

# CHARACTERIZATION FOR LOW DOSE PHOTON COUNTING CONE-BEAM CT

Hamid Ouamara

Director of thesis: Christian Morel

Group: *imXgam*

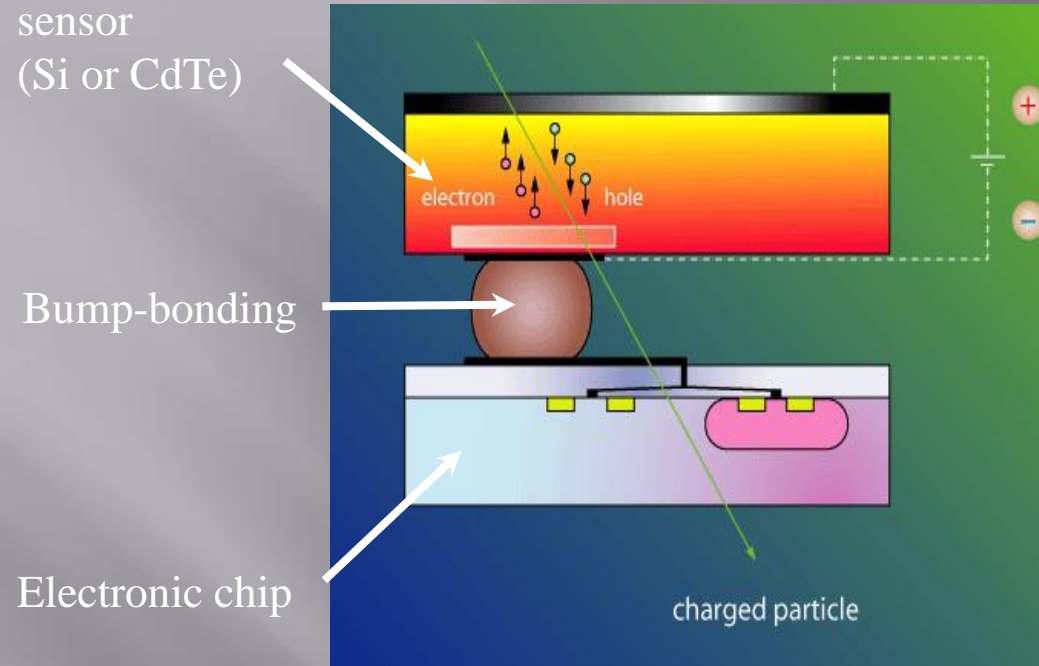


# Outline

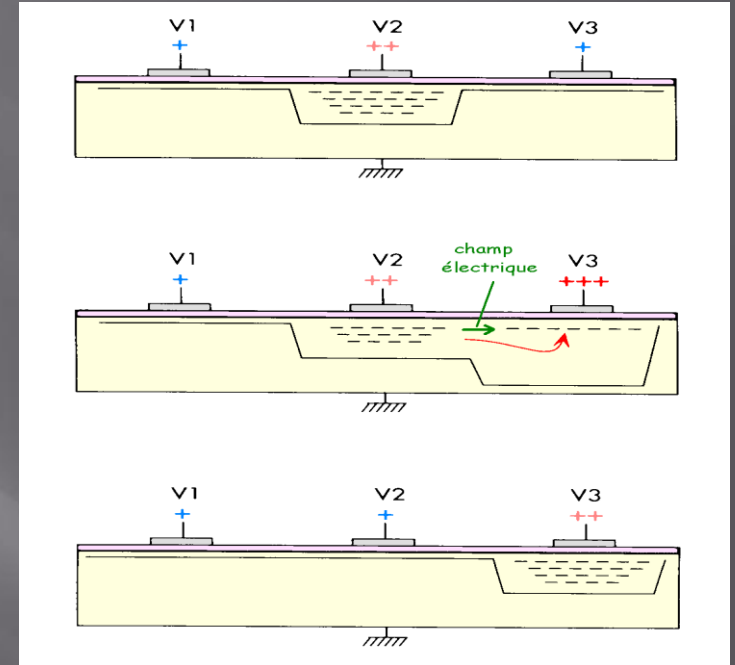
- 1- The hybrid pixel XPAD3 camera
- 2- PIXSCAN Project
- 3- Thesis context
- 4- Characterization of X-ray source
- 5- Reconstruction Algorithms
- 6- Criteria of image quality
- 7- Conclusion

# 1-The XPAD3 new hybrid pixel camera

hybrid pixel



CCD camera



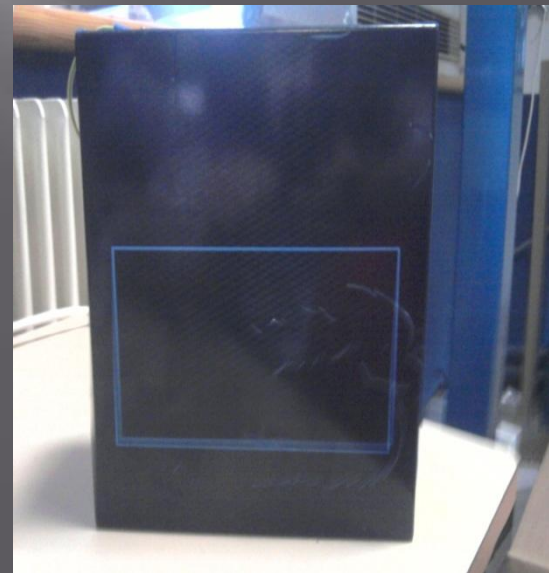
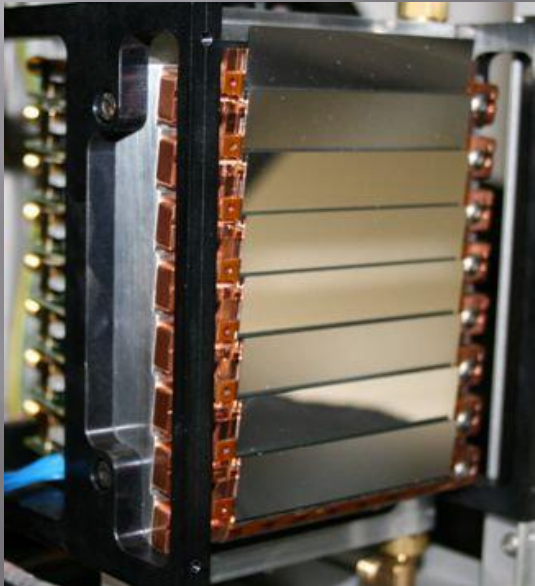
**Fundamental difference with other detectors :**  
**photon counting ! Not charge integration !**

**Existence of an energy threshold that enables counting.**

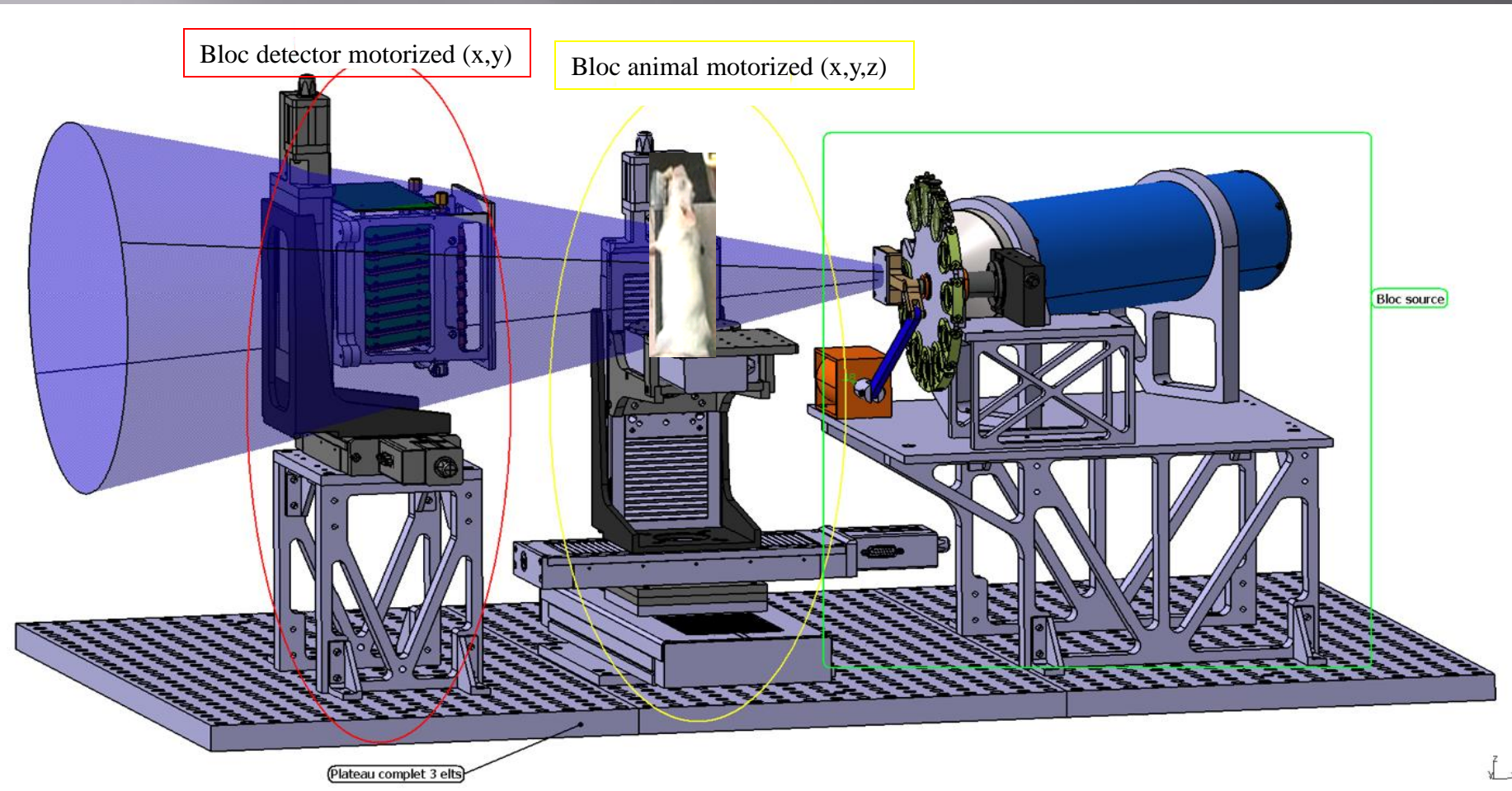
No dark noise.  Pure poisson noise only.

# 1-The XPAD3 new hybrid pixel camera

XPAD 3 hybrid pixel camera	CCD Camera
Photon counting mode	Charge integration mode
500 $\mu\text{m}$ silicon sensor thickness	Gadox
560 x 960 pixels	4160 x 2080 (x1, x2, x4)
130 x 130 $\mu\text{m}^2$ pixel size	Effective pixel size 36 $\mu\text{m}$
78 x 75 $\text{mm}^2$ detector	201 x 190 $\text{mm}^2$
Fast readout and data transfer up to 1000 frames/s (optical link and PCIeExpress)	Max. Line/Frame Rate Up to 10fps binning dependent



# 2-PIXSCAN Project



OXFORD Intruments X-ray tube

Target Voltage 10to 90kv, Target Current 1to 2 mA

W target, 13 to40  $\mu\text{m}$  focal spot size, 80 W, 33degrees Cone Angle

Complete system : 3 blocks

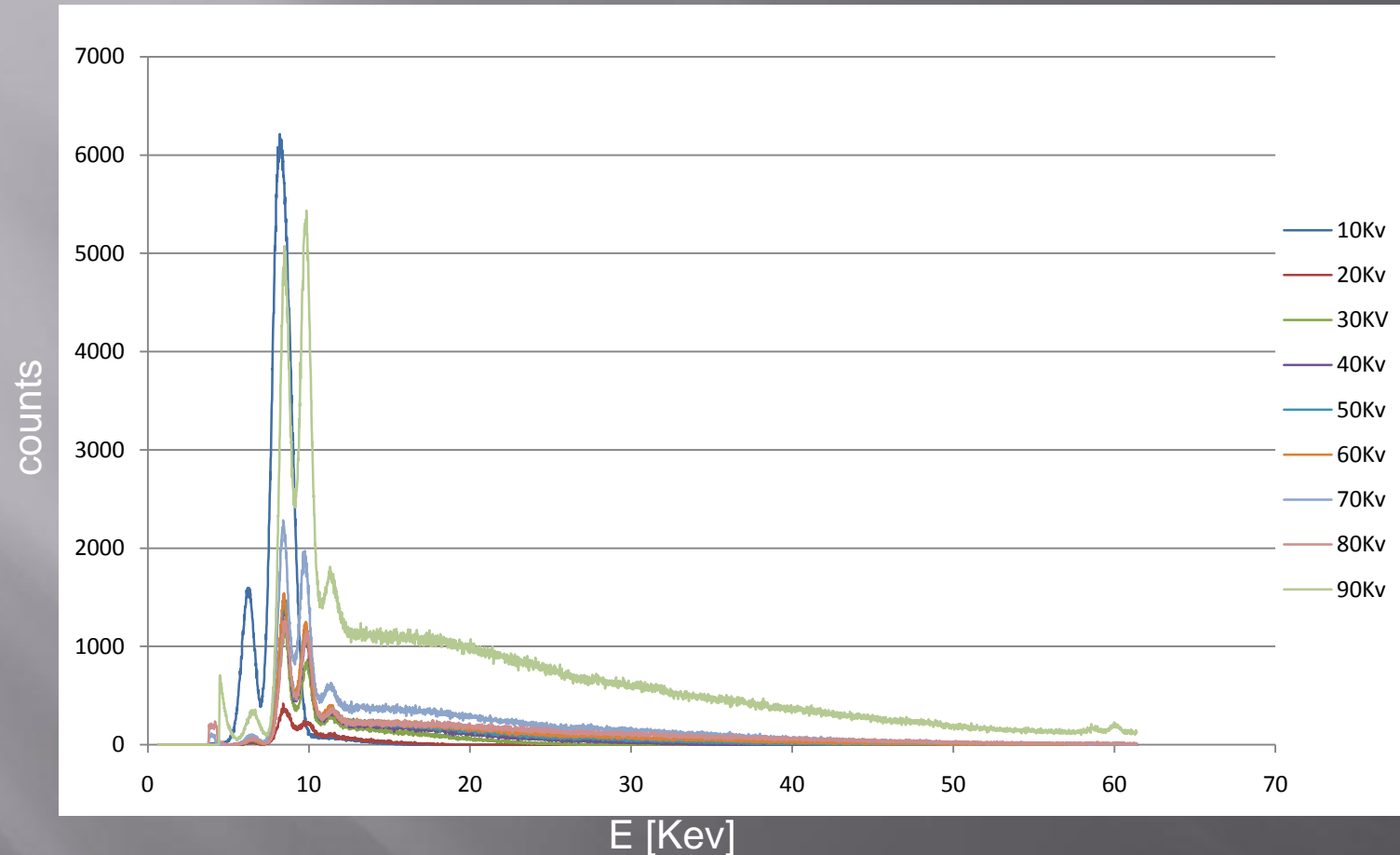


### 3-Thesis context

- ▣ Comparison of tomographic images reconstructed with the two cameras
- ▣ Asking the right questions
- ▣ Using the same techniques of reconstruction?
- ▣ Put them in the same conditions to the acquisition?
- ▣ Volume quality?

# 4- Characterization of X-ray source

Energy spectrum of the X-ray source OXFORD Instruments

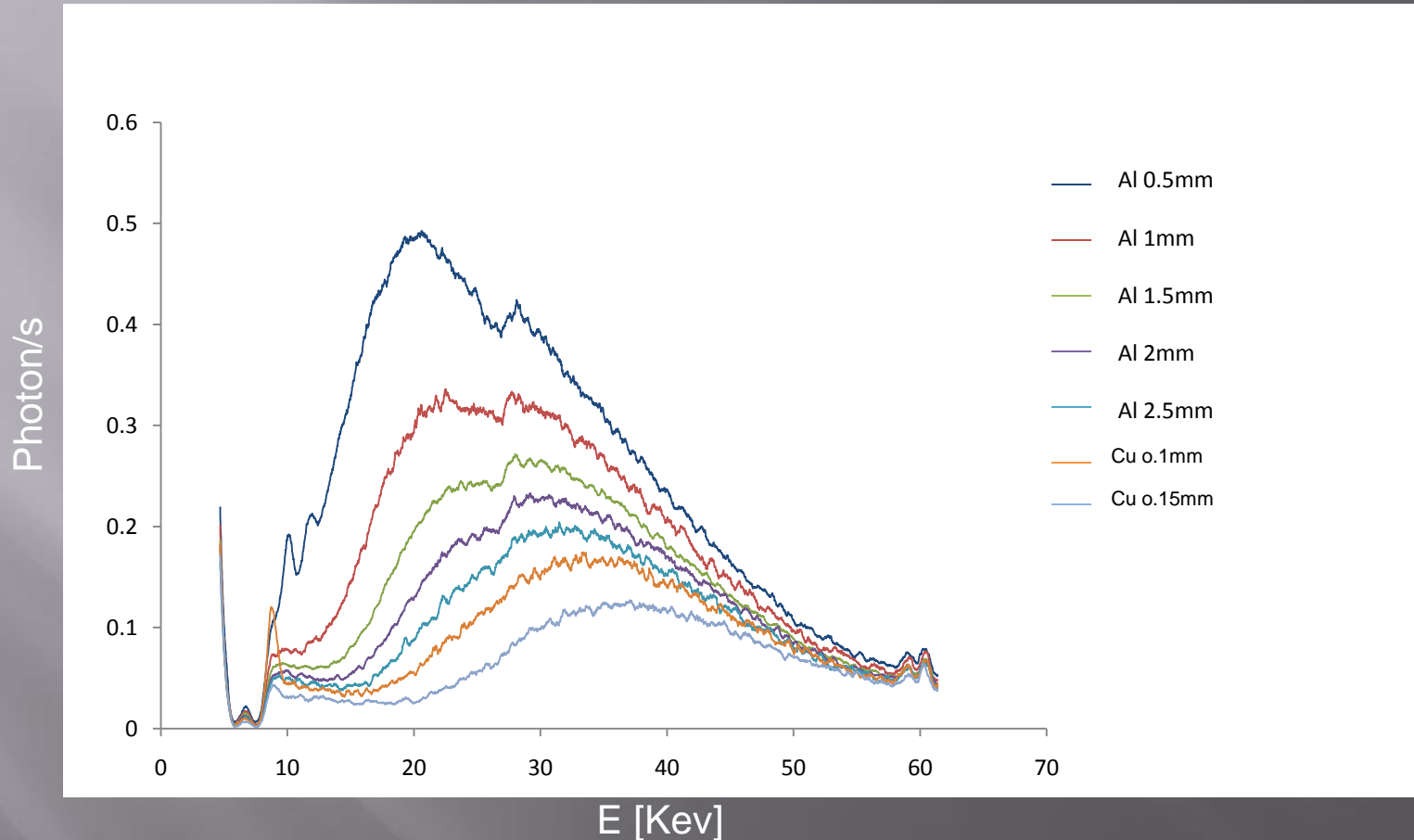


- CdTe-100T  $\gamma$ /x-ray detector ( $3\times 3\times 3\text{mm}^3$ )
- Power supply & amplifier
- Collimator kit: Collimator housing , 7 Tungsten collimator discs ( $25\mu\text{m} - 2\text{mm}$  hole)

- Laser
- Mounting system
- Acquisition software: Spectrum Techniques UCS30
- 10min acquisition

# 4- Characterization of X-ray source

Measurements of spectra with different filters



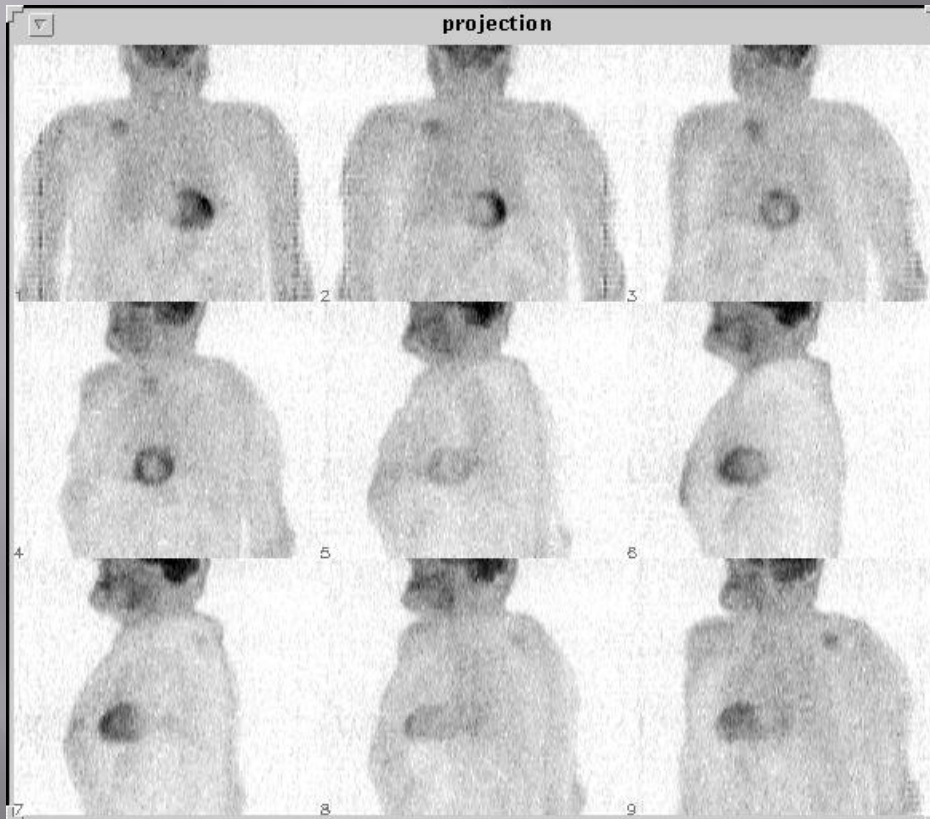
- Measurements performed with Al thicknesses of 0.5mm to 2.5mm (90Kv)
- Hardening of the spectrum to high energies



# 5- Reconstruction algorithms

## X ray Computed Tomography

Sinogramme




Same object seen under many different angles provides different projections.

By combining information from all the projections, we can get the 3D object.

X photons interact with matter.

# 5- Algorithms

## a) FDK

- ▣ Feldkamp, Davis, Kress (FDK)
- ▣ Analytical method
- ▣ Filtering projections (1D)  back-projection of filtered projections

## b) SART and ML-EM

- ▣ - Algebraic and iterative methods

$$\text{Model : } \mathbf{A}\mathbf{f} = \mathbf{p}$$

with  $\mathbf{p}$  projections,  $\mathbf{f}$  volumic function to estimate, and  $\mathbf{A}$  system matrix.

The solution is provided by the pseudo inverse matrix of  $\mathbf{A}$ .

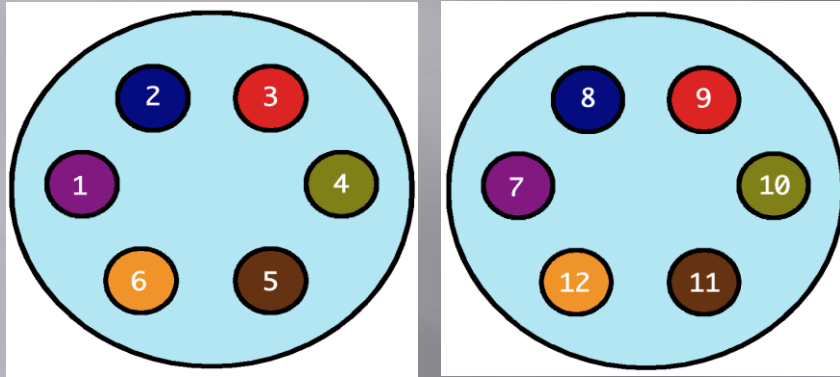
- ▣ - Simultaneous Algebraic Reconstruction Tomography (SART, extension of ART algorithm) algorithm.
- ▣ - Maximum Likelihood Expectation-Maximization (MLEM) algorithm.

## 5- 2 Simulation

- Tests have been performed on a simulated phantom with the software GATE.

First plane of balls

Second plane of balls



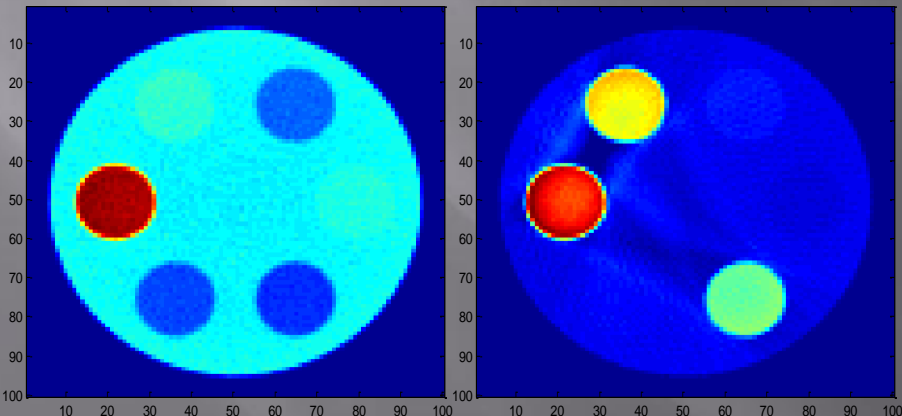
- Simulations have been performed with :
- Acquired projections of size 100 x 100 pixels, 360 projections.
  - A reconstructed volume of 100 x 100 x 100 pixels.
  - Activity (Photons/pixels) ranging from 100 to 25600.

Two horizontal planes of the cylindrical simulated phantom, with different density balls.

First plane of balls

Second plane of balls

Slice 25 (25600 photons/pixel) FDK method



1: IomeronInj, 2: Polystyrène, 3: LungMoby,  
4: Brain, 5: Adipose; 6: Blood.

7: RibBone, 8: Liver, 9: SpineBone, 10: Carbon  
11: Cartilage, 12: Skull,

FDK method 25600 photons /pixel

## 6-Criteria of image quality

For all calculations: Image to 25,600 photons / pixel is considered as reference image.

### a) PSNR (Peak Signal to Noise Ratio)

$$\text{PSNR} = 20 \log_{10} \left( \frac{\max(I_{\text{ref}})}{\text{MSE}(I_{\text{ref}} - I_{\text{rec}})} \right)$$

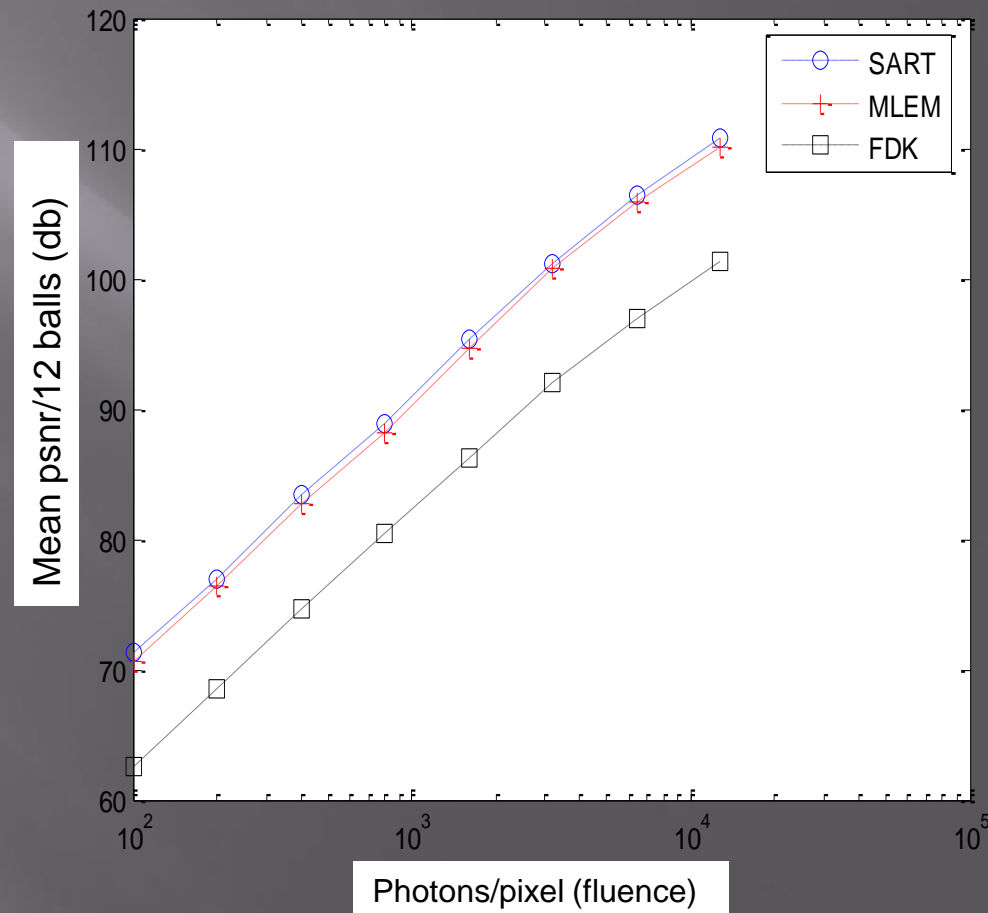
-Superiority of iterative methods according to PSNR criteria.

-Linear increasing of PSNR as a function of dose.

-Significant criterion, but not enough

-Only averaged the image

-This measure does not reflect the human perception



## 6-Criteria of image quality

### b)SS\_SSIM (Single Scale Sturctural Similarity )

- The general form of the Structural Similarity (SSIM) index between signal  $I_{ref}$  and  $I_{rec}$  is defined as:

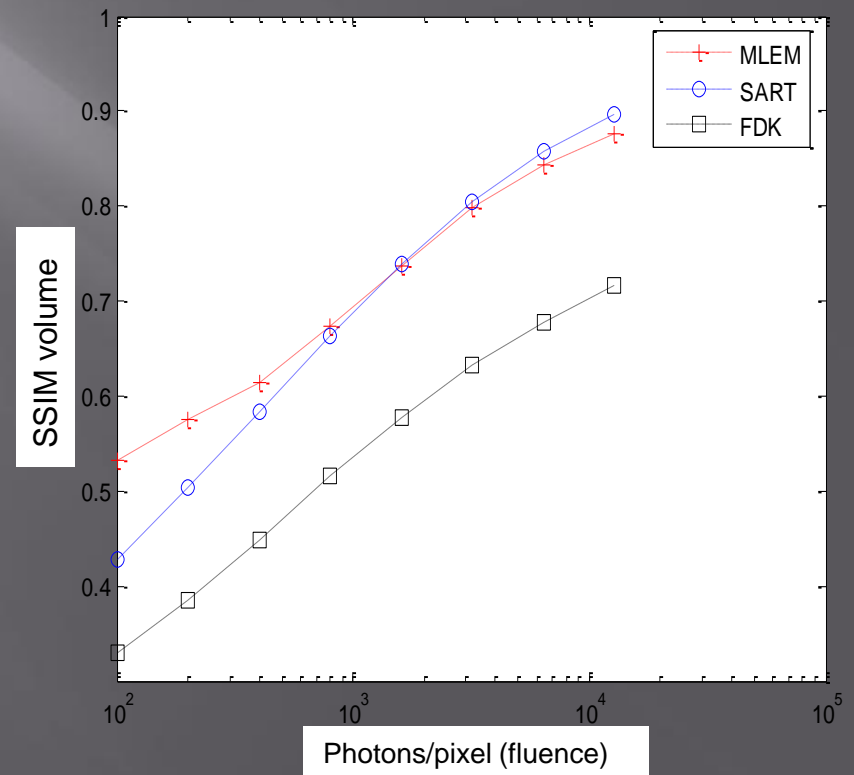
$$SSIM(I_{ref}, I_{rec}) = \frac{(2\mu_{I_{ref}}\mu_{I_{rec}} + C_1)(2\sigma(I_{ref} - I_{rec}) + C_2)}{(\mu_{I_{ref}}^2 + \mu_{I_{rec}}^2 + C_1)(\sigma_{I_{ref}}^2 + \sigma_{I_{rec}}^2 + C_2)}$$

Apply the SSIM indexing algorithm for image quality assessment using a sliding window approach.

-Results almost identical with SART and MLEM.

-MLEM and SART better than FDK

-Linear increasing of SS\_SSIM as a function of dose



## 7-Conclusion

- Iterative methods have shown their superiority on Fourier-based method.
- The quality of reconstructed images depends on the dose and on the density of the tissue concerned.
- The quality of reconstructed images linearly depends on the dose.
- Finding the right filters to perform specific experiments.
- Apply techniques to real data.
- Install the CCD camera in the PIXSCAN
- Study of the CCD camera



Thank you for your attention