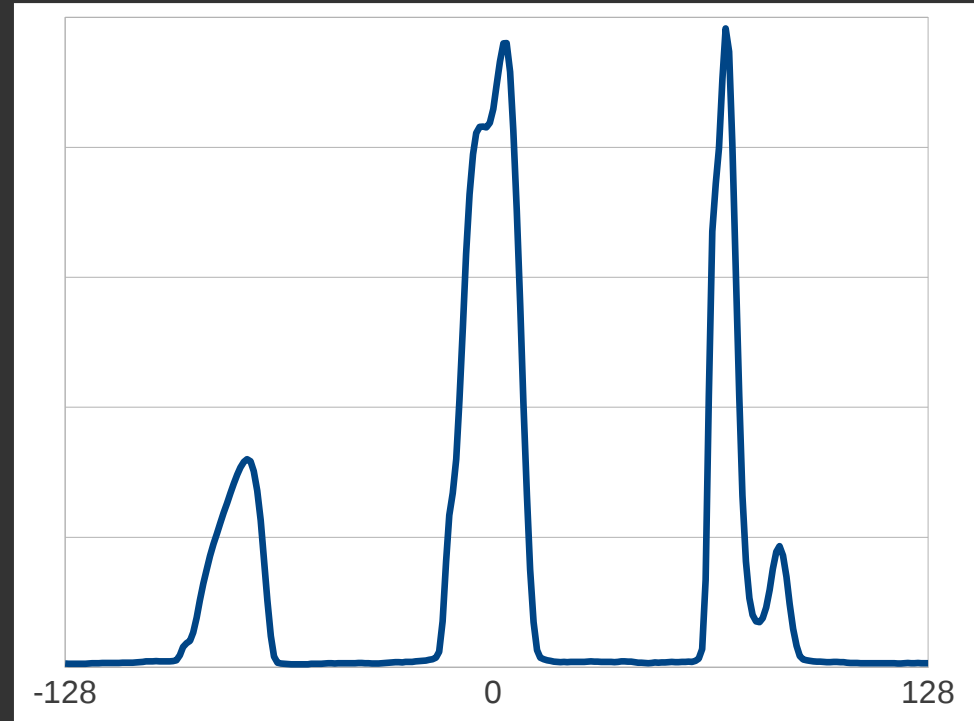
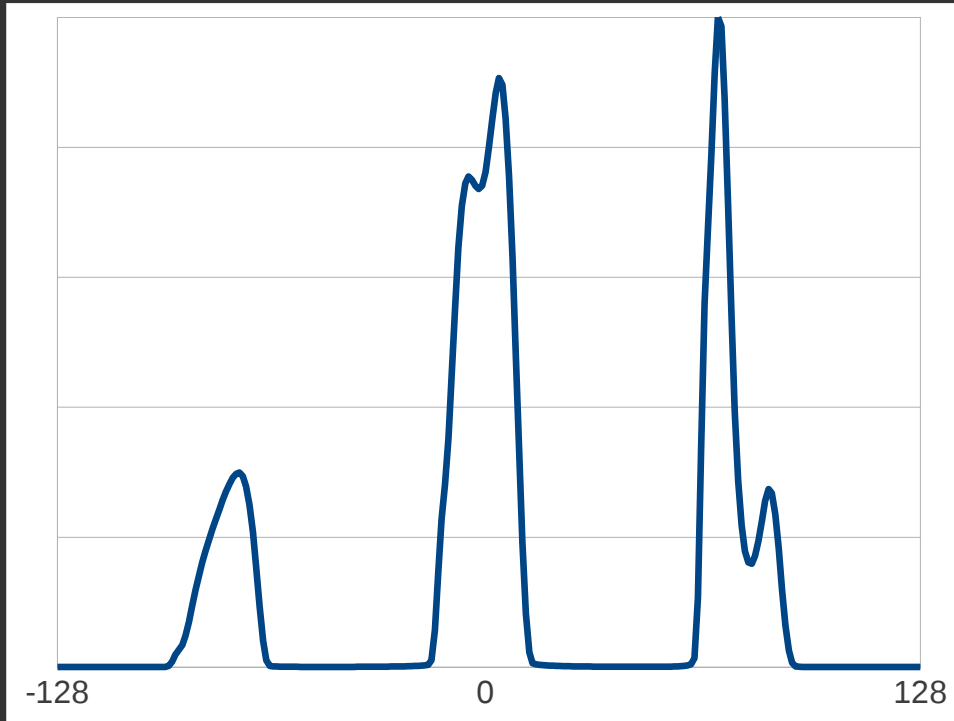
Interferometry

(39 phase encodes)

1-D Spectroscopic Imaging

Total Spectral Power

Incoherent (readout gradient)



← x →

← x →

Standard

Interferometry

(257 phase encodes)

(39 phase encodes)

$R = 6.6 \approx \sqrt{N} / 2.5$

2-D Interferometry

- Using a gradient in the x -direction, we would like to assemble

$$\Gamma(\Delta k_x, \Delta k_y, \tau)$$

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2-D Interferometry

- Using a gradient in the x -direction, we would like to assemble

$$\Gamma(\Delta k_x, \cancel{\Delta k_y}, \tau)$$

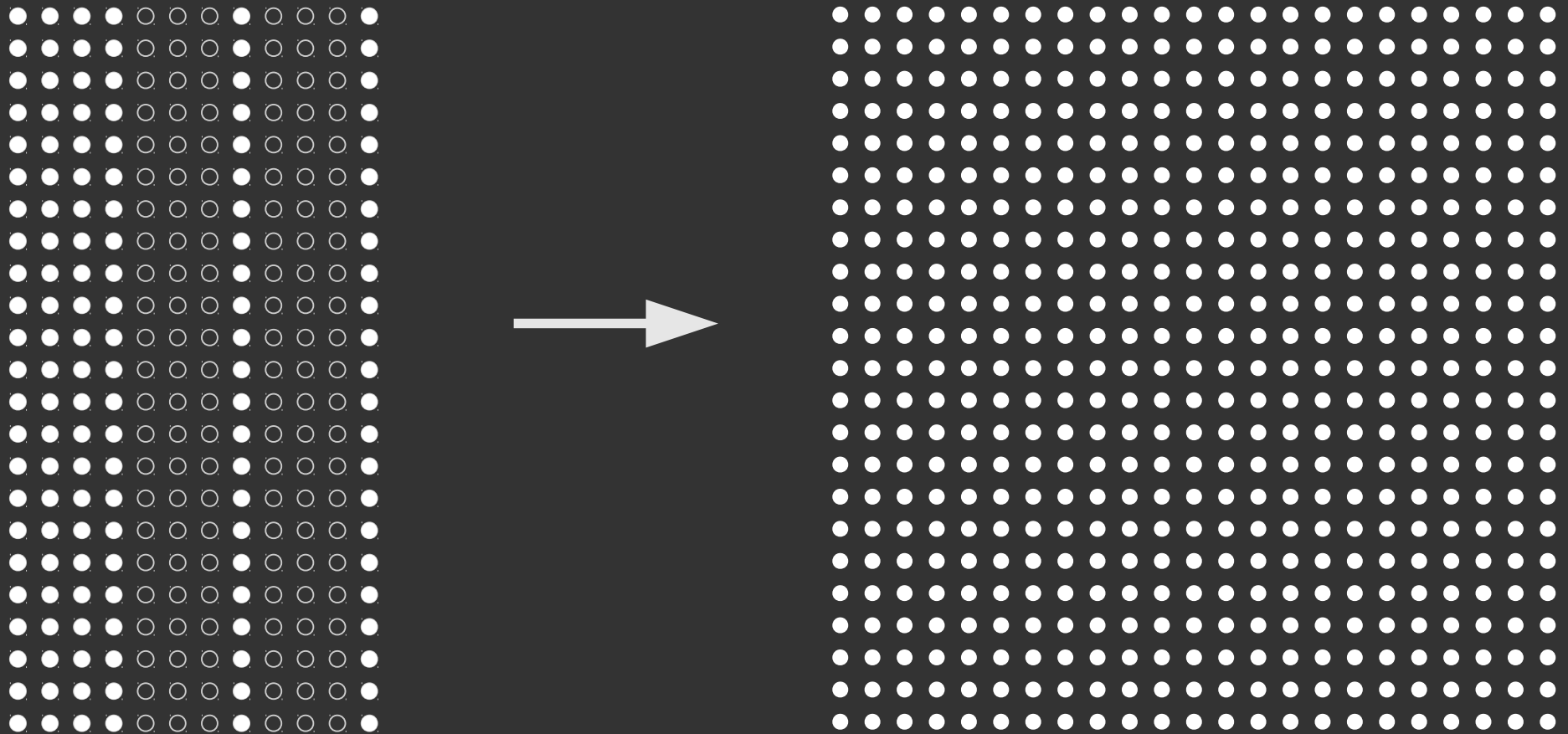
- Because of coherence in the y -direction
- The y -direction must be fully mapped

$$\Gamma(\Delta k_x, k_{y1}, k_{y2}, \tau) \underset{FT}{\Leftrightarrow} s(r_x, r_{y1}, f) s^*(r_x, r_{y2}, f)$$

- Results in a separable, but non-linear system

2-D MRSI

- The y -direction must be fully sampled, but the x -direction may still benefit

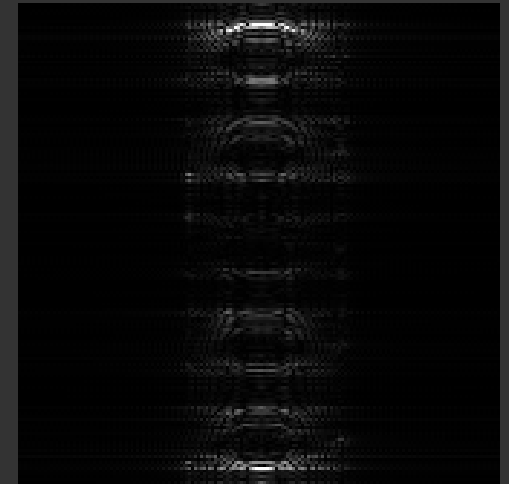


2-D Simulated MRSI



Typical

Coherent

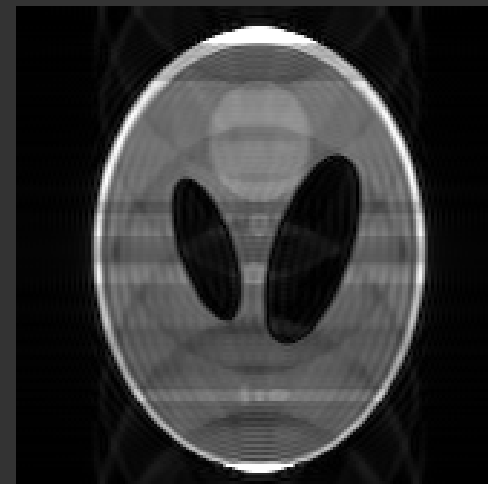


$R = 6.7$

2-D Simulated MRSI



Typical

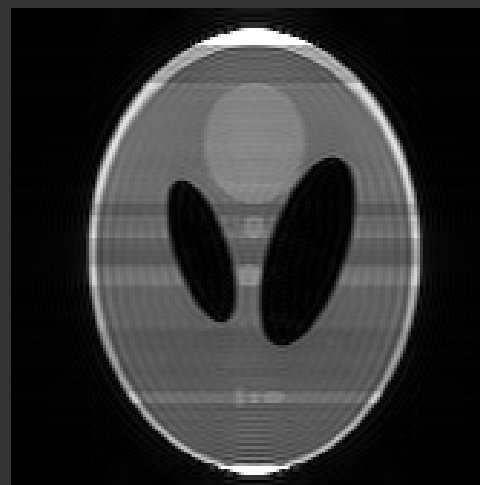


$R = 6.7$

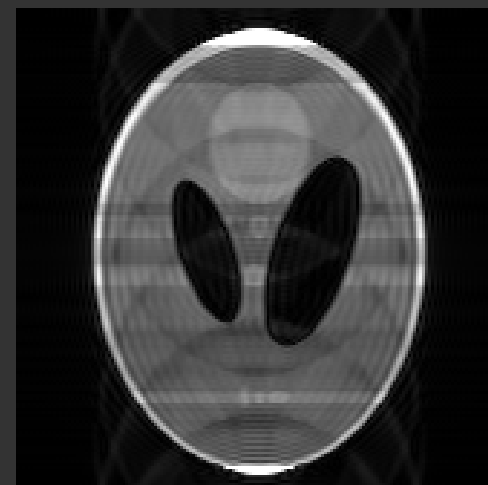
2-D Simulated MRSI



Typical



$R = 4.9$



$R = 6.7$

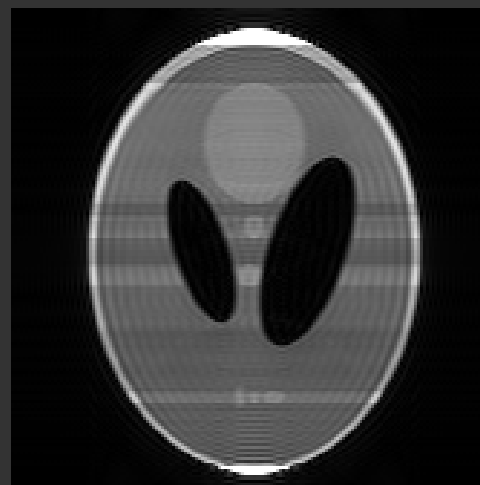
2-D Simulated MRSI



Typical



$R = 2$



$R = 4.9$



$R = 6.7$

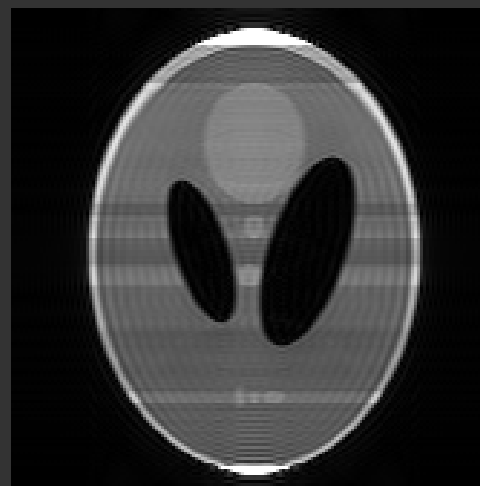
2-D Simulated MRSI



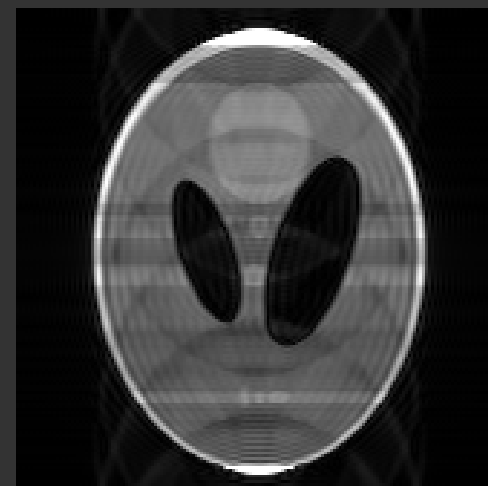
Typical



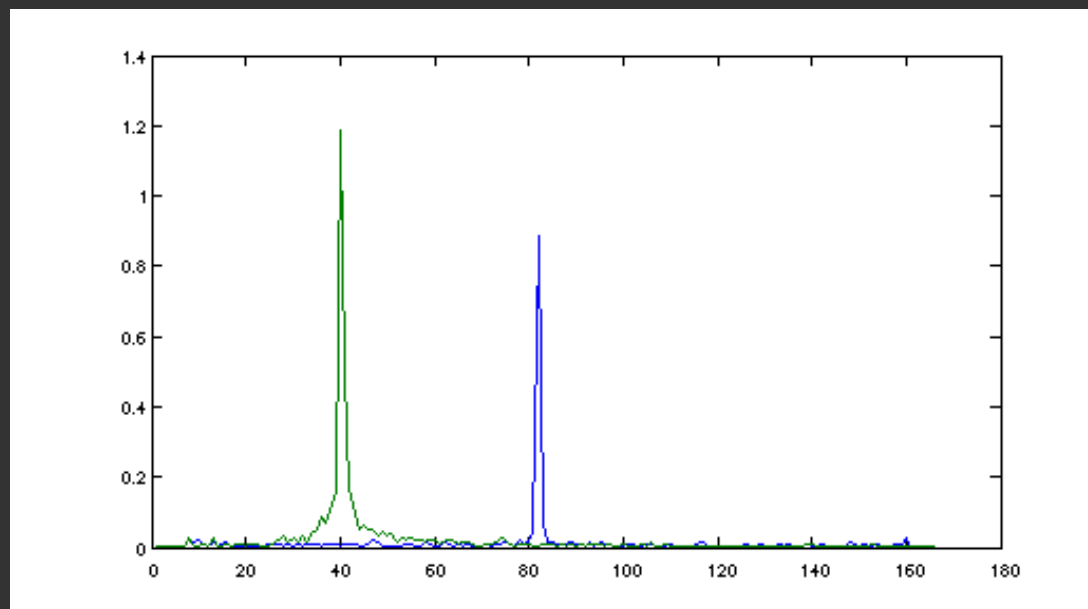
$R = 2$



$R = 4.9$



$R = 6.7$



Conclusions

- Applied interferometry to MR
- Direct application to spectroscopic MR imaging
- 1-D MRSI improved by a factor of $\approx \sqrt{N}/2.5$
- Benefits are larger with more data
- Drive new acquisition methods for MR imaging

Acknowledgements

- Craig Meyer
- NIH R01HL079110
- NIH 5T32HL007284-33