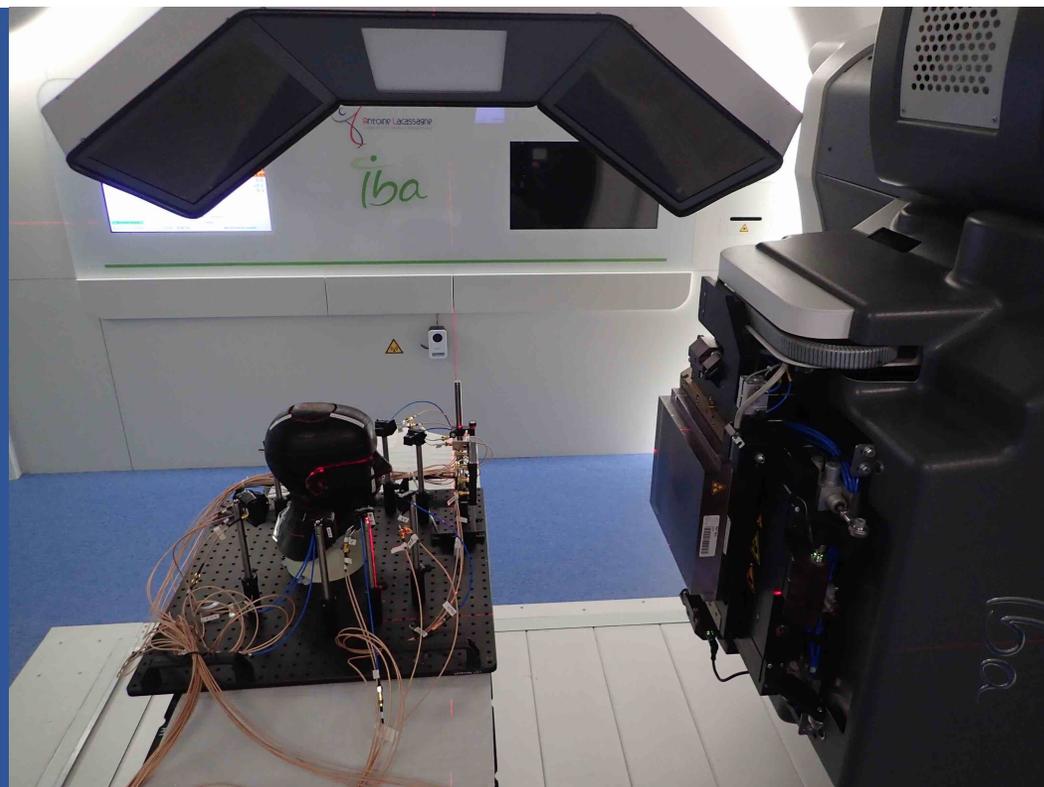


Prompt Gamma Timing and Time Imaging with the TIARA detector



Sara Marcatili, on behalf of the TIARA collaboration

CNAO-IN2P3 Collaboration meeting

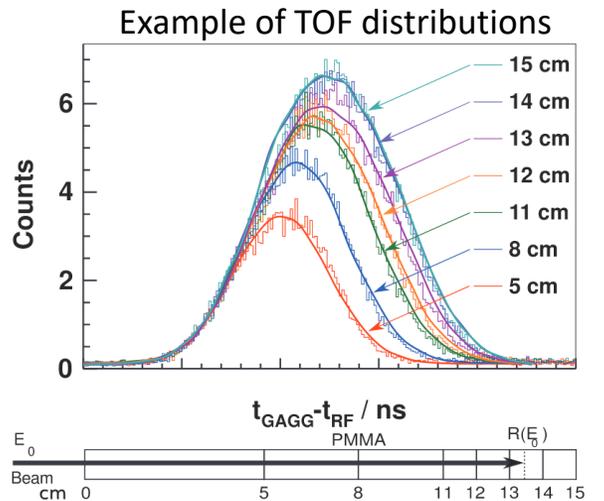
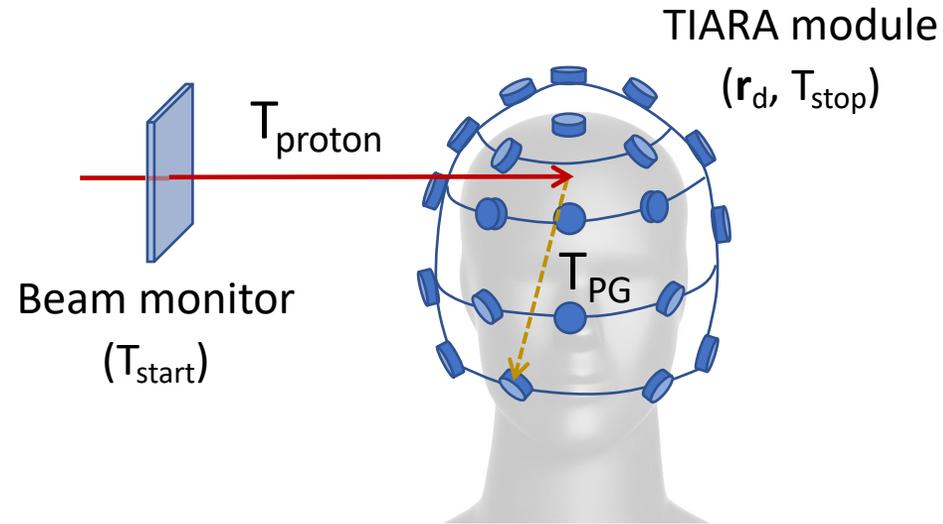
5 March 2026

CNAO, Pavia



Beyond Prompt Gamma Timing: detection principle

Prompt Gamma Timing



Golnik et al. Phys. Med. Biol. 59 (2014) 5300

$$TOF = t_{stop} - t_{start}$$
$$T_{proton}(\mathbf{r}_v, \mathbf{v}_p) + T_{PG}(\mathbf{r}_v, \mathbf{r}_d)$$

2 unknowns: \mathbf{r}_v = PG vertex \mathbf{v}_p = proton speed

The TIARA (Tof Imaging ARrAy) detector

Fast beam monitors

Plastic-based for
low intensity

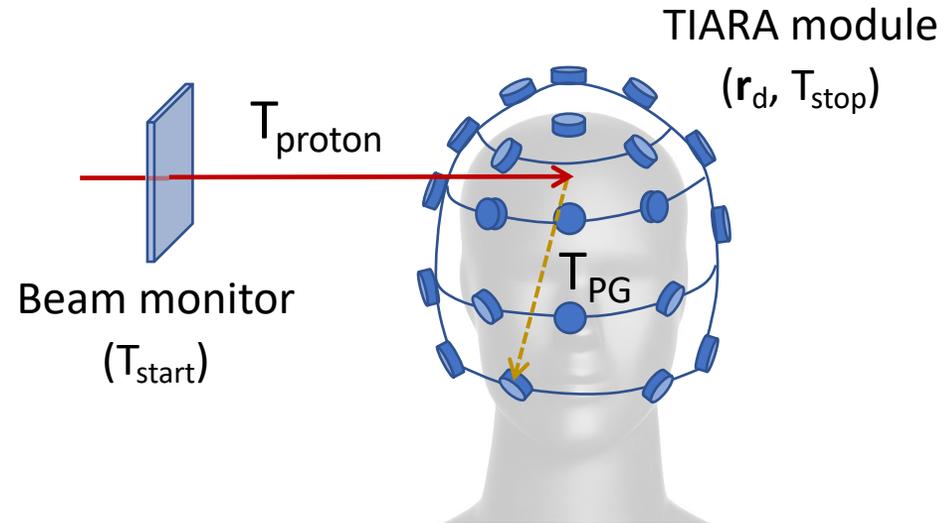


<https://arxiv.org/abs/2411.07877>

Diamond-based for
high intensity

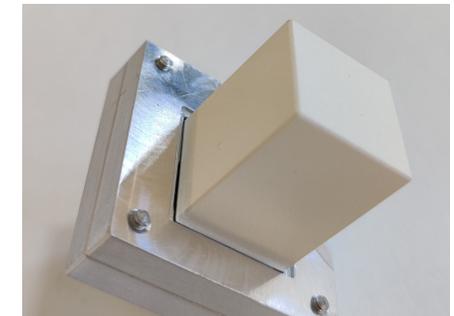


cf. Gallin-Martel's talk



Targeted coincidence time resolution (CTR):
~ **100 ps RMS** (235 ps FWHM)
for range uncertainty ~ mm

Cherenkov-based gamma detector



<http://arxiv.org/abs/2601.20457>

Adapted to all
intensities

Gamma module: understanding detector response

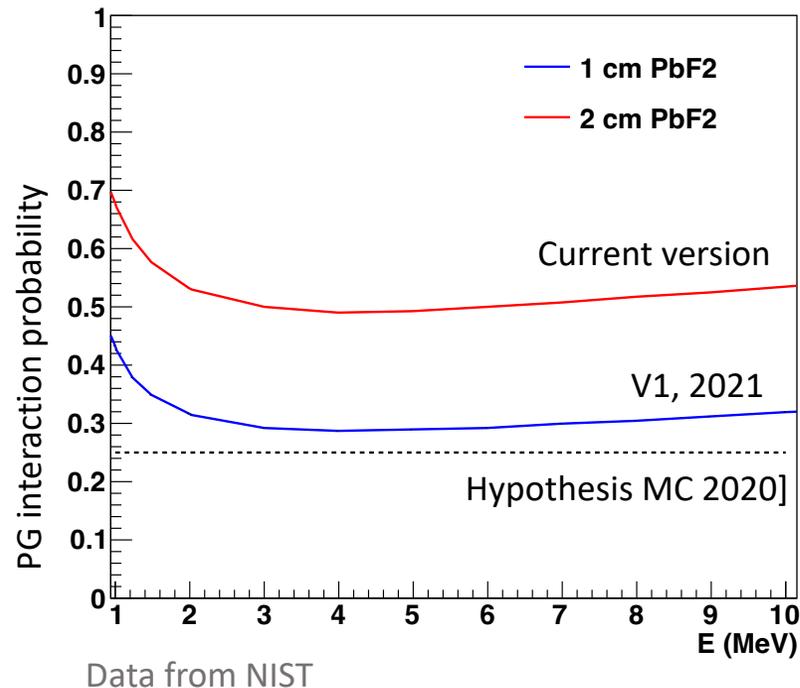
$$\epsilon = \epsilon_{geo} \times \epsilon_{int} \times \epsilon_{opt}$$

$$\epsilon \sim 0.45\%$$

Detector solid angle

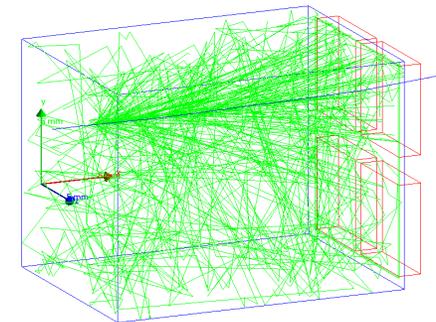
- nb. Of PG modules
- distance from beam axis

PG interaction probability



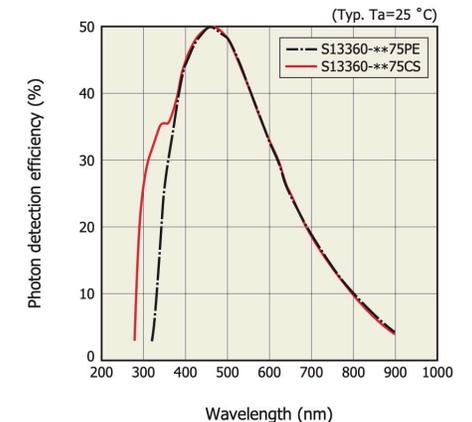
Probability that a particle interacting in the crystal is actually detected by the SiPM.

Nb of optical photons reaching the SiPM



G4 simulation

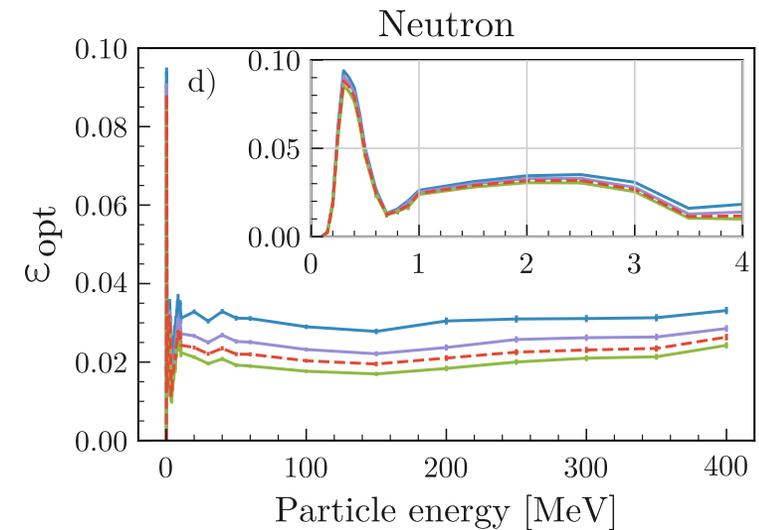
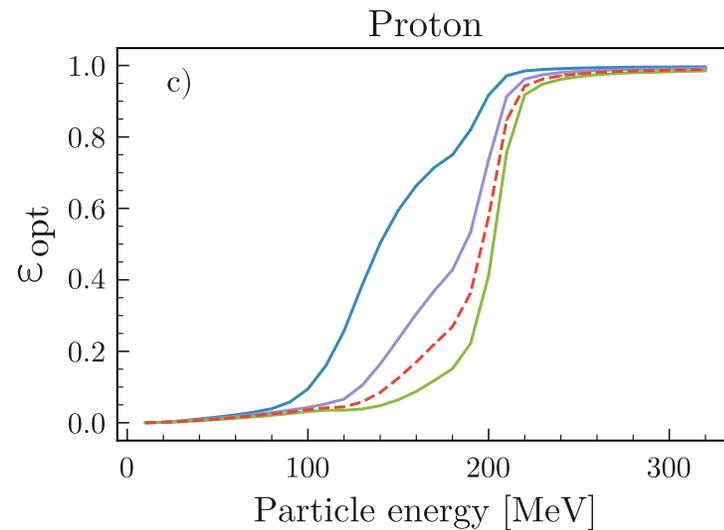
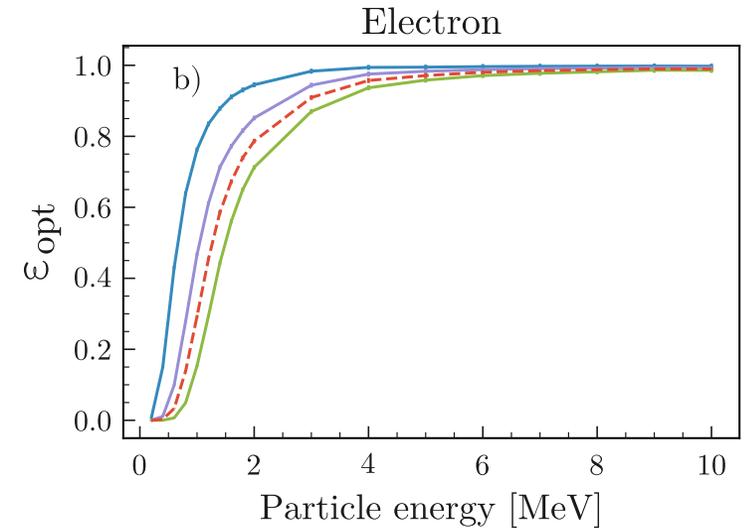
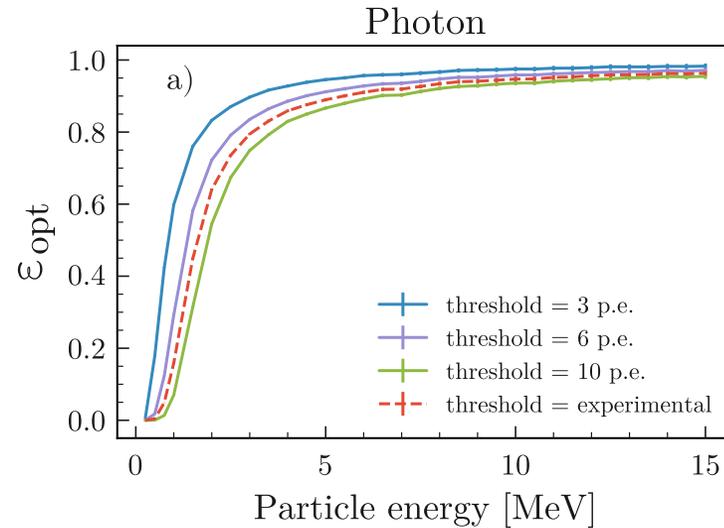
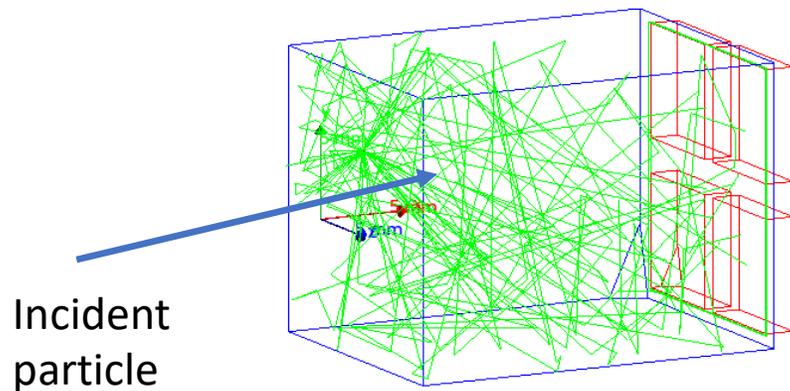
SiPM PDE



Post-analysis

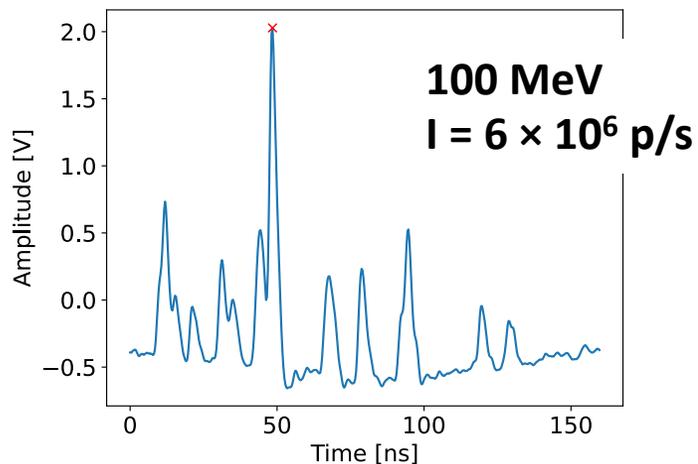
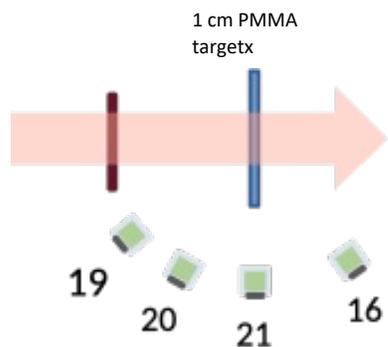
Gamma module optical response: particle sensitivity

The optical detection efficiency is determined as a function of particle incident energy

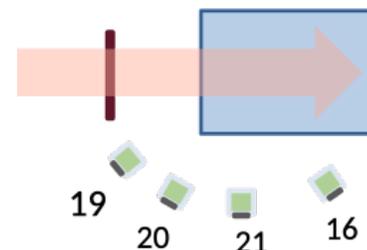


Time resolution

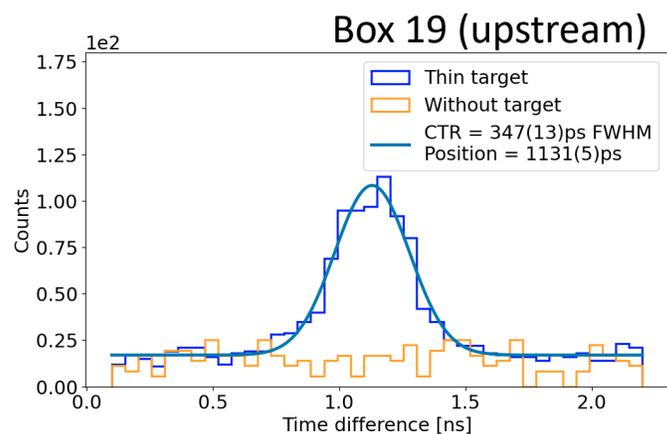
Signal from monitor not bunched at the gamma detector time-scale



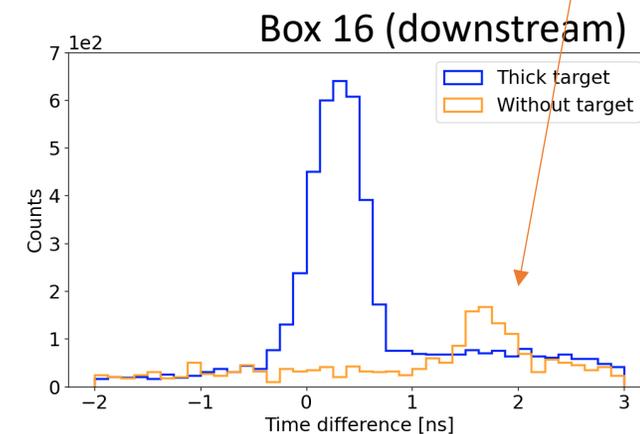
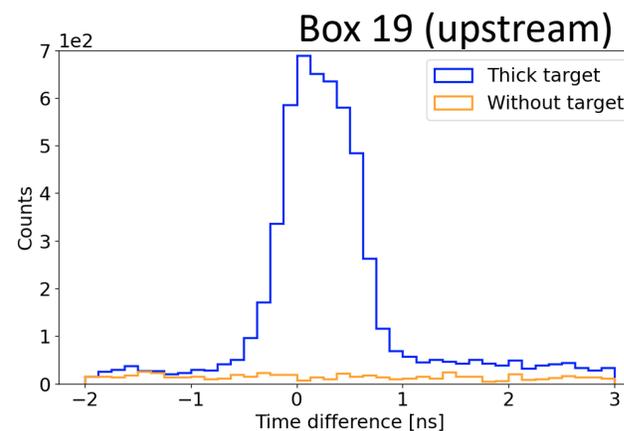
Signal-to-Noise Ratio



- Negligible background with target/patient in place
- Very high SNR both downstream and upstream



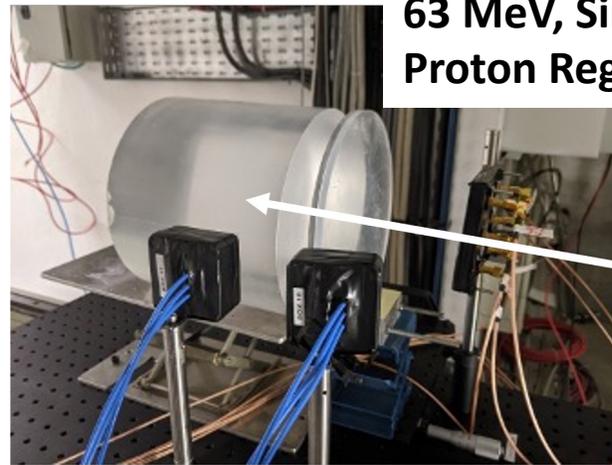
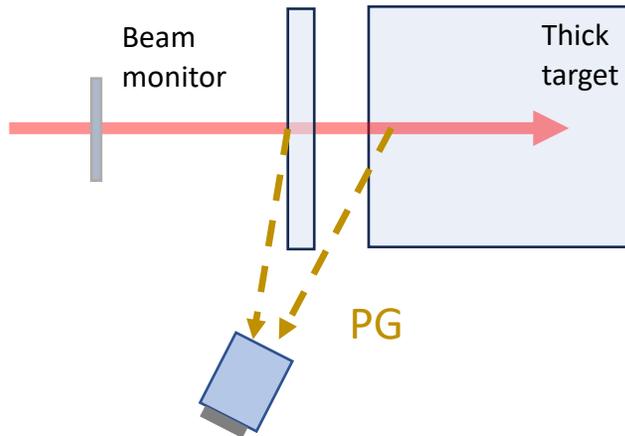
Time resolution slightly degraded (148 ps rms) as this is not Single Proton Regime.



Protons from monitor stopped in the target

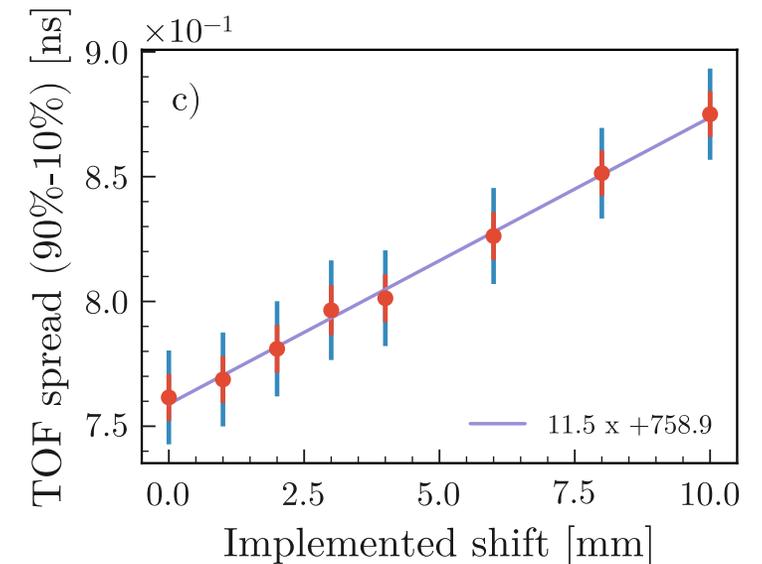
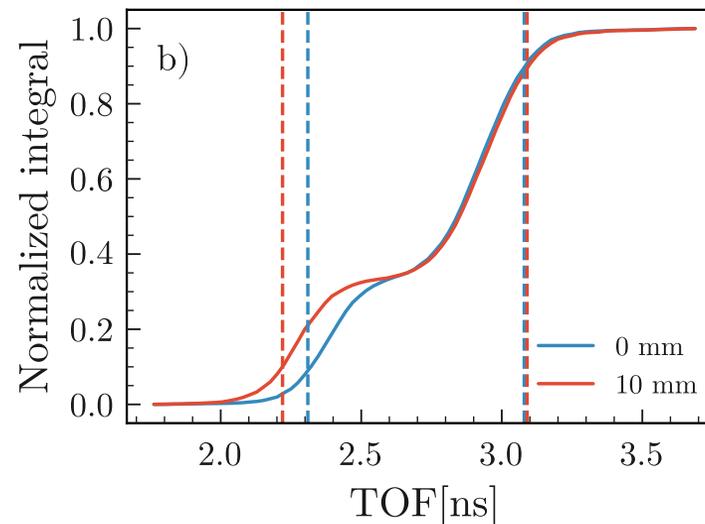
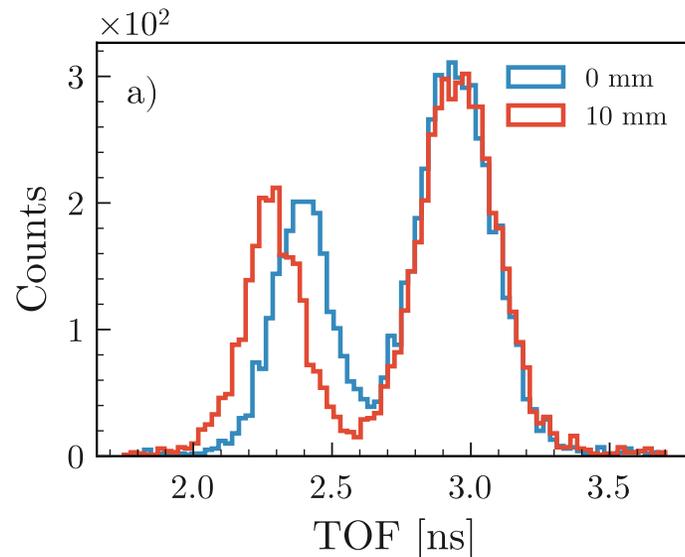
Range accuracy with protons (MEDICYC Cyclotron)

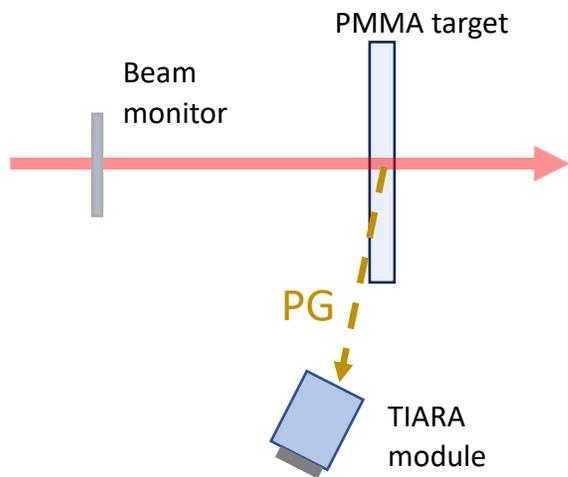
Variable thickness air gap to simulate a range shift



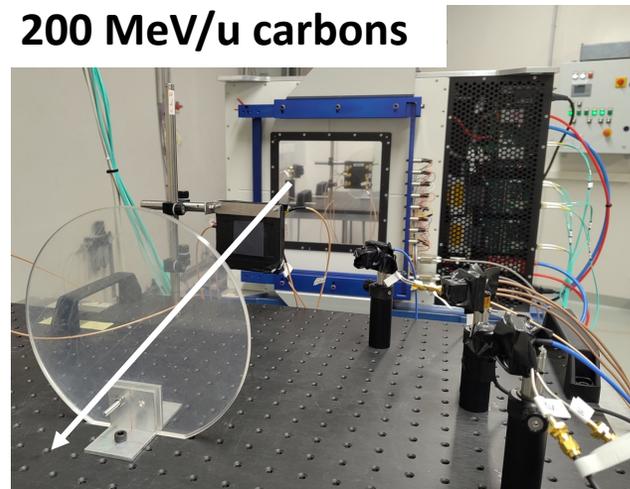
63 MeV, Single Proton Regime

Nb. Of spots	1	2
Nb. of incident protons	1×10^7	2×10^7
Range accuracy at 2σ (mm)	3.3 ± 0.1	2.3 ± 0.1

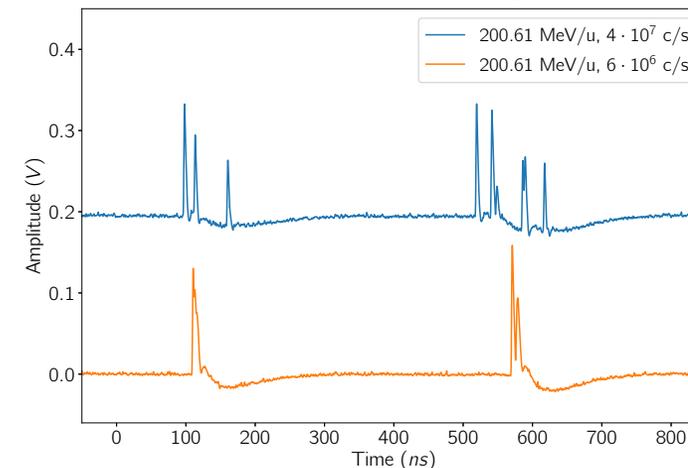




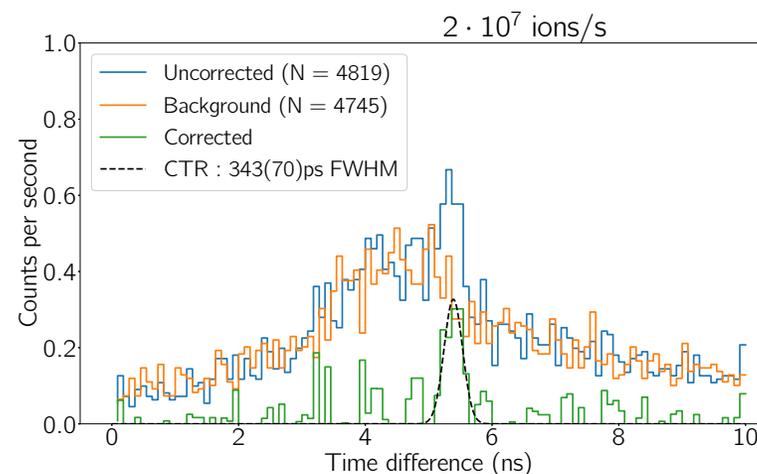
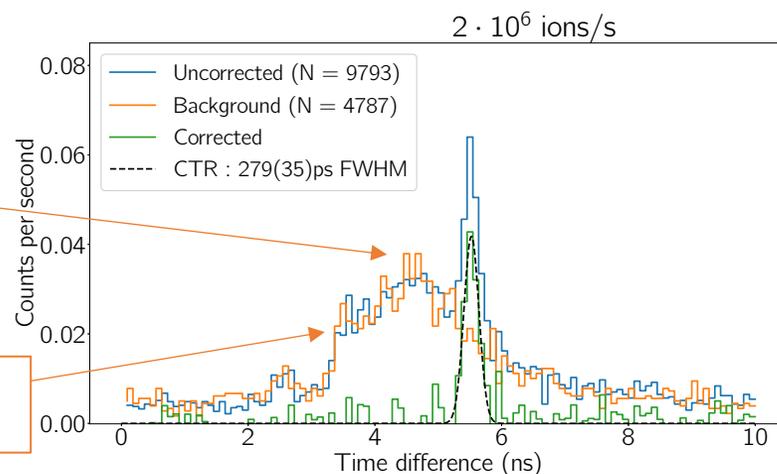
200 MeV/u carbons



Beam monitor response

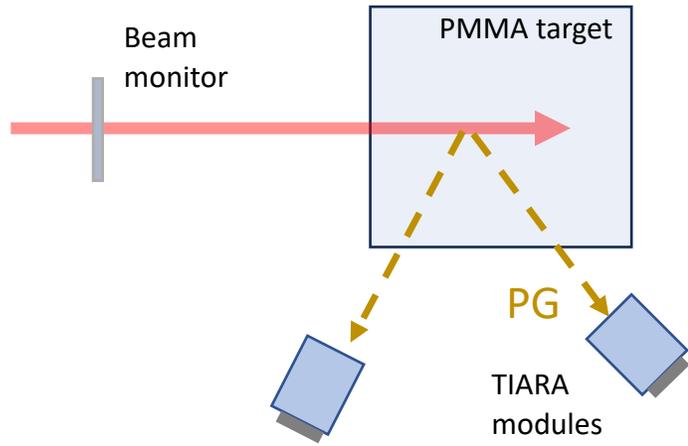


Coincidence Time Resolution

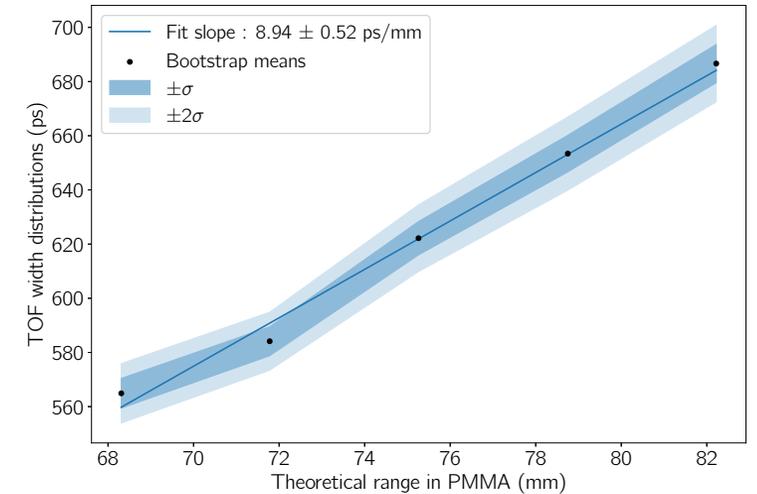
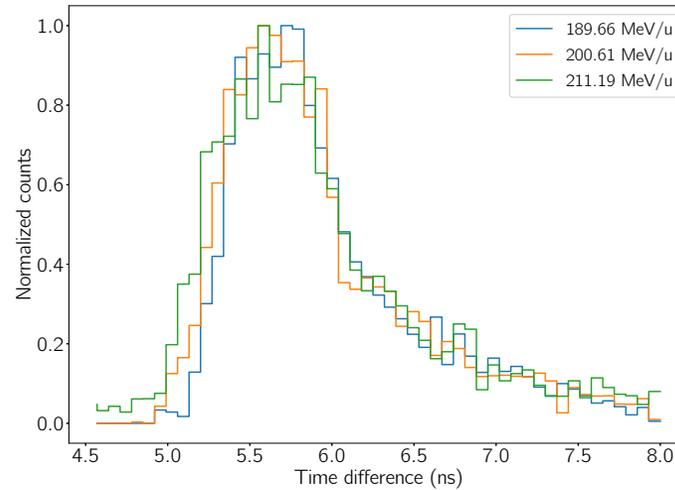


Coincidence Time Resolution

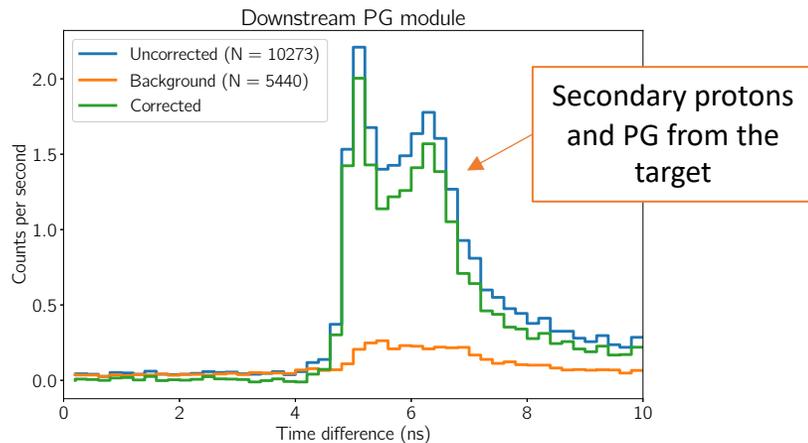
- better than proton's (347 ps FWHM)
- only slightly degraded at clinical intensity



From 189 to 211 MeV/u to induce progressive range shifts of 3.5 mm in PMMA



Downstream detection not feasible



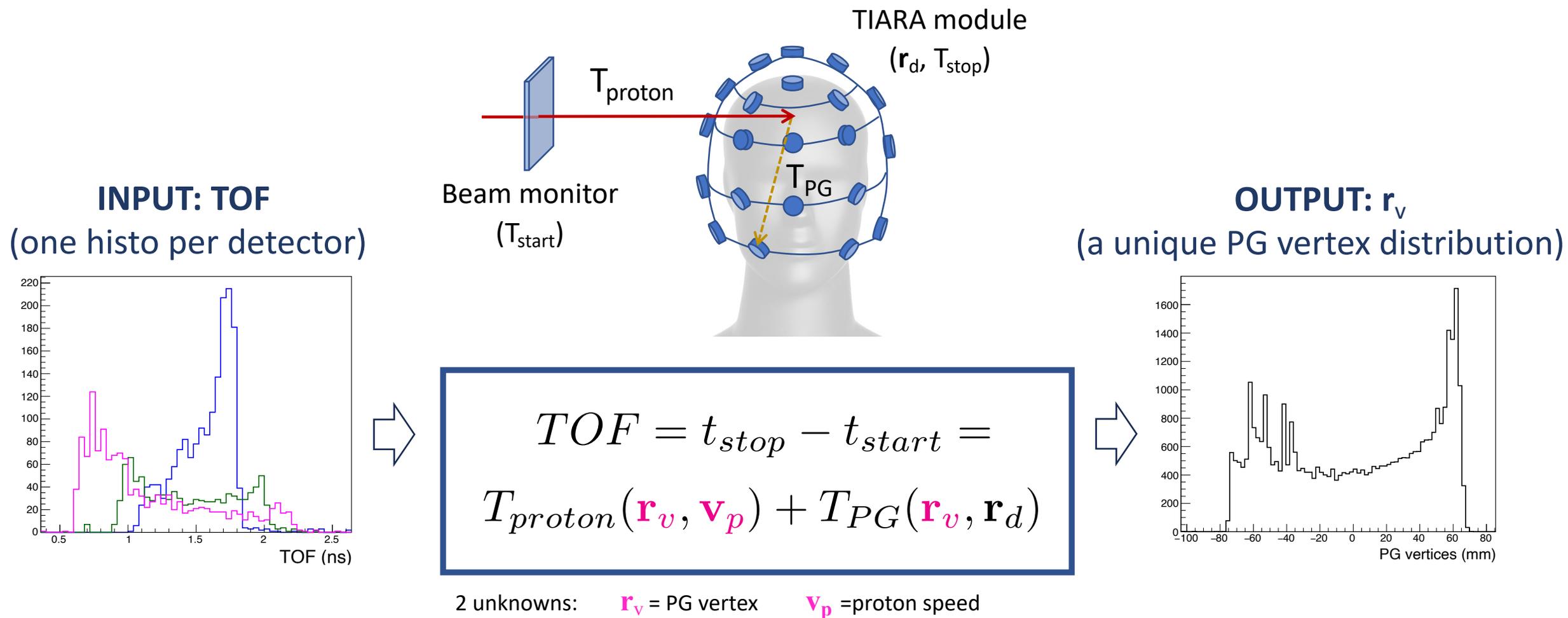
2σ range accuracy extrapolated to full TIARA detector

Clinical spots	Number of ions	N_{PG} (Counts)	$R_{acc,2\sigma}$ (mm)	
			$2 \cdot 10^6$ ions/s	$2 \cdot 10^7$ ions/s
1	$2.4 \cdot 10^6$	1400	5.42 ± 0.32	9.30 ± 0.70
2	$4.8 \cdot 10^6$	2800	3.76 ± 0.22	6.64 ± 0.50
4	$9.6 \cdot 10^6$	5600	2.68 ± 0.16	4.74 ± 0.36

<http://arxiv.org/abs/2602.18318>

Beyond Prompt Gamma Timing

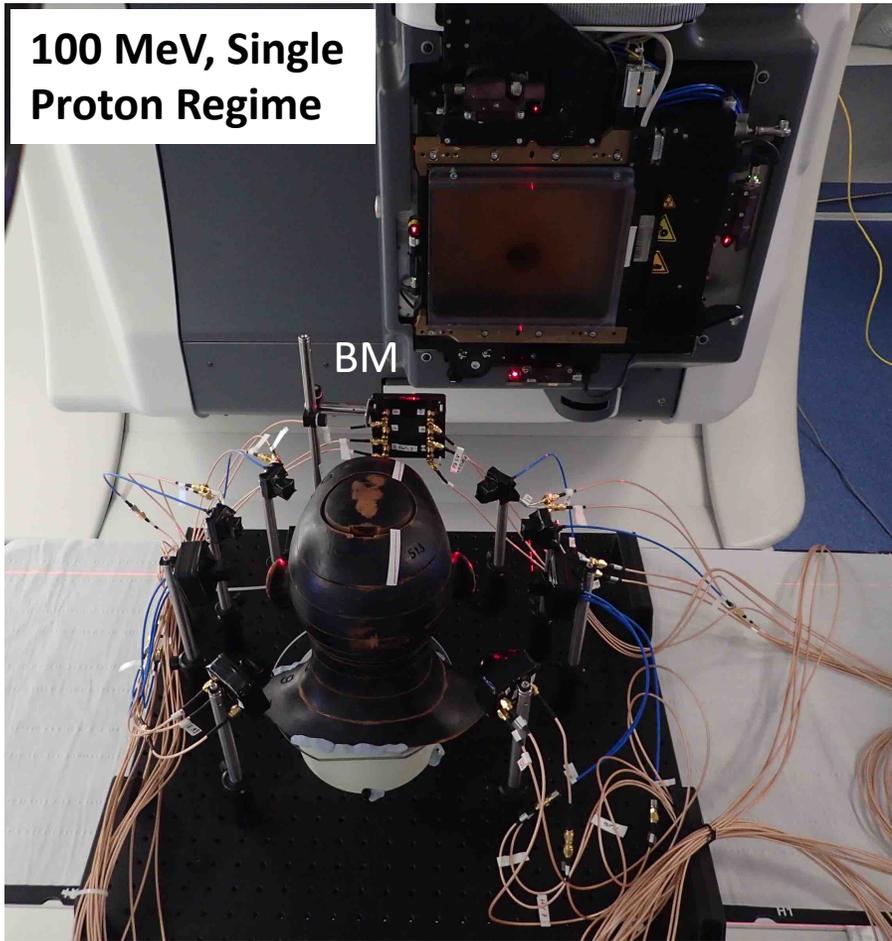
Prompt Gamma Time Imaging



$$TOF = t_{stop} - t_{start} = T_{proton}(\mathbf{r}_v, \mathbf{v}_p) + T_{PG}(\mathbf{r}_v, \mathbf{r}_d)$$

8 channels TIARA prototype

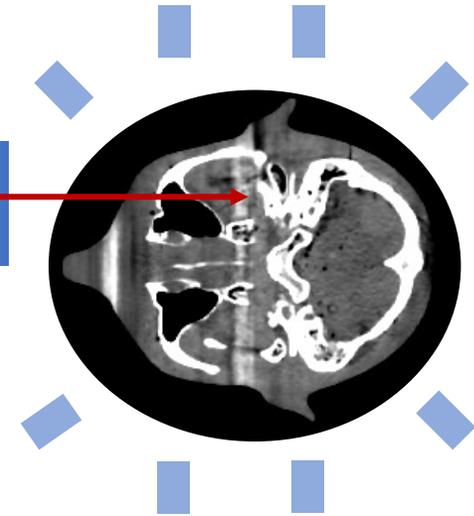
100 MeV, Single Proton Regime



Treatment planning

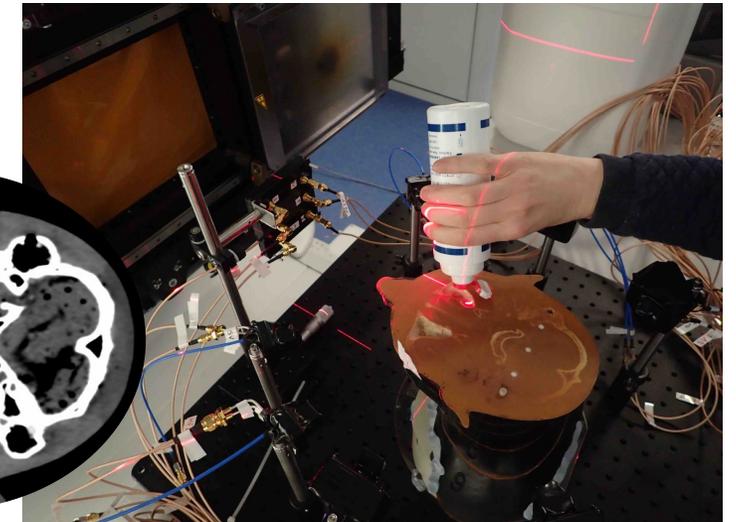
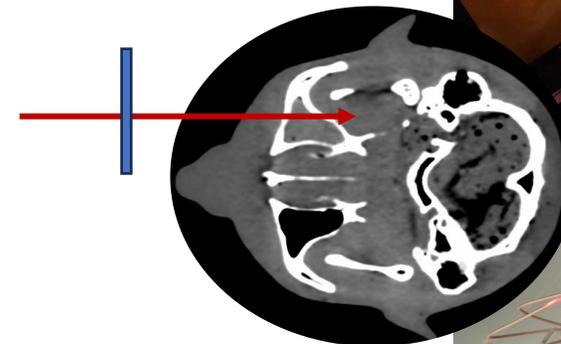
Irradiation of RANDO anthropomorphic phantom with **sinus empty**...

100 MeV protons



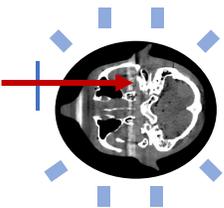
Treatment delivery

... and **sinus filled** with ultrasound gel.

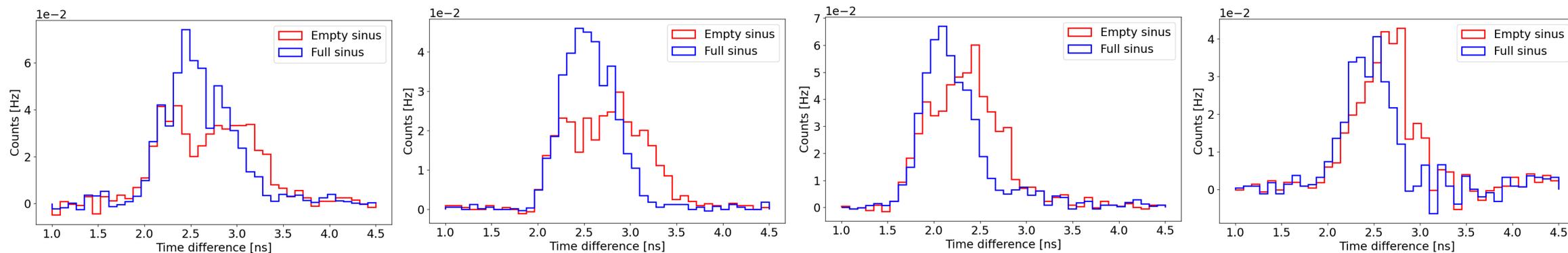


Determination of anatomical variation: TOF data

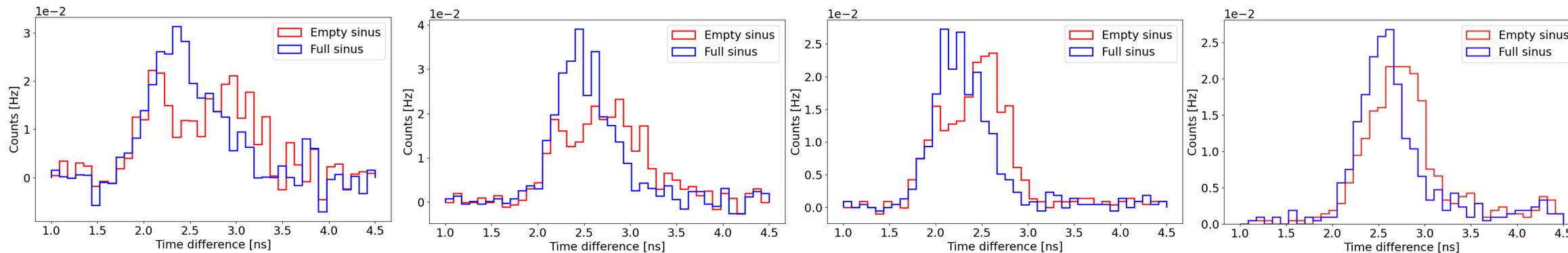
Between 500 and 1000 PGs per detector



All data after background subtraction: comparison sinus empty/filled



Beam direction 

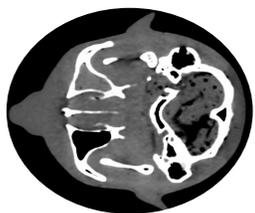


Determination of anatomical variation: reconstructed data

Possible clinical application



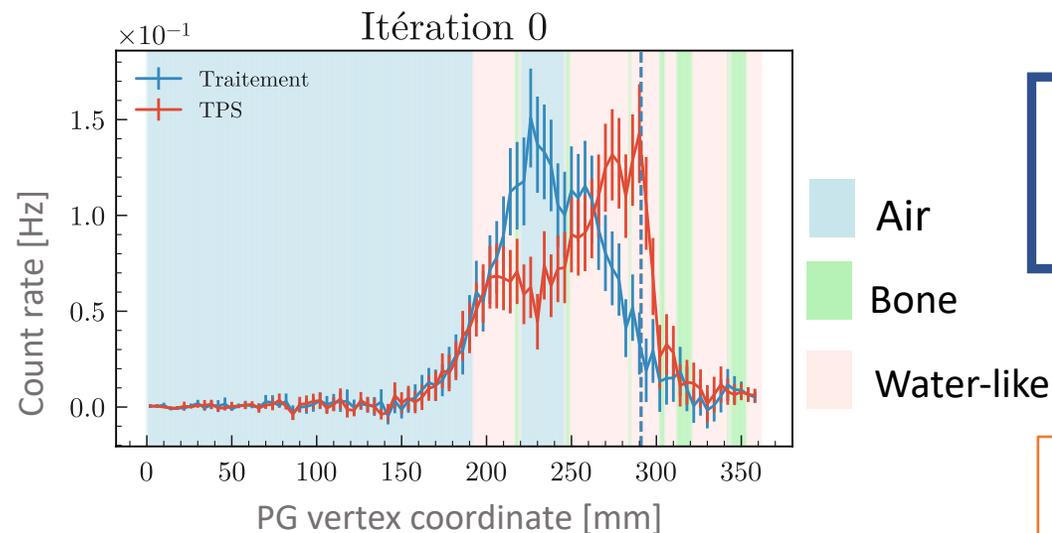
Treatment planning:
the sinus is empty



Treatment:
the sinus is filled
(inflammation)

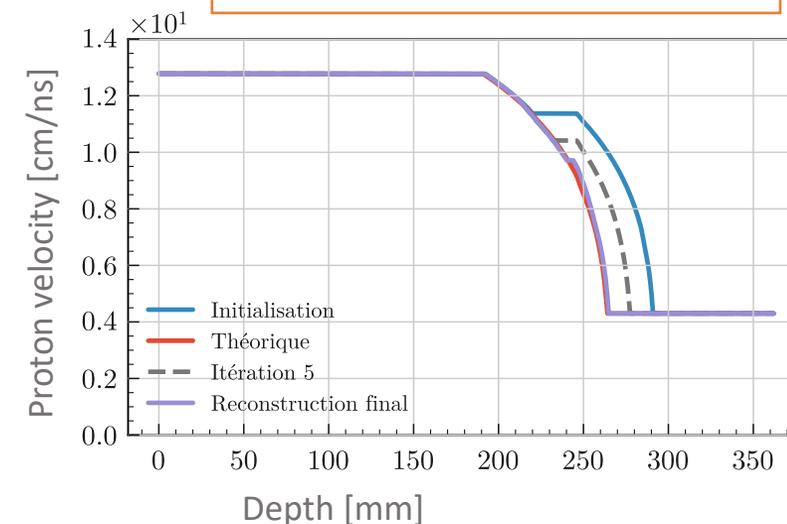
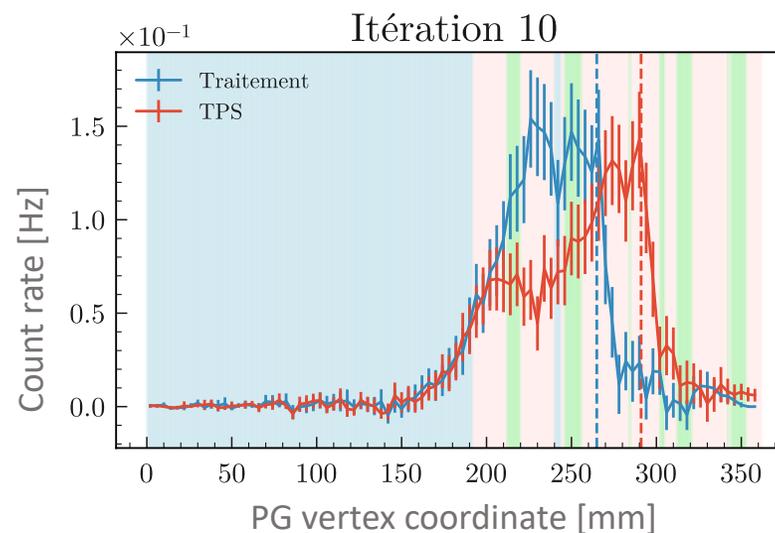
Prompt Gamma Time Imaging

- 1) Iterative reconstruction of PG vertex distribution
- 2) Identification of anatomical change
- 3) Determination of proton velocity



$$TOF = t_{stop} - t_{start} = T_{proton}(\mathbf{r}_v, \mathbf{v}_p) + T_{PG}(\mathbf{r}_v, \mathbf{r}_d)$$

Range shift
Actual = 27 ± 1 mm
Measured = 26 ± 4 mm



Conclusions

The use of **Cherenkov detectors** is promising to significantly increase the sensitivity of PG-based monitoring techniques:

- High detection efficiency ($\sim 0.45\%$)
- Higher SNR (no neutron detection)
- But sensitive to secondary protons in ^{12}C therapy

A first **8-channel prototype** has been **extensively tested**

- **with protons at low intensity regime**, with cyclotrons, synchro-cyclotrons and synchrotrons .
- with carbon ions at CNAO

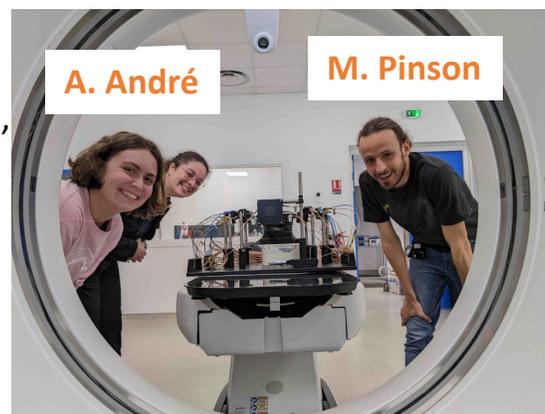
The PGTI reconstruction algorithm may allow to **identify anatomical changes** between treatment planning and delivery.

Acknowledgements and credits

The TIARA Collaboration



LPSC: S. Marcatili, **A. André**, G. Fanciulli, ML. Gallin-Martel, L Gallin-Martel, C. Hoarau, P. Kavrigin, J-F Muraz, P. Paris, **M. Pinson**
CPPM: Y. Boursier, C. Abid, M. Dupont, A. Garnier, C. Morel
CAL: D. Maneval
Roma Tor Vergata: N. Toschi, D. Psarras



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Petter Hofverberg (CAL), **Marco Pullia** (CNAO) and their teams for the nice reception

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M. Jacquet PhD thesis, ED physique
A. André PhD thesis, ED physique



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Beam time at CNAO and related travel expenses



2 internships

