

Comparison of radiation damage effects in plastic scintillators after ultra-high dose rate irradiations of 9-MeV electrons, 200-MeV electrons, and 87-MeV protons

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Cloé Giguère,

Uwe Titt, Arthur Lalonde, Luc Beaulieu and Sam Beddar

IC3DDose 2026 | June 17th

Novel dosimetry for the clinic today and for the emerging irradiation modalities of tomorrow

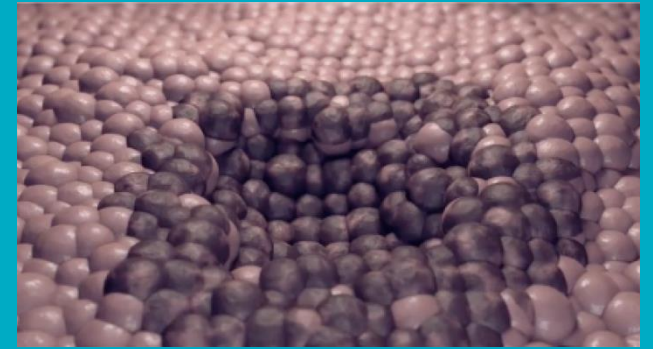


FLASH-RT: The Future of Radiotherapy?

What

Radiotherapy using ultra-high dose rates (UHDR)

- $> 100 \text{ Gy/s}$ VS $\sim 0.1 \text{ Gy/s}$ current clinical standard



Conventional Radiotherapy
Possible side effects



FLASH Radiotherapy
Less side effects



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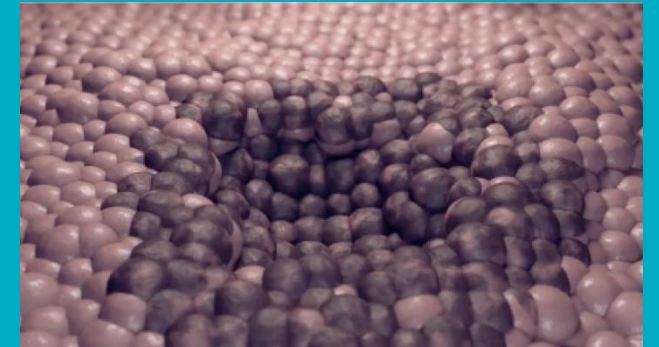
Why

The FLASH effect appears at UHDR

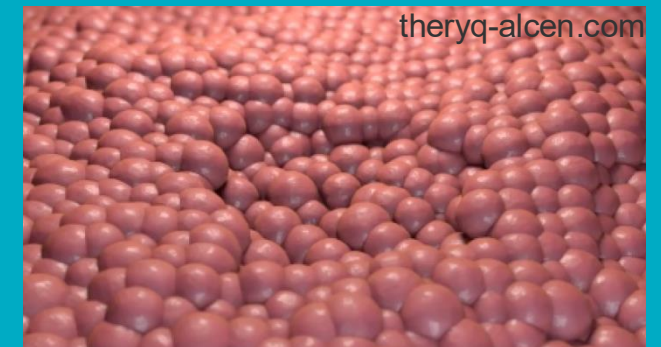
⬇ of healthy tissue toxicity

= anti-tumour response

Discovered in
2014 by
Favaudon *et al.*



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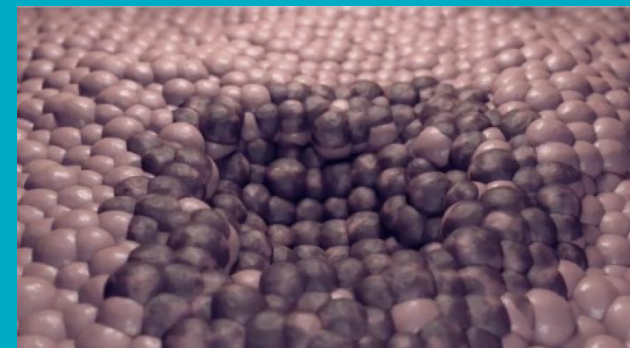
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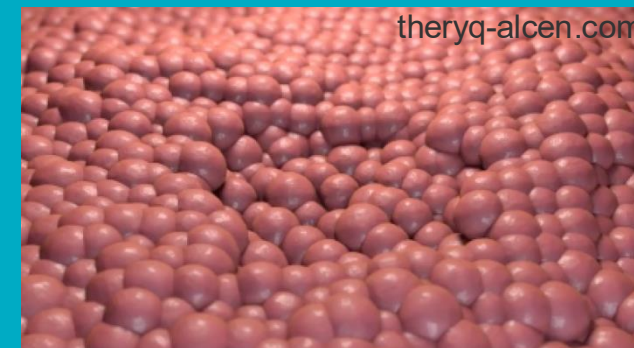
↓ of fractions/treatments

↓ of irradiation time

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Conventional Radiotherapy
Possible side effects



FLASH Radiotherapy
Less side effects



FLASH-RT: Challenges Before the Clinic

1

FLASH mechanism: how/why does it work?

- Oxygen depletion, reactive oxygen species, radicals, DNA damage, immune & inflammatory responses, ... ?



FLASH-RT: Challenges Before the Clinic

- 1 FLASH mechanism: how/why does it work?
 - Oxygen depletion, reactive oxygen species, radicals, DNA damage, immune & inflammatory responses, ... ?

- 2 What are the factors influencing the FLASH effect?
 - Treatment parameters: dose ≥ 10 Gy, single fraction or multiple, tissue sensitivity
 - Beam delivery parameters: modality (photons, protons, electrons), energy, instantaneous dose rate, average dose rate, dose per pulse, duration, etc.



≥ 40 Gy/s
 $\neq$ always
FLASH
effect!



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Plastic scintillation detectors (PSDs)

Plastic Scintillation Dosimetry

- ✓ Water equivalent
- ✓ Energy independent
- ✓ Small sized ($< 1 \text{ mm}^3$)
- ✓ High temporal resolution
- ✓ Linear response to dose
- ✓ Dose rate independent

In conventional
clinical
conditions

Scintillation
light $\propto$ dose!

To photodetector

Optical fiber

Radiation beam

Plastic scintillator

Plastic Scintillation Dosimetry

- ✓ Water equivalent
- ✓ Energy independent
- ✓ Small sized ($< 1 \text{ mm}^3$)
- ✓ High temporal resolution
- ✓ Linear response to dose (up to $\sim 45 \text{ Gy}$ in a single pulse)
- ? Dose rate independent
- ✗ Sensitive to radiation damage

In FLASH?



Scintillation
light $\propto$ dose!

To photodetector

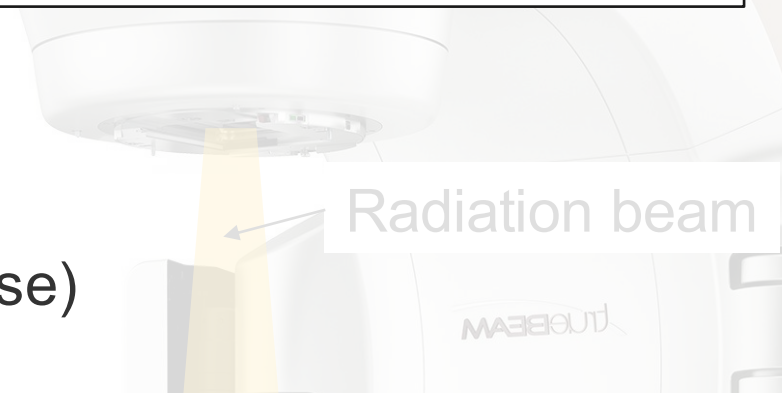


Scan to read

Submitted to Physics in Medicine and Biology,
in second round of reviews

**Characterization of radiation damage sensitivity in
plastic scintillators and optical fibers for proton
FLASH real-time dosimetry**

Cloé Giguère^{1,2,3}, Uwe Titt^{3,4}, Luc Beaulieu^{1,2*} and Sam Beddar^{3,4*}



PAPER • OPEN ACCESS

Radiation damage and recovery of plastic scintillators under ultra-high dose rate 200 MeV electrons at CERN CLEAR facility

Cloé Giguère, Alexander Hart, Joseph Bateman, Pierre Korysko, Wilfrid Farabolini, Yoan LeChasseur, Magdalena Bazalova-Carter* and Luc Beaulieu

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[Physics in Medicine & Biology](#), Volume 70, Number 7

Citation Cloé Giguère et al 2025 *Phys. Med. Biol.* **70** 075018

DOI 10.1088/1361-6560/adc234



GOAL:

Study the effect of radiation type on PSD radiation damage and recovery processes, by comparing UHDR irradiations of

- 200 MeV very high energy electrons (VHEEs)
- 9 MeV electrons
- 87 MeV spread-out Bragg peak (SOBP) protons

Methods

UHDR irradiation parameters

Particle type	Beamline	Energy (MeV)
VHEEs	CERN CLEAR	200
Electrons	CHUM Mobetron	9
SOBP protons	MD Anderson PTC 1	87

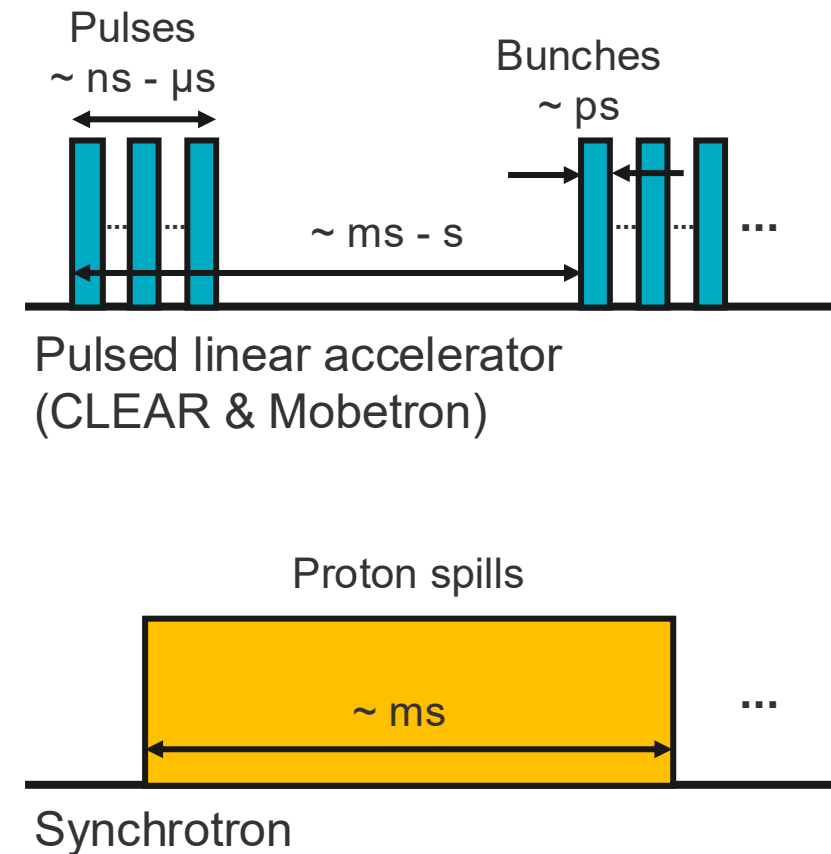
Linear electron accelerator

Linear electron accelerator

Synchrotron

UHDR irradiation parameters

Particle type	Beamline	Energy (MeV)	Pulse or spill length (ns)	
VHEEs	CERN CLEAR	200	1-125	~ns
Electrons	CHUM Mobetron	9	$(1-3.78) \times 10^3$	~ μ s
SOBP protons	MD Anderson PTC 1	87	$(27-71) \times 10^7$	~ms



UHDR irradiation parameters

$$\text{Dose rate} = \frac{\text{Dose per pulse or spill}}{\text{Pulse or spill length}}$$

Particle type	Beamline	Energy (MeV)	Pulse or spill length (ns)	Dose per pulse or spill (Gy)	Dose rate (Gy/s)
VHEEs	CERN CLEAR	200	1-125	~5-90	(0.22-4.60) $\times 10^9$
Electrons	CHUM Mobetron	9	(1-3.78) $\times 10^3$	0.90-3.39	(8.86-9.19) $\times 10^5$
SOBP protons	MD Anderson PTC 1	87	(27-71) $\times 10^7$	7-18	252-259

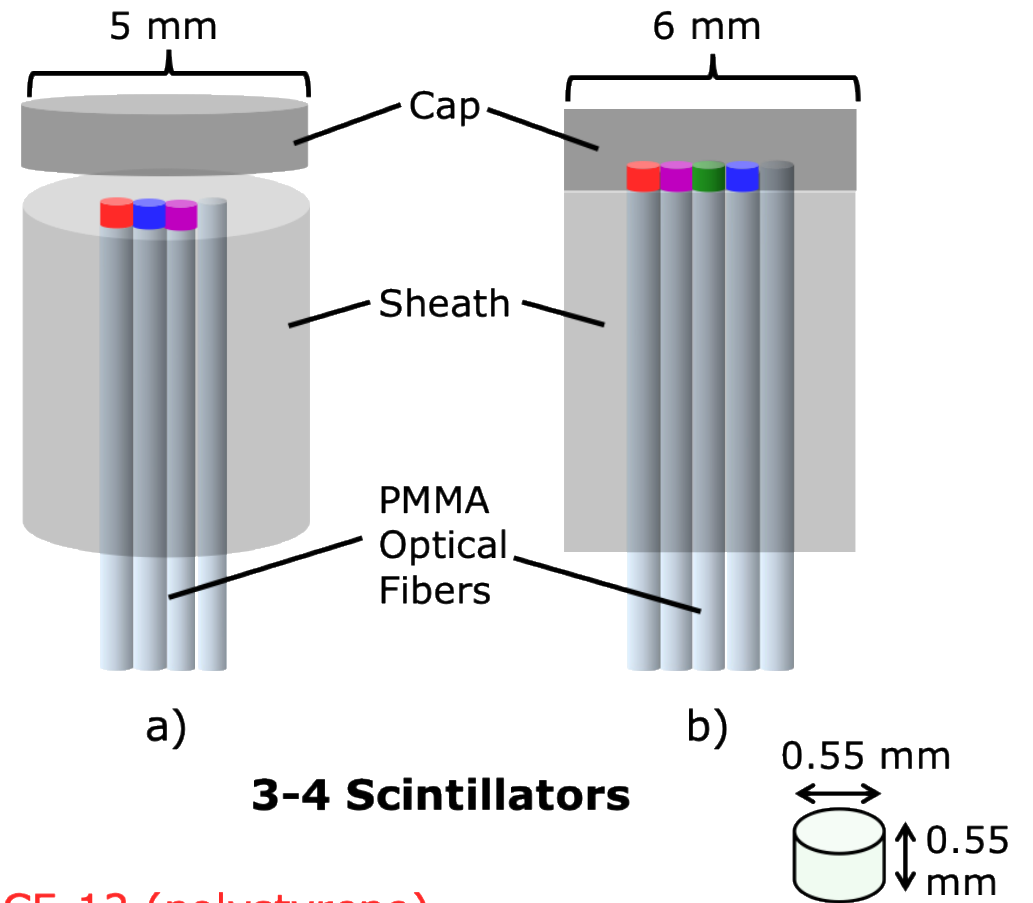
UHDR irradiation parameters

Particle type	Beamline	Energy (MeV)	Pulse or spill length (ns)	Dose per pulse or spill (Gy)	Dose rate (Gy/s)	Cumulative dose (kGy)
VHEEs	CERN CLEAR	200	1-125	~5-90	$(0.22-4.60) \times 10^9$	37.2
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SOBP protons	MD Anderson PTC 1	87	$(27-71) \times 10^7$	7-18	252-259	10.4

Experimental set-up

- (a) VHEEs & 9 MeV: 4-channel PSD
- (b) Protons: 5-channel PSD
- Last channel without a scintillator for stem-effect light removal
- Light acquisition with the Medscint Hyperscint RP-200 dosimetry platform

4-5 channel PSD



3-4 Scintillators

BCF-12 (polystyrene)

EJ-212 (polyvinyltoluene)

Scint02 (polystyrene)

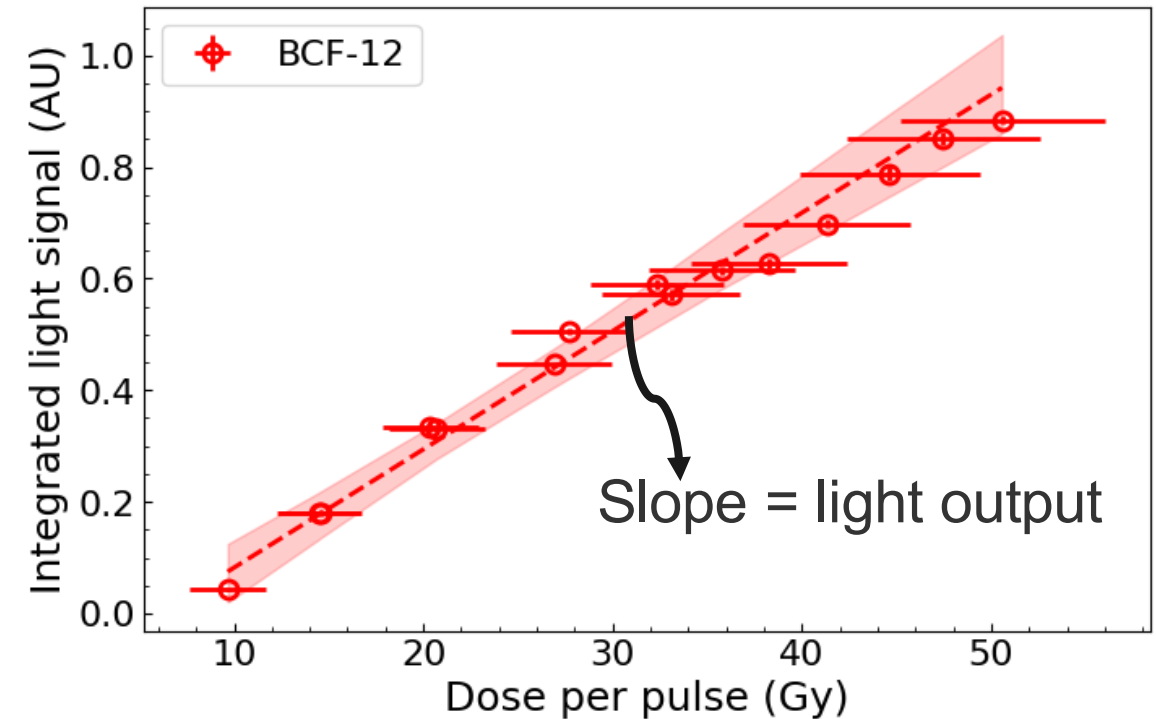
BCF-60 (polystyrene)

1 Blank optical fiber (PMMA)

Evaluation of Radiation Damage

Light output decrease

- Linearity response of scintillators to varying dose per pulse or spill
- Slope of linear fits = light output
- Repeat of linearity measurements + high dose irradiations
- Light output tracked with cumulative dose
- Short-term rest (hours-days)

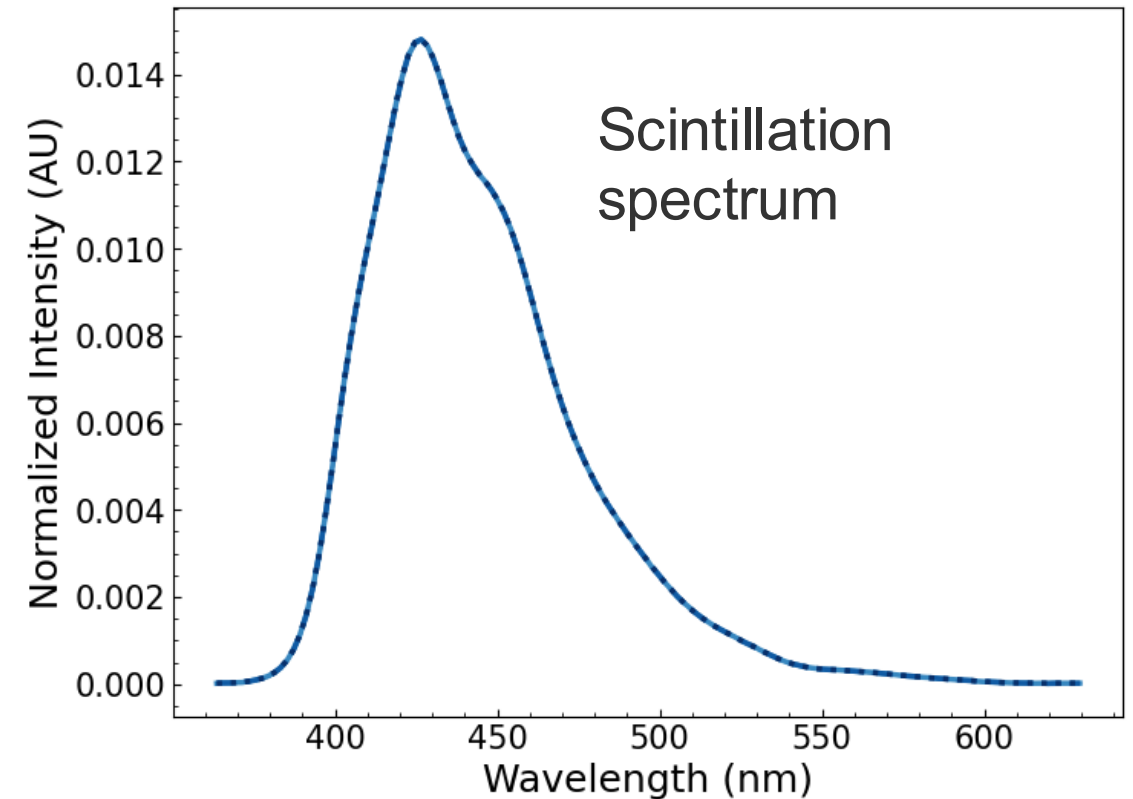


Evaluation of Radiation Damage

Spectral changes

- Spectral centroid (SC): average over the spectrum's wavelength bins ($\lambda(n)$), weighted by the intensity values ($I(n)$)

$$SC = \frac{\sum_{n=0}^{N=136} I(n)\lambda(n)}{\sum_{n=0}^{N=136} I(n)}$$



Long-term Recovery Measurements

Light output

- 6 MV photon beam of TrueBeam Linac
- 500 MUs, 10 cm depth in solid water

Scintillation spectrum

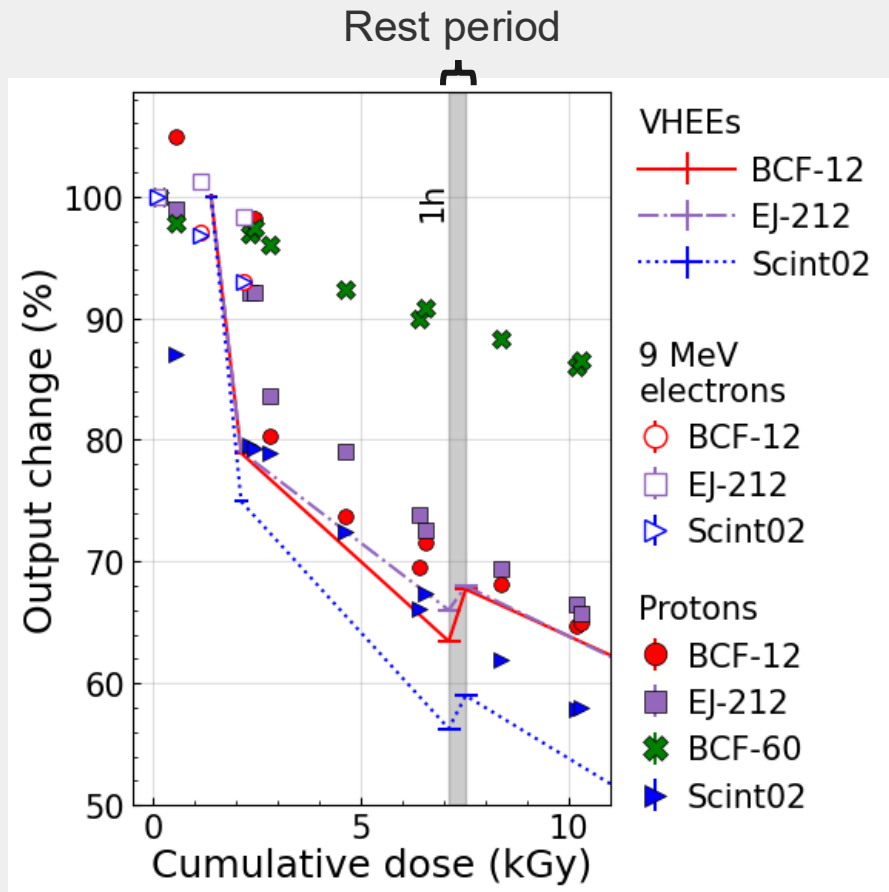
- 90 kV tube of TrueBeam Linac

Tracked with recovery time (50-300 days)



Results

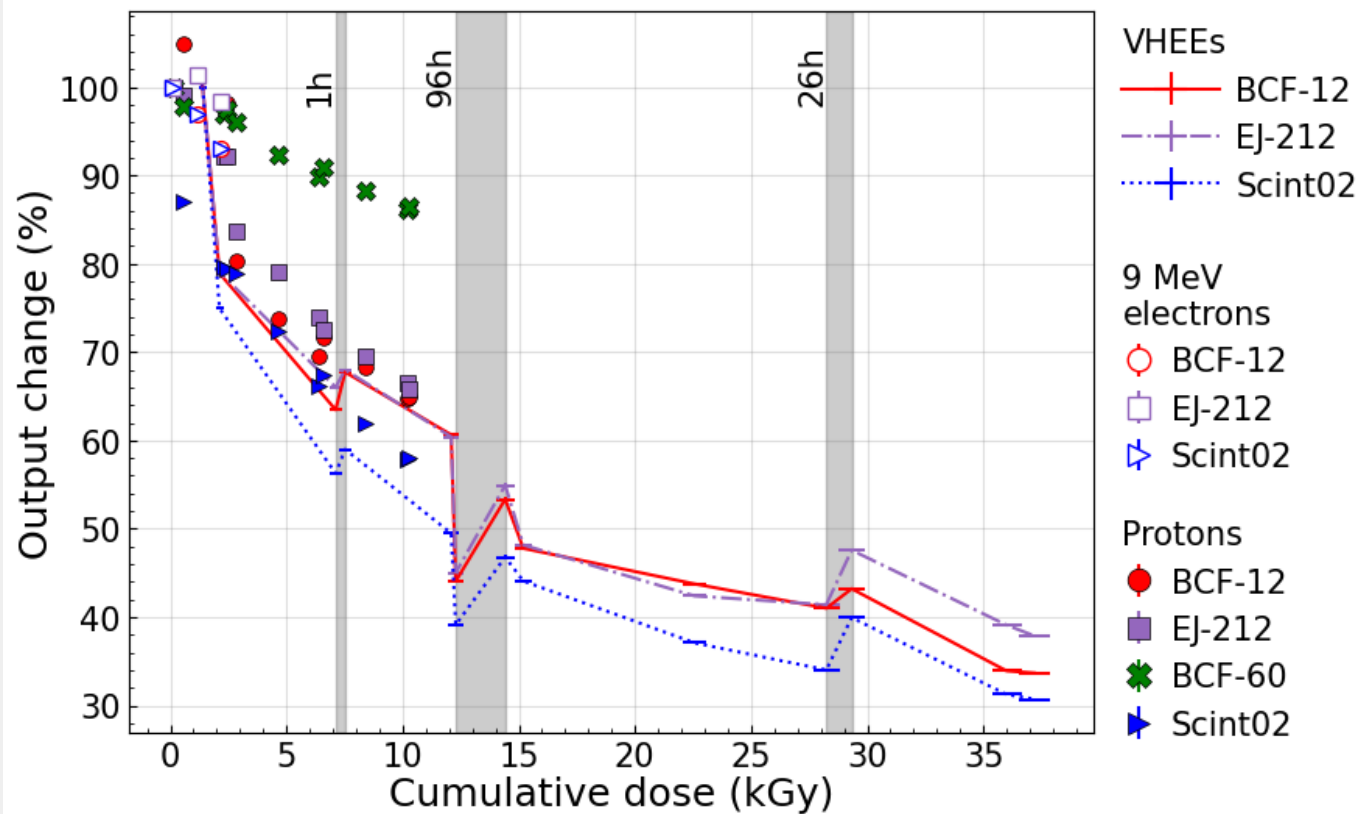
Light Output Decreases



First 10 kGy of cumulative dose

- Similar decreases for VHEEs, protons and 9 MeV electrons
- Recovery of output after 1 hour rest for VHEEs
- No short-term recovery observed for protons (15 min, 7 days, 20 days)

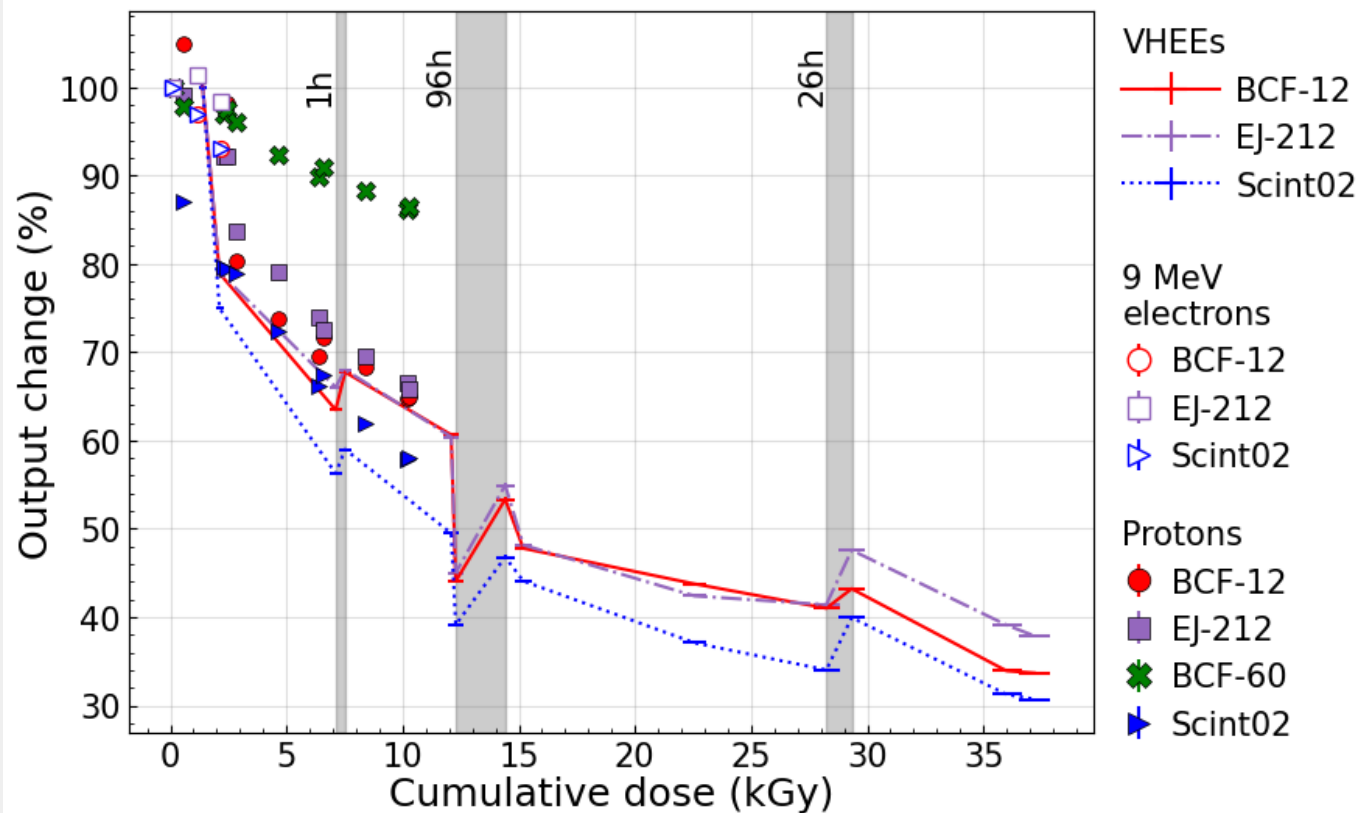
Light Output Decreases



Full range of cumulative dose

- After ~10 kGy of dose, VHEE data transitions to slower decrease
- Similar trend for protons and 9 MeV electrons?
- Recovery of output after 96h and 26h hour rest for VHEEs

Light Output Decreases

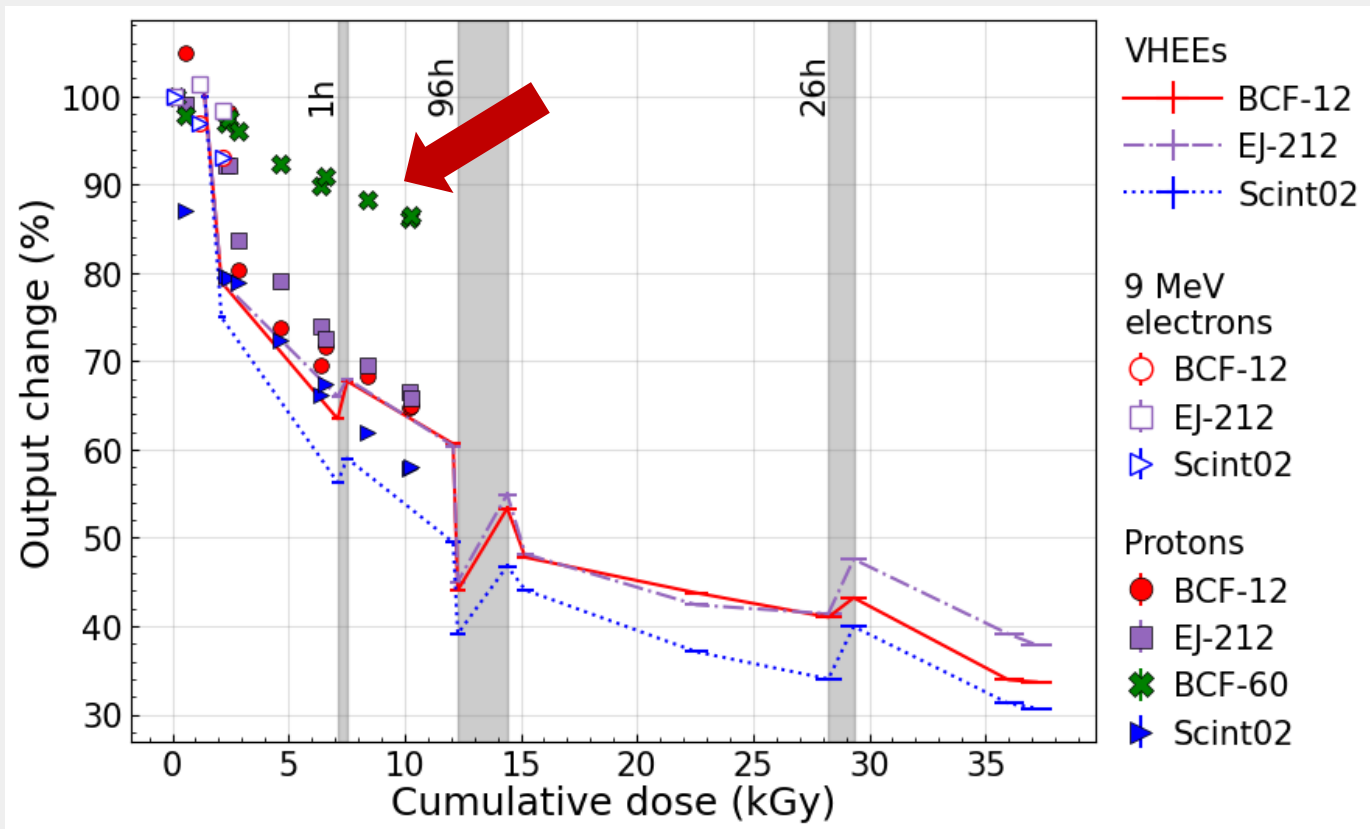


Average light output decreases (%/kGy)

	VHEEs	SOBP protons	9-MeV electrons
BCF-12	1.78	3.40	3.20
EJ-212	1.67	3.32	0.78
BCF-60	-	1.31	-
Scint02	1.86	4.08	3.24

~x2 average decreases for protons & 9 MeV electrons compared to VHEEs

Light Output Decreases

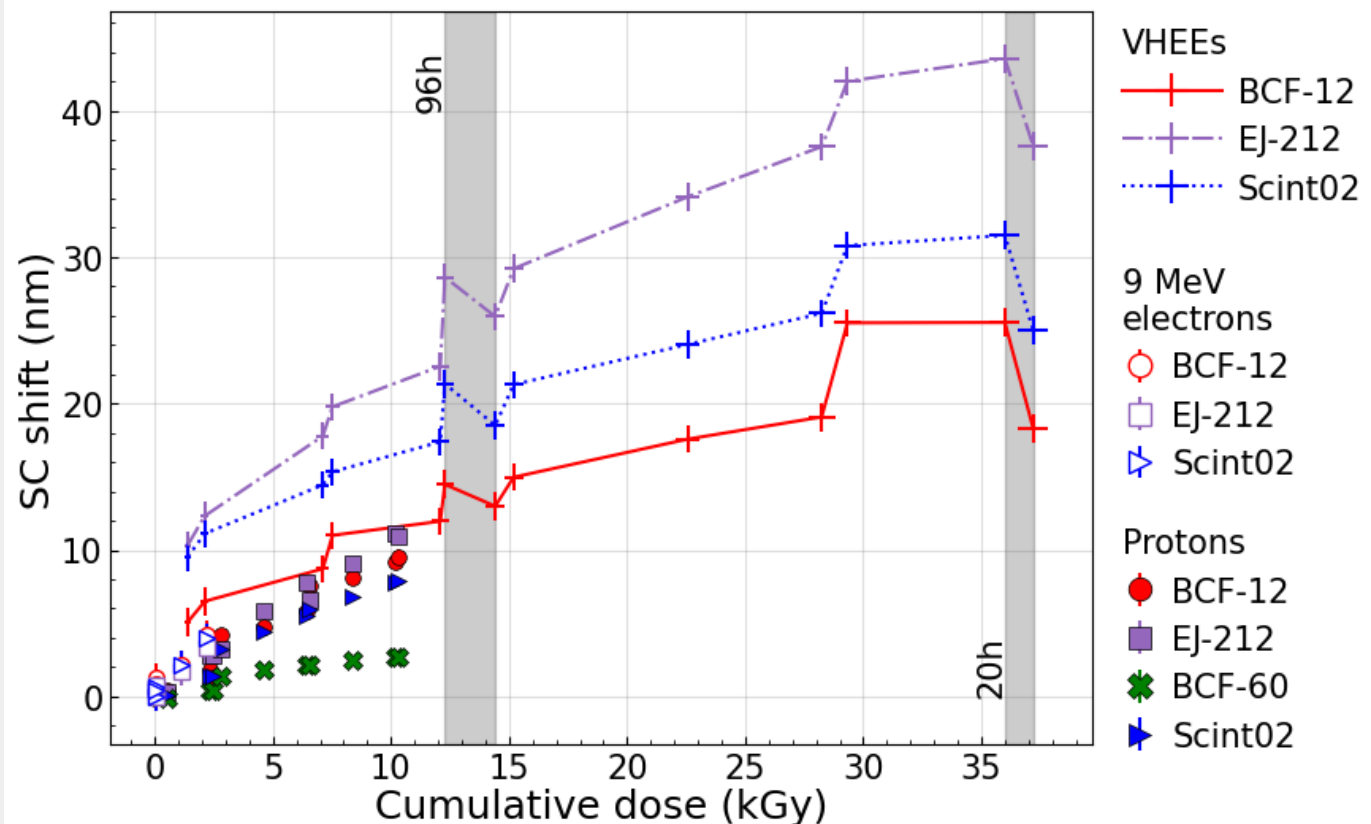


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Superior radiation hardness of BCF-60 scintillator with green emission (~550 nm)

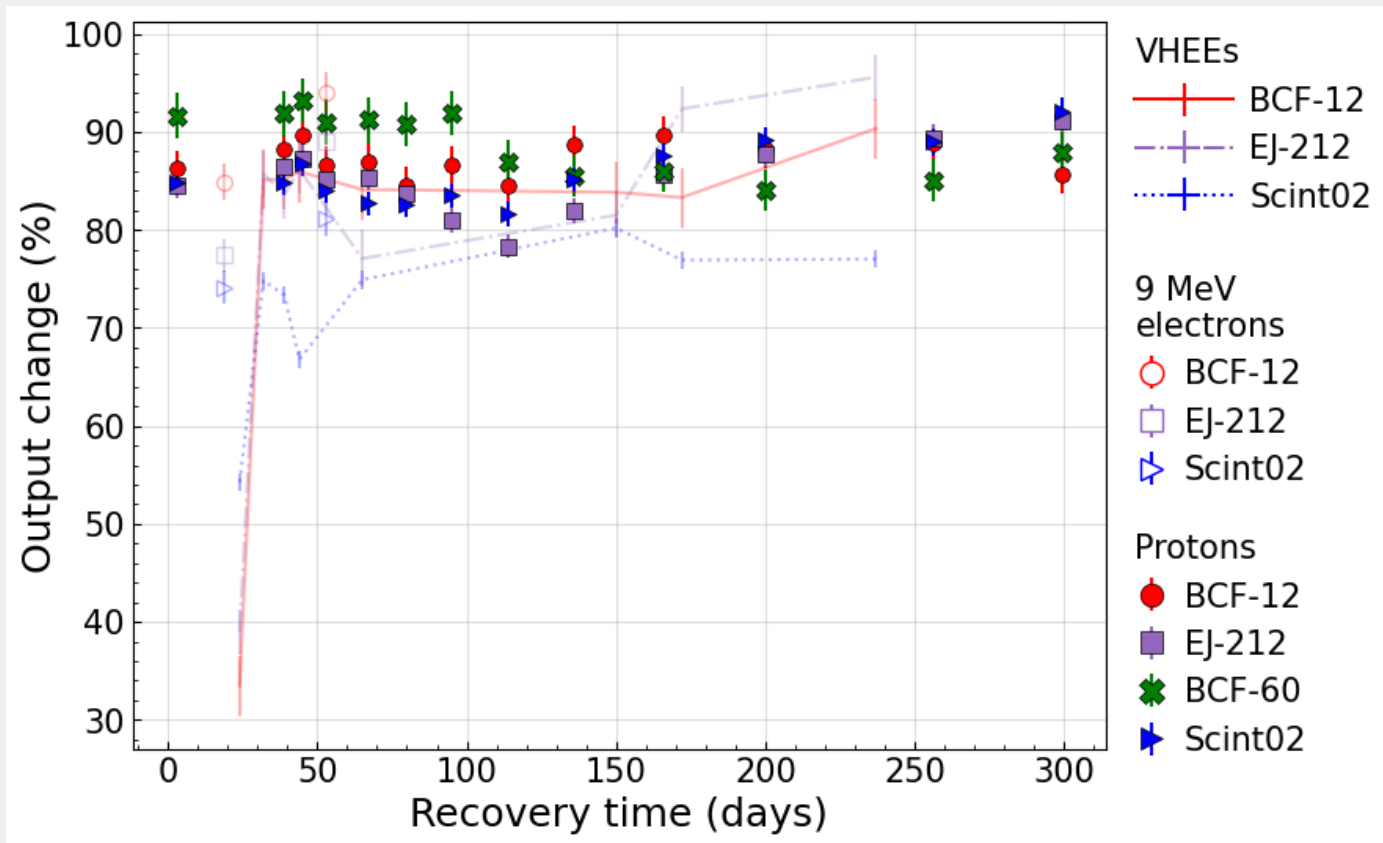
Spectral Changes



Spectral centroid shift increases

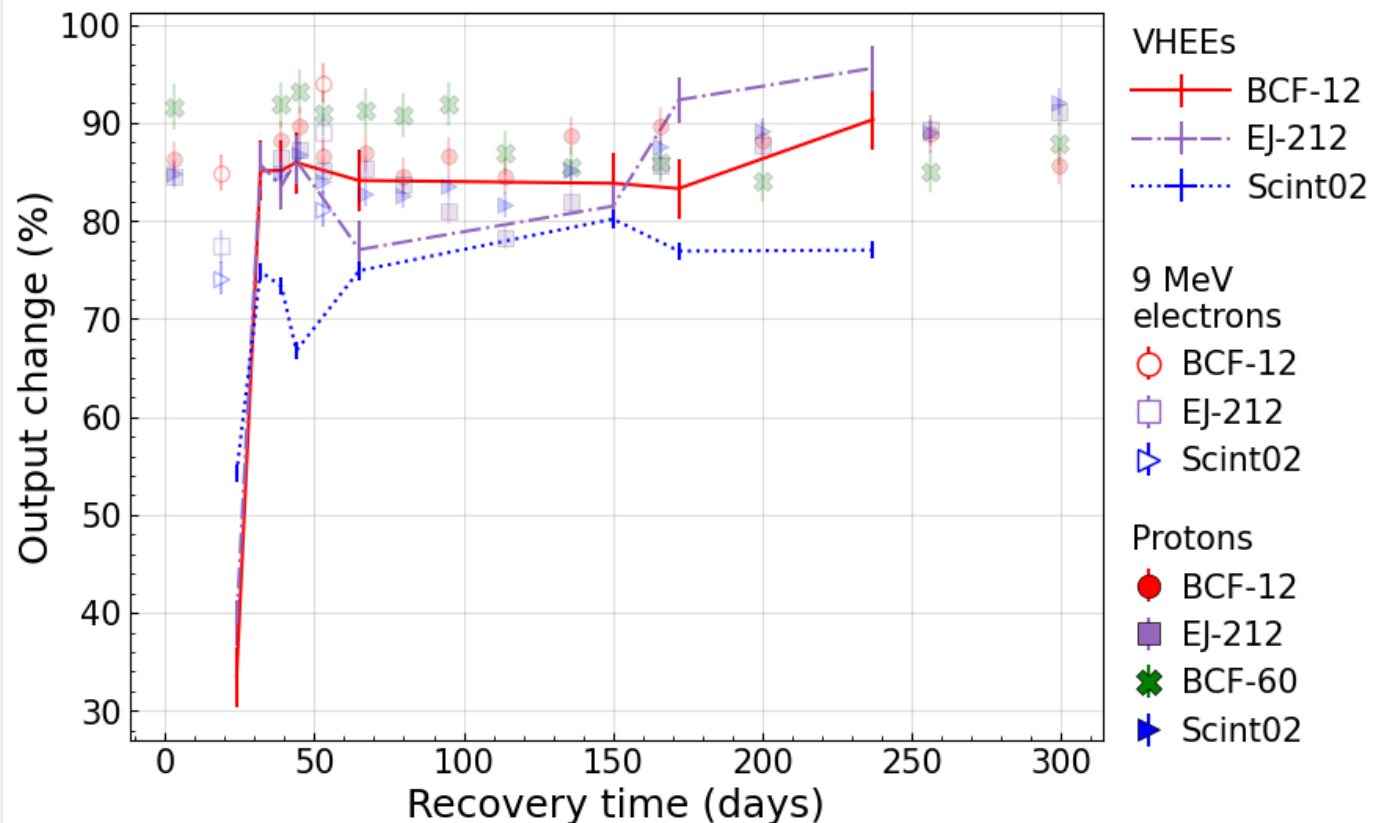
- Similar spectral changes between VHEEs, protons and 9 MeV electrons
- Recovery of spectral changes for VHEEs, after 96h and 20h rest

Long-term Recovery of Light Output



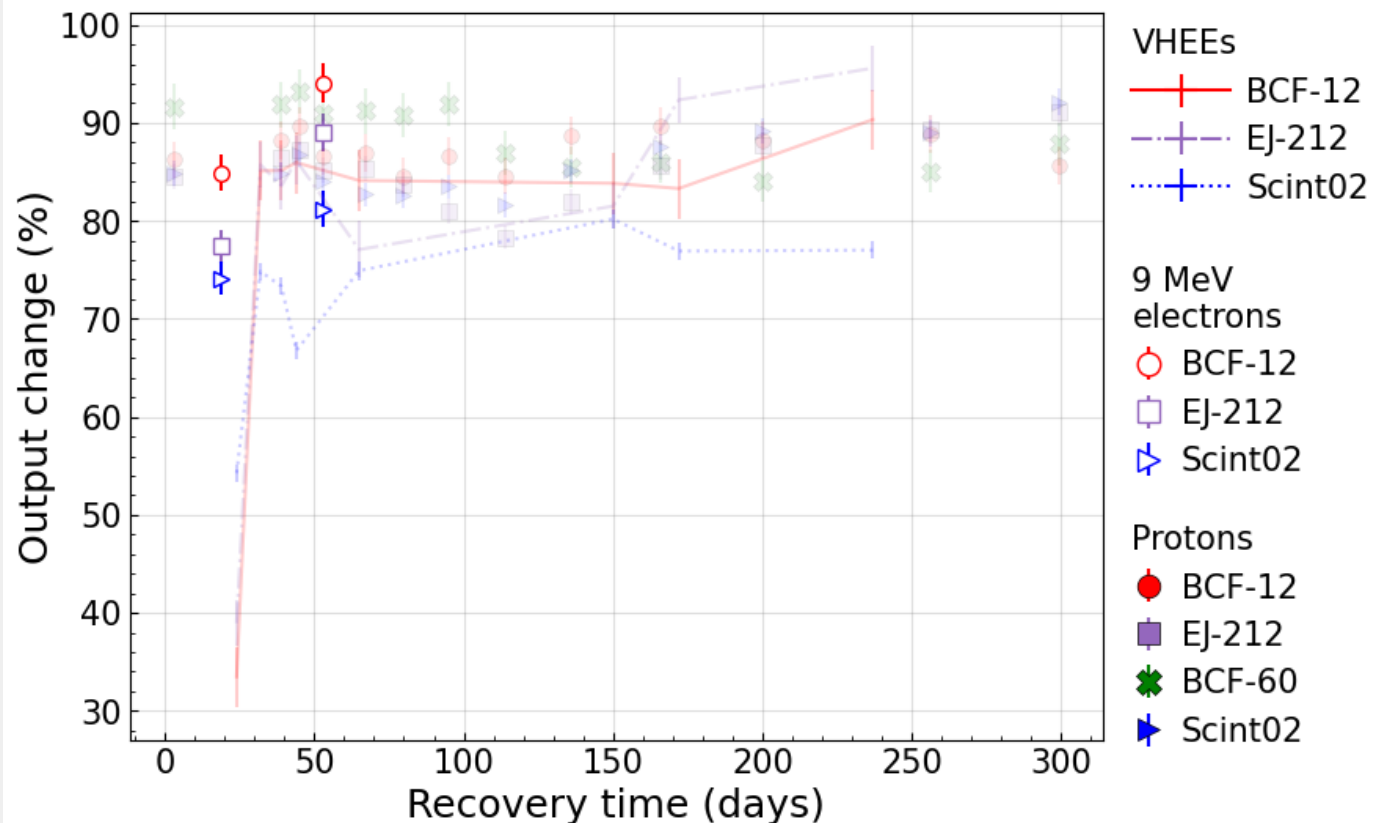
- Minimal light output recovery for protons
- Significant recovery of light output for VHEEs after 32-172 days
- Significant recovery around 50 days for 9 MeV electrons

Long-term Recovery of Light Output



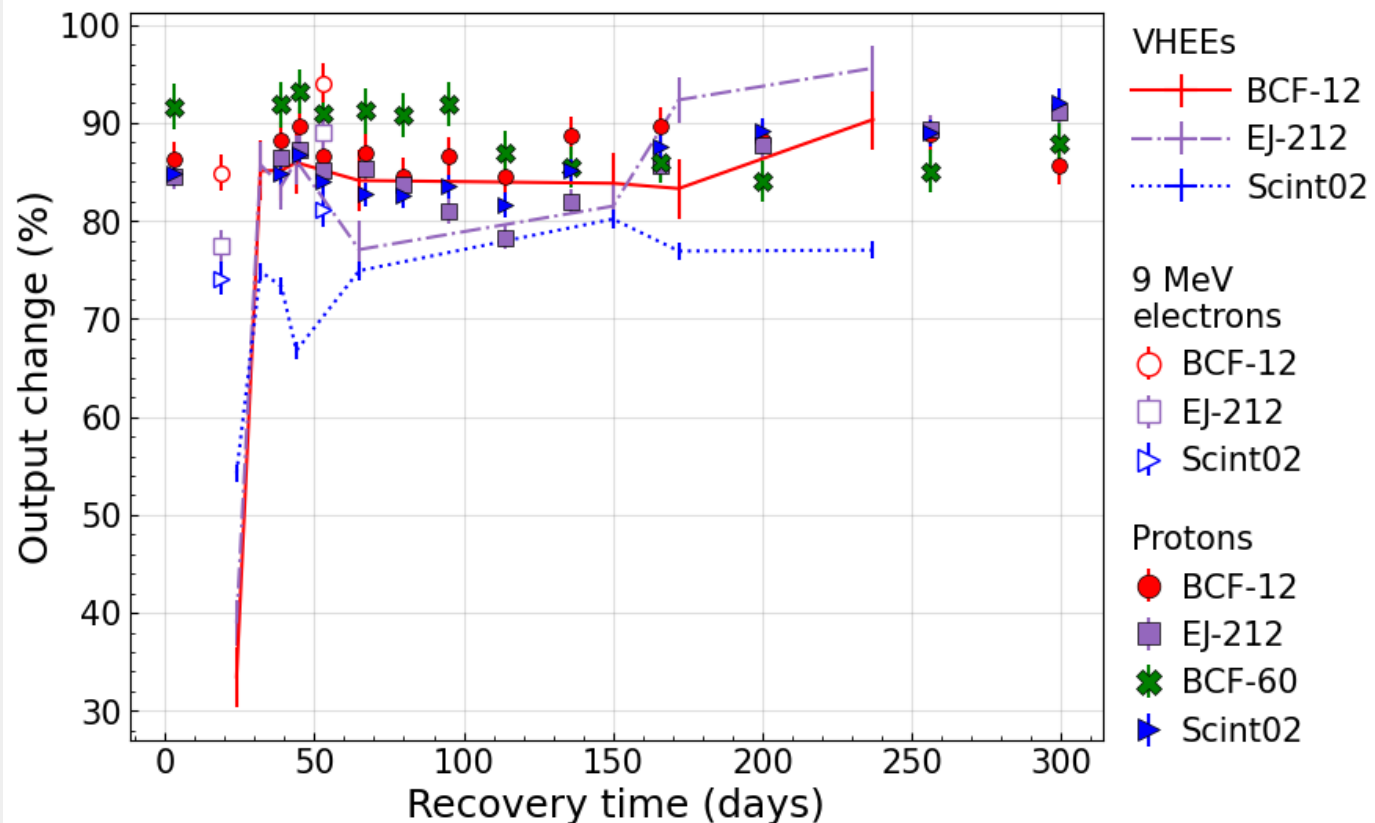
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Long-term Recovery of Light Output



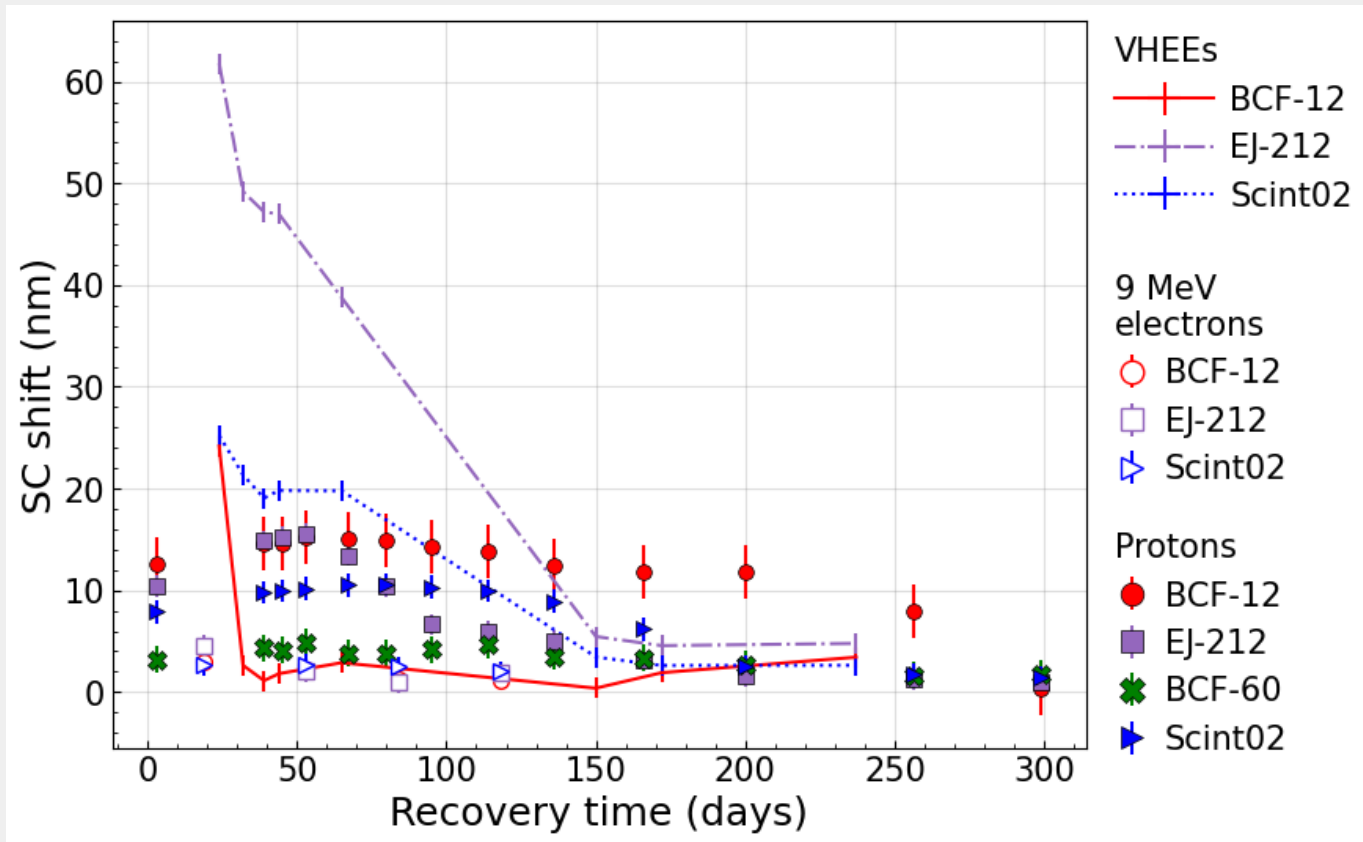
Effect of linear energy transfer (LET)

- High-LET radiation creates higher density of radicals
- Enhanced reactions between radicals
- Shown to lead to more permanent radiation damage (not recoverable)

Possible effect of beam time structure

- Pulsed vs near-continuous

Long-term Recovery of Spectral Changes



Spectral shift

- Complete recovery of spectral changes for all modalities
- Very slow (~300 days) for protons

Conclusions



Conclusions

Radiation damage

- First ~10 kGy: Similar effects for all modalities
- After ~10 kGy: VHEE-irradiated scintillators become more radiation-hard

Recovery

- Minimal for protons, but significant for electrons
- High-LET protons create more permanent damage

Takeaways

- Type of radiation influences radiation damage and recovery processes
- Green-emitting BCF-60 is more radiation-hard

Thank you!

Merci!



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Thank you to my collaborators from CERN
CLEAR, CHUM and MD Anderson!

Work funded by



Groupe de recherche en physique médicale (GRPM)



ICCR 2027 - XXIth International Conference on the use of Computers in Radiation Therapy

Quebec Congress Centre • July 4-8, 2027



ICCR is one of the longest-running conferences in radiation therapy. Held only every three years, it attracts medical physicists, clinicians, and academic scientists from across the globe who are using computers to drive advances in radiation therapy. Many important innovations have been unveiled at ICCR and the conference enjoys a very high standing in the international radiation oncology community.



We look forward to welcoming you in Québec in July 2027!

Thank you!

Merci!



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Experimental set-up

VHEEs:

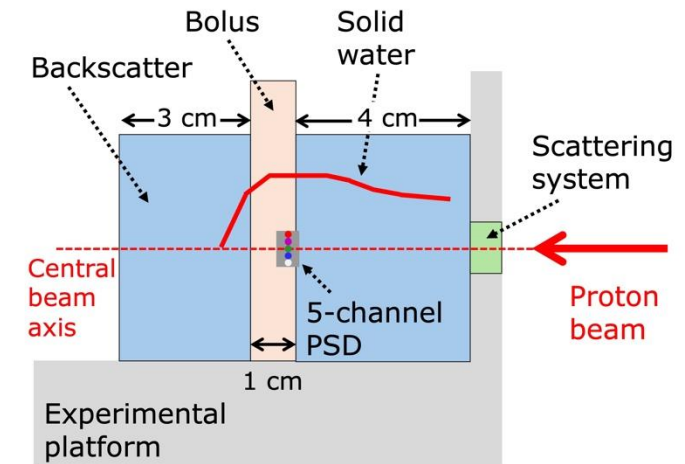
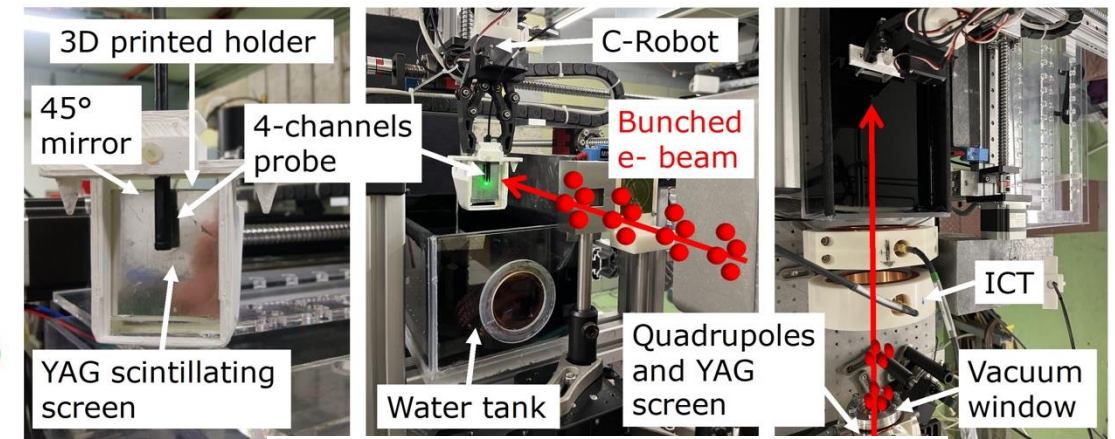
- ICT & MD-V3 films
- Water tank, 4 cm depth

Protons:

- Advanced Markus chamber
- Solid water, 4 cm depth (plateau region)

9 MeV electrons:

- BCT
- Solid water, 1 cm depth

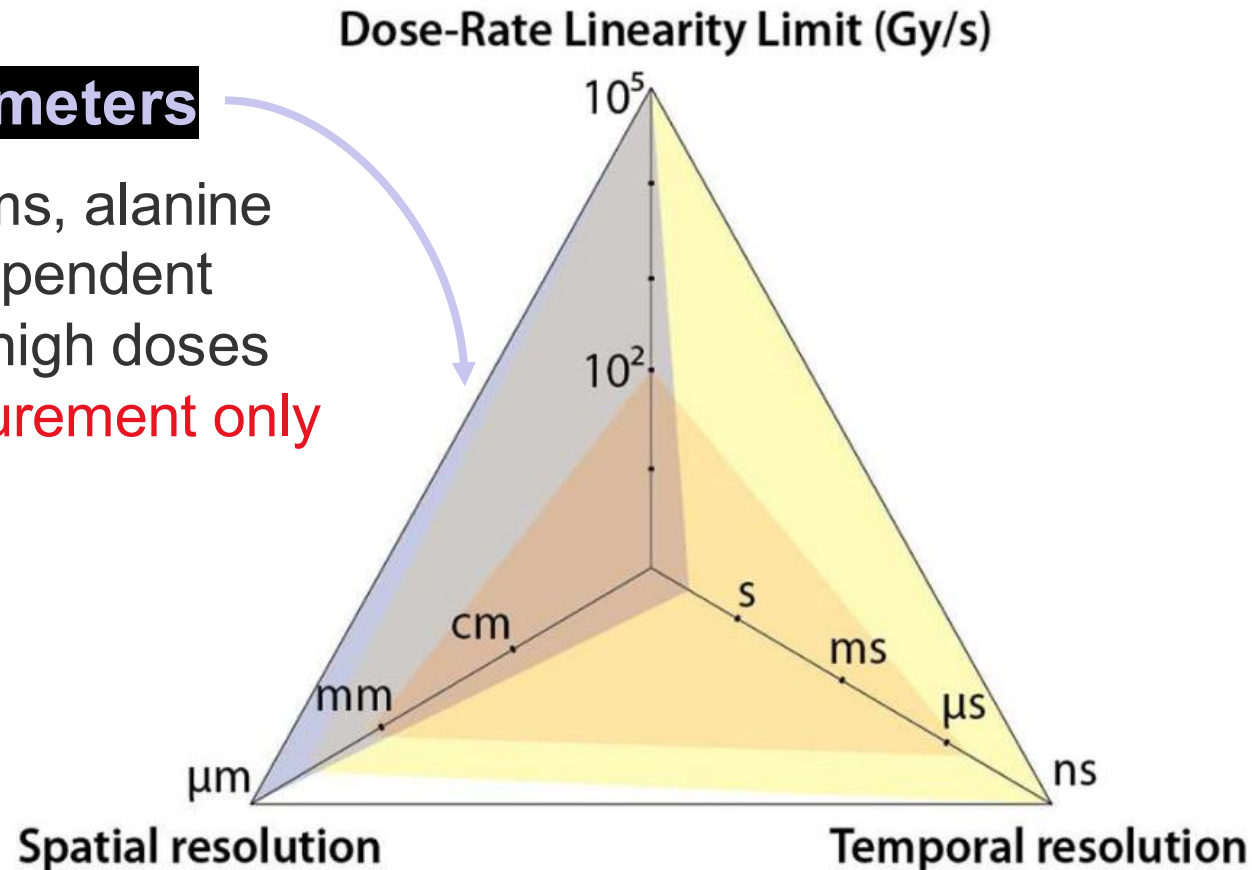


Dosimetry in UHDR conditions

Chemical dosimeters

Radiochromic films, alanine

- Dose-rate independent
- Can measure high doses
- **Passive measurement only**



Dosimetry in UHDR conditions

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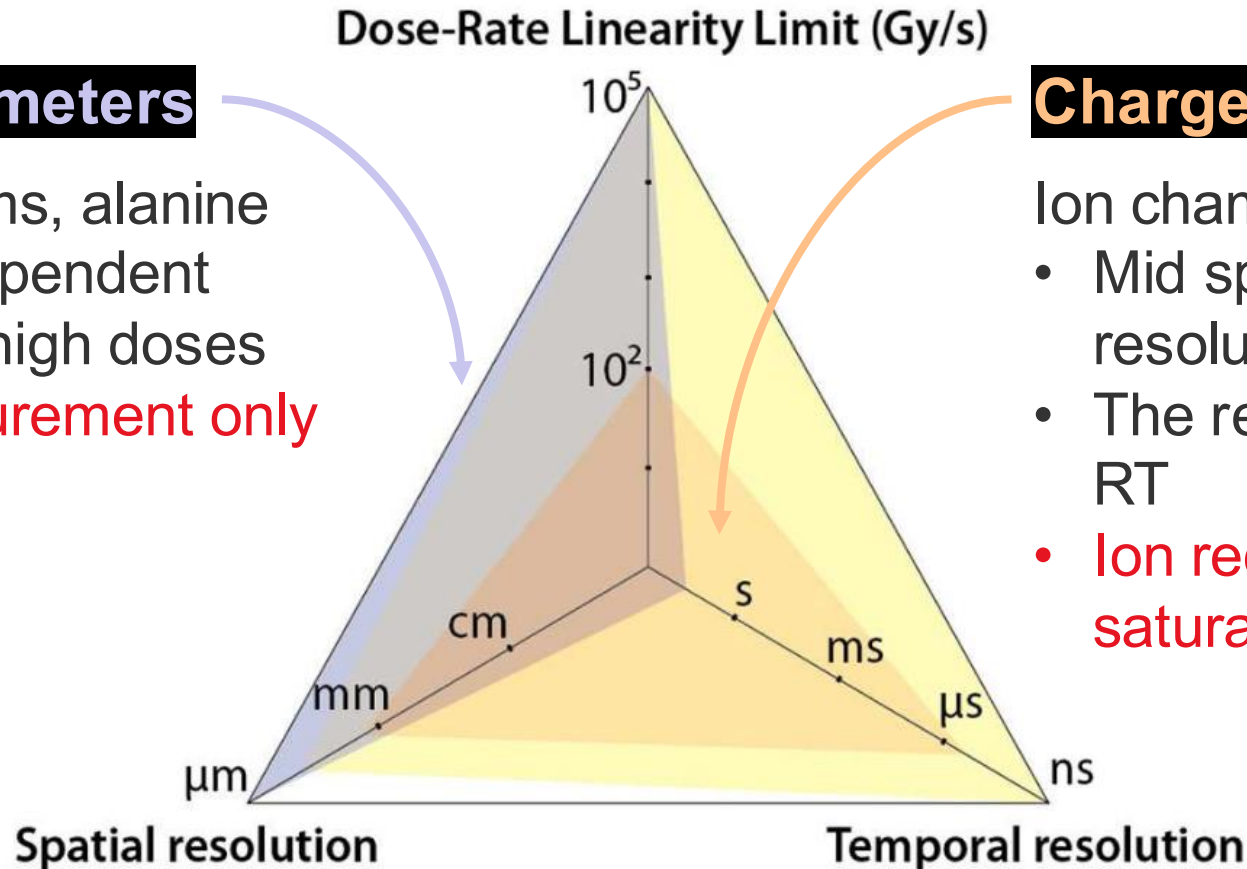
Radiochromic films, alanine

- Dose-rate independent
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Charge-based dosimeters

Ion chambers

- Mid spatial and high temporal resolutions
- The reference dosimeter in RT
- **Ion recombination & saturation at UHDR**



Dosimetry in UHDR conditions

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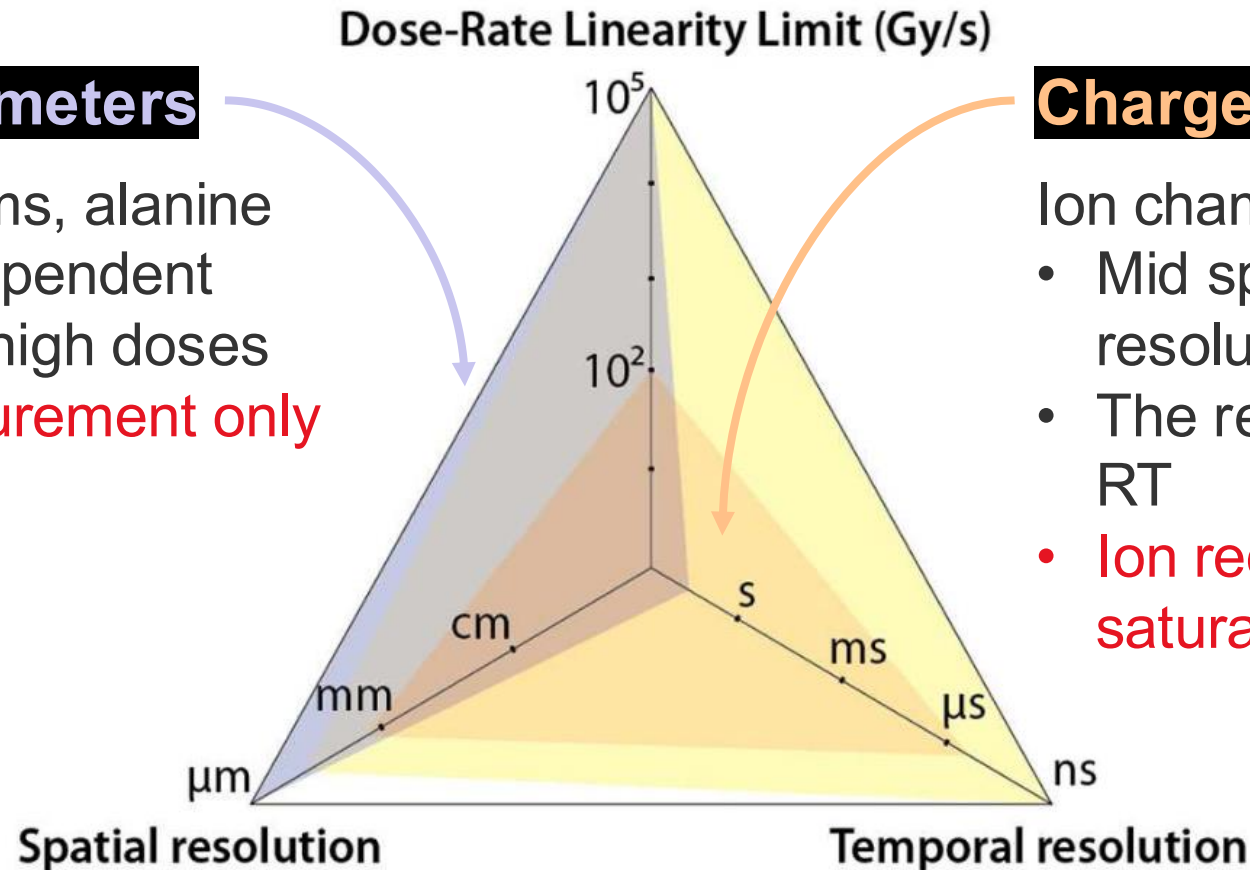
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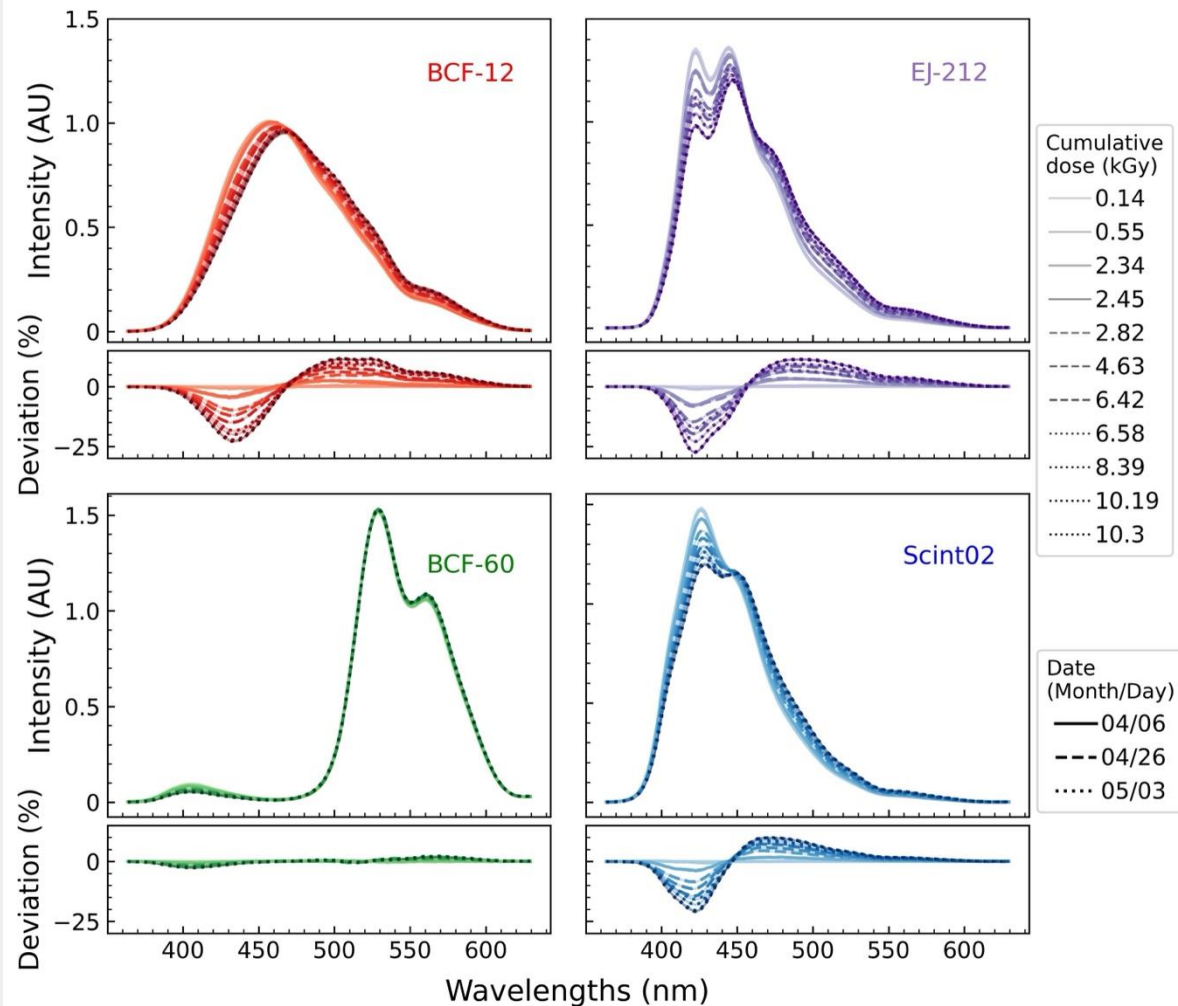
Luminescence-based dosimeters

Light Output Decreases

Mechanism of radiation damage

- Creation of free radicals in the polymer base: colour centers
- Absorption of scintillation photons and loss of transmittance
- Loss of light output and yellow discoloration

Spectral changes



- Decrease of scintillation emission mostly in the UV-blue (380-500 nm) region
- Shift of spectrum towards yellower wavelengths
- BCF-60 emits above the most affected spectral region

Fig.2: Scintillation spectra at increasing cumulative dose, for proton irradiations.

LET effect in radiation damage of plastics

Bodmann et al. 2001 & 2003

- High LET radiation lead to higher density of reactive intermediate species in the longitudinal track structure and to an overlapping of radicals along the path of the ionizing particle. Could cause enhanced interactions like reactions between radicals or recombination of radicals.
- Permanent damage in PS and PVT after recovery in air is larger for neutron than for gamma

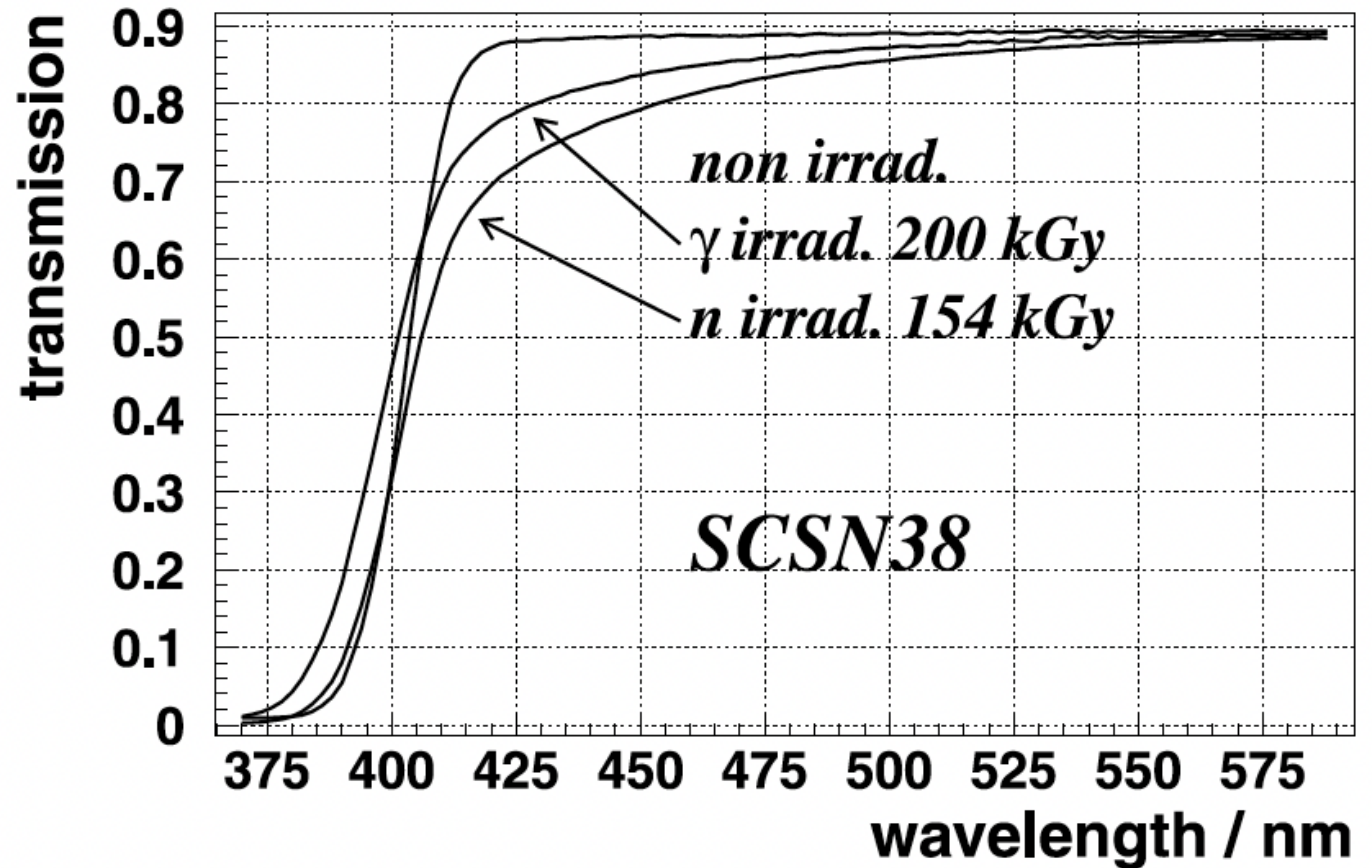
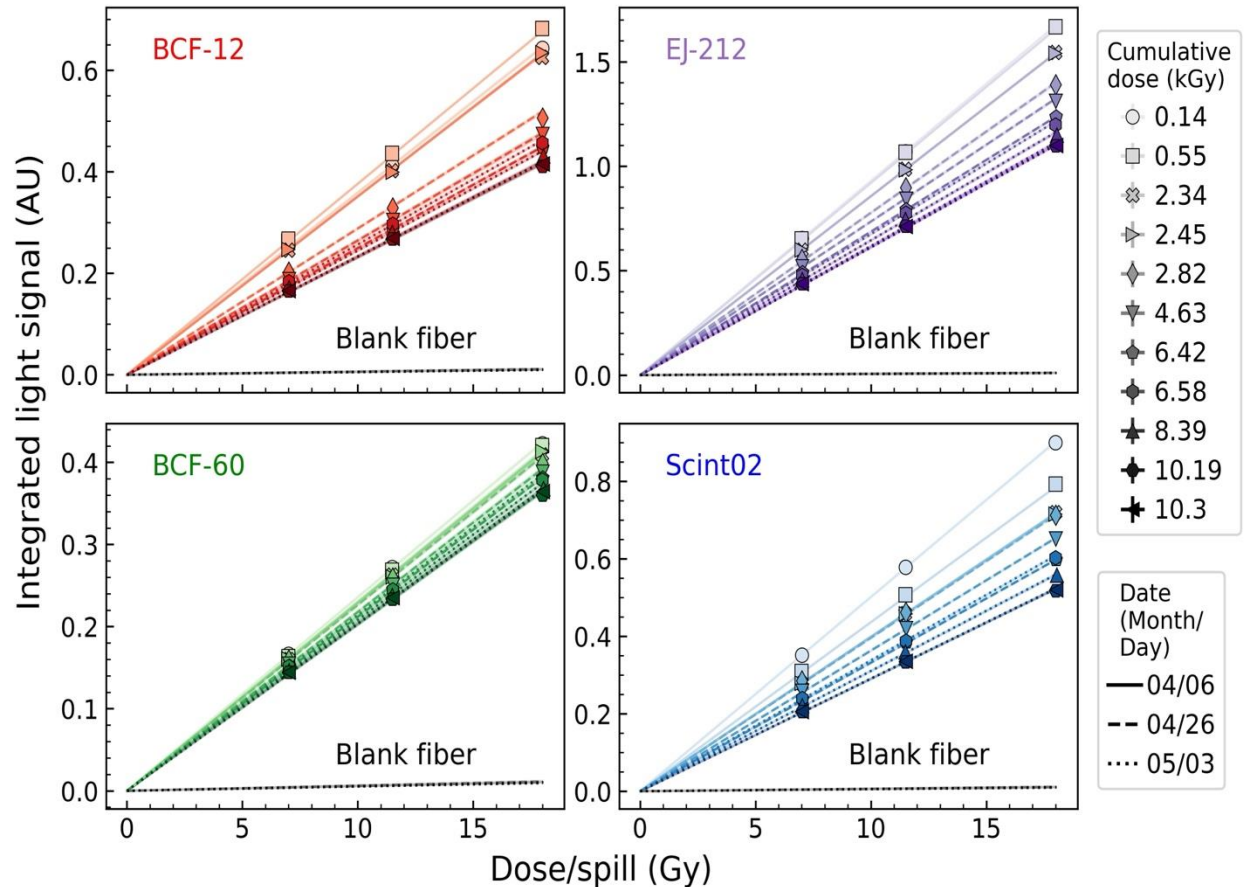


Fig. 2. Spectral transmissions of 2.6 mm thick SCSN38 samples before and after irradiation with 200 kGy γ and 154 kGy neutron (reactor) after complete annealing.

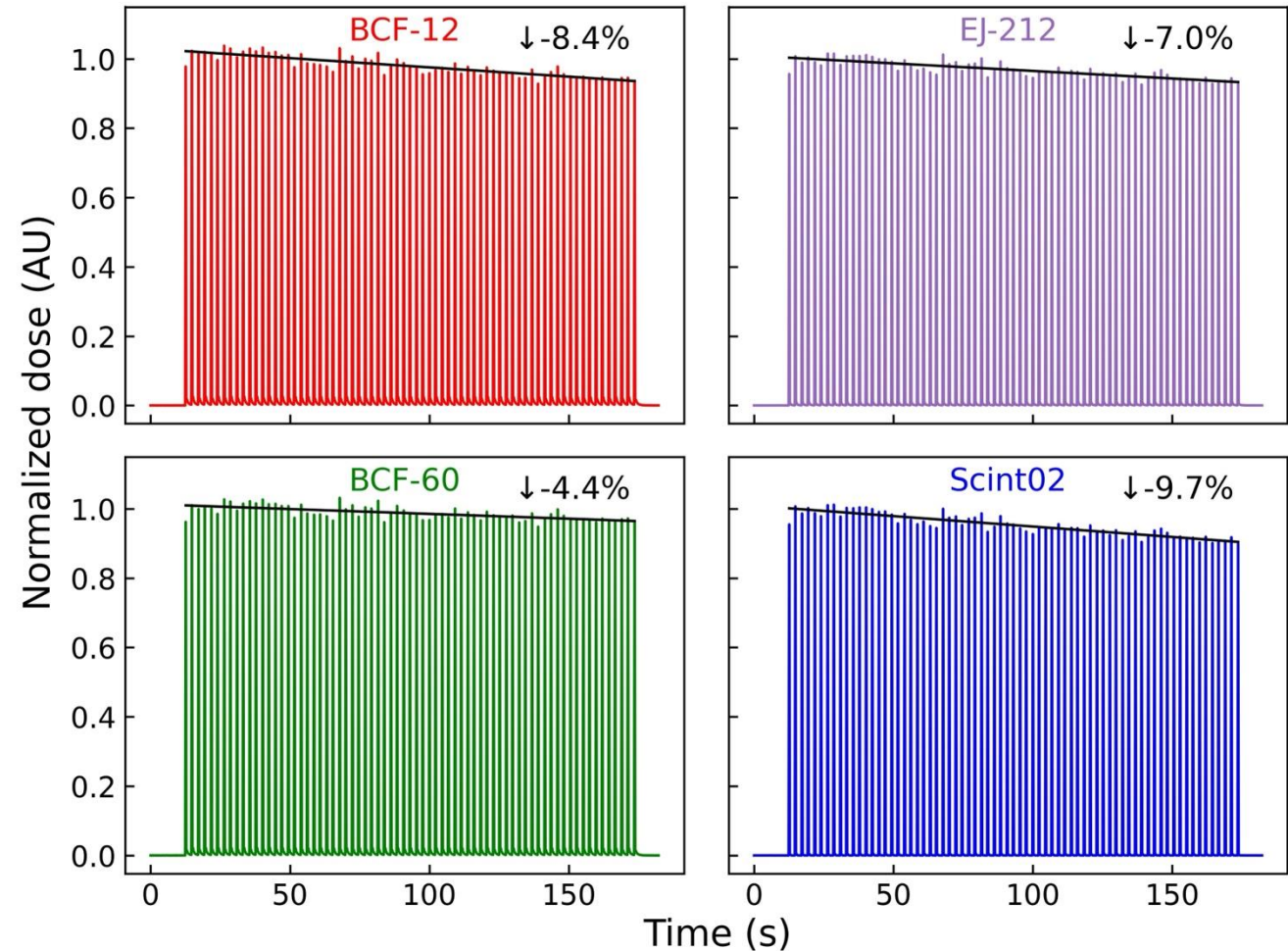
Protons Linearity Measurements

- Response linearity to dose per spill of 7, 11.5 and 18 Gy
- Repeated multiple times across the three experiment days
- Excellent linearity ($R^2 > 0.999$)
- Light output decrease with accumulation of dose



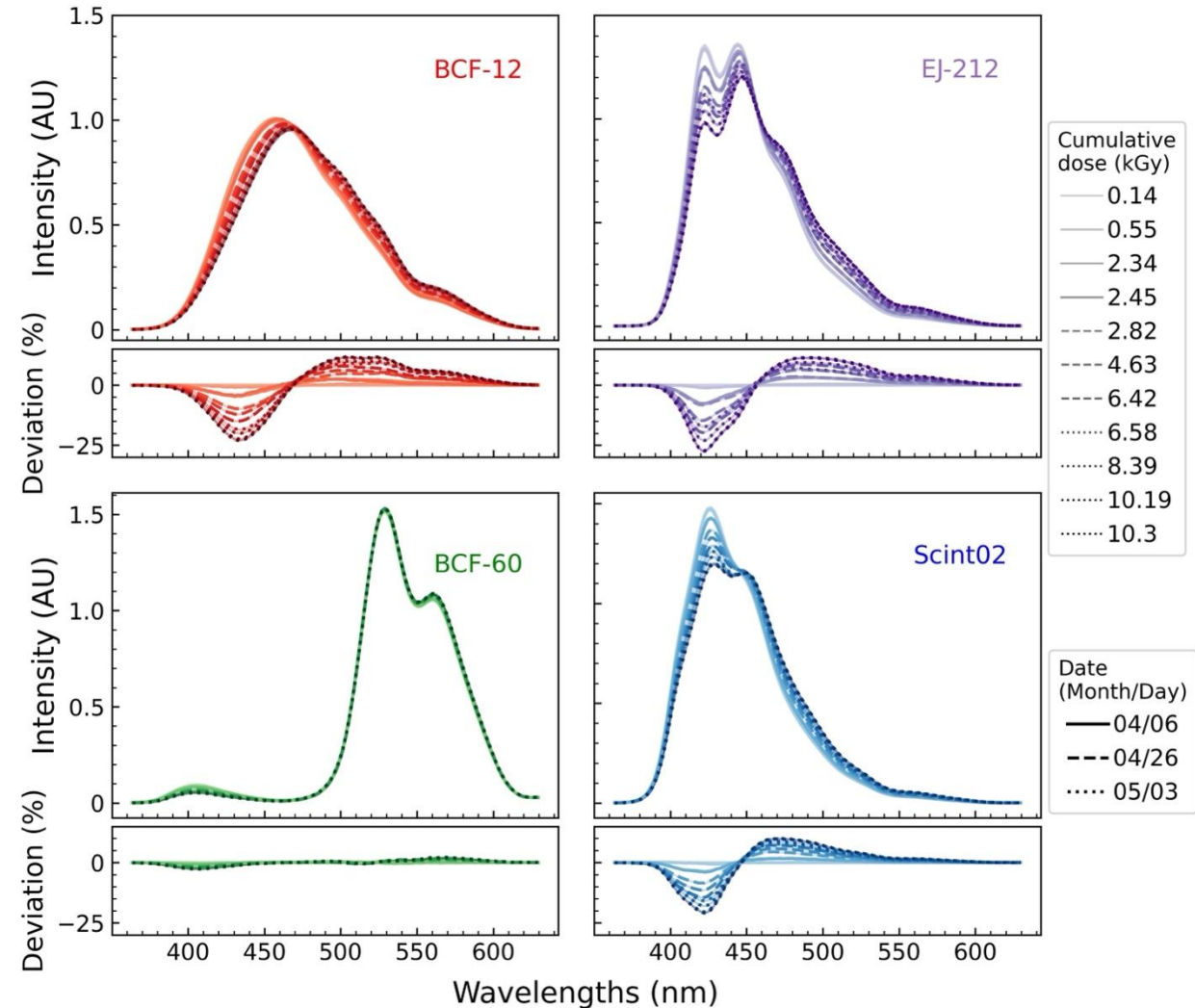
Protons High Dose Irradiations

- Five ~1680 Gy irradiations
 - Delivered in spills of ~18 Gy, sent out every 2 s (~3 min total)
- Important decreases in this short time



Protons Spectral changes

- Spectra measured at spills of ~ 11.5 Gy, normalized by area under the curve (AUC)
- Shift towards longer yellow/orange wavelengths
- Decrease of light emission preferentially in the 380-500 nm region (blue)

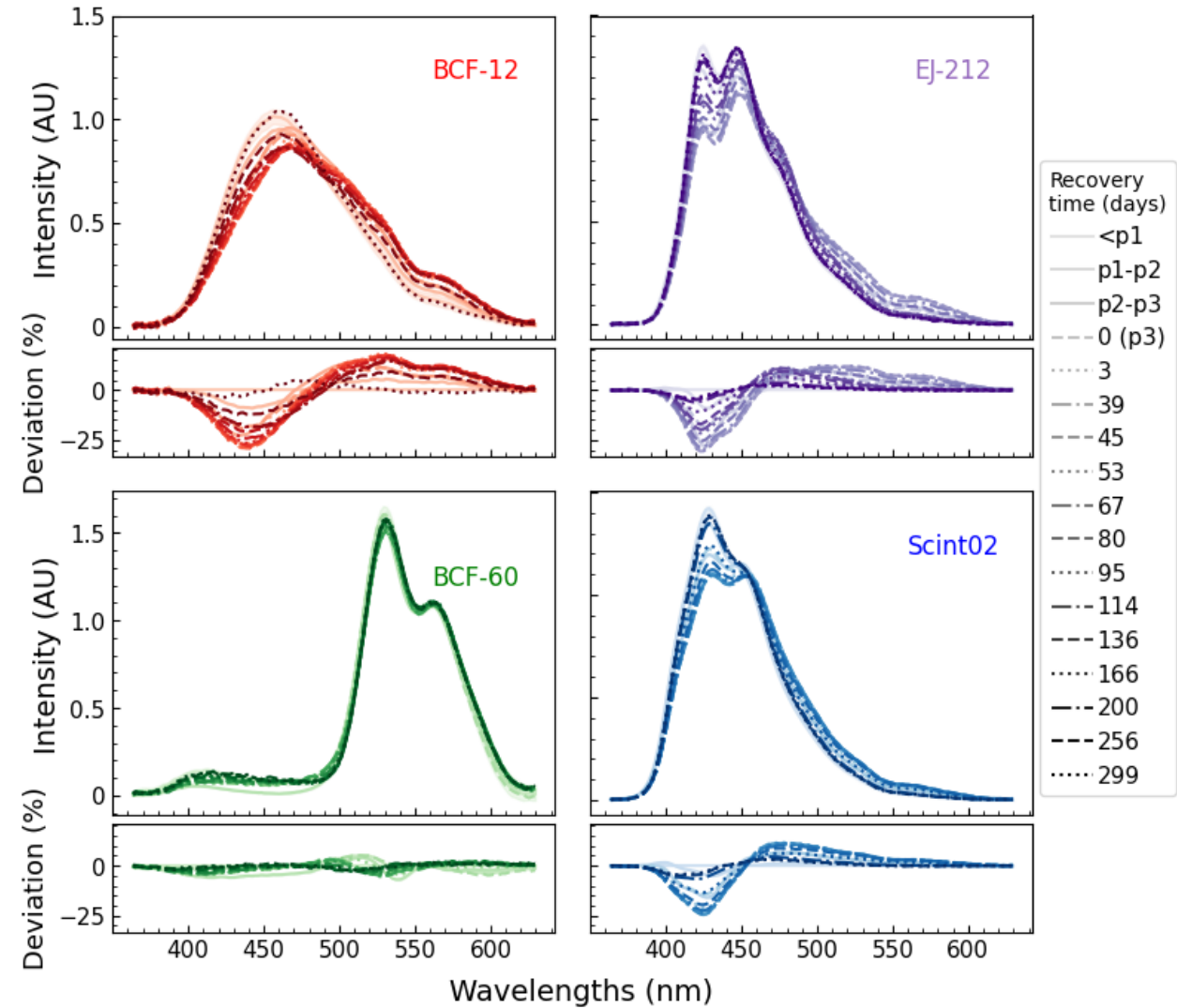


Long-term Recovery

Spectral recovery

- Slow (> 100 days) process
- Near complete recovery for Scint02 and EJ-212 (will continue tracking)

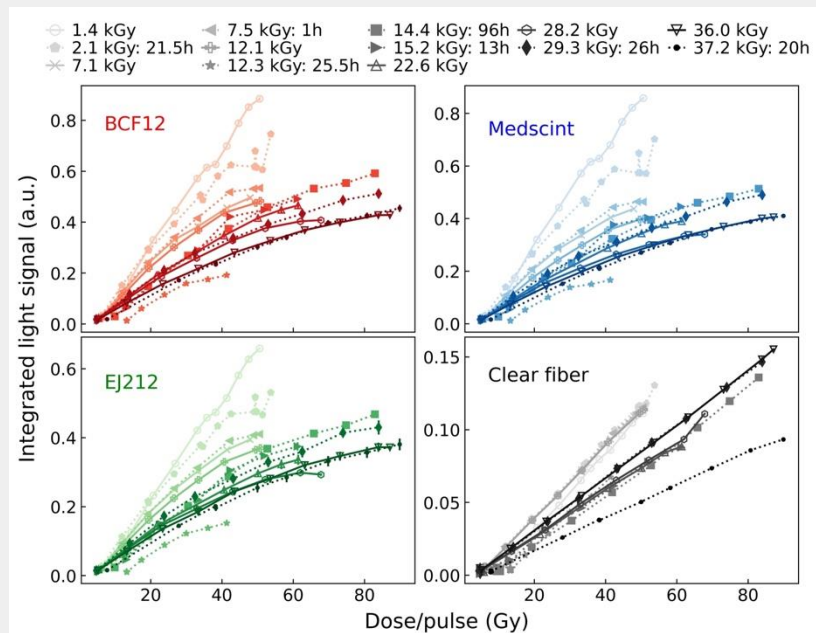
< p1: before 1st proton experiment
p1-p2: between proton experiments 1 and 2
p2-p3: between proton experiments 2 and 3



PSDs in FLASH VHEEs

Main takeaways:

- Blank fiber linear over whole dose range
- Scintillators lose linearity at ~45 Gy/pulse



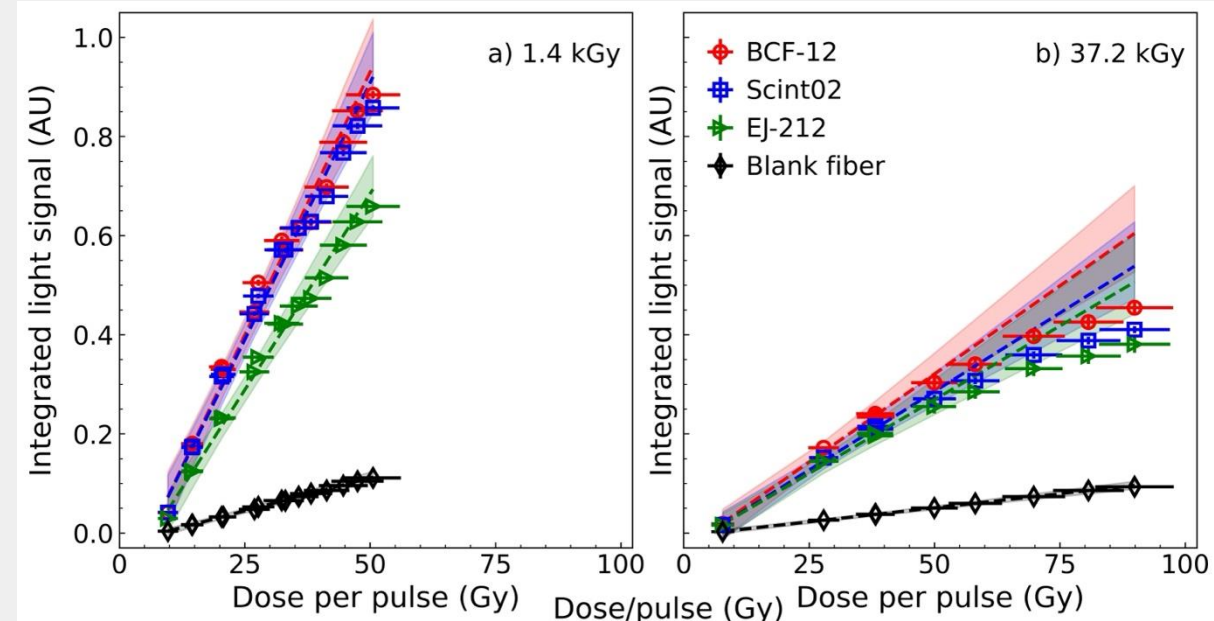
PAPER • OPEN ACCESS

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Published 27 March 2025 •   2025 The Author(s). Published on behalf of Institute of Physics and Engineering in Medicine by IOP Publishing Ltd

[Physics in Medicine & Biology](#), Volume 70, Number 7



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- Radiation damage causes decrease of light output ($\leq 1.87\%/kGy$) and shift of spectra towards yellow

		BCF-12	Medscint	EJ-212	Blank fiber
Output (%)	Last irradiation (± 0.2)	33.4	30.4	37.8	42.7
	Recovery ^a (± 2)	85	78	94	89
Centroid shift (nm)	Last irradiation (± 1)	18	25	38	7
	Recovery ^a (± 1)	2	3	5	2

^a Recovery values are mean values measured after stabilization of response.

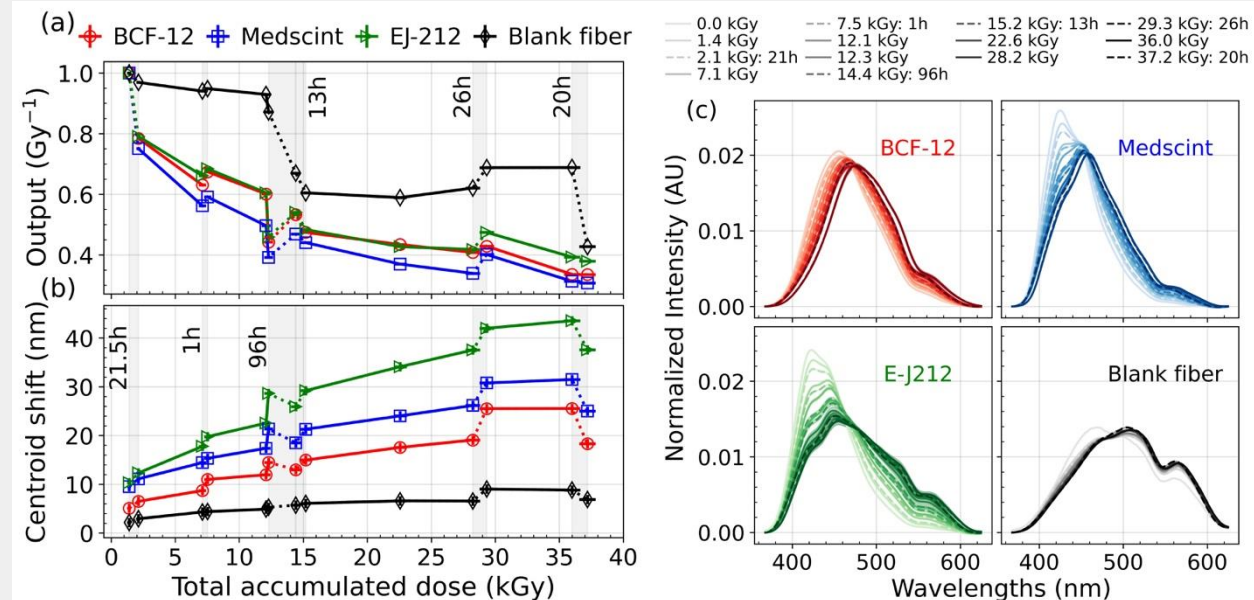
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PSDs in FLASH VHEEs

Main takeaways:

- Blank fiber linear over whole dose range
- Scintillators lose linearity at ~45 Gy/pulse
- Radiation damage causes decrease of light output ($\leq 1.87\%/kGy$) and shift of spectra towards yellow
- Short-term (<100h) recovery observed
- Long-term (<172 days) recovery observed with partial output recovery (6-22% damage remaining after stabilization) and complete spectral recovery

		BCF-12	Medscint	EJ-212	Blank fiber
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	Recovery ^a (± 1)	2	3	5	2

^a Recovery values are mean values measured after stabilization of response.

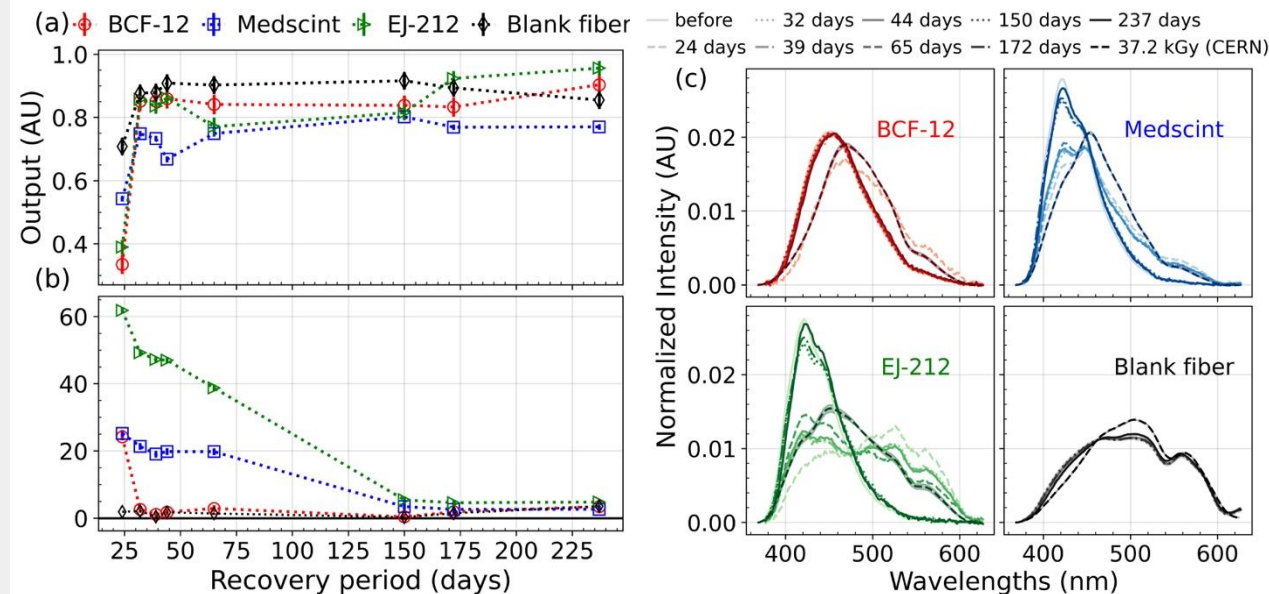
PAPER • OPEN ACCESS

Radiation damage and recovery of plastic scintillators under ultra-high dose rate 200 MeV electrons at CERN CLEAR facility

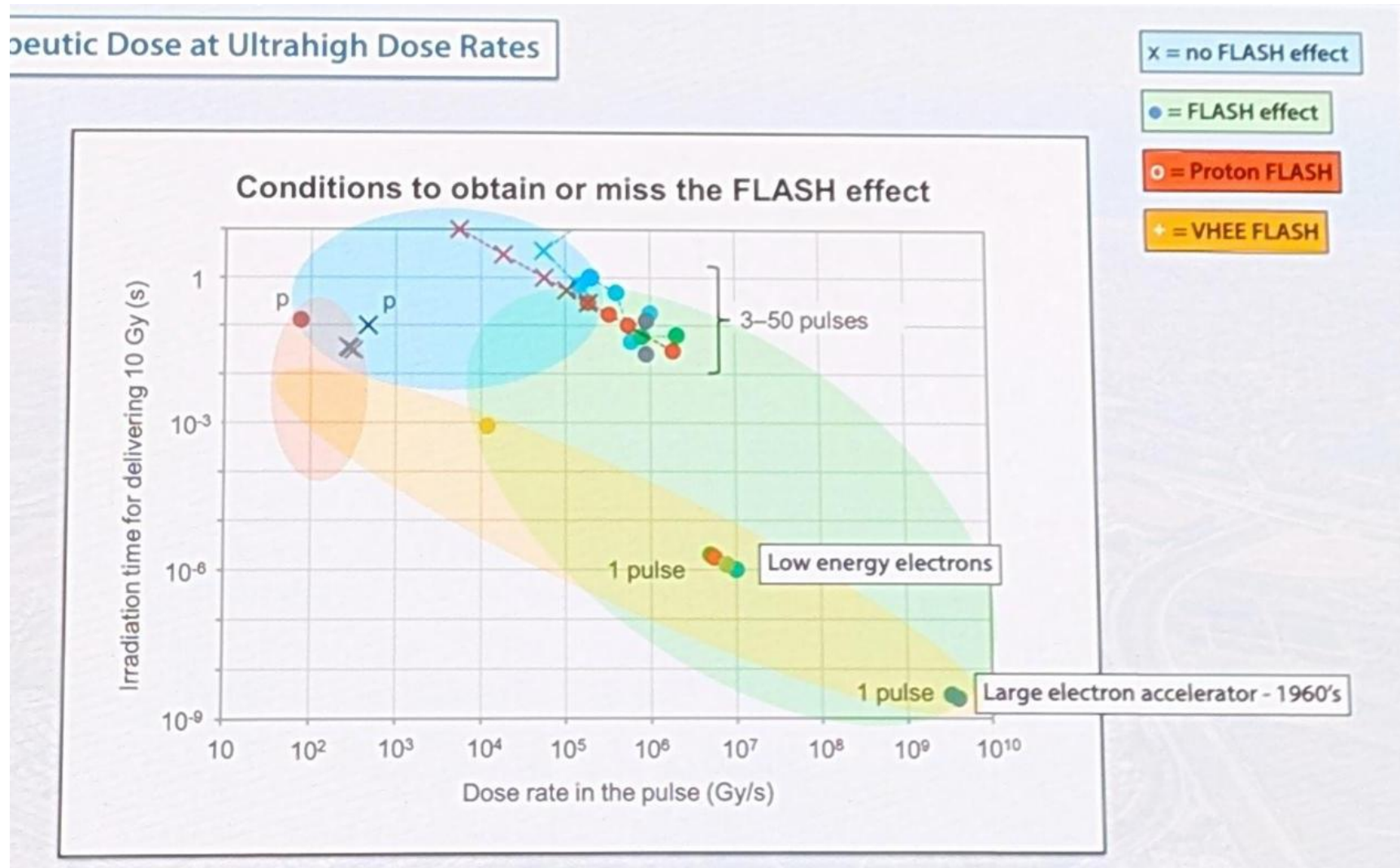
Cloé Giguère, Alexander Hart, Joseph Bateman, Pierre Korysko, Wilfrid Farabolini, Yoan LeChasseur, Magdalena Bazalova-Carter* and Luc Beaulieu

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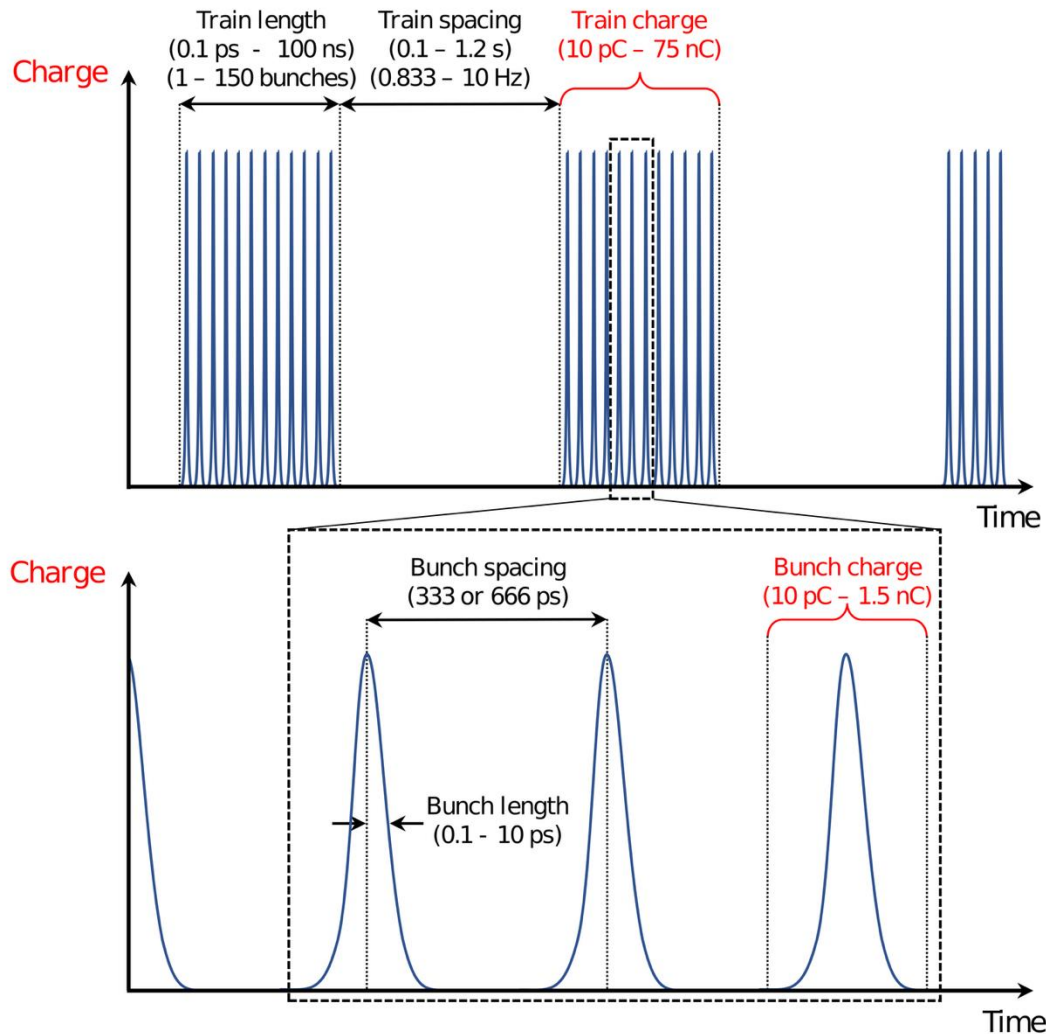
[Physics in Medicine & Biology](#), Volume 70, Number 7



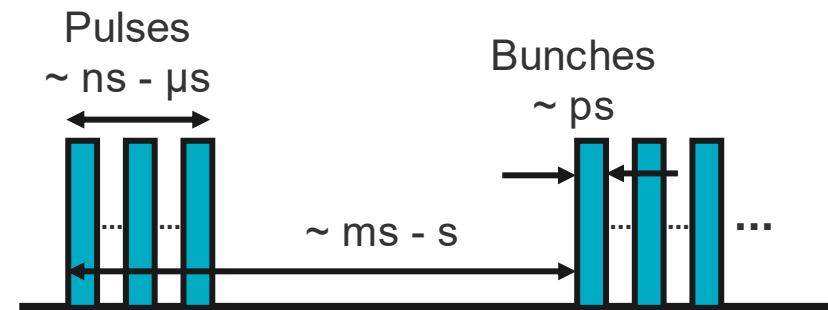
Conditions for FLASH



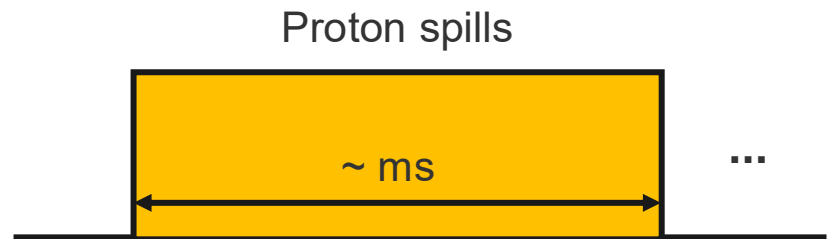
Beam Time structure



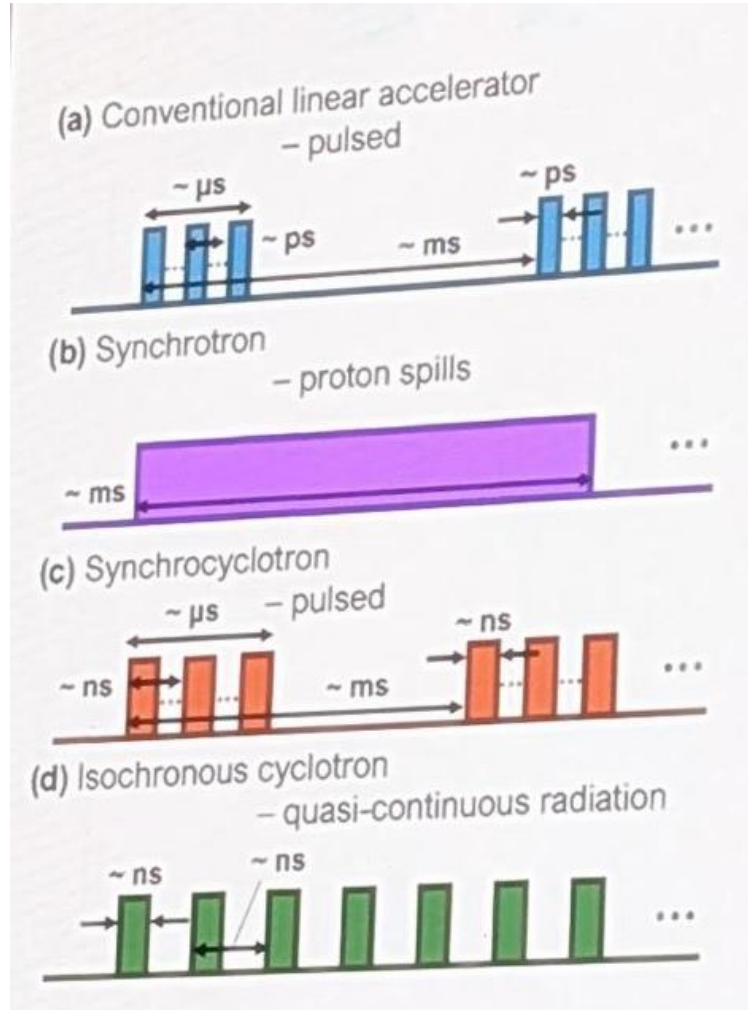
a) Pulsed linear accelerator (CLEAR & Mobetron)



b) Synchrotron

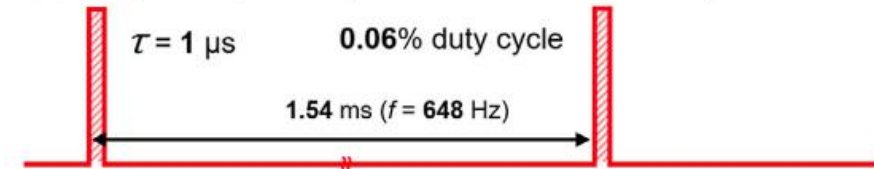


Beam Structure

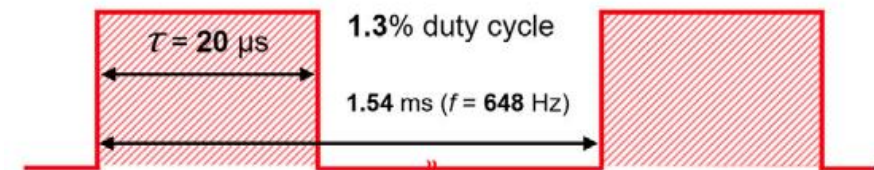


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(a) Synchrocyclotron (low-intermediate dose rate)



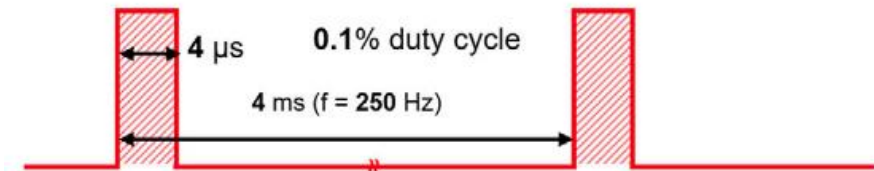
(b) Synchrocyclotron (FLASH dose rate)



(c) Continuous radiation (radioactive source) 100% duty cycle



(d) Linac



(e) Isochronous cyclotron (quasi-continuous radiation)

($f = 72.8 \text{ MHz}$, 2nd Harmonic)

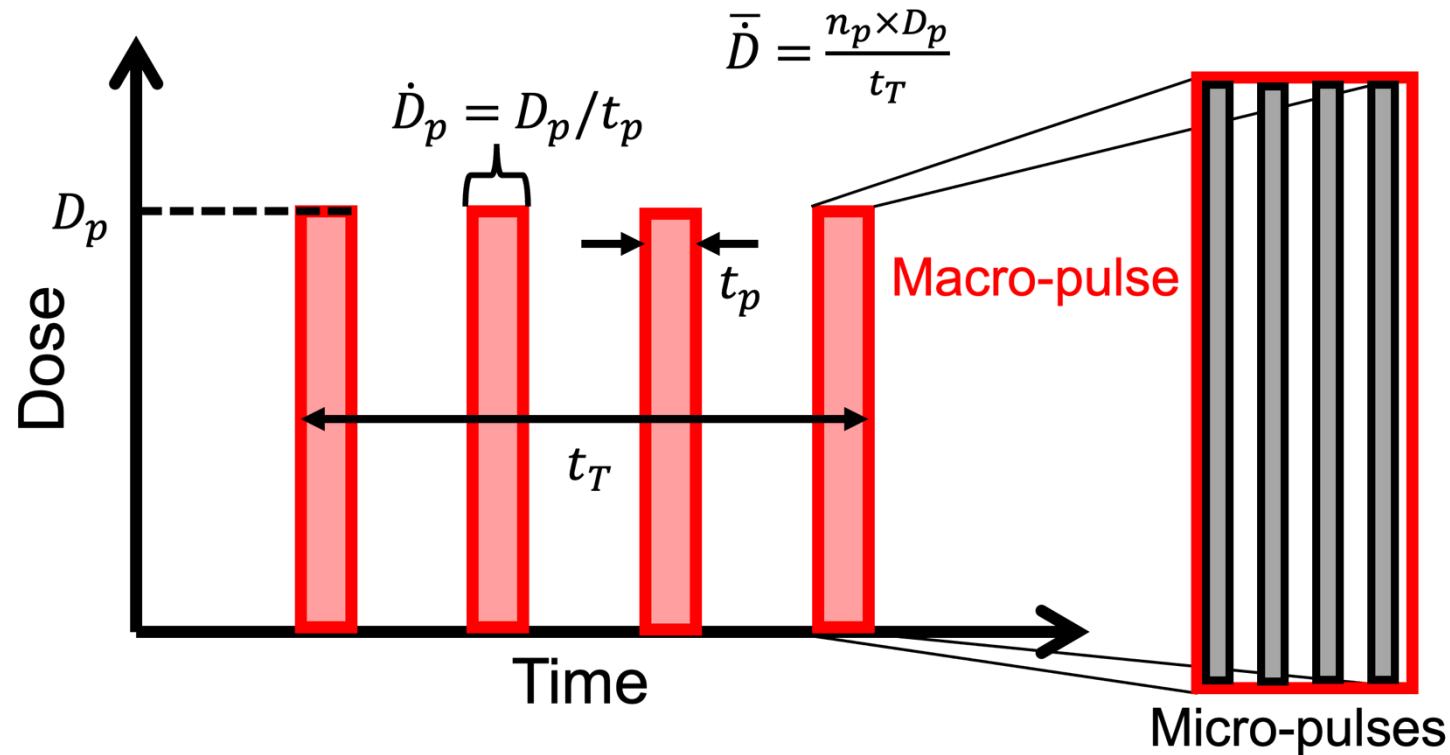


Beam Parameters in UHDR

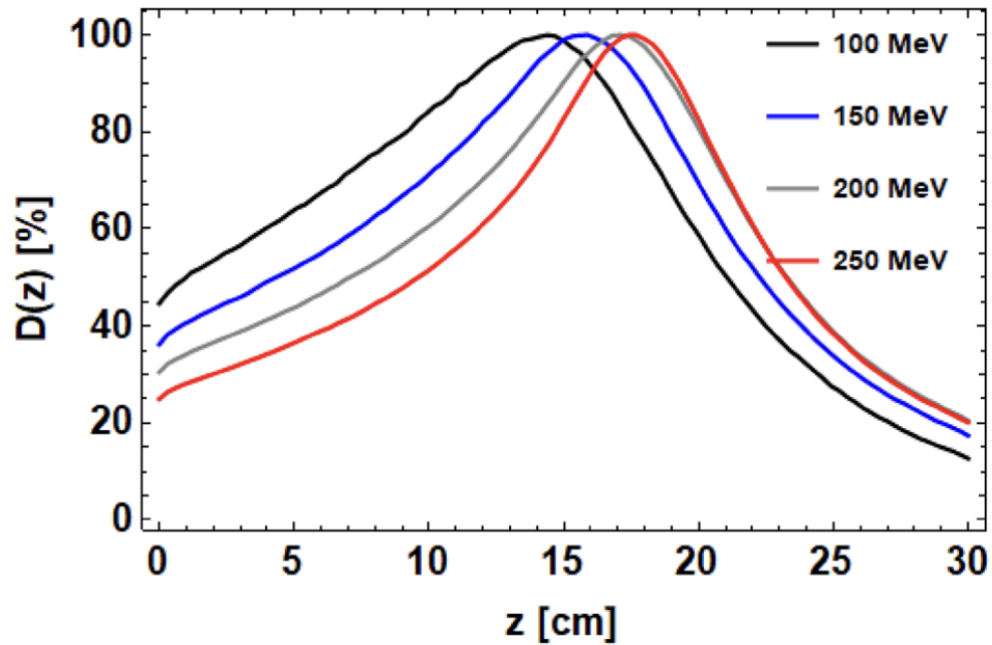
$\bar{D}$: Average dose rate (DR) D_p : Dose per pulse

$\dot{D}_p$: Instantaneous DR t_p : Pulse duration

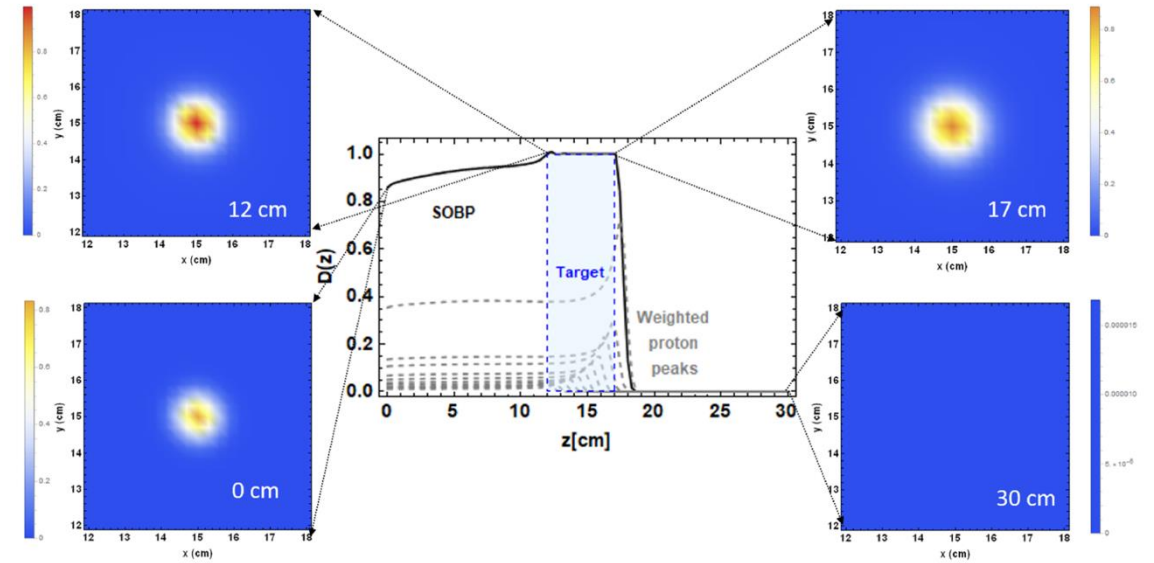
n_p : # of pulses t_T : Total treatment time



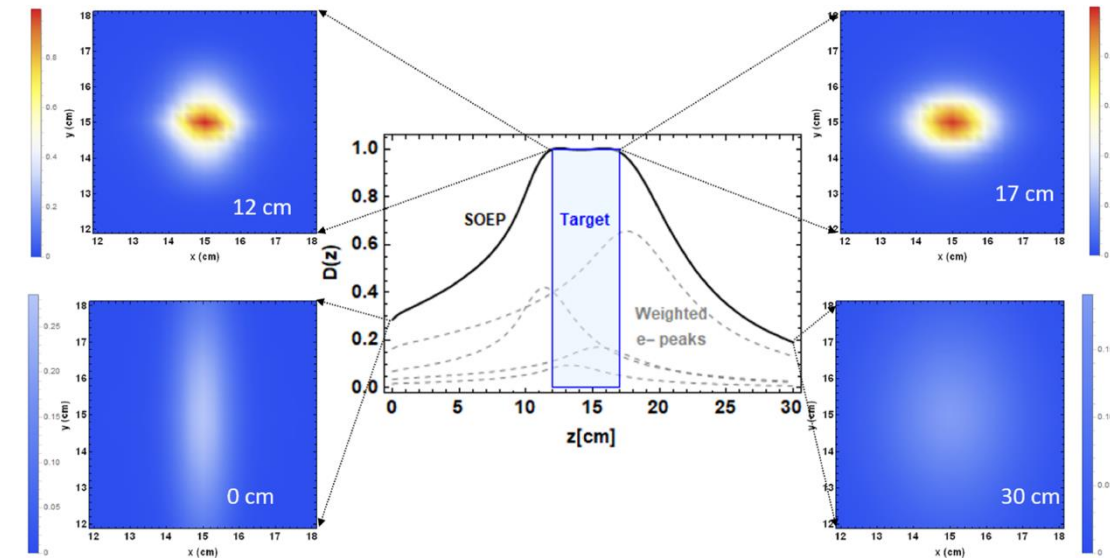
Focused VHEEs VS protons



TOPAS-based Monte Carlo simulations of the on-axis dose plots for 100, 150, 200 and 250 MeV asymmetrically focused VHEE beams in water. Differences in focusing is due to the increasing penetration power and reduced scattering of VHEE with beam energy.



(a) SOBP with 11 contributing proton peaks, with the transverse dose at entrance, 12 cm, 17 cm and exit of phantom shown.



(b) SOEP with 4 contributing electron peaks, with the transverse dose at entrance, 12 cm, 17 cm and exit of phantom shown.

Inhomogeneities VHEE VS protons

