





# CaLIPSO group: development of the ultra-fast gamma detectors for particle physics and Positron Emission Tomography

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> DPhP's CSTD October 2, 2024

# Introduction

- Fast photodetectors :
  - Timing layers at LHC
  - Cherenkov detectors for particle identification
  - Timing measurements at test beams
- Time-of-Flight Positron Emission Tomography
- Main components:
  - Cherenkov Radiators or Fast Scintilation Crystals
  - Fast photodetectors: MCP-PMT / SiPM
  - Dedicated electronics
  - Adequate time reconstruction for signals and events

# Positron Emission Tomography

- PET is a nuclear imaging technique used widely in oncology, cardiology and neuropsychiatry.
- Allows to detect at pico-mol level the the biochemical activity.
- PET scan in a nutshell:
  - Inject one of the radioactive tracer
     e.g. <sup>18</sup>F-FDG, τ~110 min, ~1/2 hour rest time
  - emits positrons ⇒ annihilation with an electrons ⇒ two 511 back-to-back gamma.
  - Gamma detection in coincidence ⇒ register ~100M lines-of-responce ⇒
  - 3D image reconstruction



SIEMENS Biopgraph Vision PET/CT scanner Credit: https://www.siemens-healthineers.com

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# Scanner Types

- Preclinical (small animals)
  - Small aperture
  - High spatial resolution (~1 mm)
  - Small sensitivity
- Brain scanner
  - Limited aperture
  - High sensitivity
  - Good spatial resolution (1.6 3 mm)
- Whole-body
  - Large aperture  $(\sim 0.9 \text{ m})$
  - High sensitivity
  - Low spatial resolution (4 6 mm)
  - Full body dose ~ 5 15 mSv (natural radioactivity per year France : 2 mSv)







Credit: SHFJ

# **PET Evolution**

- Combined modalities: CT/PET, MRI/PET
- Improvement sensitivity: total-body PET

   → 40 fold improvement in sensitivity
- *Reduce bias: depth-of-interaction reconstruction*



- Time-of-flight technique (TOF) ⇒ see next slides
- New developments in electronics, and gamma-detection





Credit: Simon R. Cherry, University of California, Davis https://www.cancer.gov

# **TOF** Technique



- TOF techniques: measure the difference in time between two photons ⇒ improve S/B
- Contrast of the image directly correlated to the S/B and available statistics.

TOF gain estimation: 
$$G = \frac{S/N_{TOF}}{S/N_{noTOF}} \sim \sqrt{\frac{D}{\delta x}} \sim \sqrt{\frac{D}{c/2 \ \delta t}}$$

- D=20 cm ⇒ Coincidence Time Resolution (CTR)=150 ps (FWHM) ⇒ G~2.9 ⇒ 8x lower dose
- Best commercial detectors: ~210 ps (FWHM, CTR)
- In the Lab: below 100 ps, but on small crystals  $\rightarrow$  low efficiency

# Use of the Cherenkov photons

- The 10ps time-of-flight capabilities is a contemporary "holy grail" for PET.
- Current performance are limited by the several factors:
  - Time scale of the scintillation: rise time and quantity of the "fast" photons
  - Fluctuation in time during photon collection within a crystal
  - Performance of the photodetectors (TTS, Efficiency)
  - Limitations of the read-out electronics
- To overcome these limitations our strategy is to use the *Cherenkov photons*.



Radiator

# Cherenkov photons: Two Approaches

- Use pure Cherenkov radiators: PbF2, Pb glass
  - very good timing performance, but difficult to use with SIPM, *low detector efficiency*, limited suppression of the Compton background
  - see, e.g. Kopar et. al., 2011, Canot et al. 2019, Ota et al., 2021
  - Results: CTR FWHM; 30 ps 300 ps
- Use scintillation + Cherenkov: BGO, LYSO
  - limited improvement, because of the low number detected Cherenkov photons per event
  - See e.g. Kwon et al. 2016, Brunner at al. 2017, Kates et al. 2019, Kratochwil et al. 2020, Gundacker et al. 2023
  - Results: CRT, FWHM : 100 300 ps (BGO), bellow 100 ps (LSO).
- In most of those studies → small crystals (3x3x3 mm<sup>3</sup>), two channels, use scope or conventional electronics
- *Our Goal* → study with a "scanner size" module, MCP-PMT, multiple channels, custom made electronics.

### MCP-PMT readout scheme

### Previous Studies: MCP-PMT Pixel Readout

- Measure time difference between MCP-PMT *Planacon* from Photonis (25µm pores) and pulse laser (20 ps beam duration)
- Drawbacks: signal sharing between channels, signals time propagation fluctuation inside channel, limited spatial resolution



⇒ Propose to use a "continuous" readout



C. Canot et al, 2019, J. Inst. 14 P12001

# Transmission Line Read-out

- Use 32 lines (50 Ohm impedance) to readout 32x32=1024 pixels
- Signals are readout from both ends.
- Amplifiers (IJCLab): 2x20dB, 700 MHz
- *SAMPIC digitizer:* 6.4 GSample/s, 64-channels
- Use *charge on lines* for **y-coordinate**
- Use *time difference* between right-left signals for the **x-coordinate**







# Readout Tests

- Use Planacon MCP-PMT XP85122 from Photonis (10µm pores)
- Use the pressure-sensitive anisotropic conductive interface: *3M adhesive tape* or *Shin-Etsu MT-type* of *Inter-Connector* 
  - reworkable, but require careful pressure adjustment
- Use 20 ps pulsed laser for tests in the single-photon regime







# **Time Resolution**



 $- dt = t_{\rm R} + t_{\rm L} - t_{\rm LASER}$ 

• Scan all surface to measure PMT response in each position

*M.* Follin et al, 2022, NIM A, vol. 1027, p. 166092



# Single Photoelectrons Detection: Conclusion

- Obtain uniform quasi-continuous readout with the limited number of channels
- Time resolution marginally improved vs the pixel readout 70 ps (FWHM)
- Achievable spatial resolution is much improved (see following slides)





CaLIPSO/BoldPET project: High spatial resolution for the brain preclinical PET

for the BOLPET collaboration

# **BOLD-PET** project

- **High spatial resolution** for the brain *preclinical PET: CaLIPSO/ BOLDPET* project
- Dual read-out: ionization and light (Cherenkov signal)
- Innovative liquid as a detection medium: TMBi (trimethylbismuth)
- Spatial resolution: 1x1x1 mm<sup>3</sup>(FWHM)
- Resolution in time < 150 ps (FWHM)
- Use MCP-PMT for the optical signal read-out
  - Expected number of photons: 1-2
- Collaboration: IRFU, IJClab, Münster University

CEA Patent 2010: D. Yvon, J-Ph Renault, « Détecteur de photons à haute énergie », WO2011/117158 A1



2.10.2024

# Test With Optical Prototype





- Cell size
  - $-60 \times 60 \times 20 \text{ mm}^3$
- Filled with TMBi
  - ref. Index 1.6 (@425nm)
  - Density 2.3 g/cm<sup>3</sup>
- *MCP-PMT XP85122* from *Photonis* 
  - 10 μ**m** pores





### Test Bench: Measurement with <sup>22</sup>Na source





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# Spatial resolution



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# **Time Resolution**



- Detector time resolution of about 150 ps (FWHM)
  - Limited mainly by the photon propagation in the demonstrator (see next slide)
- The detection of the ionization is more difficult than expected:
  - Low ionization yield
  - Reactivity of the TMBI
  - Require extremely high purity of the liquid

Roman Chyzh et al. 2024, JINST 19 P07018



# ClearMind Project : TOF, high spatial resolution, efficient large PET detection module

for the ClearMind Collaboration





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D. Yvon et al., 2020, JINST 15 P07029

 Second crystal face instrumented MCP-PMT or SiPM Matrix

22

# Why photocathode deposit on crystal ?

- Cherenkov Photons in  $PbWO_4 @ 511 \text{ keV} \sim 20$
- Regular assembly (optical gel)
  - Refrac. index: PbWO<sub>4</sub> ~ **2.2**, Optical contact gel ~ **1.5**
  - $R_{\text{Fresnel}} \sim 3.6$  %, ..... But total reflection angle ~ 43°
    - $\rightarrow~73\%$  of solid angle reflected....
  - ! Photons hardly escape the crystal !
- **PhotoElectric Layer deposited on Crystal** 
  - Refraction index  $\sim 2.7 3$
  - $R_{\text{Fresnel}} \sim 2.5$  %, ..... no total reflection effect .....
  - Up to a factor 4 in light collection efficiency + light collection time shortened !

..... But .....

**Difficult for crystals with High-Z components.** 

# **ClearMind Collaboration**

- CEA Saclay DRF/IRFU
  - D. Yvon & V. Sharyy, Thomas Proslier, R. Belkacem, Z. Zobundzija,
    - (+ D. Baudin, et al.)
- CNRS/IN2P3/IJC-Labs, Serv. d'Electronique : *Analog & Digital readout* 
  - D. Breton, J. Maalmi et al.
- CNRS/IN2P3/CPPM Marseille : Optical simulation / PET imaging hardware simulator
  - C. Morel, M. Dupont, Y. Boursier, et al.
- CEA-DES/ISAS: Machine Learning / IA
  - G. Daniel, ( + J-M. Martinez)
- CEA-DRF/ISVFJ/SHFJ : Medical Physicists. *Full scanner GATE simulation / Image reconstruction / IA* 
  - O. Kochebina, C. Comtat, S. Jan

# First Prototype (Photek): Lines read-out



Anode



Readout Board

- Prototype produced by Photek on the base of MAPMT253 (10 μm pores)
- Transmission line readout :
  - 32 lines
  - Connected throw Shin-Etsu MT-Interconnect
  - Apply compression with metallic brace
  - Double stage amplification: 2 x 20 db, 700 MHz (IJC Labs)



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### First Prototype Assembly









SAMPIC crate digitizes the signals @ 6.4 GS/s (IJC Labs/IRFU)

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# Single Photon detection





×10<sup>3</sup>



Time difference between the laser and the Clear Mind prototype signals over all the detector.



Reconstructed x-coordinate

(along the transmission line)

### ClearMind-one Gamma detection test setup



# **ClearMind-one Gamma detection**

- Successful deposition of photocathode on PbWO<sub>4</sub> Optical window
  - But low Photocathode QE : 16%
  - Thick Passivation layer
- **Efficiency** on 5 mm thick crystal :
  - 28 ± 3 % (28.6% Expected from MC)
- **Spatial resolution** (no IA) : *3.5 mm* across lines & **5.4** *mm* along lines (FWHM)
- **Time resolution** 
  - **330 ps** (FWHM) ... far from our goals
  - **48% of PE event** include a detected Cherenkov photon.
  - Thick Passivation layer
    - $\rightarrow$  Lower Photon detection efficiency
    - $\rightarrow$  Reflections : Random delay of fast photon detection
  - MCP + Lead loaded glass detectors\* achieve < 50 ps</li> (FWHM)

*Cherenkov Only* → Severe loss in efficiency  $\rightarrow$  No positioning



A. Galindo-Tellez et al., JINST, 2024 \*S.I. Kwon, Nature Photon, 2021, L. Chen, NIM A 2024

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Counts (arb.) 250 200

150

100

50

30

40

# Ongoing developments with INCOM (USA)

- Study and optimize timing and position resolution of MCP-PMT photo-detection
  - Using *standard HRPPD MCP-PMT* photo-detector
  - Tails minimization in MCP-PMT distribution in also important !
- ALD barrier coating compatibility with Photocathodes
  - High efficiency photocathodes (30%)
  - Recent progress with Thomas Proslier (IRFU) & M. Miserques (CEA-DES)
- Lead Tungstate Window Sealing trials
- Fabricate 56 x 56 mm<sup>2</sup> thick scintillating crystal MCP-PMTs
- Maintain low contribution from Read-Out Electronics, e.g. :
  - Employ Pulse Shape Measurement Techniques
  - Implement Advanced Time Estimation Algorithms
  - Keep Electronic Noise Levels at a Minimum Level
- Improve Depth of Interaction (DOI) Reconstruction Precision :
  - Correct for the time reconstruction biases
  - + Working on *thicker crystal*

AAIMME Project : Machine Learning for Molecular Imaging and the Medicine of the Future

for the AAIMME collaboration

# Simulation

- Gate/Geant4 simulation is used to understand the detector.
- Detailed simulation of the optical photon propagation
  - Surface properties adjusted to the measurement with the optical microscope
- Innovative approach to the photocathode simulation
  - Specify the refractive index of the Bialkali photocathodes using the published measurement
  - Leave Geant4 to simulated the reflection and absorption at the photocathode
  - Parameterize the extraction probability and intrinsic quantum efficiency using the PMT photocathode calibration.
  - Use of the dedicated simulation for the thin layer frustrated transmission (CPPM Marseilles, added to Geant4 v11.2)
  - Will share this code inside DRD4 CERN collaboration
- Simulate in the detailed PMT response and signal shape using parameterized analytical functions.



Simulated signals read out at the left (blue) and right (red) ends of the line

Ch.-H. Sung et al. NIM A Volume 1053, 2023, 168357

Ch.-H Sung, PhD thesis, Université Paris-Saclay, Orsay, 2022

L. Cappellugola et al., in 2021 IEEE NSS/MIC Conference

# **2D** Spatial Reconstruction

- Develop an innovative method of NN gamma vertex 2D reconstruction  $\rightarrow$  modify the Loss function:
  - Estimate the unc
  - take into account of the detector w

Set of pulses as registered recorder for a 511 keV energy deposit (simulation). Only the pulses registered on one side of the transmission lines are shown. SAMPIC Pulse Left

- 
$$\log(L(\theta)) = \sum_{i} \sum_{z \in \{x,y\}} \log\left(\Phi\left(\frac{b - \mu_{\theta,z}(\mathbf{s}_i)}{\sigma_{\theta,z}(\mathbf{s}_i)}\right) - \Phi\left(\frac{a - \mu_{\theta,z}(\mathbf{s}_i)}{\sigma_{\theta,z}(\mathbf{s}_i)}\right)\right)$$
  
+  $\frac{1}{2}\log(2\pi\sigma_{\theta}^2(\mathbf{s}_i)) + \frac{(z_i - \mu_{\theta,z}(\mathbf{s}_i))^2}{\sigma_{\theta,z}^2(\mathbf{s}_i)}$   
G. Daniel et al.,  
Engineering Applications of Artificial Intelligence,  
Volume 131, 2024, 107876

G. Daniel et al. Engineering Applications of Volume 131, 2024, 107876

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# Grid of sources



- Simulate a grid and reconstruct in three different approaches:
  - Preprocessing using robust statistics
  - Conventional
  - Account for the physical limits throw the truncated Gaussian
  - Account in addition for the uncertainties (weighting)





### Reconstruction Precision in X (along lines)





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# AAIMME Project: To be continued

- Encouraging results → *uncertainties are needed* at the image reconstruction level
- ANR AAIMME: time/DOI reconstruction, image reconstruction

CEA – DES / ISAS CEA – DRF / IRFU CEA – DRF / ISVFJ/SHFJ CNRS – IN2P3 / CPPM



#### 2.10.2024

# *Chronography\** Cutting edge gamma detector instruments

# for TOF-PET & High-Speed Calorimeter

for the future collaboration

\* **Ch**erenkov and **cr**oss-lumi**n**escence timing for highly time-res**o**lved ionizin**g ra**diation detectors for **ph**ysics and societ**y** 

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# Chronography Collaboration

- CEA Saclay & BIOMAPs Orsay
  - D. Yvon, V. Sharyy, Thomas Proslier & Olga Kochebina, Claude Comtat, Sébastien Jan
- FZU, Univ. Prague
  - Robert Kral, Martin Nikl
- Univ. Tartu
  - Vitali Narginoi, Marco Kirm
- Institute for Crystal Growth (IKZ), Berlin
  - Iroki Tanaka
- CERN
  - Etiennette Auffray
- Univ. Marseilles, CPPM
  - Christian Morel, Univ. Marseilles, CPPM
- No Industrial accepted to be involved yet
  - St Gobain Cristaux (V. Ouspensky, Luxium Solutions), Hellma, Korth Kristalle, MEGA Materials

# Chronography goals : Two breakthroughs

- Ultra-fast, bright, dense scintillating crystal of heavy compounds
  - *Cherenkov yield* : *high optical index* and *UV transparency*
  - Cross-luminescence scint., *intrinsic* (*ps*), *shortest decay times* (*sub-ns*), *yield* ~1000 ph/MeV
- Study ternary Rb, Cs and Ba *fluorides* containing a second, heavy, cation
  - From *Lu* (Z=71) *to lead and bismuth*,
  - High Gap  $\rightarrow$  Deep UV transparent  $\rightarrow$  More Cherenkov light.
    - → Cross-luminescent crystal, *an ambitious challenge*.
- Light extraction and detection of dense UV-scintillating crystals
  - SiPMs : QE ~15% in the deep UV. Optical contact damps photons l < 200 nm.
  - *MCP-PMT* : *Thin optical, deep UV coating* to passivate the crystal surface
     → before photocathode deposition : optical window of a cutting edge MCP Gamma detector.
    - → *no total reflection at the crystal/grease interface*, thanks to frustrated transmission
    - $\rightarrow$  improves fast photon collection time and light collection efficiency (up to a factor 4)
  - Good commercial *deep UV photomultiplier photocathodes reach 30% efficiency*
- Fully meet the specifications of a gamma detector for TOF- PET imager.

# **Tasks Sharing**



Crystal development / Gamma Detector Dev. & Models / PET Scan optimization

# Work Package Organisation



Organisation / Crystal development / Single pixel detec. and related technologies / Proof of Concept detectors and PET Scan modeling

### Long term vision

Chronography Proof of Concept	Total-body TOF-PET prototype at PASREL	Total-body TOF-PET scanner industrialization	Future: Clinical use
Detector modules with unrivaled time-resolution few tens <u>ps</u> 1/ Pixelated detector PoC 2/ Monolithic detector <u>PoC</u>	<ol> <li>Demonstration of the scanner prototype's low dose potential</li> <li>Collaboration with nuclear medicine MDs- Medical studies + (BioMaps)</li> </ol>	<ol> <li>1/ Early diagnosis &amp; research on aging's diseases</li> <li>2/ Low Dose pregnant women imaging 3/ Longitudinal clinical monitoring Drug development - Therapies</li> </ol>	Diagnostic and therapeutic evaluation 1/ Neurology: Alzheimer/Parkinson/Psychiatry 2/ <u>Cancerology</u> : Targeted therapies/ <u>Immunotherapy</u> 3/ Pharmacology: Drug development
			Cancer:
EIC Pathfinder (1 – 4 year)	EIC Transition (5 – 8year)	EIC Accelerator (9 – 15 year)	Before treatment After treatment
		umu	

From a detector prototype

To a PET-Scan prototype (PASREL)

To PET-Scan industry

To medical

applications

# Conclusion : Instrumental skills in lab

- Expertise in fast photo-detection technologies and MeV gamma-ray detectors.
- At the forefront of fast single-photon detection, with MCP-PMTs and SiPMs.
- Tests benches on key photodetector characteristics
   Quantum efficiency, time response, Positioning accuracy
   high-performance, fast electronics (analog amplifiers and SAMPIC).

   => original and high-performance photo-detection chain.
- Extensive experience in Monté-Carlo simulations for gamma ray detectors (Geant4 & GATE)
- Innovative AI approaches for event reconstruction.
- Closely following advances in scintillation crystal technologies (Crystal Clear collab.)

### Conclusion : Positioning within IRFU and CEA

- Representing IRFU at the Crystal Clear collab. (Scintillators Crystal dev. & applications, Dominique).
- Representing IRFU at DRD-6 collab., (WP3, crystal calorimeters, Dominique).
- Representing IRFU at DRD-4 collab., (Photodetectors, MCP-PMTs, Instruments & simulations, photocathode models, Slava).
- Associated Researchers to the UMR BioMaps (CEA-SHFJ + Univ. Paris-Saclay + INSERM + CNRS) (Dominique, Slava), Headed by Prof. V. Lebon, leader of the *PASREL Research Hospital* being build in Saclay
- Membre du CoPil RTR Physique-Biologie de la DRF (Dominique).
- Membre de CSTD du DPhP (Slava)
- Coordinator of two collaborations, *ClearMind* (France) and *Chronography* (Europe).
- Major contributor to the AAIMME collaboration (CEA, CNRS, INRIA, Univ. Paris-Saclay).

### Our request

- <u>ManPower</u>:
  - *Ambitious, rich and motivating, scientific and technological program*. Major prospects for valorization.
  - Program in synergy with the major priorities of CEA and active prospects at CERN
  - Yet *only two permanent scientists* take care of it. Dominique will be 60 in 2025.

For an ambitious future to these developments, **strengthening the group** is needed in the short term

- <u>Budget :</u>
  - *ANR funding*, *P2I prototype and DPhP R&D budget* will cover the planned program with INCOM.
  - *Chronography project cannot be carried with French expertise alone.* The budget for the European collaboration : 3.1 M€, including 1.4 M€ for the CEA.
     EIC funding application : 4% success rate.
  - The competition is increasely powerful, particularly in the USA/Japan.

We are asking the CSTD and the heads of labs *support for our scientific and technological program and reliable source(s) of funding for this ambitious project*