

# A cavity-enhanced hydrated electron sensor for real-time, tissue-equivalent measurement of individual clinical radiation pulses



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**What?** Develop an *in vivo* water-based radiation dosimeter as tiny as a human hair

For conventional and ultrahigh dose rate EBRT

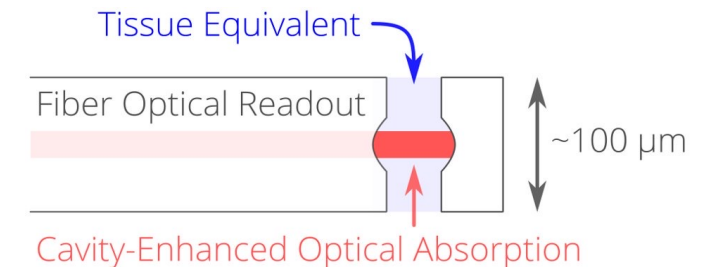
**Why?** Use quantum optics skills to address dosimetry limitations



Measuring the reference quantity for radiotherapy D<sub>w</sub>:

- 10 cm long ionization chamber
- Ionization current
- Average dose in the air cavity
- **Dose in water in one point**

- Micron-scale optical fiber cavity
- Tissue equivalent (water) detection
- Real-time sub-mGy readout
- *In situ* dosimetry

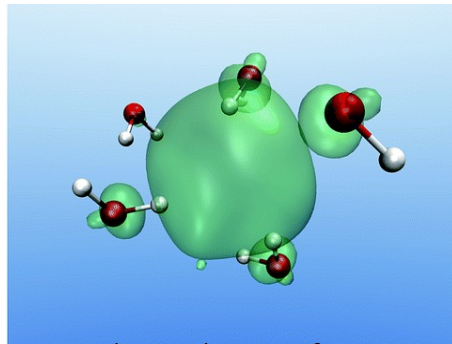


**How?** Monitor the concentration of hydrated electrons ( $e^-_{aq}$ ) using cavity-enhanced absorption spectroscopy

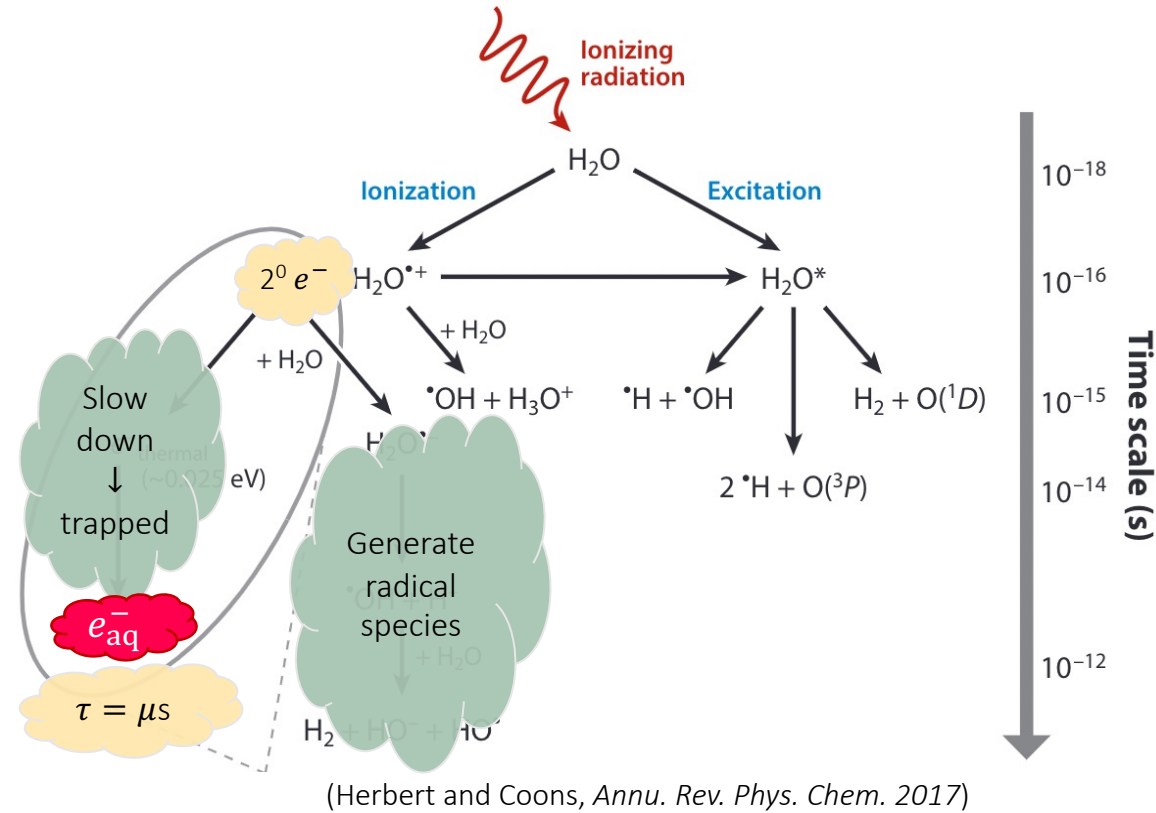
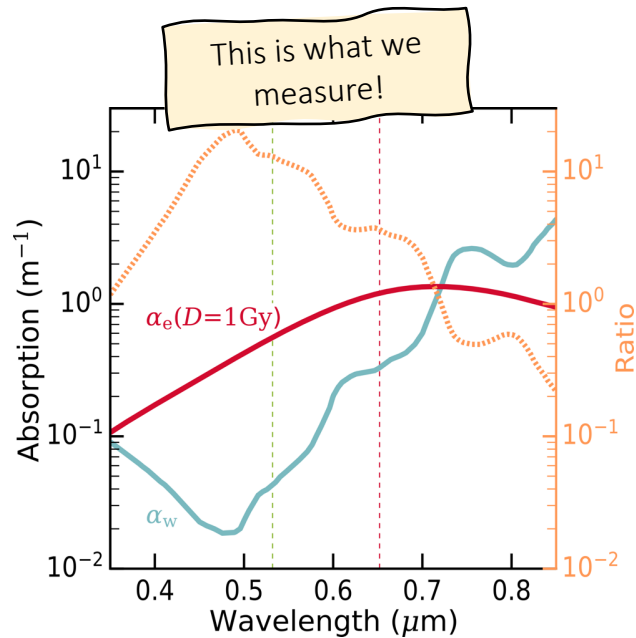
# A cavity-enhanced hydrated electron sensor for real-time, tissue-equivalent measurement of individual clinical radiation pulses



**How?** Determine dose by monitoring the concentration of **hydrated electrons ( $e^-_{aq}$ )** using fast cavity-enhanced absorption spectroscopy



Charge density of  $e^-_{aq}$ .  
(Pizzochero *et al.*, 2019)



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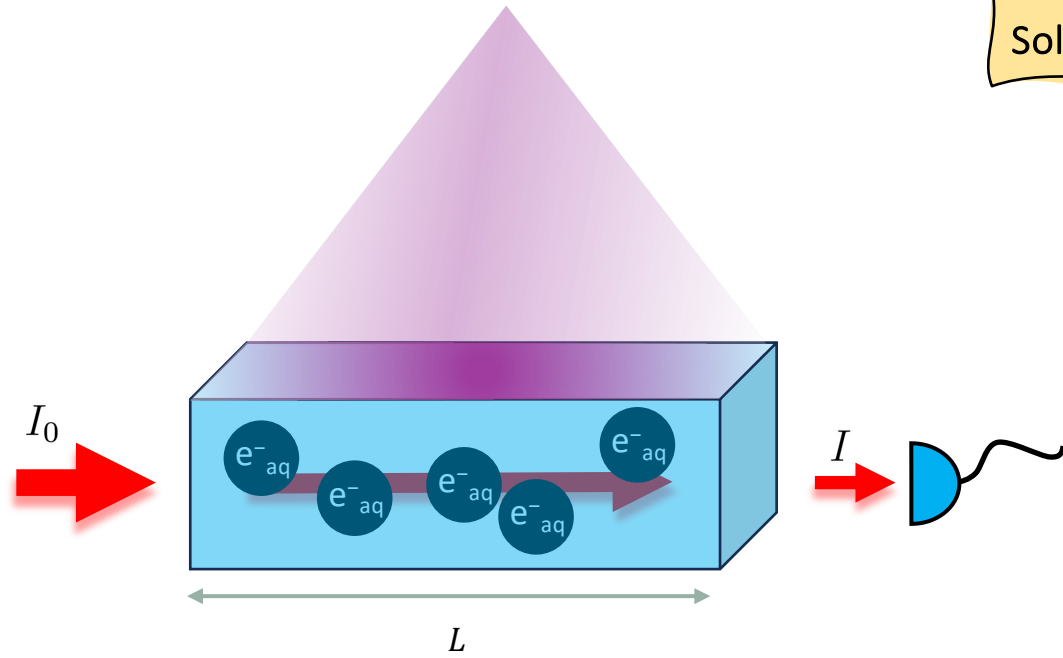


How? Determine dose by monitoring the concentration of **hydrated electrons ( $e^-_{aq}$ )** using fast cavity-enhanced absorption spectroscopy

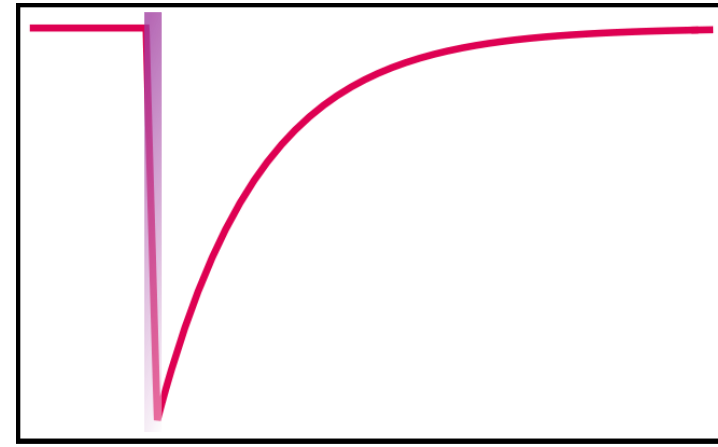
$$I = I_0 e^{-\alpha L}$$

$\alpha \propto \text{Dose}$

**Problem:** long optical path (or absurd pulse) is required for a detectable signal ( $\propto 1\text{m}$ )  
**Solution:** **optical cavity enhancement**



Super big, useless device



Absurd pulse

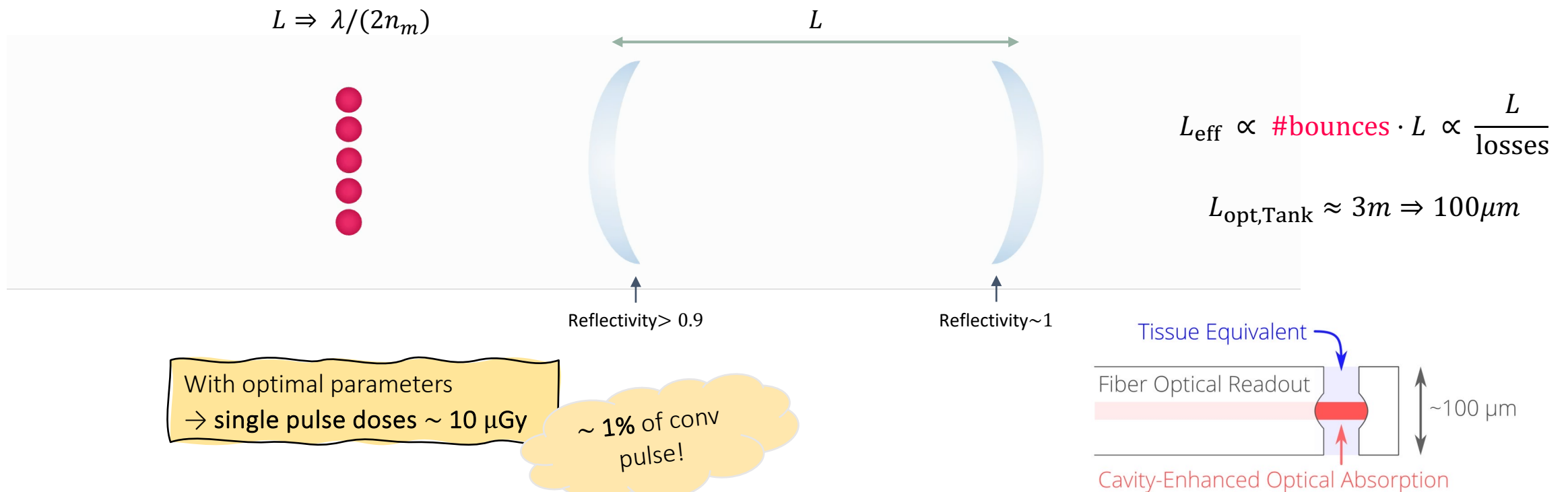
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How? Determine dose by monitoring the concentration of **hydrated electrons ( $e^-_{aq}$ )** using fast **cavity-enhanced absorption spectroscopy**

## Optical cavity:

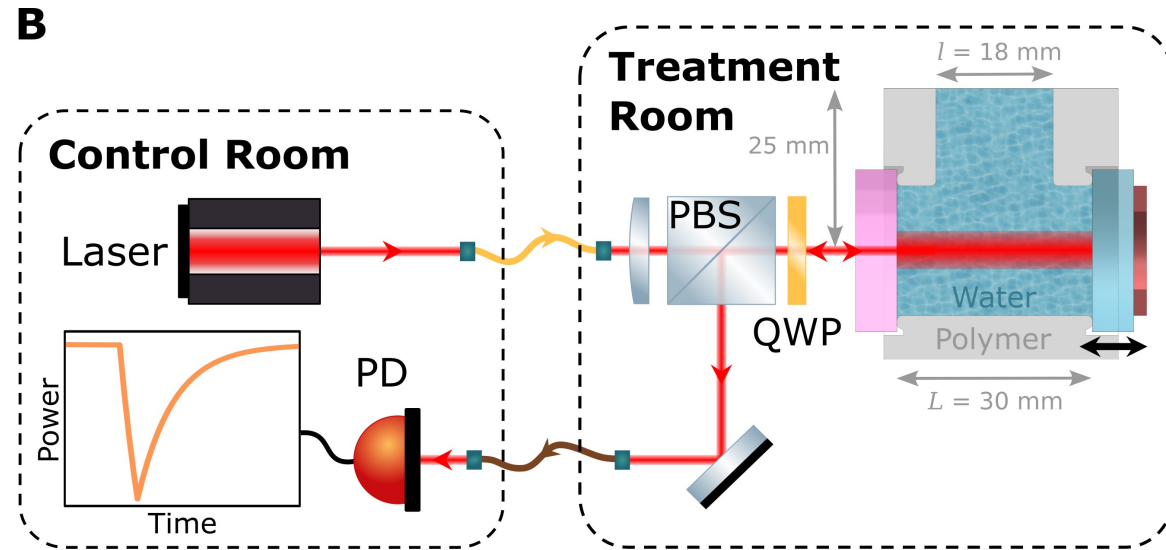
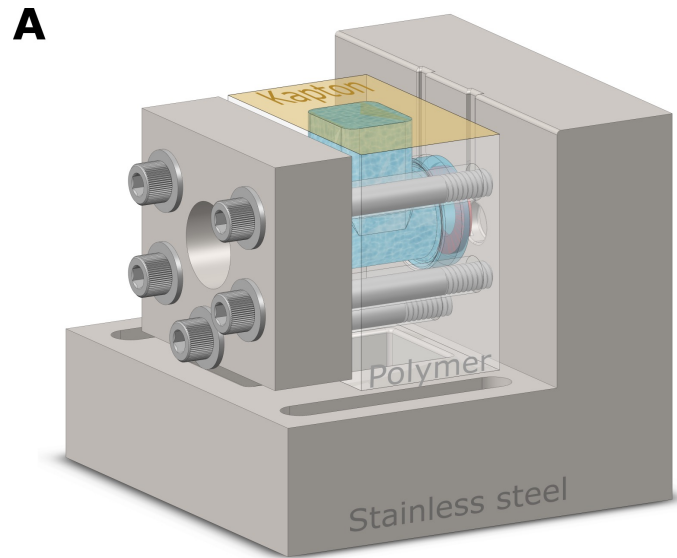
“Folds” meter-long paths to sub-millimeter  $\rightarrow$  enhances interaction with sample  
Small sensor sensitive to tiny absorption signals



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Currently: performing tests in a 3-cm proof-of-concept cavity → CONV photon & e<sup>-</sup> therapy



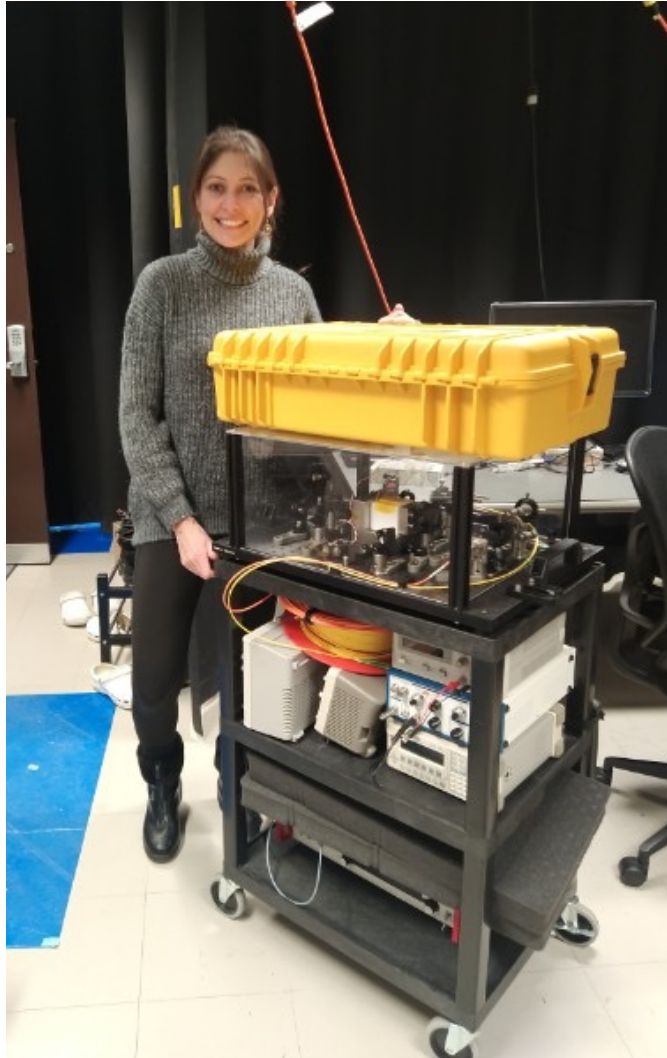
$L = 3 \text{ cm}$   
 $L_{\text{eff}} \approx 1.3 \text{ m}$

Resonance condition kept with a Pound-Drever-Hall locking scheme feeding back to a piezo transducer on the back mirror

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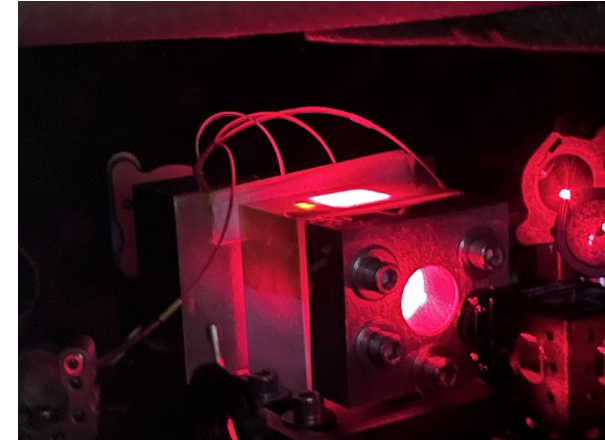
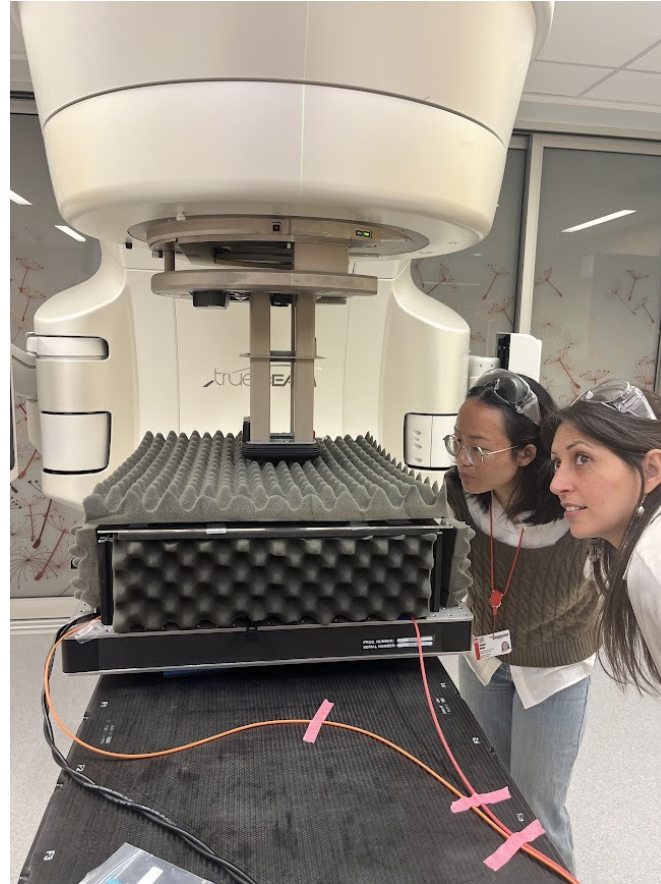
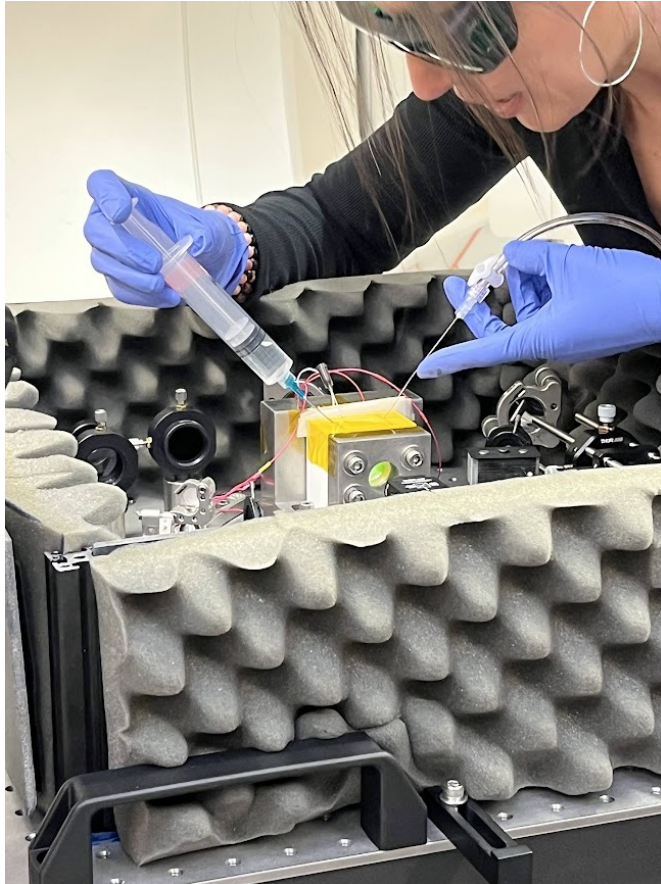
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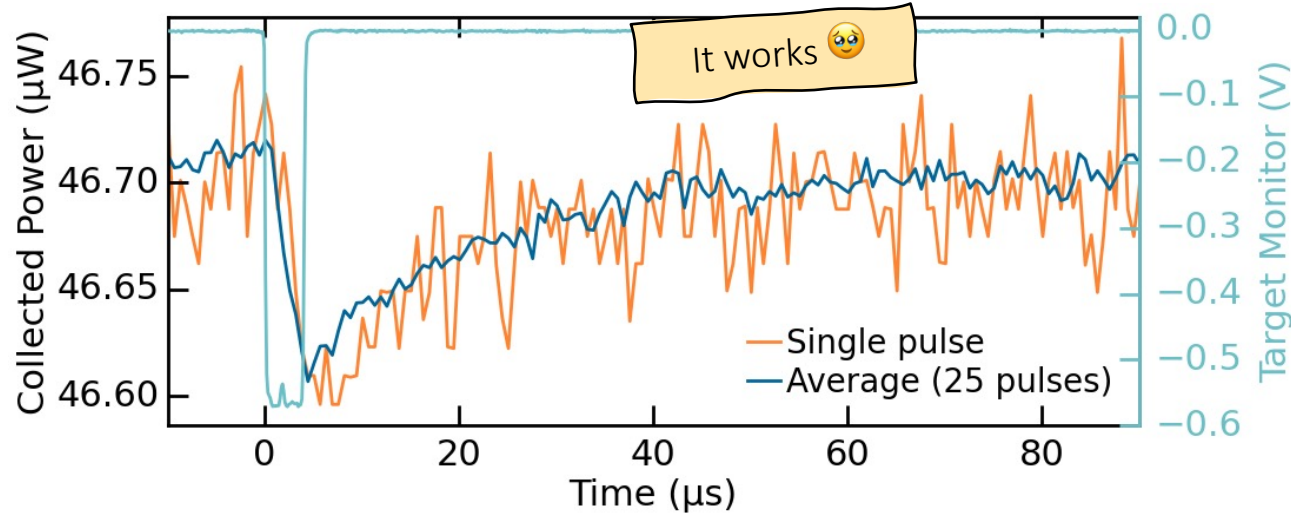
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$$P_{out} \approx P_{in} (\eta R + 1 - \eta)$$

$$R \approx \left( \frac{\mathcal{L}_0 + \mathcal{L}_{rad}(t) - T_1}{\mathcal{L}_0 + \mathcal{L}_{rad}(t) + T_1} \right)^2$$

$$\mathcal{L}_{rad} = 2\alpha_e l$$

molar concentration [M=mol/L]

$$\alpha(t) = \ln(10) \underbrace{\varepsilon}_{\text{molar absorption coeff [1/(M}\cdot\text{m)]}} n_e(t)$$

molar absorption coeff [1/(M·m)]

$$\frac{dn_e}{dt} = \underbrace{\rho G_e d(t)}_{\text{creation}} - \underbrace{\frac{1}{\tau} n_e(t)}_{\text{decay}} \approx \rho G_e \frac{\mathcal{D}}{\Delta t} - \frac{1}{\tau} n_e(t)$$

Rate eq for  $e_{aq}^-$  number density

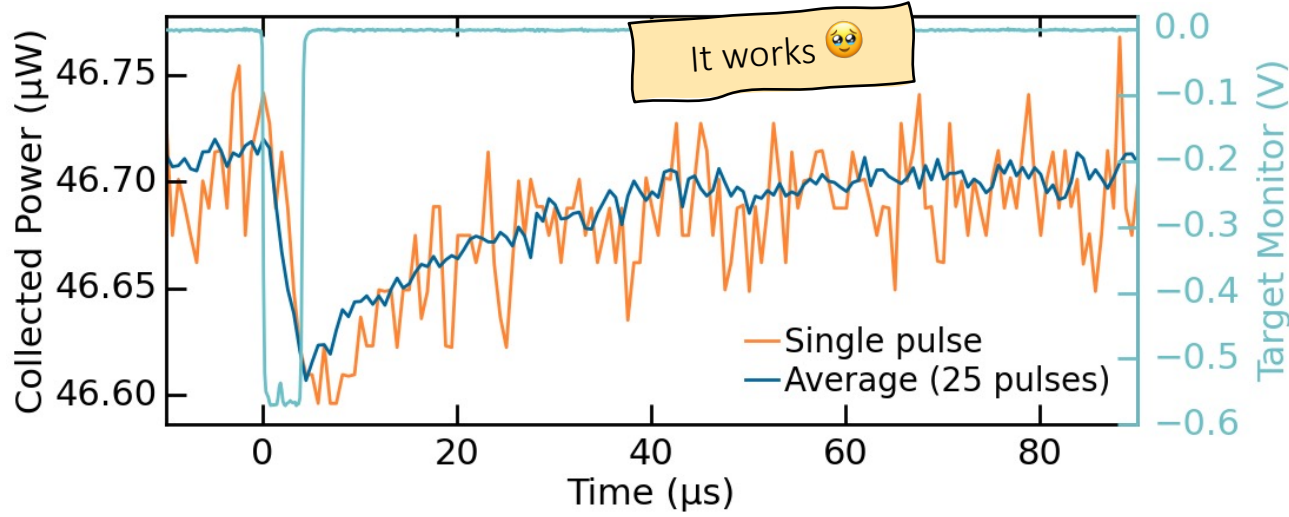
$$n_e(t) = \rho G_e \frac{\mathcal{D}}{\Delta t} \tau \begin{cases} 0 & t < 0 \\ 1 - e^{-t/\tau} & 0 \leq t \leq \Delta t \\ (e^{\Delta t/\tau} - 1) e^{-t/\tau} & t > \Delta t \end{cases}$$

Problem to solve: getting the value of the quantity from the instrument output

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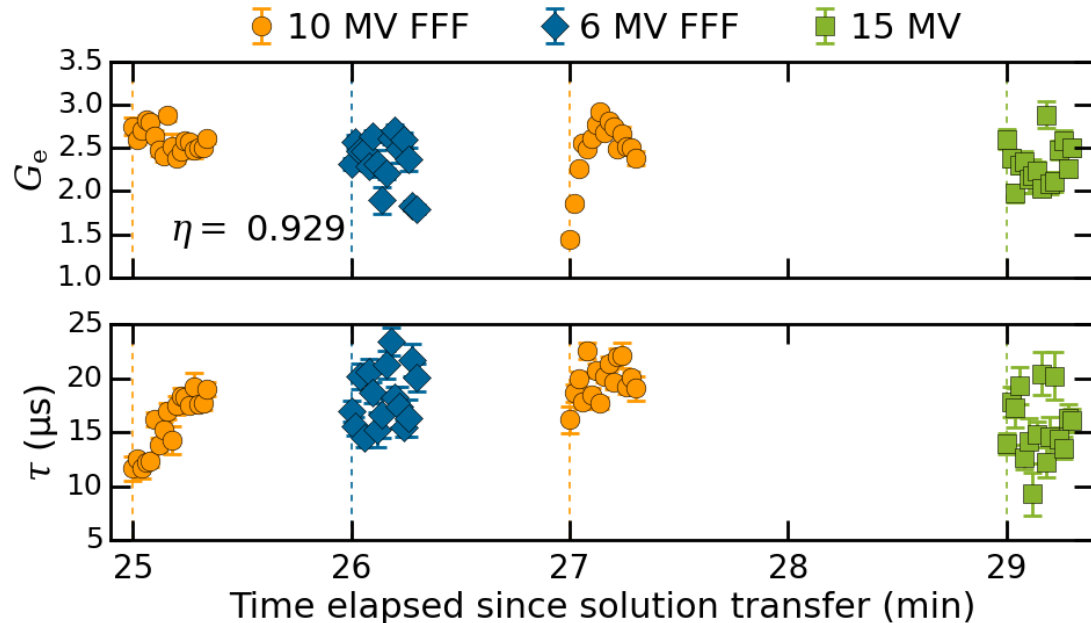
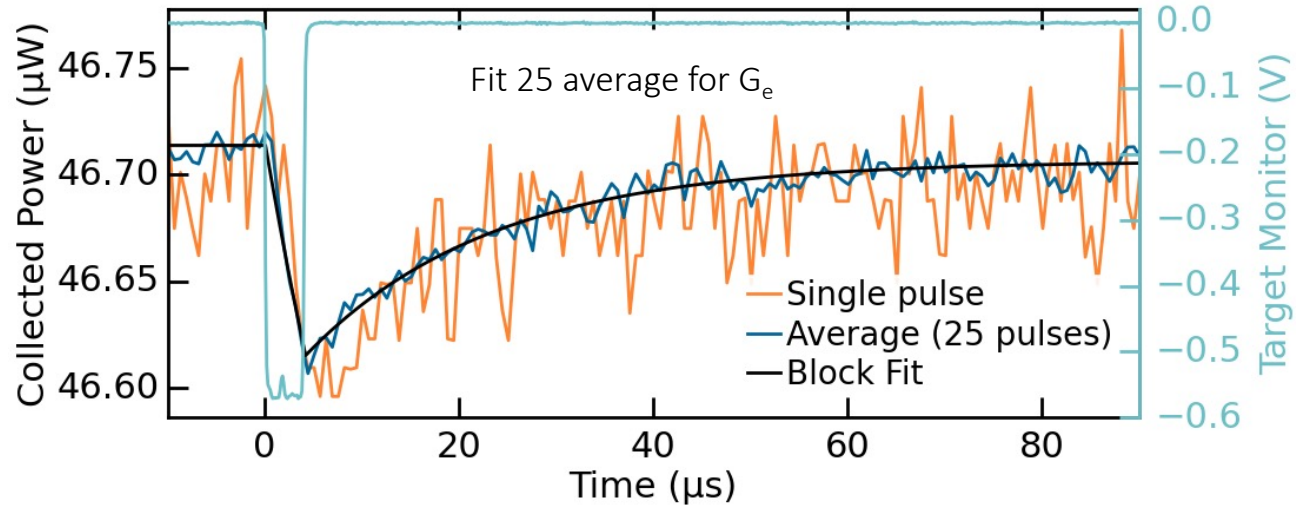
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# particles / radiation energy

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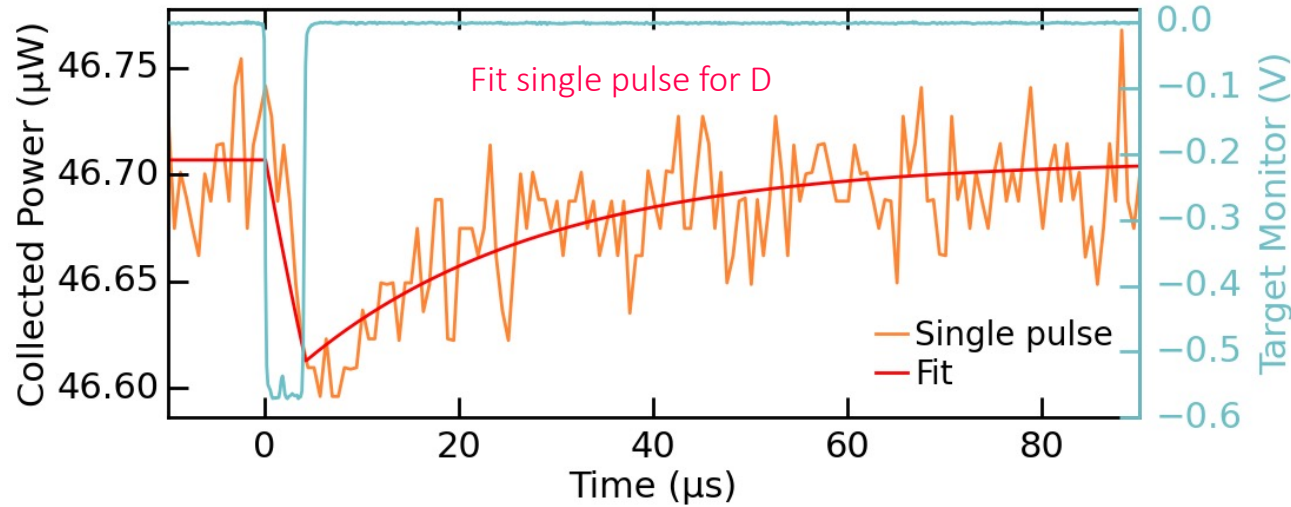


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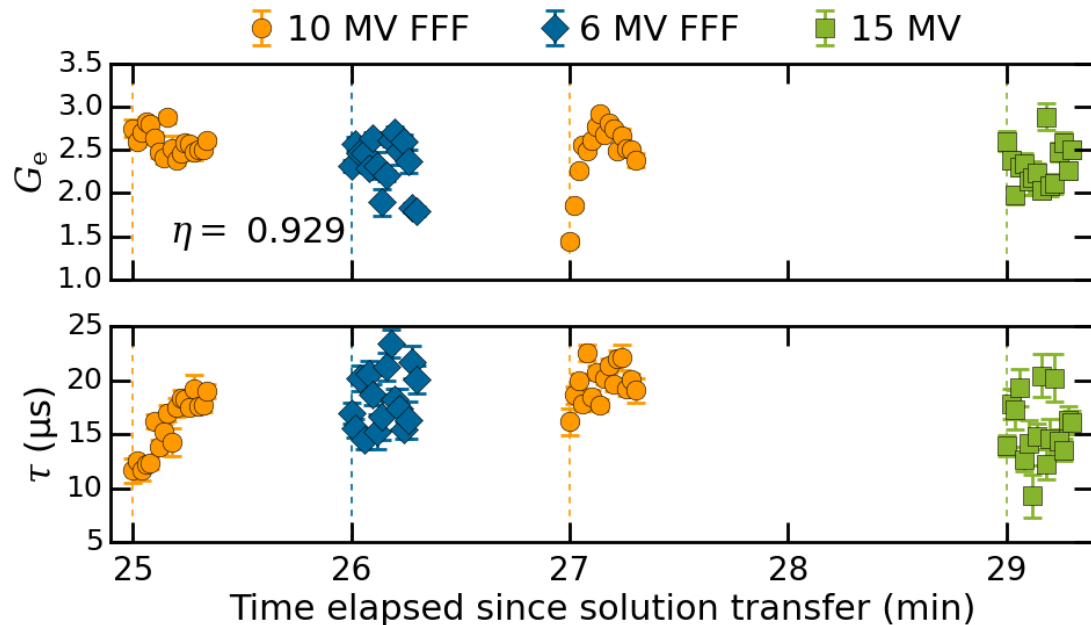
Min detectable  $D \approx 150 \mu\text{Gy}$

Pulse Dose  $\approx 2 \text{ mGy}$

Pulse length  $\approx 4 \mu\text{s}$

→ Instantaneous dose rate  $\approx 500 \text{ Gy/s}$

Beam size =  $2 \times 2 \text{ cm}^2$

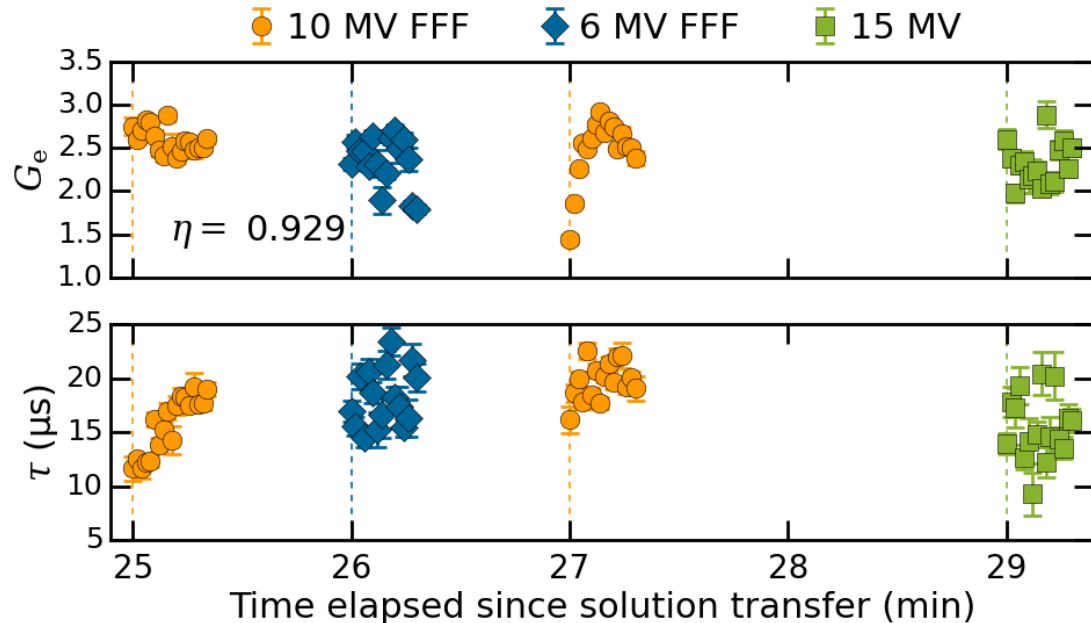
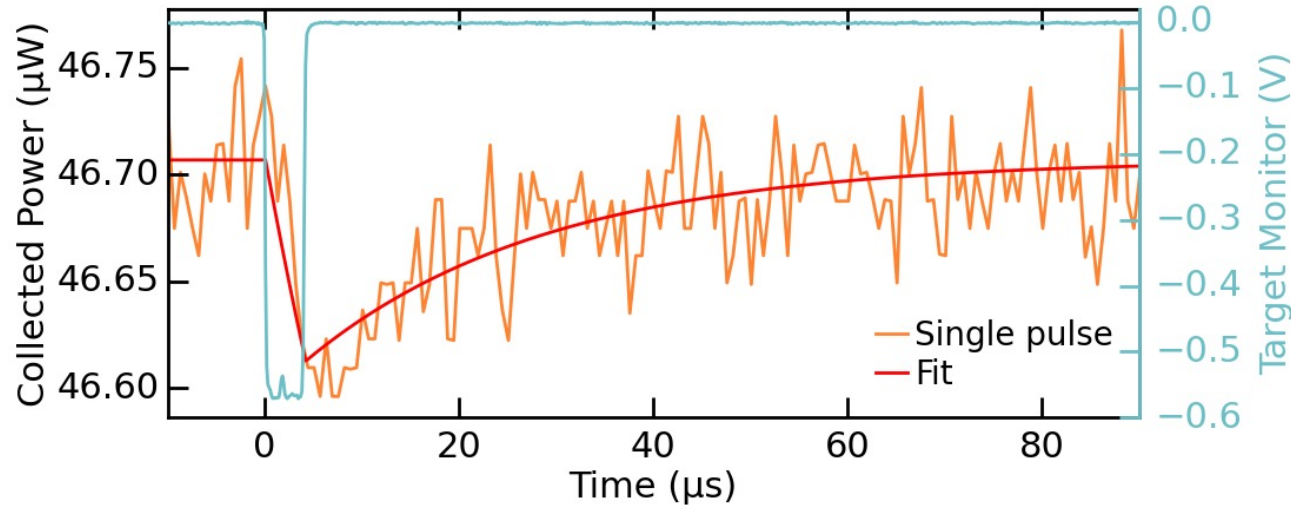


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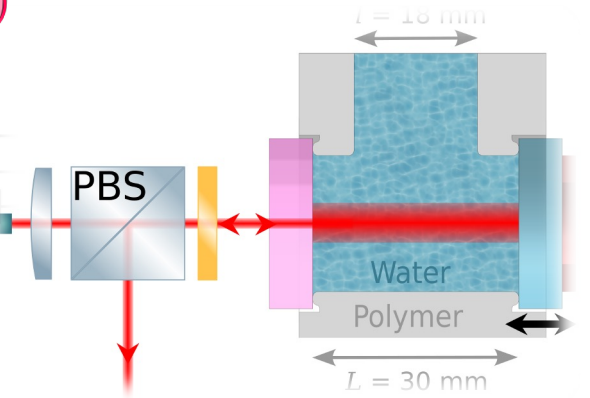
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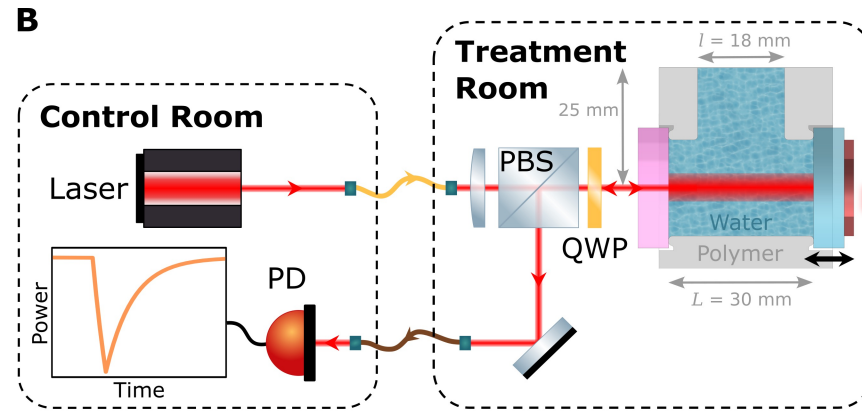
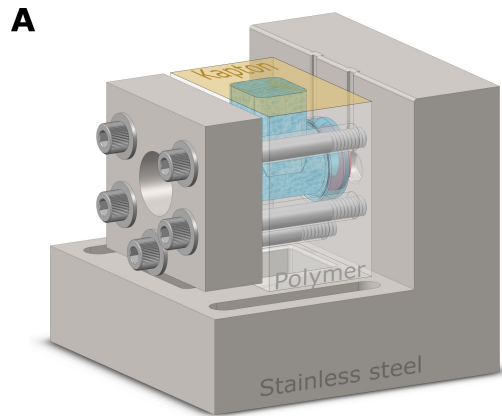
Drifts in mode coupling  $\eta$  due to thermal refractive-index variations

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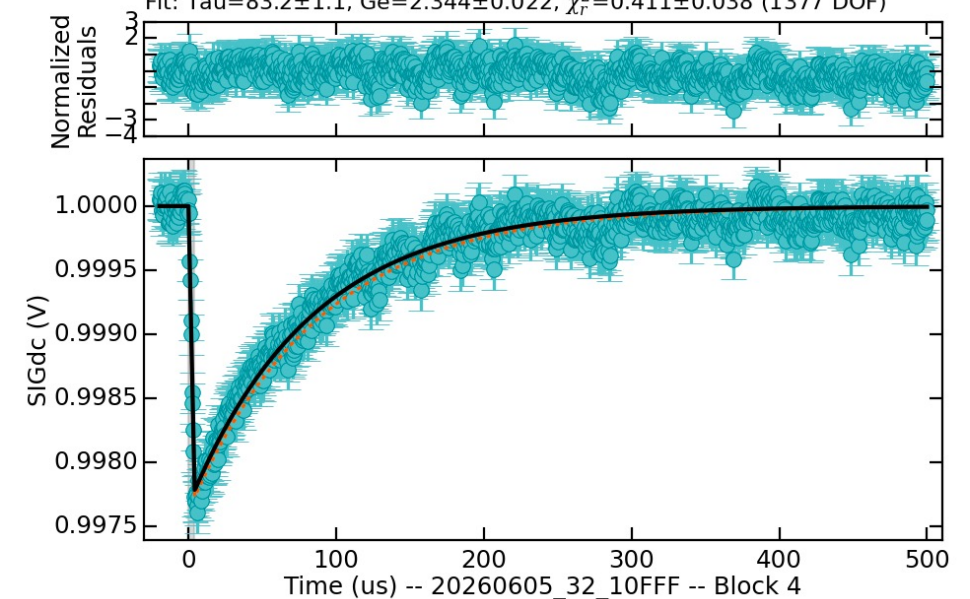
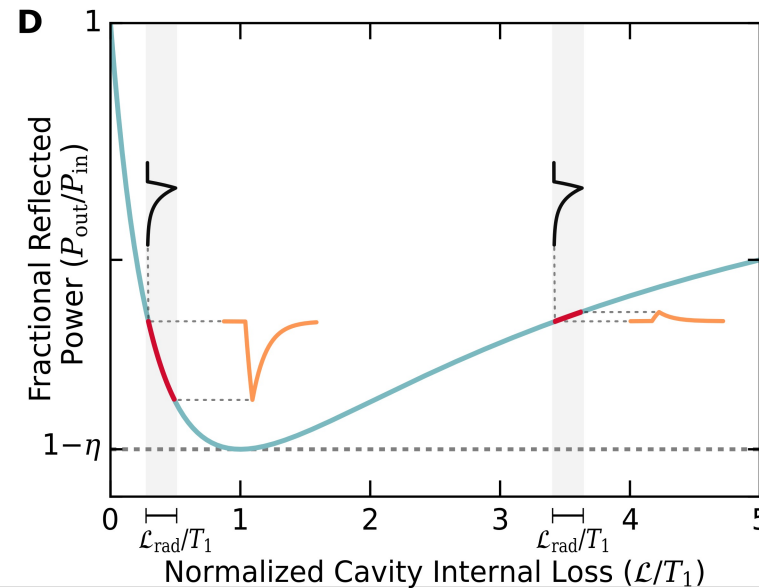
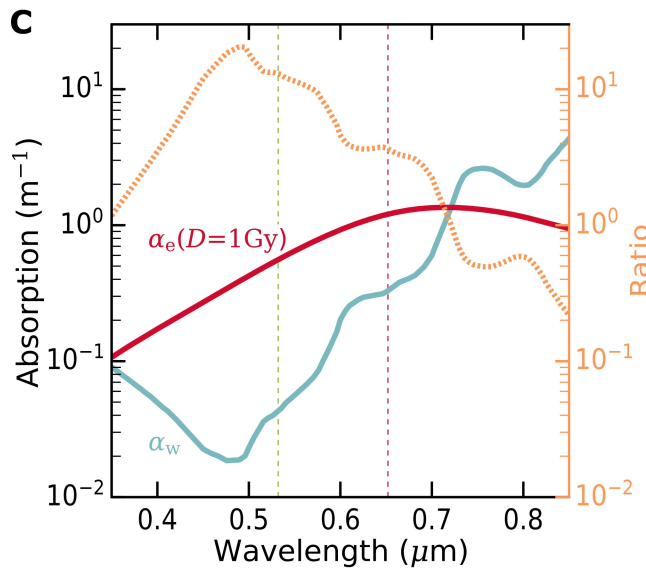


Solution: transmission measurement

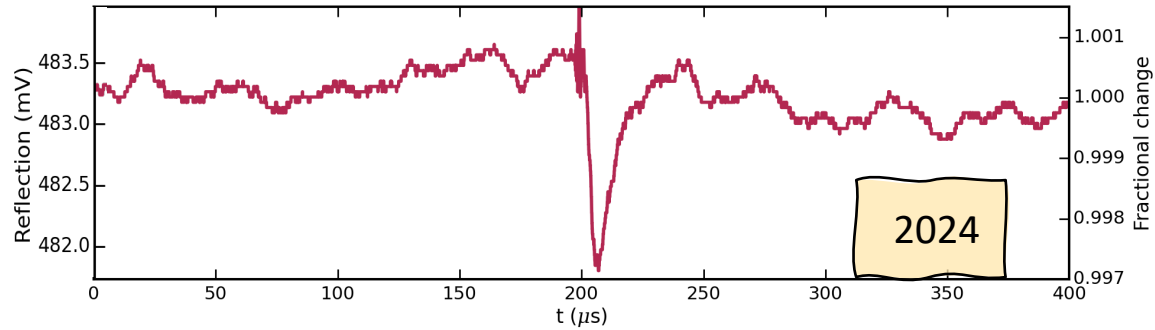


Collect T  
No interferences!

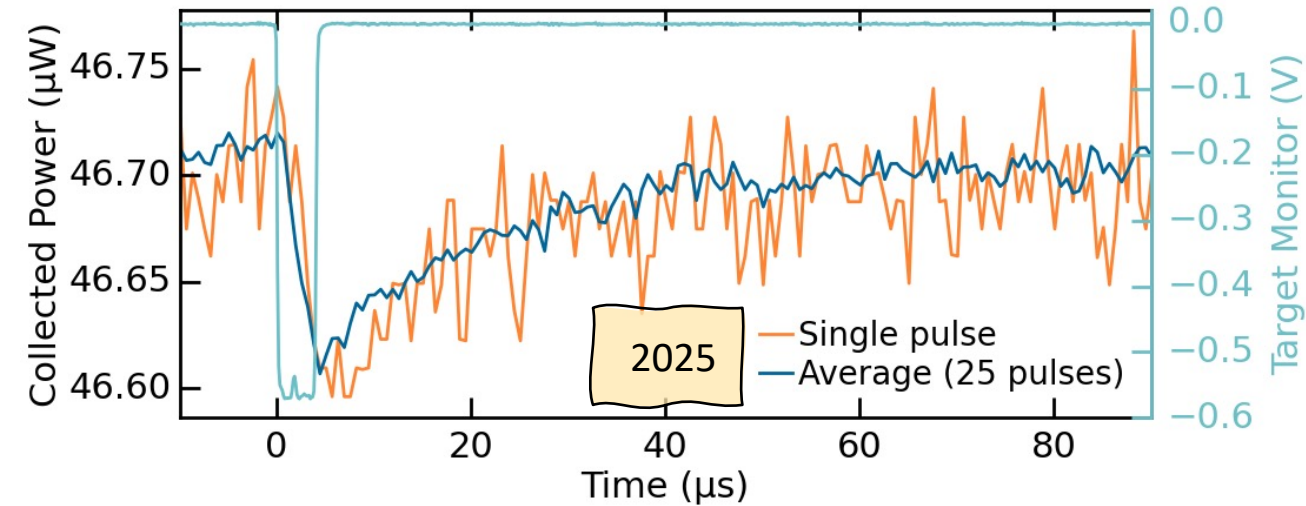
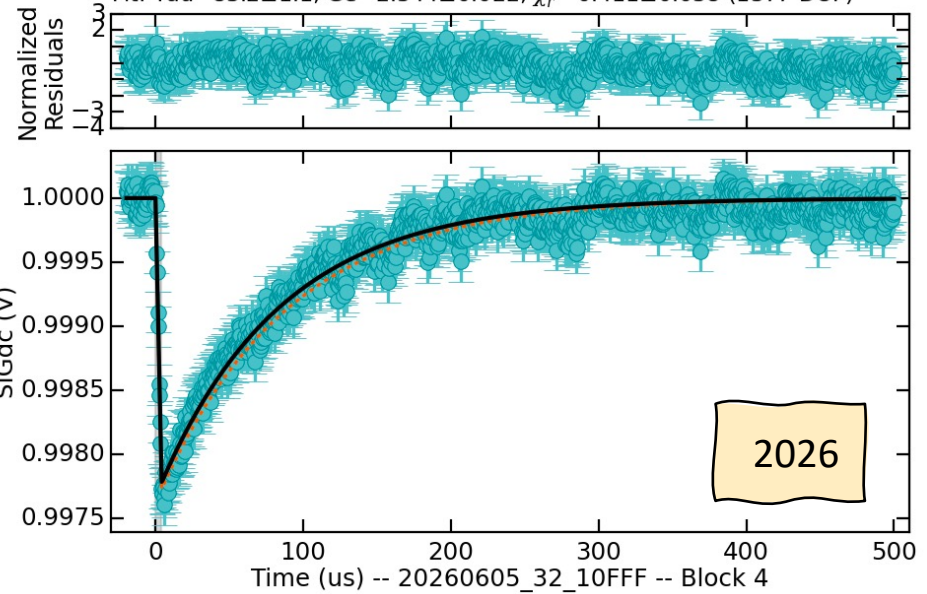
Function (0/0):  $y = \text{pulse}(x-t_0, dt\_rad, \text{Tau}, D, \text{Ge}, \text{GH}, T_1, L_0\_i, L_0\_f, l)$   
 Constants:  $t_0=0.018707$ ,  $dt\_rad=4.1625$ ,  $D=0.00208028$ ,  $T_1=0.0136$ ,  $l=0.015$ ,  
 $L_0\_i=0.04$ ,  $L_0\_f=0.04$ ,  $\text{GH}=0$   
 Fit:  $\text{Tau}=83.2 \pm 1.1$ ,  $\text{Ge}=2.344 \pm 0.022$ ,  $\chi^2_r=0.411 \pm 0.038$  (1377 DOF)



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So, what, why and how?

## A new sensor

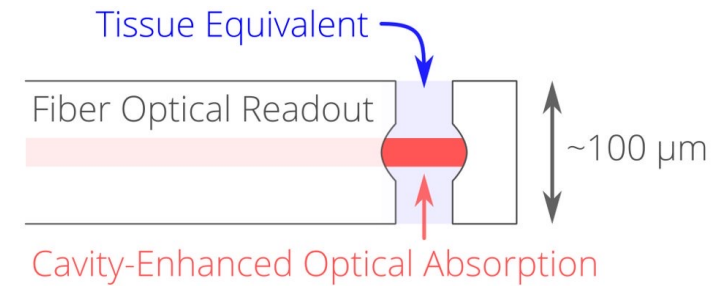
- **Water medium** → independence on dose rate and beam energy
- **Absolute measurement** of absorbed dose

### 1. cm-scale devices

- Tissue-equivalent, absolute dosimeters (linac QA)
- Sub-mGy sensitivity
- Works well with small fields
- Can handle dose rates > 400 Gy/s

### 2. water-filled microcavities

- Detect **dose to a point** with excellent sensitivity
- *In vivo, in situ* dosimetry with instantaneous readout



Thank you!!

## Acknowledgments:

Kate Szabo, Jingyi Bian, Julien Megroureche, Simon Bernard, Tanner Connell, Hamed Bekerat, Robert Hopewell, Lilian Childress, Shirin Enger, Jack Sankey

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