

Towards multiphoton imaging @ **J-PET**

with  simulations :-)

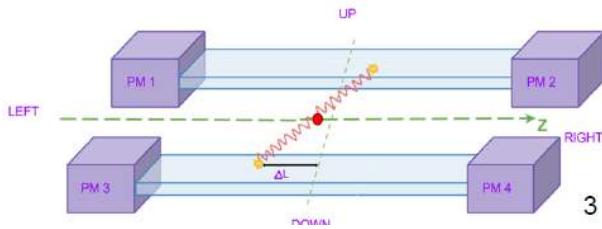
Wojciech Krzemień
On behalf of the J-PET collaboration

Jagiellonian Positron Emission Tomography



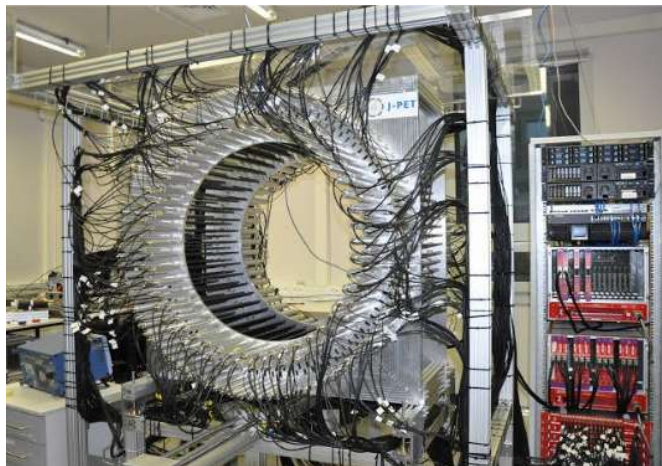
Cost-effective total body solution

$$\Delta l = \frac{(t_2 - t_1) \cdot v}{2} \approx \frac{(t_2 - t_1) \cdot c}{4}$$



$$\Delta x = \frac{(t_l - t_r) \cdot c}{2} \implies \Delta x = \frac{\Delta t}{2} \cdot c$$

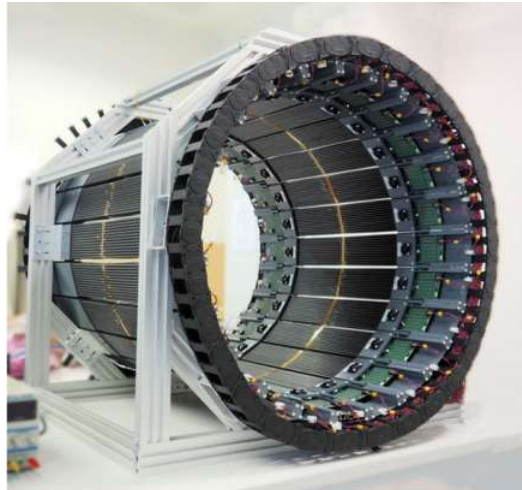
First prototype



Acta Phys Pol. B 48 (2017) 1567

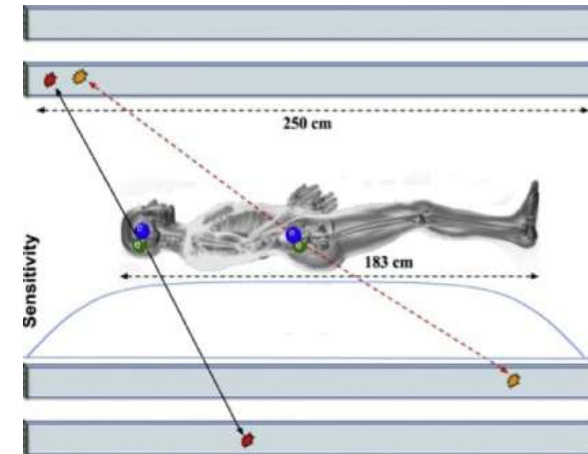
- 50 cm AFOV
- 192 plastic strips
- Readout → vacuum tube photomultipliers

Modular J-PET



- 50 cm AFOV
- 24 modules x 13 strips
- Readout → silicon photomultipliers matrices

Total-body

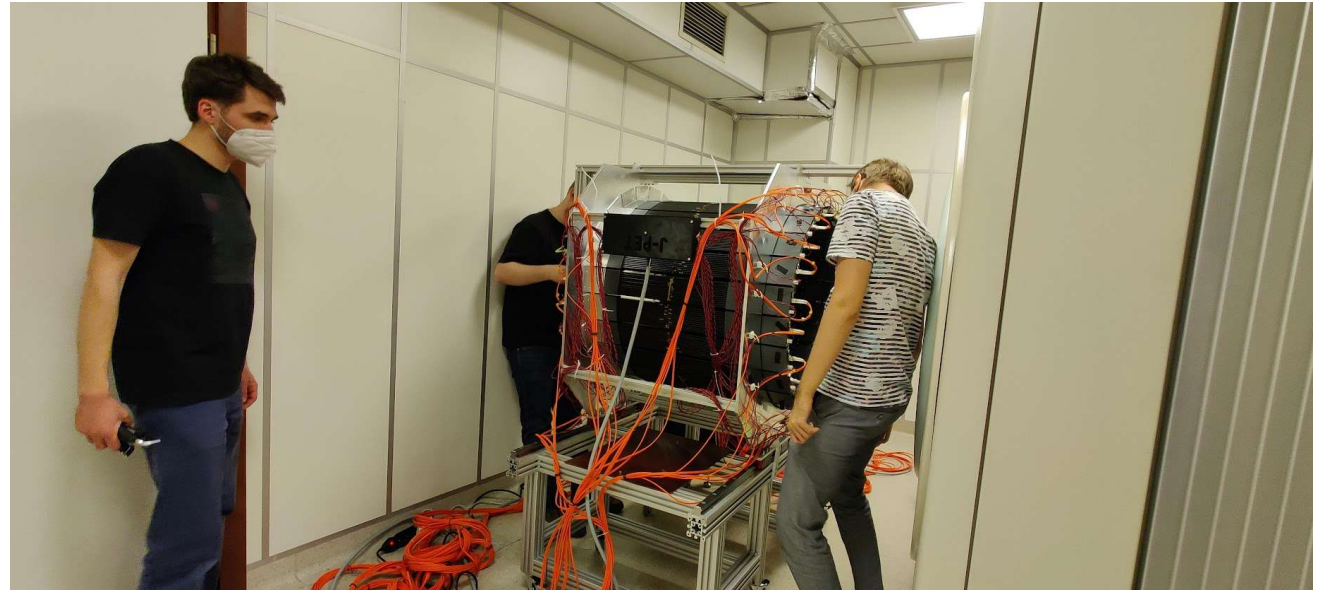
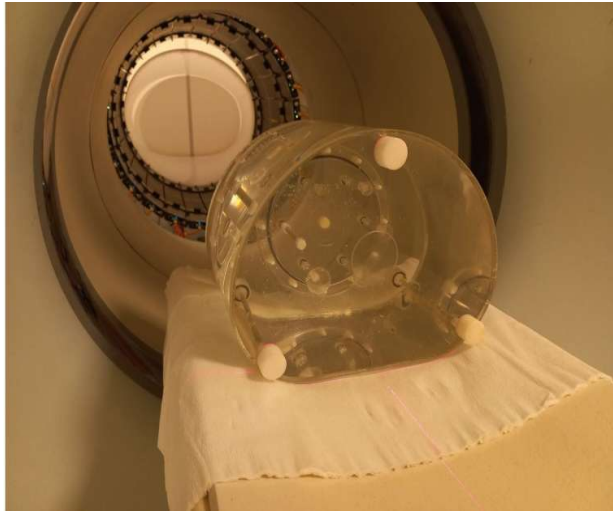
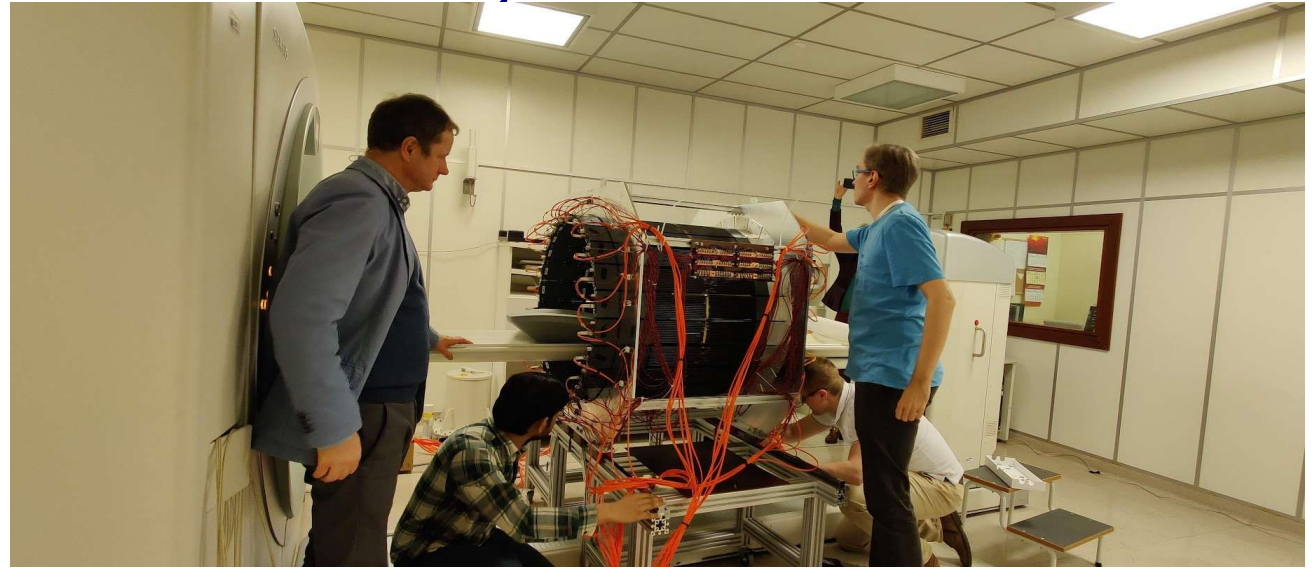
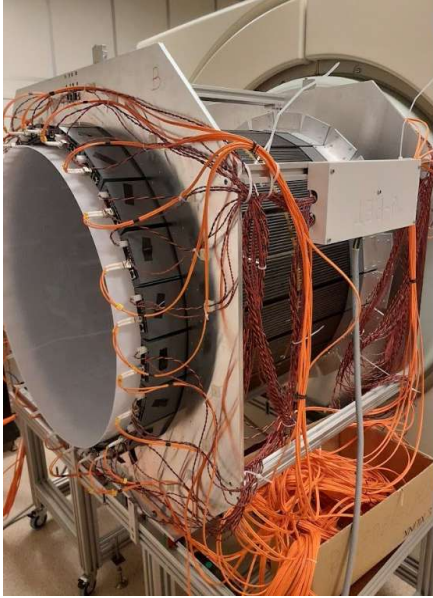


PET Clinics 15 (2020) 439
Phys. Med. Biol. 66 (2021) 175015

- 250 cm AFOV
- Additional layers of wavelength shifters → better axial resolution



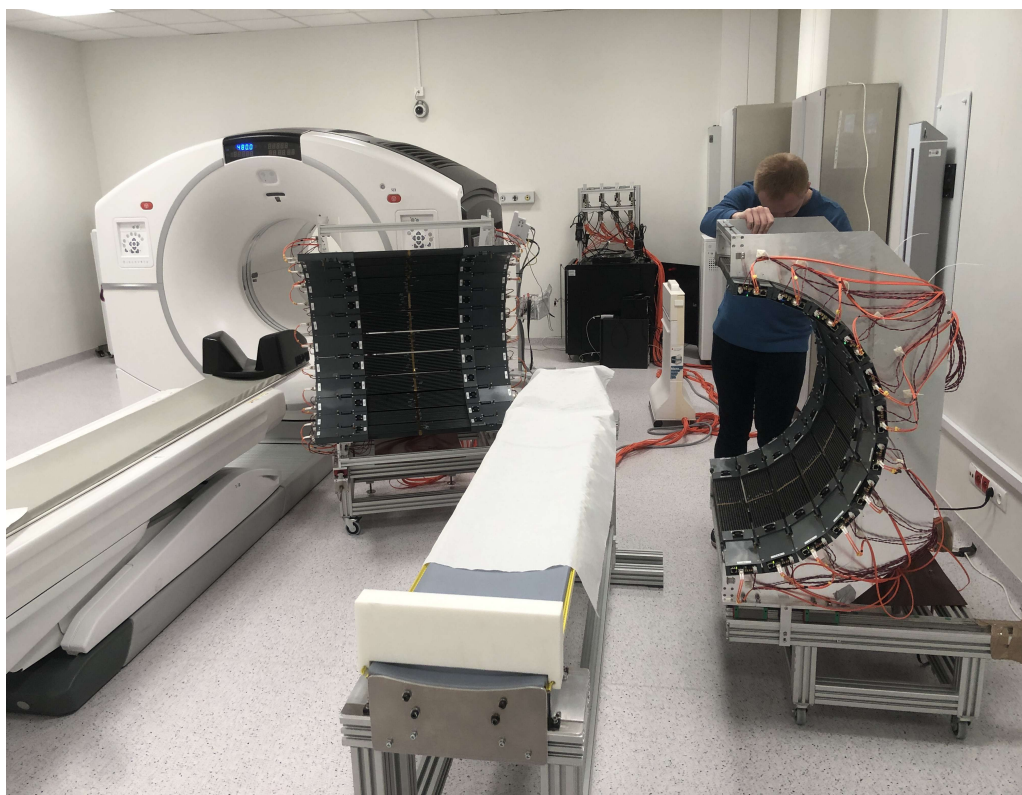
First test measurements with patients @Medical University of Warsaw



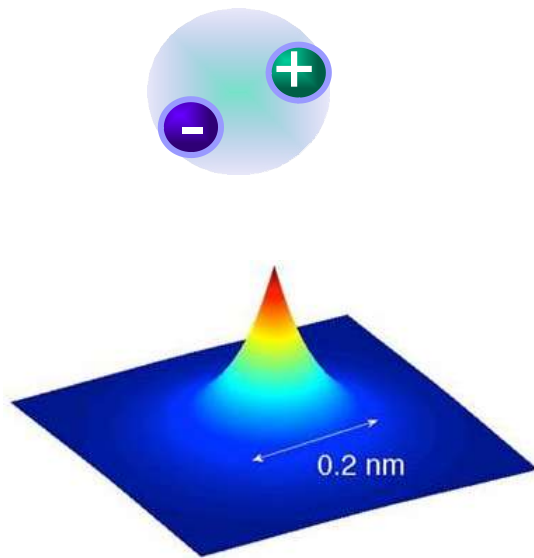
- ^{68}Ga and FDG – phantoms and patients
- data also taken with Biograph Truepoint PET-CT

"First positronium image of the human brain in vivo" P. Moskal et al.,
medRxiv:2024.02.01.2329902, article submitted.

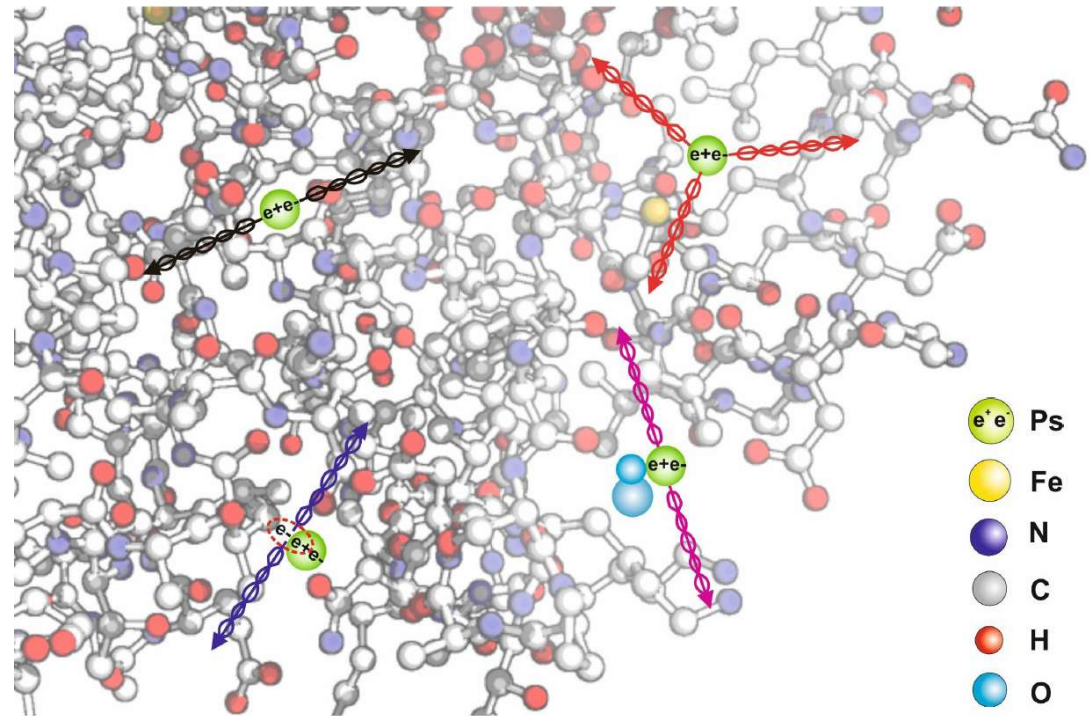
Currently - measurements with patients @University Hospital in Cracow



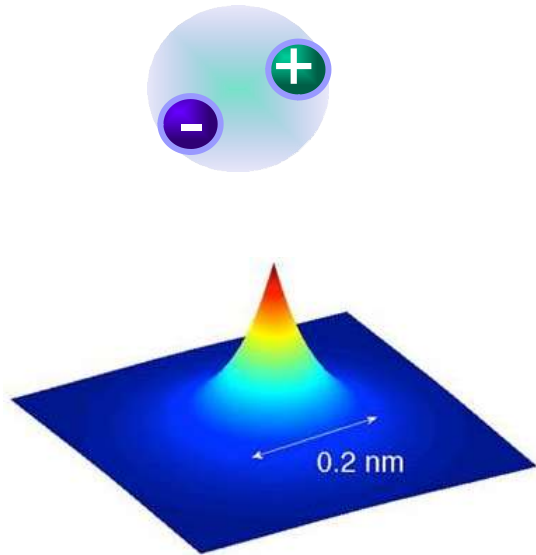
Multi-photon imaging



Model of the hemoglobin molecule



Positronium in PET

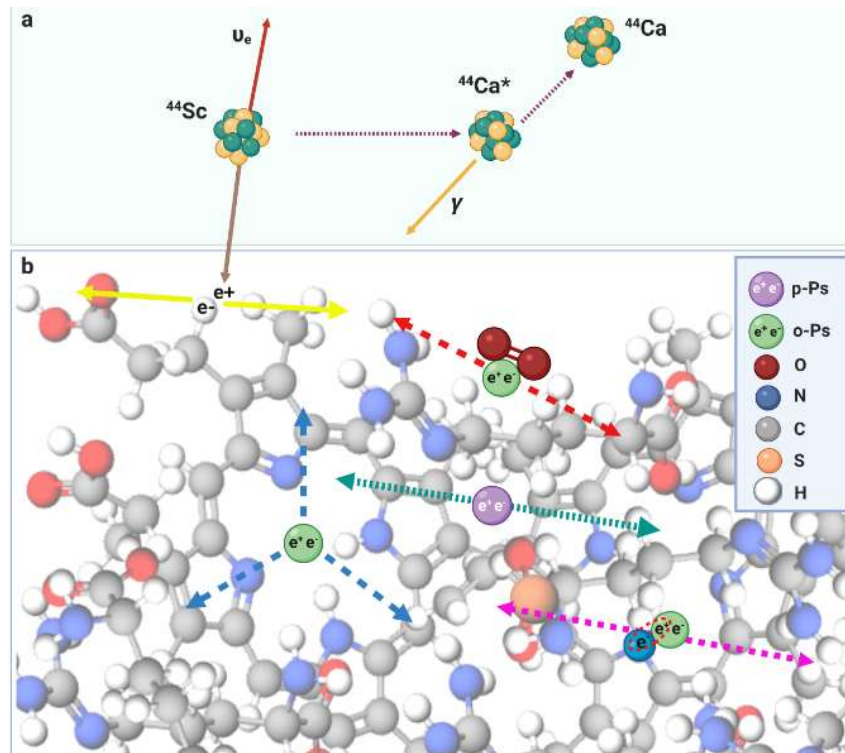


Para-positronium:

- lifetime ~ 125 ps
- two-photon decay

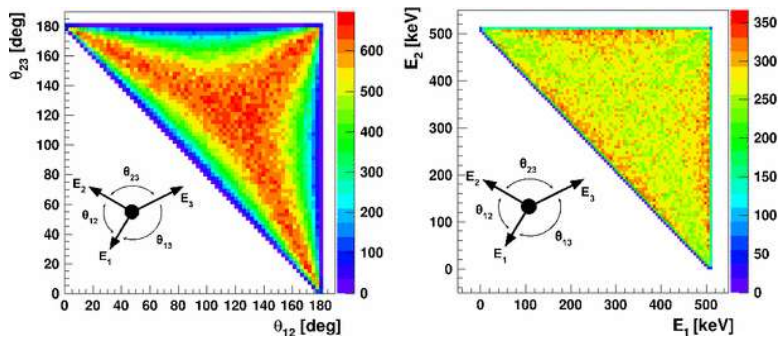
Ortho-positronium:

- lifetime ~ 142 ns
- three-photon decay



Fundamental searches with positronium decays @J-PET

- Study of the CP symmetry:
P. Moskal, E. Czerwiński, J. Raj et al., Nature Communications 15 (2024) 78
- Testing of CPT symmetry:
P. Moskal, A. Gajos et al. Nature Communications 12 (2021) 5658
- Study of the forbidden decays (p-Ps \rightarrow 3 photons)- conjugation symmetry
M. Skurzok **Acta. Phys. Polon. A 137 (2020) 134**
- Invisible decays, dark matter searches, rare decays (ps \rightarrow 4 photons, ps \rightarrow 5 photons),
E. Perez del Rio, P. Tanty, J. Mędrala
Acta Phys. Polon. A 142(3) (2022) 386-390
- Many more physics topics:
P. Moskal et al. Acta Phys. Polon. B 47 (2016) 509



S. Bass et al. Rev. Mod. Phys. 95 (2023) 021002
 P. Moskal et al., Phys. Med. Biol. 64 (2019) 055017
 P. Moskal et al. Eur. Phys. J. C 78 (2018) 970
 D. Kaminska et al., Eur. Phys. J. C (2016) 76:445

Implementation of QED-compliant description of ortho-positronium decay

GateExtendedVSource

- Positronium decays (pPs, oPs, mixed)
- Polarization supported
- Configurable decay properties:
 - prompt gamma emission
 - prompt gamma energy
 - positronium life time
 - fraction of pPs and oPs decays

GateVSource
 Inherited Gate Source class functionality

Positronium decays

Mateusz Bała

available in GATE >= v9.0

Simultaneous scans = standard image + lifetime image

Positronium imaging with the novel multiphoton PET scanner

PAWEŁ MOSKAŁ, KAMIL DULSKI, NEHA CHUG, CATALINA CURCEANU, ERYK CZERWIŃSKI, MEYSAM DADGAR, JAN GAJEWSKI, ALEKSANDER GAJOS, GRZEGORZ GRUDZIEN, WOJCIECH WIŚLICKI +27 authors Authors Info & Affiliations

SCIENCE ADVANCES • 13 Oct 2021 • Vol 7, Issue 42 • DOI: 10.1126/sciadv.abh4394

3,485



Abstract

In vivo assessment of cancer and precise location of altered tissues at initial stages of molecular disorders are important diagnostic challenges. Positronium is copiously formed in the free molecular spaces in the patient's body during positron emission tomography (PET). The positronium properties vary according to the size of inter- and intramolecular voids and the concentration of molecules in them such as, e.g., molecular oxygen, O₂; therefore, positronium imaging may provide information about disease progression during the initial stages of molecular alterations. Current PET systems do not allow acquisition of positronium images. This study presents a new method that enables positronium imaging by simultaneous registration of annihilation photons and deexcitation photons from pharmaceuticals labeled with radionuclides. The first positronium imaging of a phantom built from cardiac myxoma and adipose tissue is demonstrated. It is anticipated that

Kamil Dulski

CURRENT ISSUE



Control of lysosomal-mediated cell death by the pH-dependent calcium channel RECS1

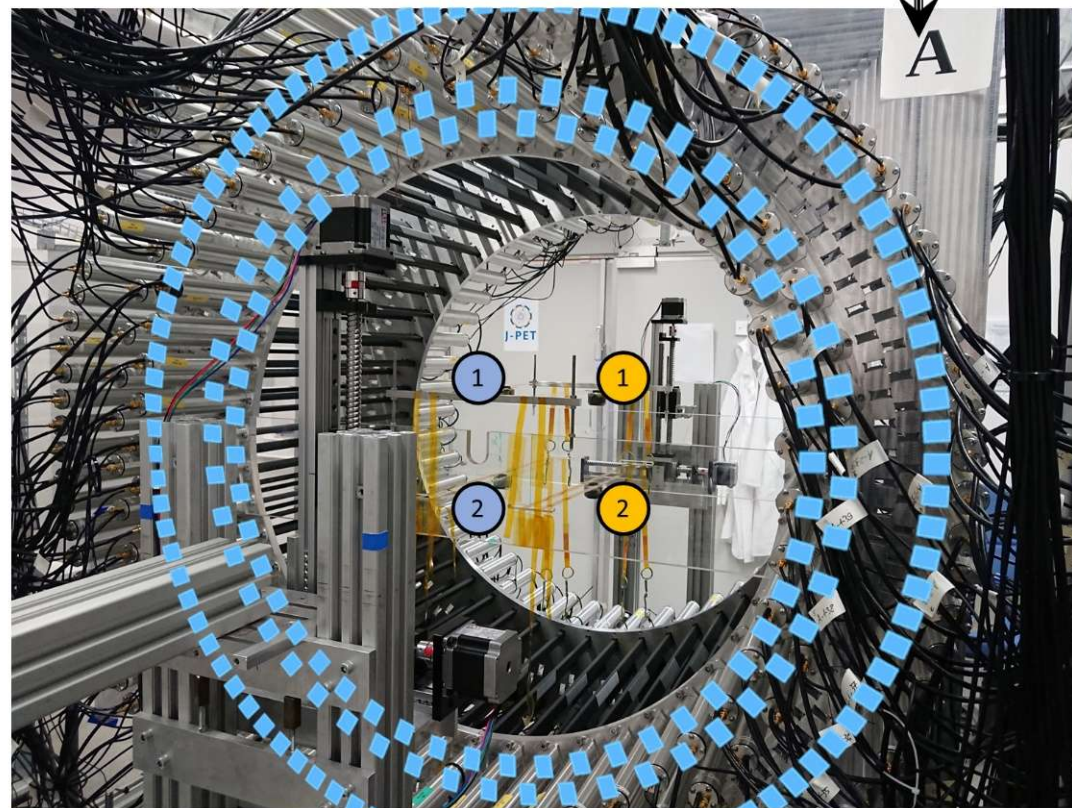
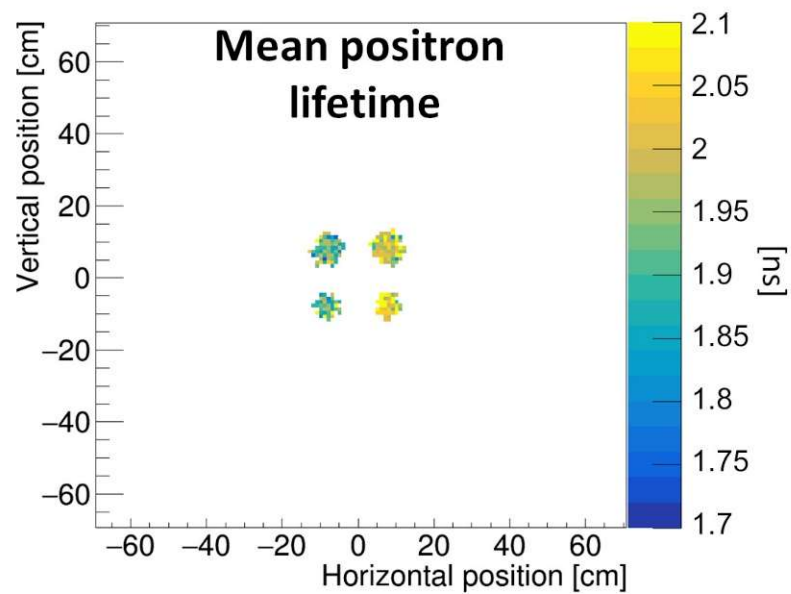
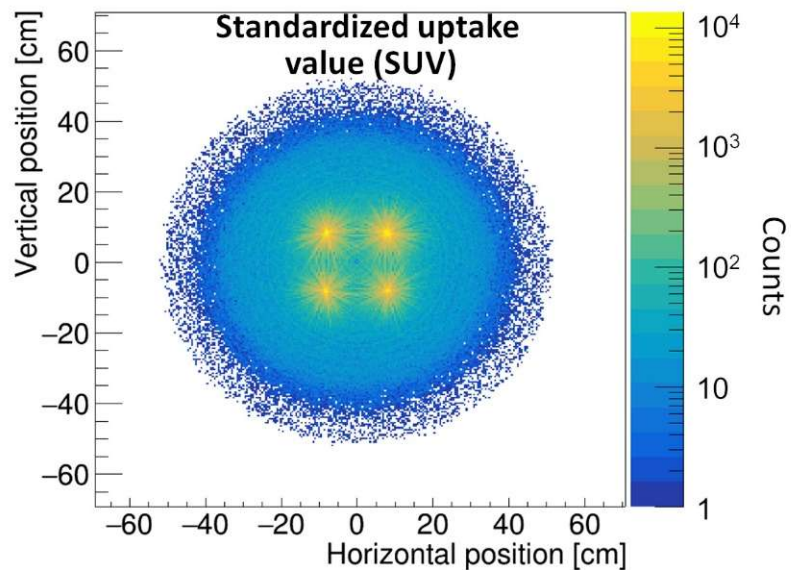
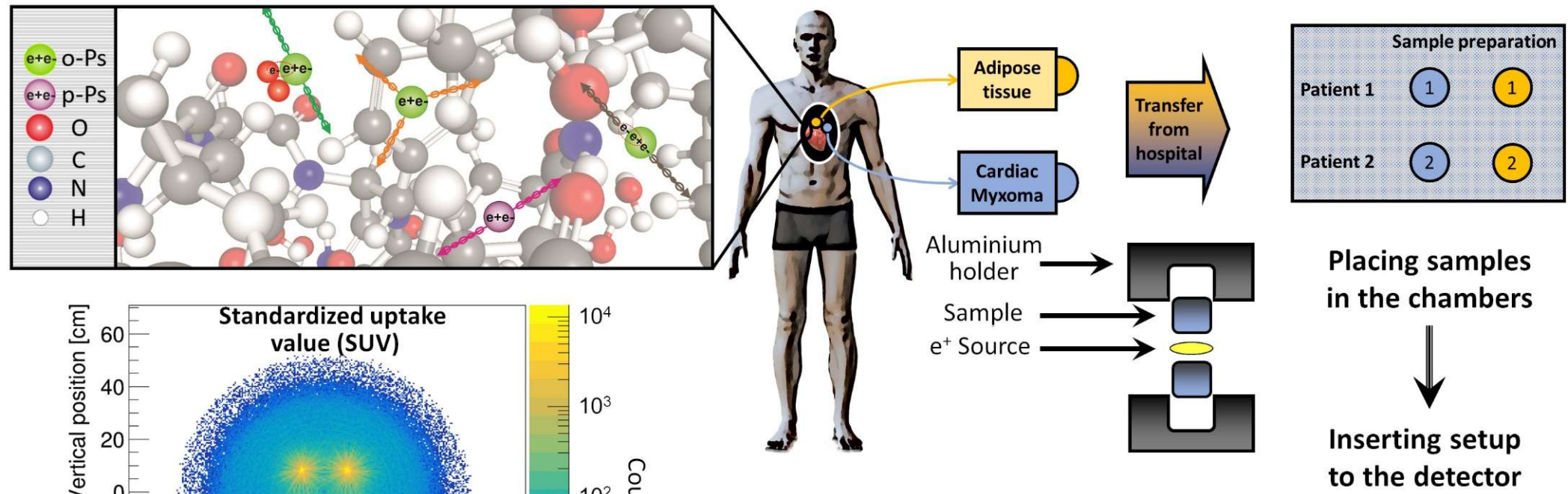
BY PHILIPPE PIHAN, FERNANDA LISBONA, ET AL.

Epitope-preserving magnified analysis of proteome (eMAP)

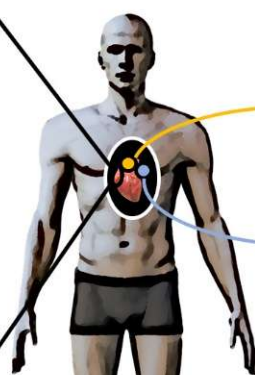
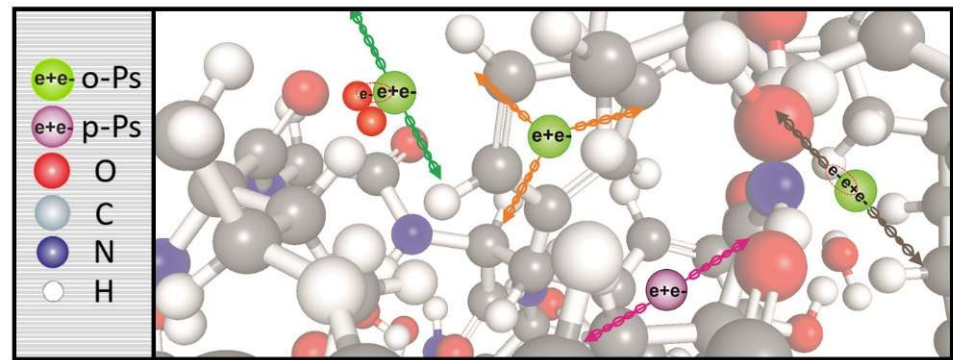
BY JOHA PARK, SARIM KHAN, ET AL.

Speckle-free holography with partially coherent light

Also : Shibuya, K., et al. Nature Commun Phys 3, 173 (2020).



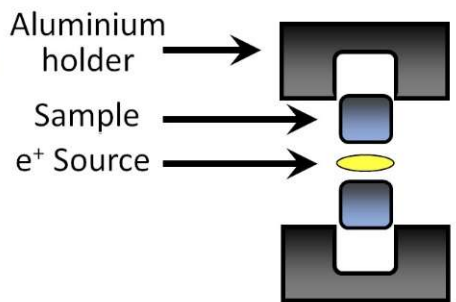
Kamil Dulski



Adipose tissue
Cardiac Myxoma

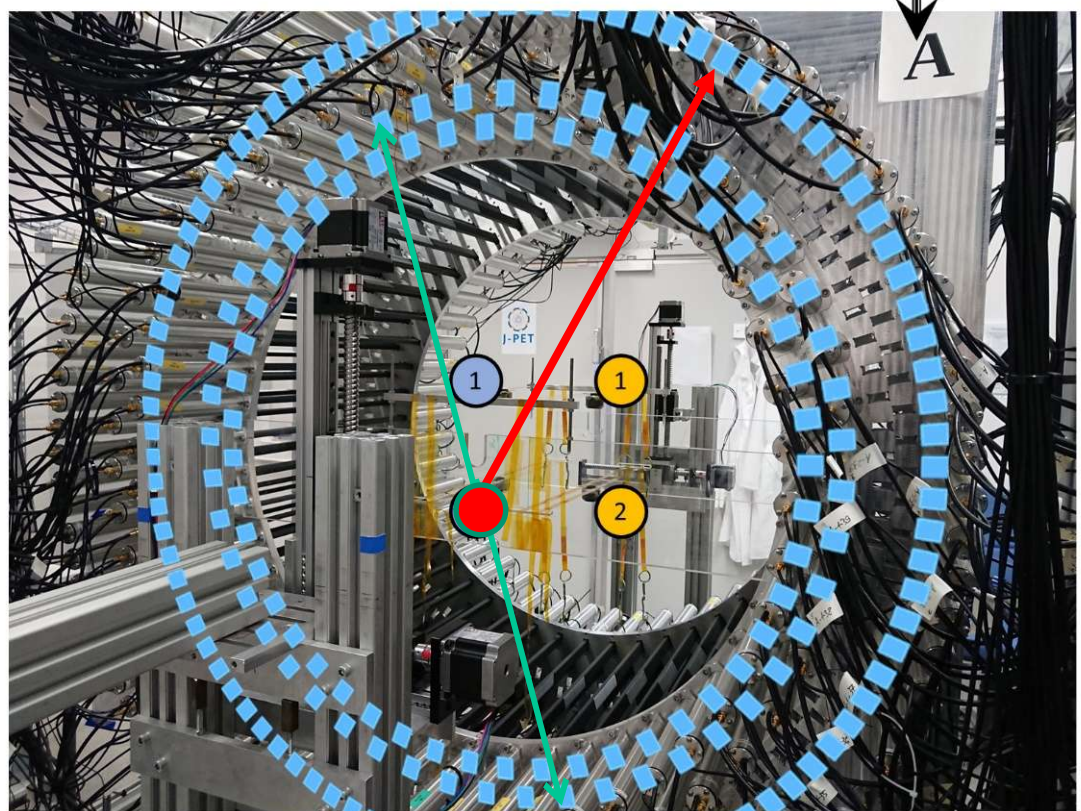
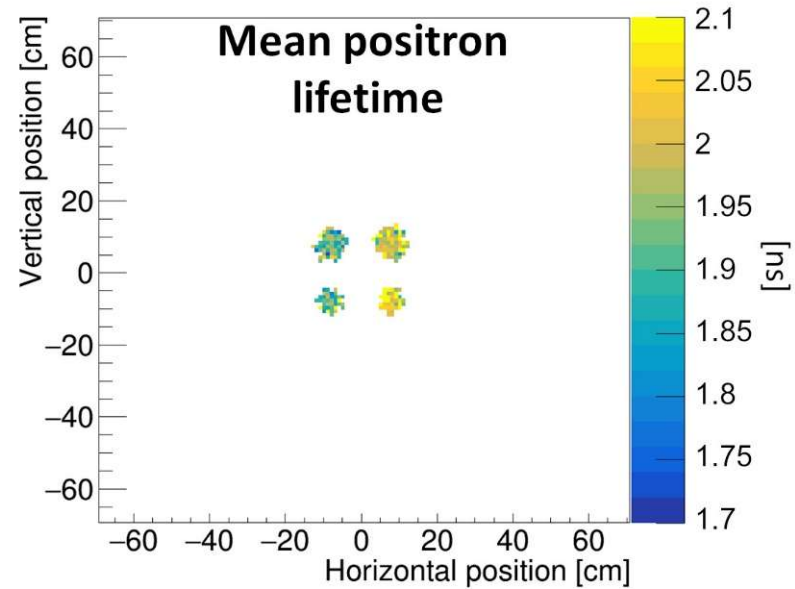
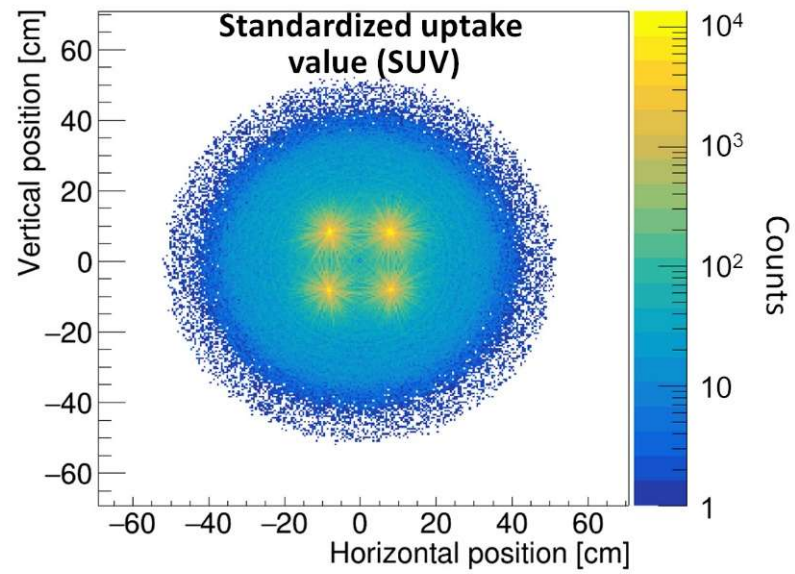


Sample preparation		
Patient 1	1	1
Patient 2	2	2

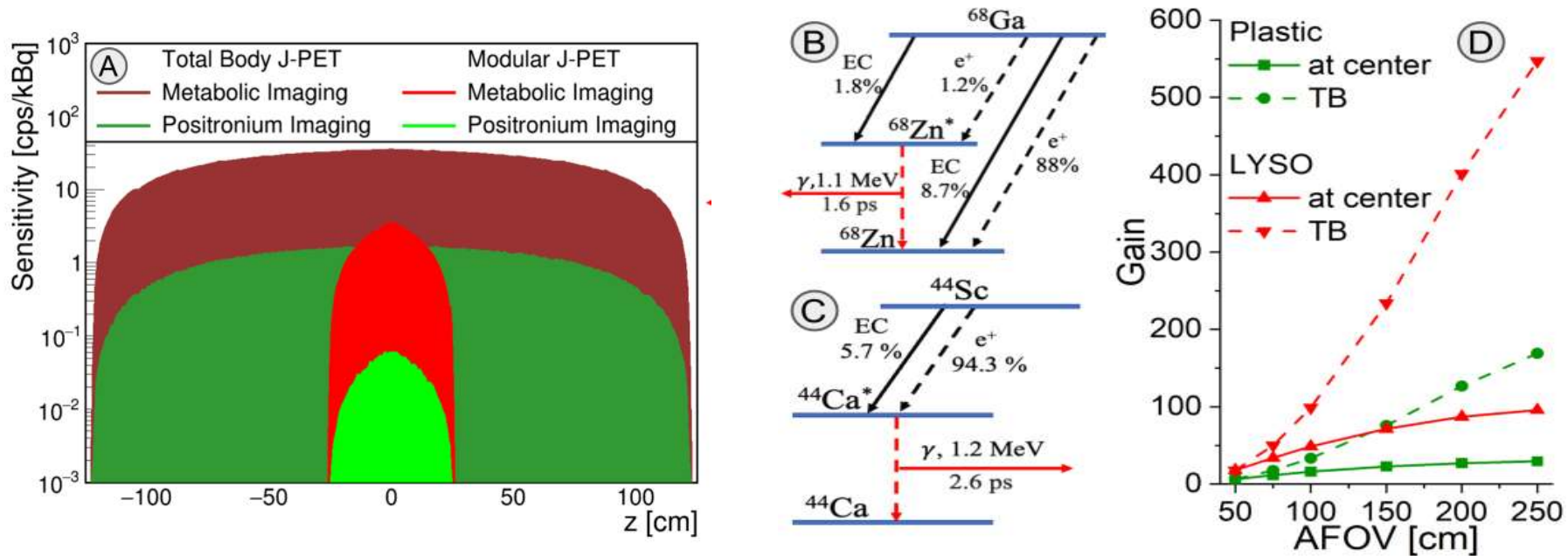


Placing samples in the chambers

Inserting setup to the detector



Multi-photon tomography challenges



- Efficient (triple) coincidence selection
- New reconstruction algorithms:
 - R. Shopa, K, Dulski Bio-Algorithms and Med-Systems 18(1) (2022) 135-143
 - B. Huang et al., IEEE Transactions on Medical Imaging, doi: 10.1109/TMI.2024.3357659
- Background coincidences (randoms, scatters) reduction



Triple coincidence selection

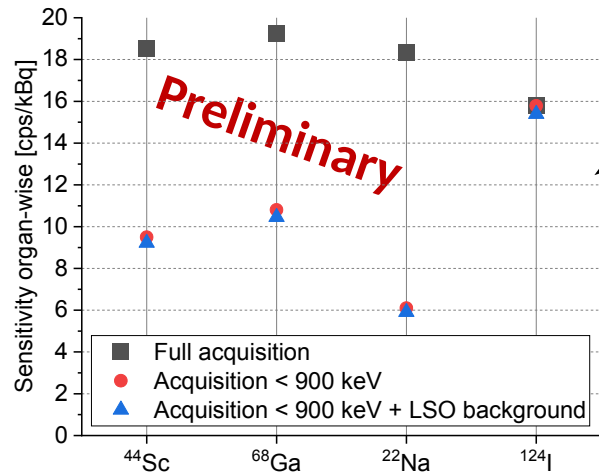
- Gate version 9.1
- Modified to J-PET needs*
- Further modified due to issues with saving proper scattering statistics for 3rd photon
- Source type: pPs + deexcitation photon (resembling ^{44}Sc)
- Simulation up to the level of Singles
- Personal Coincidence sorter for triple coincidences

*<https://github.com/JPETTomography/Gate>

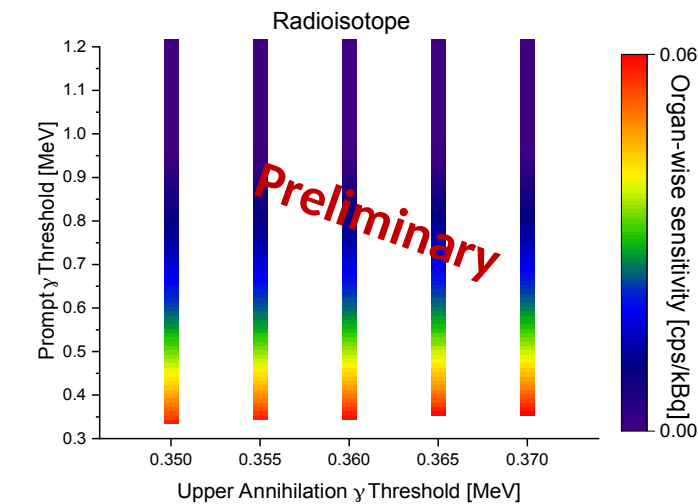
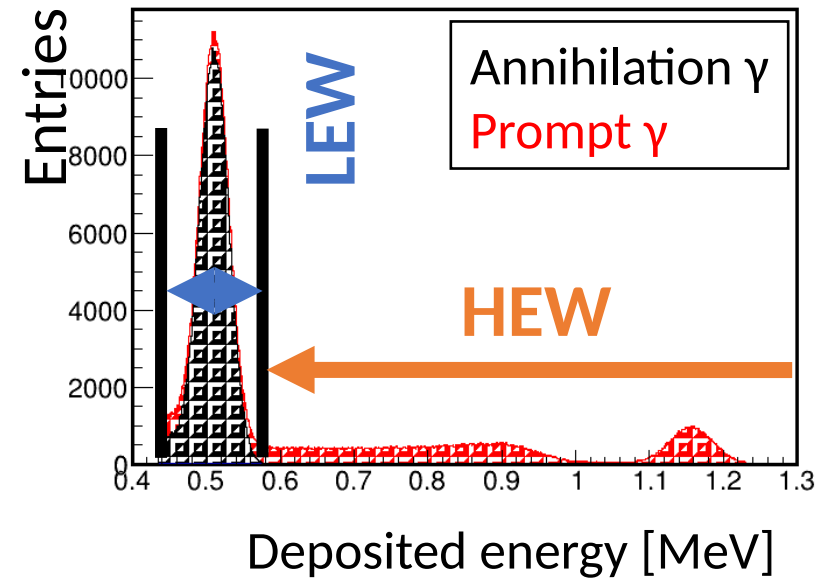
Earlier preliminary results:

Triple coincidence selection

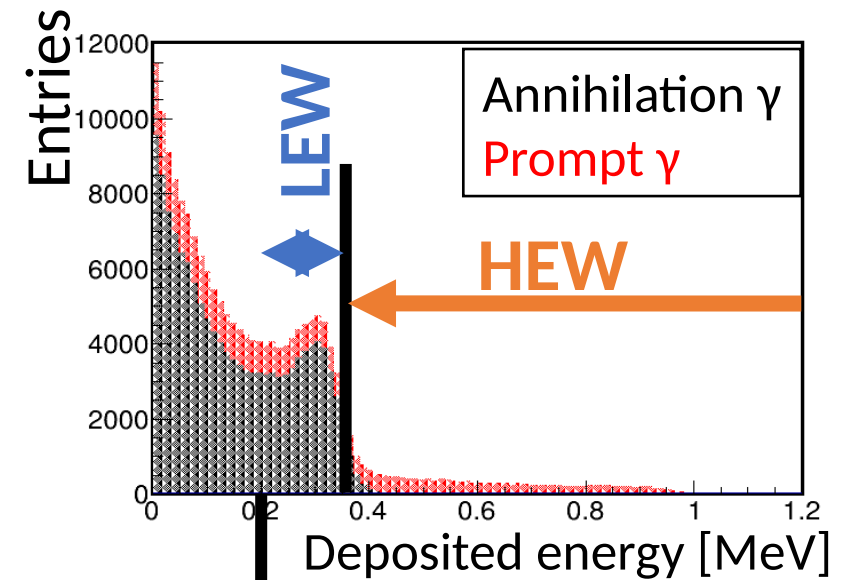
- Definition: 2 photons from **Low Energy Window** + 1 photon from **High Energy Window**
- Possible candidate triples:
 - 2 × Annihilation γ - Annihilation/**Prompt γ**
 - Annihilation γ + **Prompt γ** - Annihilation/**Prompt γ**
 - 2 × **Prompt γ** - Annihilation/**Prompt γ**



Biograph Vision
Quadra

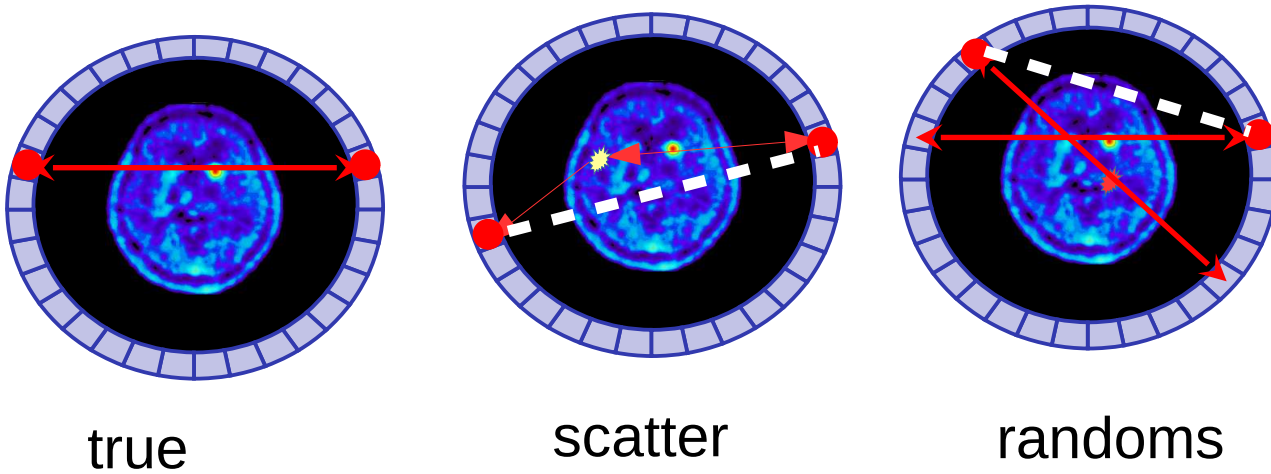


Modular J-
PET

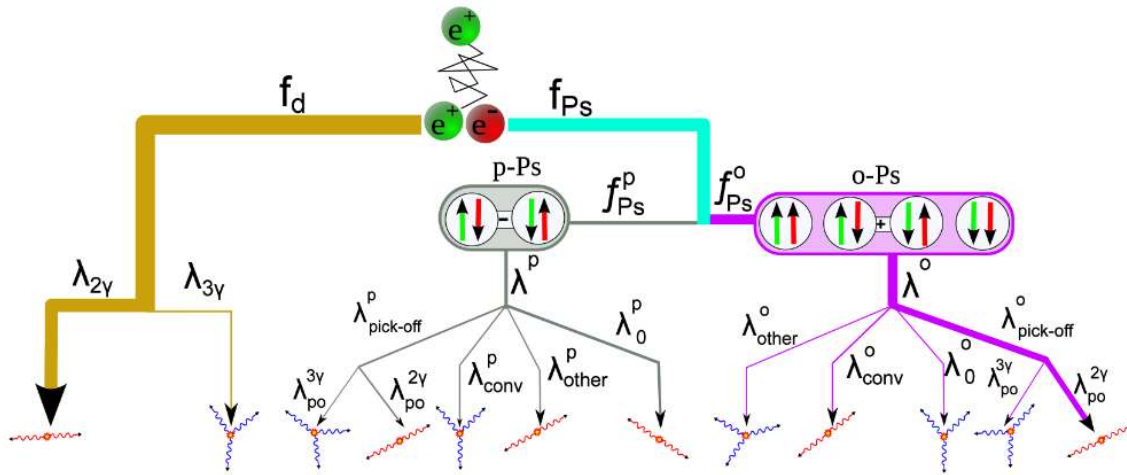


Figures: Exemplary energy spectrum of annihilation + prompt photons; GATE software

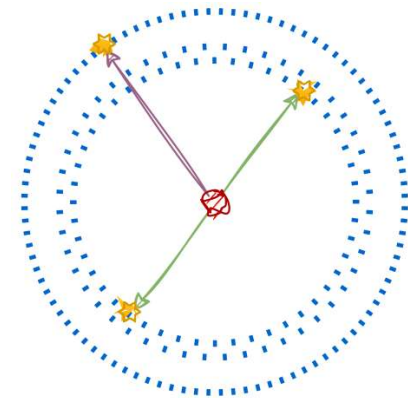
Coincidence classes (multi-photon tomography)



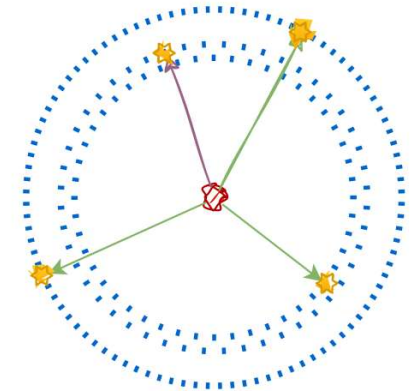
Coincidence classes (multi-photon tomography)



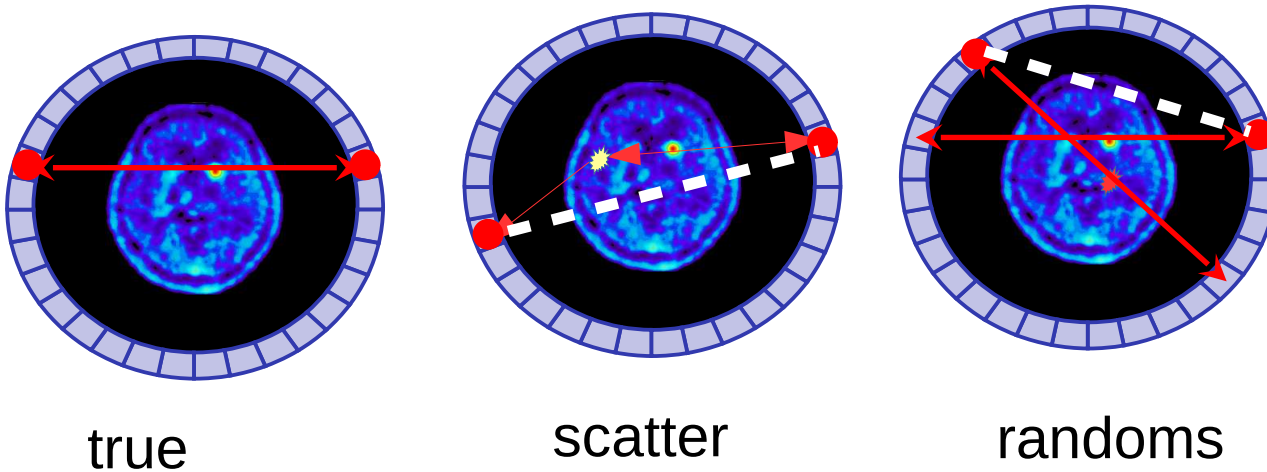
From Rev. Mod.Phys. S. Bass, S. Mariuzzi, P. Moskal, E. Stępień
<https://arxiv.org/pdf/2302.09246.pdf>



2 annihilation photons + 1 high energy photon



3 annihilation photons + 1 high energy photon



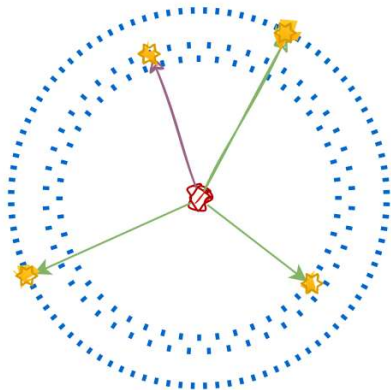
true

scatter

randoms

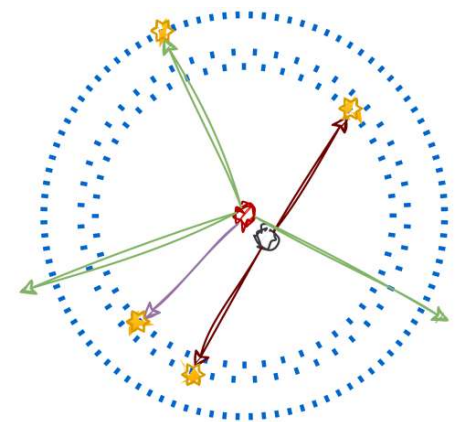
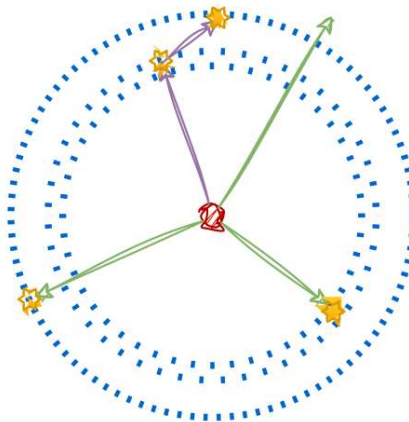
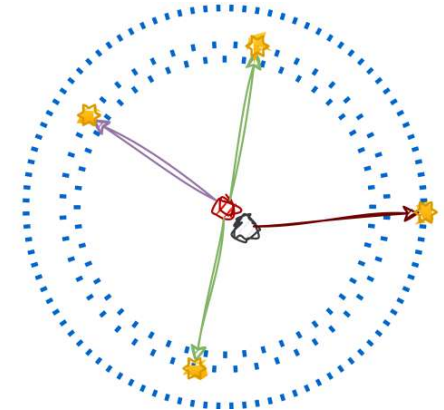
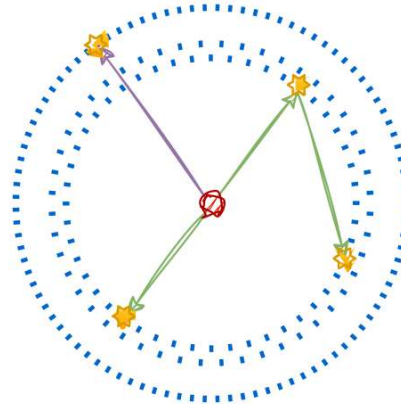
Coincidence classes (multi-photon tomography)

SIGNAL



3 annihilation photons + 1 prompt photon

BACKGROUND CASES (JUST EXAMPLES)



Application of Deep Learning methods for event classification in multi-photon case

Can we apply ML for event selection in view of positronium lifetime tomography?

ScienceAdvances

Current Issue First release papers Archive About Submit manuscript GET OUR E-ALERTS

HOME > SCIENCE ADVANCES > VOL. 7, NO. 42 > POSITRONIUM IMAGING WITH THE NOVEL MULTIPHOTON PET SCANNER

RESEARCH ARTICLE BIOPHYSICS

Positronium imaging with the novel multiphoton PET scanner

ESMER MORKAL, KAMAL DUKER, NEHA CHILUKI, CATALINA CUCURANU, ERYK CZERNINSKI, MEYSAM DAQDAR, JAN GAJEWSKI, ALEKSANDER GAJEV, GREGORZ GRUBISZYK, L.J. WLODZIMIR WISLICH, +27 authors, Authors Info & Affiliations


SCIENCE ADVANCES • 13 Oct 2023 • Vol 7, Issue 42 • DOI:10.1126/sciadv.adf4354

3,485

Abstract

In vivo assessment of cancer and precise location of altered tissues at initial stages of molecular disorders are important diagnostic challenges. Positronium is copiously formed in the free molecular spaces in the patient's body during positron emission tomography (PET). The positronium properties vary according to the size of inter- and intramolecular voids and the concentration of molecules in them such as, e.g., molecular oxygen, O₂; therefore, positronium imaging may provide information about disease progression during the initial stages of molecular alterations. Current PET systems do not allow acquisition of positronium images. This study presents a new method that enables positronium imaging by simultaneous registration of annihilation photons and deexcitation photons from pharmaceuticals labeled with radionuclides. The first positronium imaging of a phantom built from cardiac myxoma and adipose tissue is demonstrated. It is anticipated that

CURRENT ISSUE

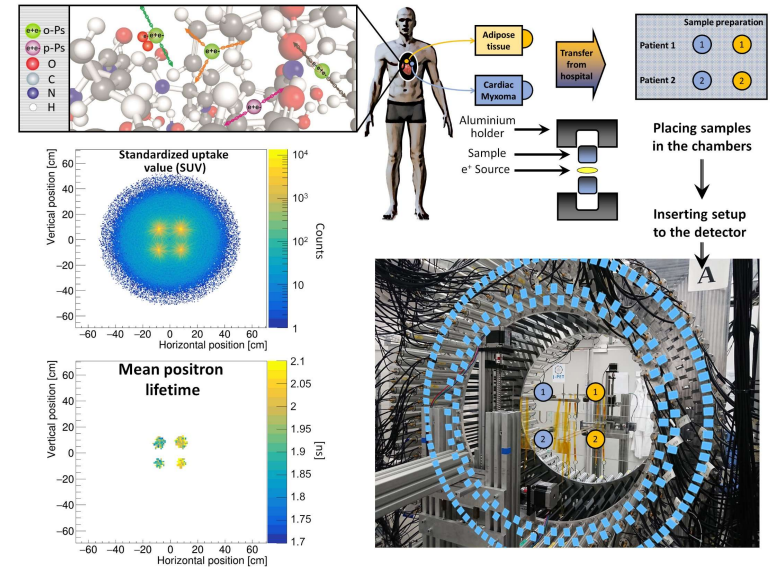


Control of lysosomal-mediated cell death by the pH-dependent calcium channel RECS1
BY PHILIPPE PIRHAN, FERDANDA LISSONA, ET AL.

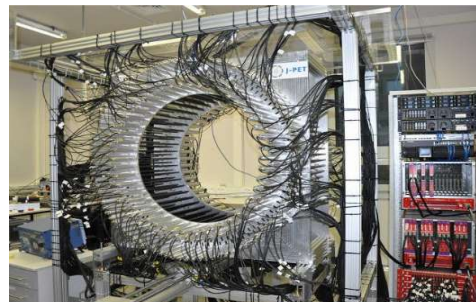
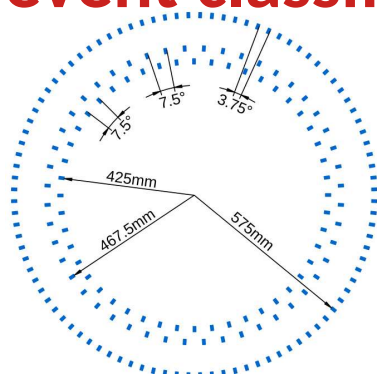
Epitope-preserving magnified analysis of proteome (eMAP)
BY JOHA PARK, SARIM KHAN, ET AL.

Speckle-free holography with partially coherent light

PDF Help



Application of Deep Learning methods for event classification in multi-photon case



Large Barrel geom.

- 50 cm AFOV
- 192 plastic strips
- 3 layers

Setups:

- Two point sources (0,0,0) cm and shifted (5,0,5) cm
- Small cylinder (R=5cm, L=5cm)
- Positronium lifetime = 2ns

Acta Phys Pol. B 48 (2017) 1567

MC Simulation

- Phenomenological time, energy and positional resolution
- Preselection cuts (~17% of background rejected, ~0.6% of signal rejected)
- $S \sim 5 \cdot 10^2$, $B \sim 1.3 \cdot 10^7$
- Additional signal-only simulations: 10^5

Feedforward Neural Network

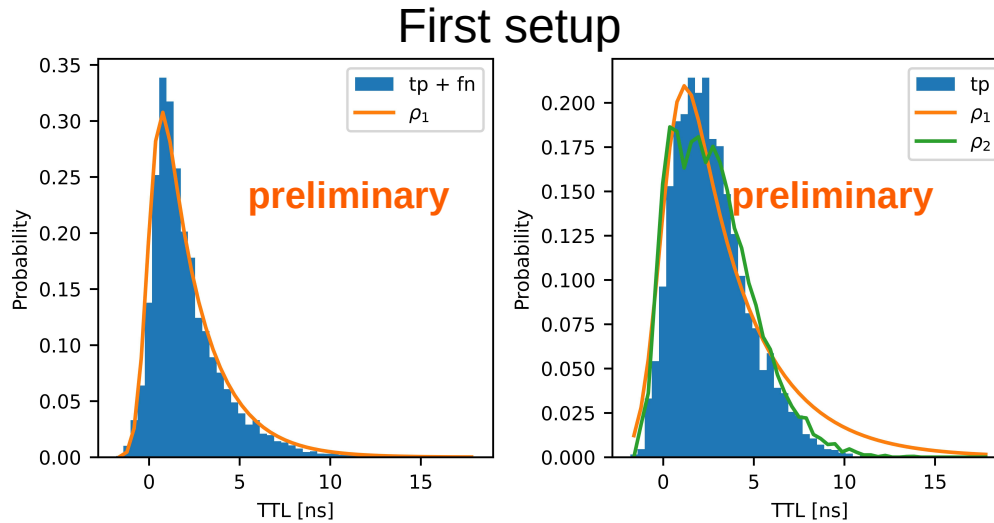
 PyTorch

Hyperparameter tuning



- Optimizer: Adam
- Loss: Customized loss function
- Optimization: Tree-Structure Parzen Estimation
- Feature space: 46 variables

Application of Deep Learning methods for event classification in multi-photon case



$$\rho(t) = \begin{cases} \frac{1}{\tau} \exp(-\frac{t}{\tau}), & t \geq 0 \\ 0, & t < 0 \end{cases}$$

$$S(t) = \frac{1}{\sigma\sqrt{2 * \pi}} \exp\left(-\frac{t^2}{\sigma_t^2}\right)$$

$$\rho_1(t) = (\rho * S)(t)$$

$$\rho_2(t) = \rho_1(t) \cdot \text{eff}(t)$$

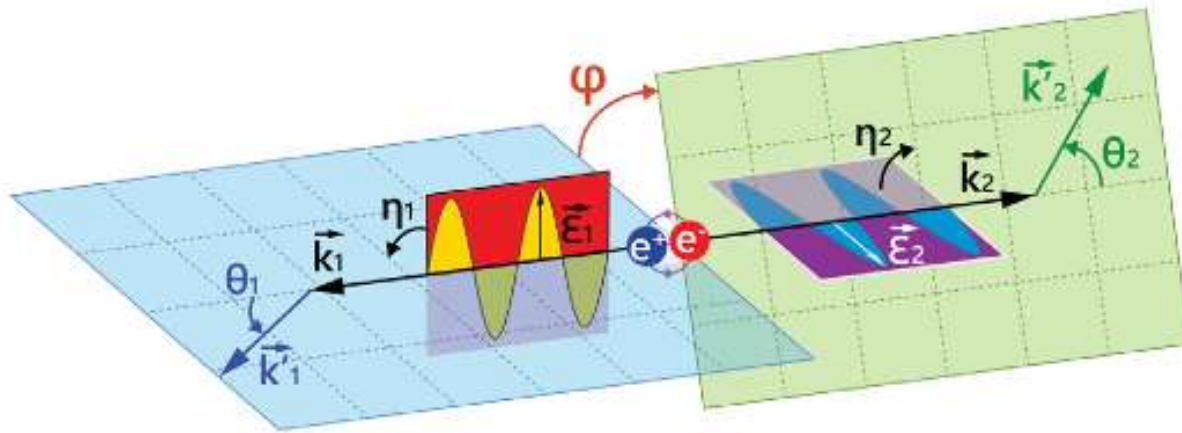
preliminary

Nominal value 2 ns

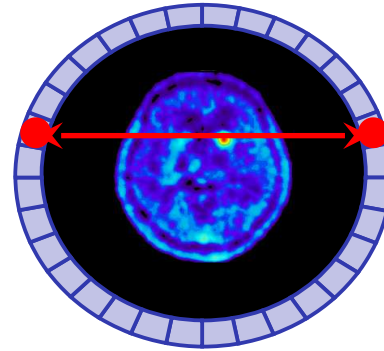
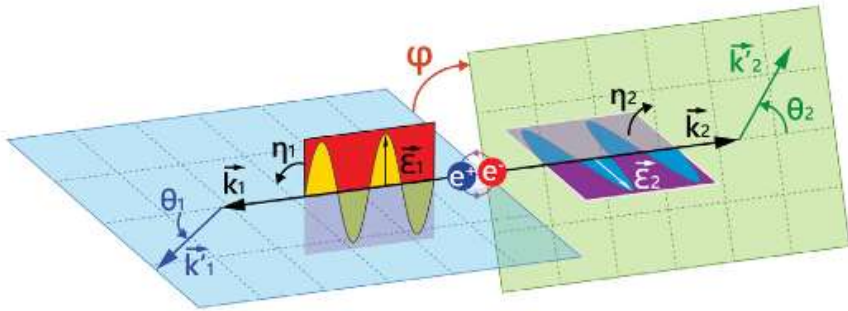
TP + FN	ρ_1	τ	2.163(90)ns
		σ_t	0.525(41)ns
TP	ρ_1	τ	3.272(216)ns
		σ_t	0.918(106)ns
	ρ_2	τ	2.024(88)ns
		σ_t	0.700(77)ns

- Comparison with respect to „standard” J-PET selection criteria show 10x improvement in signal to noise terms

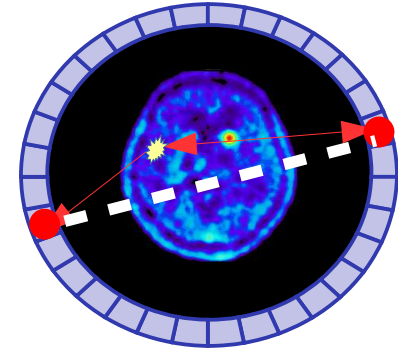
Exploiting photons polarization



Two-photon correlations for PET applications



True events



(Noisy)scattered events

Different modalities (MC estimations):

Kuncic, Z., et al. Instrum. Methods Phys. Res. A 648, S208 (2011)

McNamara, A. et al. Z. Phys. Med. Biol. 59, 7587 (2014)

P. Moskal et al. Eur. Phys. J. C 78, 970 (2018)

Yoshida, E. et al. Phys. Med. Biol. 65, 125013 (2020)

Theory:

B. C. Hiesmayr, P. Moskal Sci. Rep. 7 (2017) 15349

B. C. Hiesmayr, P. Moskal Sci. Rep. 9 (2019) 8166

Experimental results:

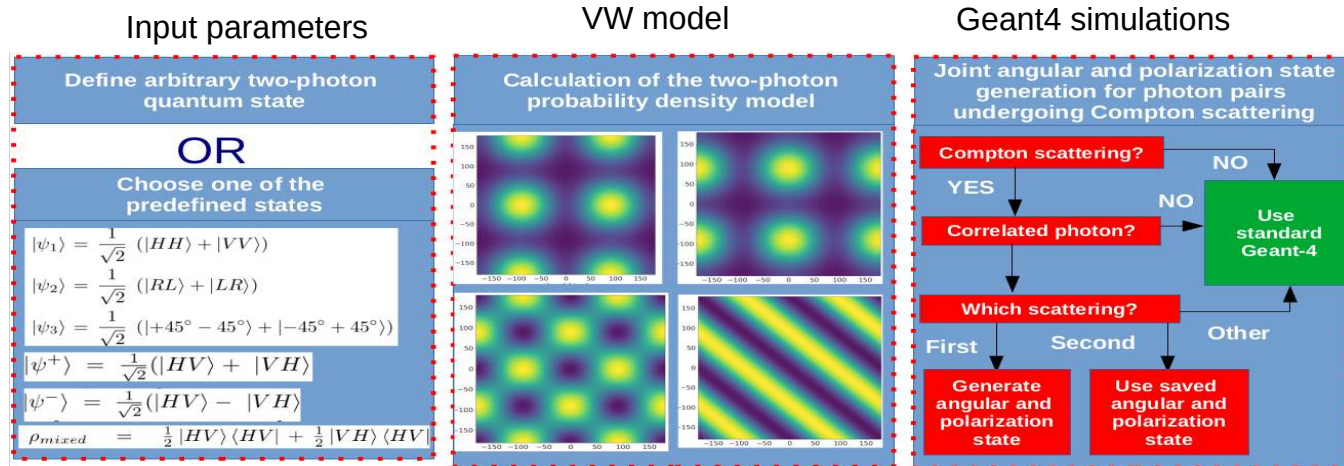
D. Watts et al. Nature Communications 12 (2021) 2646

A. Ivashkin et al. Scientific Reports 13 (2023) 7559

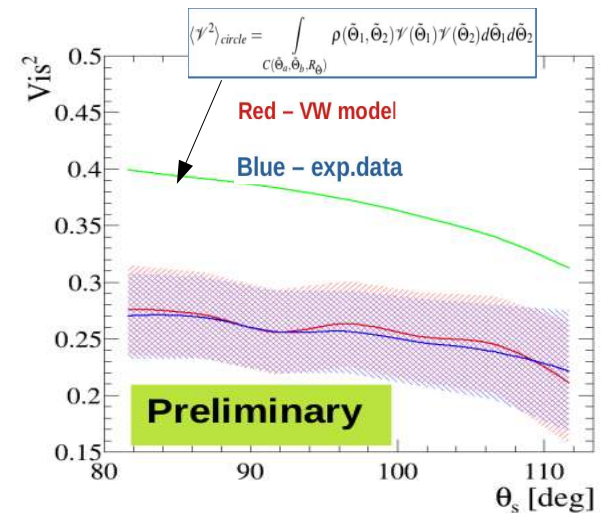
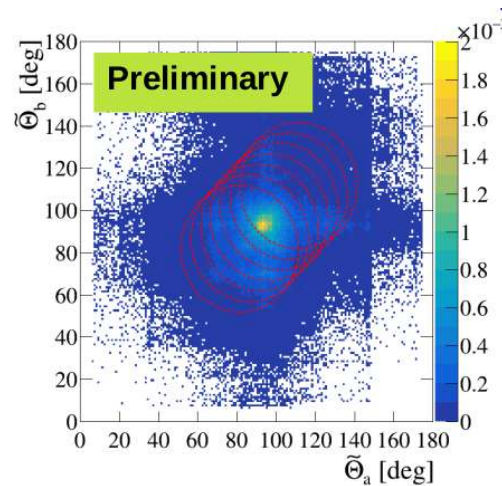
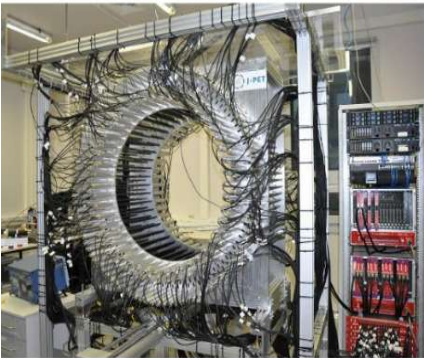
S. Parashari et al. Phys. Lett. B 852 (2024) 138628

P. Moskal et al., article submitted (2024)

Two-photon correlations for PET applications



Model validation with data taken by the J-PET scanner



New (multi)scattering formalism:
 Hiesmayr, B.C., Krzemień, W. & Bała, M. Sci Rep 14, 9672 (2024)

Other activities

PET imaging toolbox

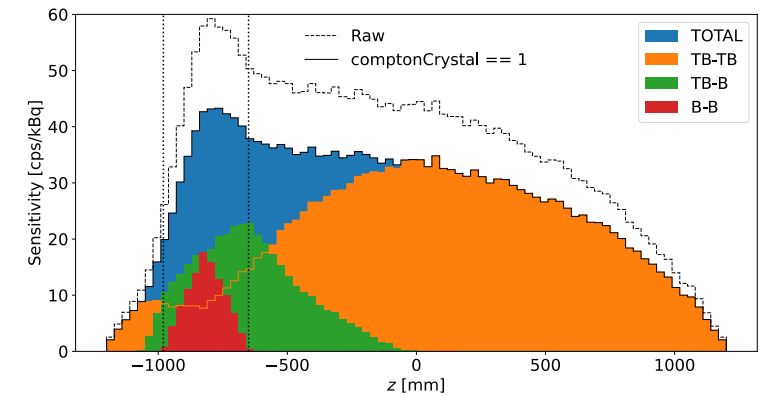
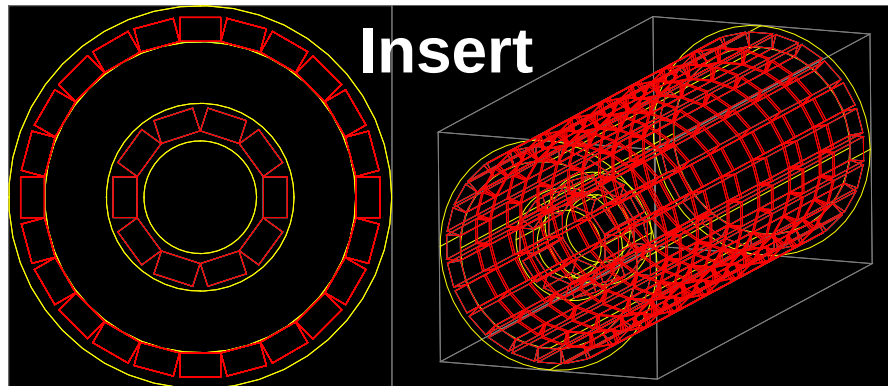
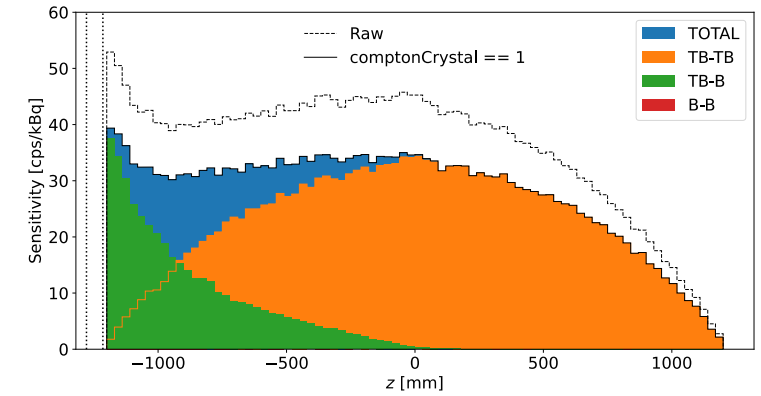
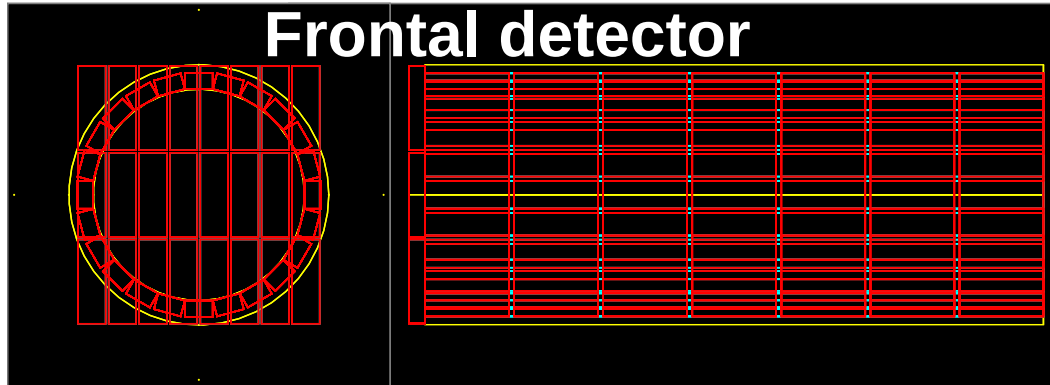
- Written in Python
- Currently under (private) development on GitHub
- Collection of tools (initially developed for J-PET) to:
 - Interact with CASToR datafiles
 - Interact with Interfile images
 - Apply some transformations on GATE output files
 - ...

Example use case: Bootstrap error estimates for the image quality metrics

Example use case: MLP/KDE reconstruction of the PET images

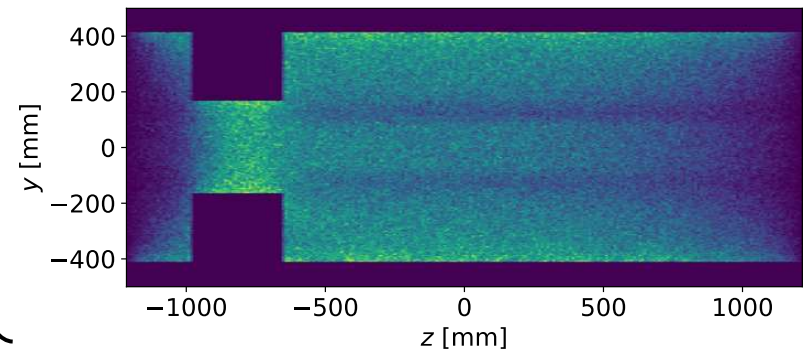
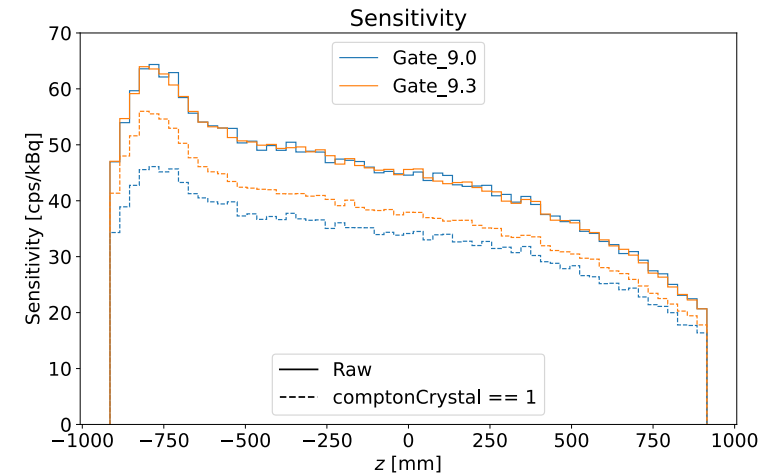
Simulation of multi-detector geometries

Combining the J-PET total body scanner with a second scanner intended for brain imaging



Issues found in Gate 9.3

- Ambiguity due to hard coded coincidence sorter “Coincidences”
- Compton scatter counts in detector
- MinSectorDifference: Comparing rSectorID from different scanners



2nd International Workshop on Machine Learning and Quantum Computing Applications in Medicine and Physics

WMLQ2024

04 to 07 June 2024, Warsaw Poland



<https://events.ncbj.gov.pl/event/314/>

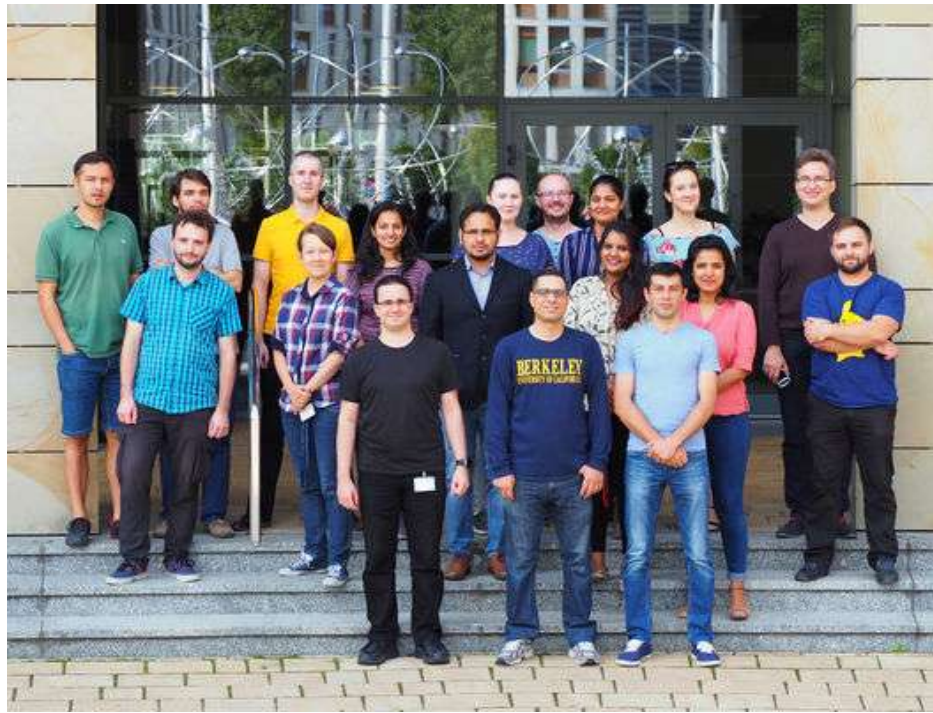


First edition:

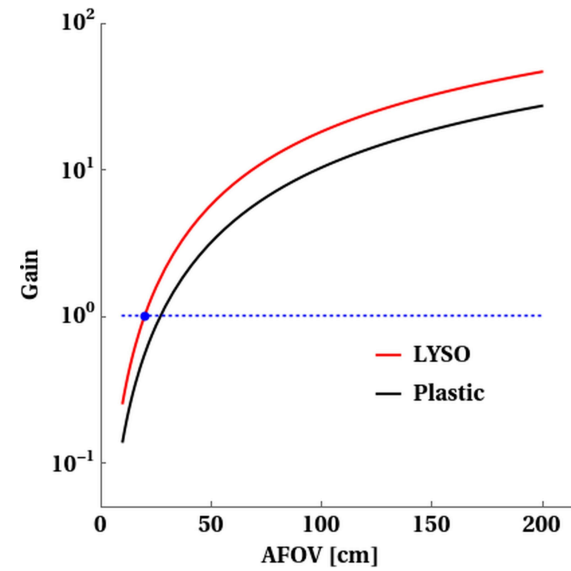
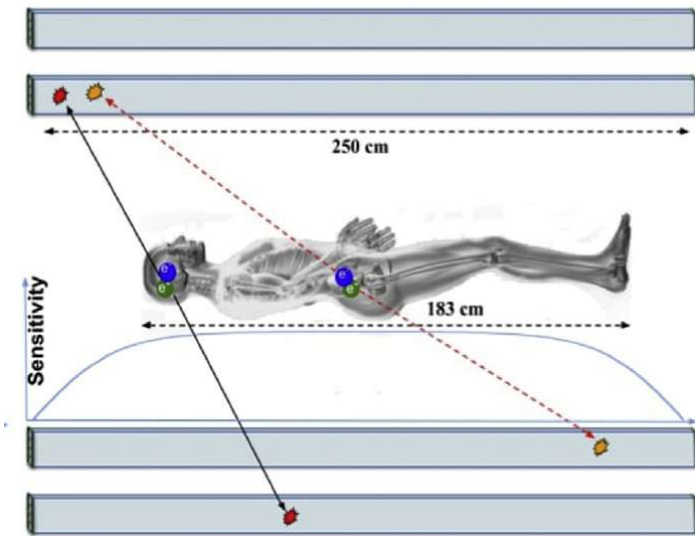


<https://events.ncbj.gov.pl/event/141/page/65-home>

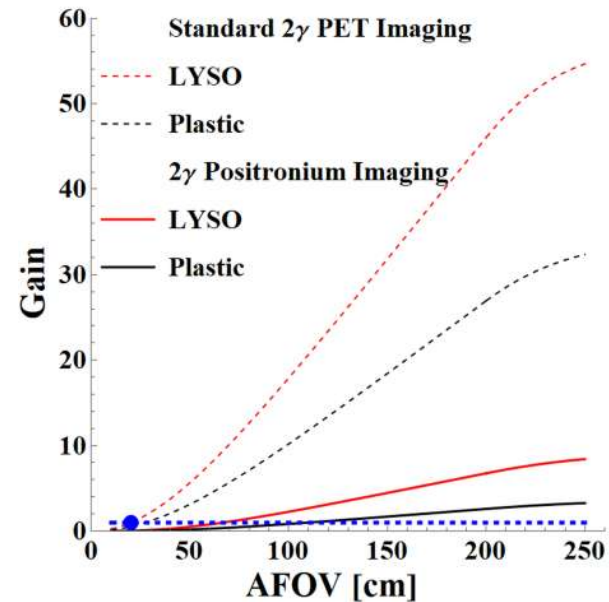
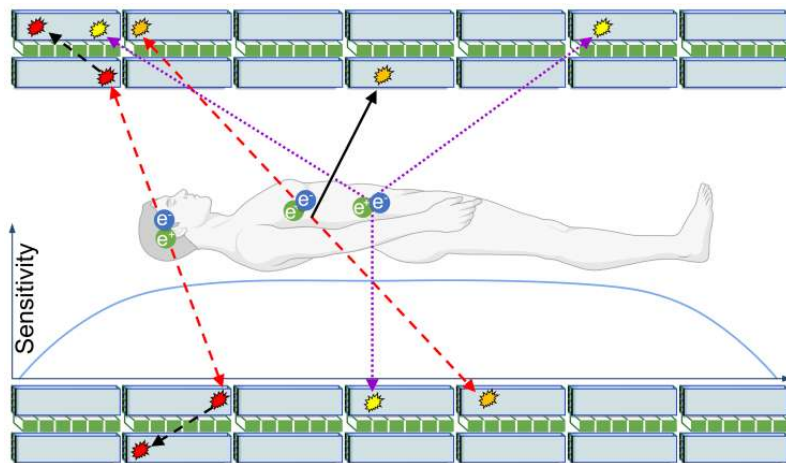
Thank you for attention



More materials available at:
<http://koza.if.uj.edu.pl/pet/>



P. Moskal, E. Ł. Stępień,
PET Clinics 15 (2020) 439

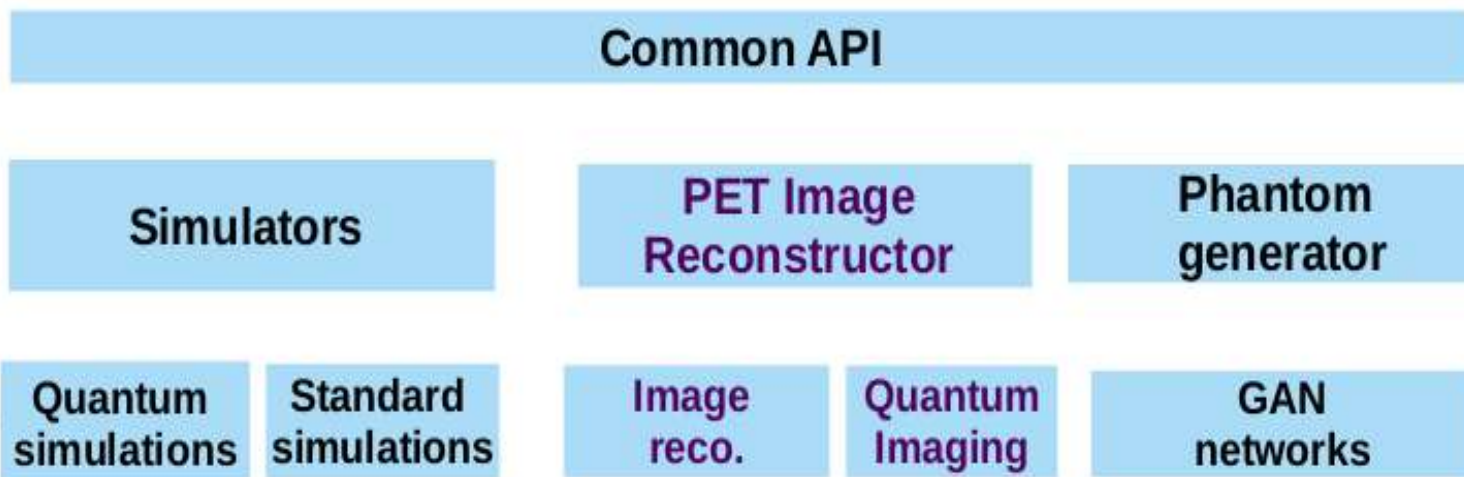


Quantum simulations and medical imaging software platform

Group:

- Wojciech Krzemień
- Konrad Klimaszewski
- Mateusz Bała
- Oleksander Fedoruk
- Lech Raczyński
- Tobiasz Jarosiewicz

Services



Libraries



Software for total-body J-PET

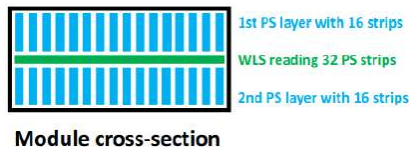
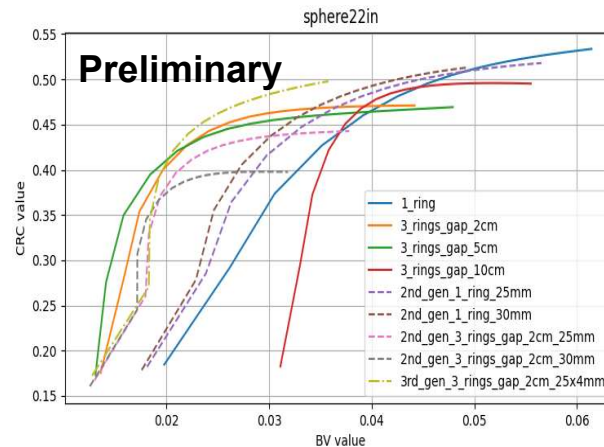
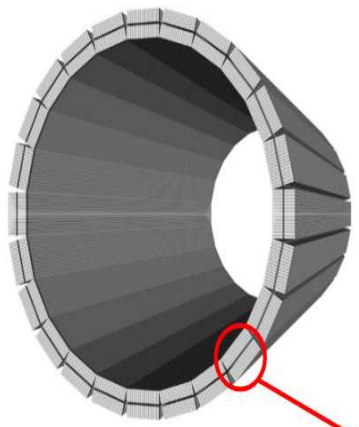
- scatter and random correction for total-body scanners
(see **Szymon Parzych talk tomorrow**)
- Normalization corrections
(see **A. Coussat's talk this afternoon**)
- point-spread functions
- system matrix parametrization
- Multi-photon + conventional PET reco. algorithms
- **Machine learning techniques for background reduction**
- Various software tools

Coordinator: W. Krzemien

- Jakub Baran
- Lech Raczynski
- Szymon Parzych
- Mateusz Bała
- Paweł Kowalski
- Aurelien Coussat
- Damian Trybek



Extensive usage of GATE simulations



Python

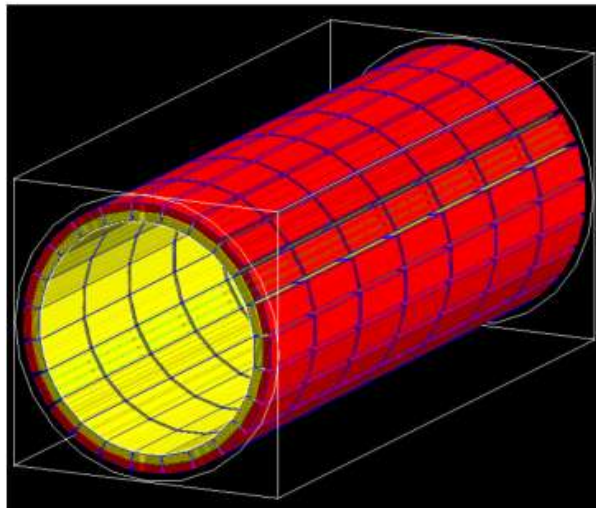
C++



GitHub

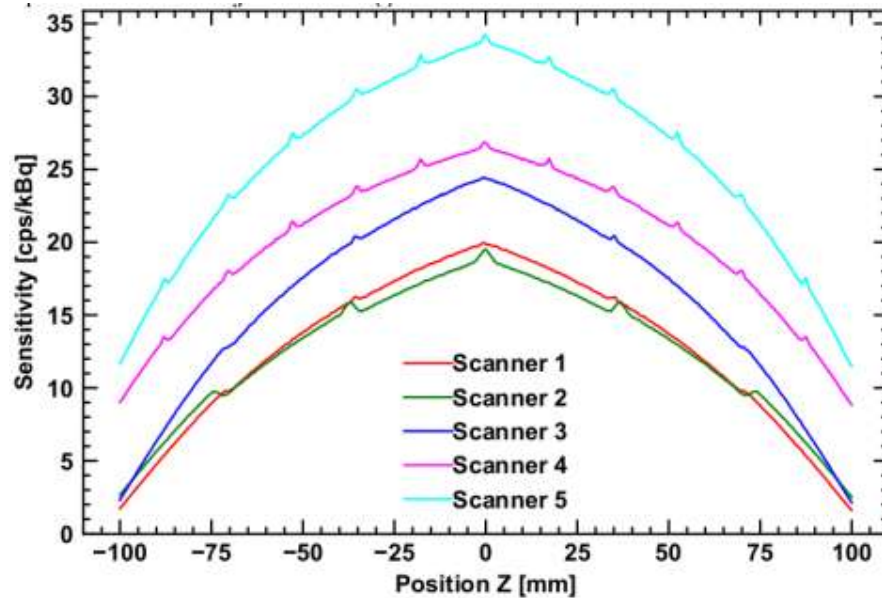


Total-Body J-PET Geometry Optimization

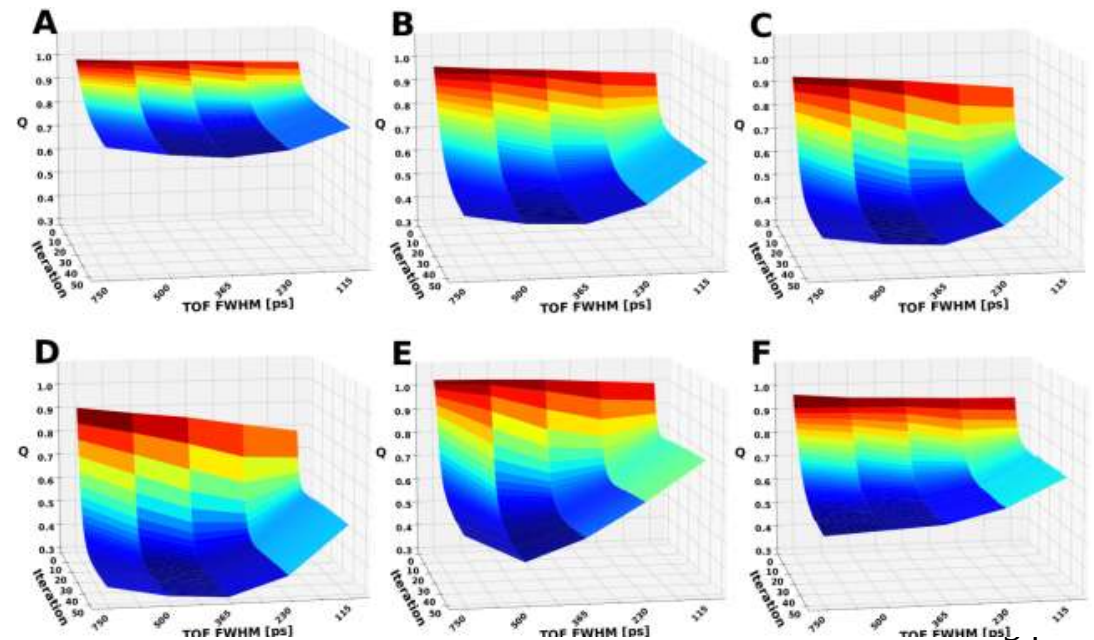


Property	Scanner geometry				
	<i>S1</i>	<i>S2</i>	<i>S3</i>	<i>S4</i>	<i>S5</i>
Radius [mm]	506	506	425	414.65	414.65
Axial FOV [mm]	2099.2	2159.2	2099.2	2430	2430
Scintillator length [mm]	686.4	686.4	686.4	330	330
Scintillator cross-section [mm]	25x5.7	25x5.7	25x5.7	25x6.0	30x6.0
No of adjacent rings	3	3	3	7	7
Gap between adjacent rings [mm]	20	50	20	20	20

preliminary Sensitivity

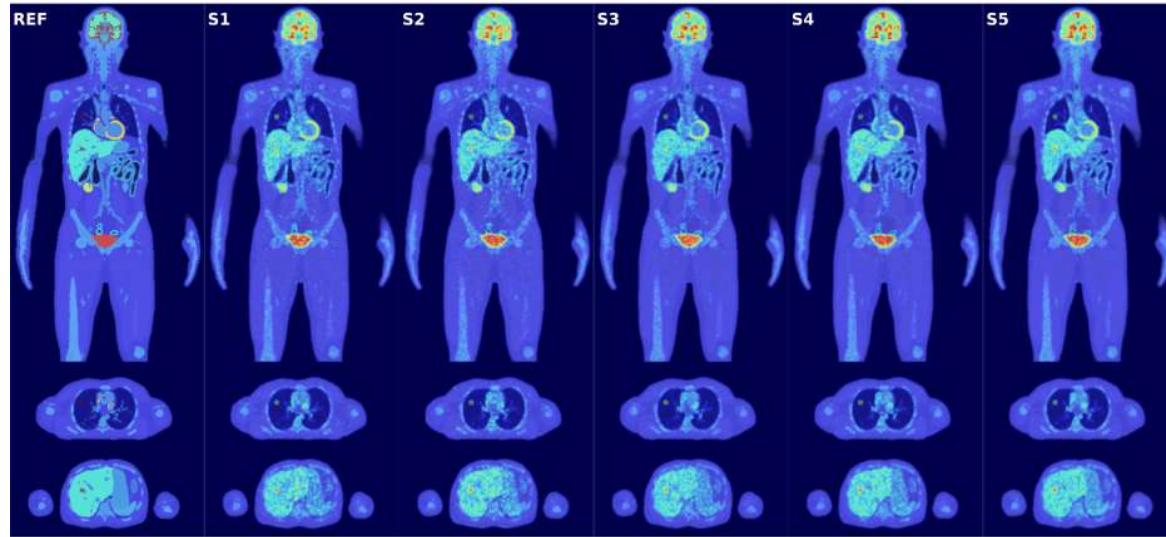


TOF kernel choice



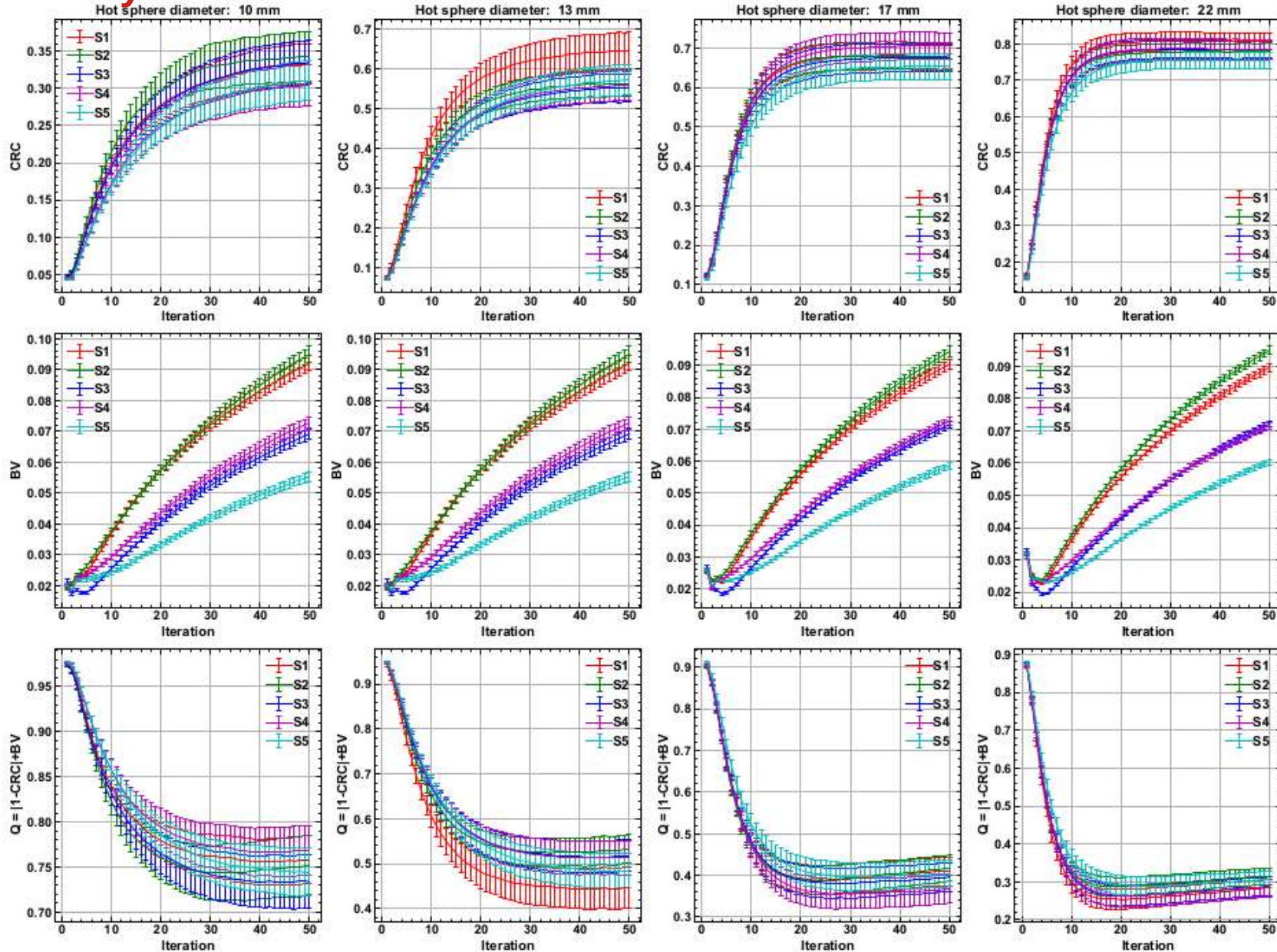
Total-Body J-PET Geometry Optimization – XCAT phantom

preliminary



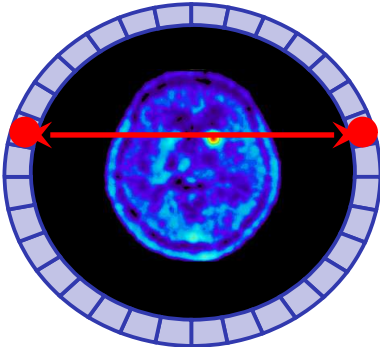
Total-Body J-PET Geometry Optimization – XCAT phantom

preliminary

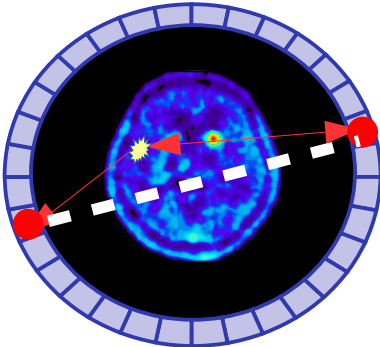


Coincidence classification for total-body J-PET

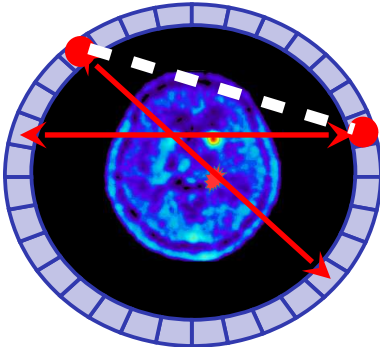
True events



Scattered events

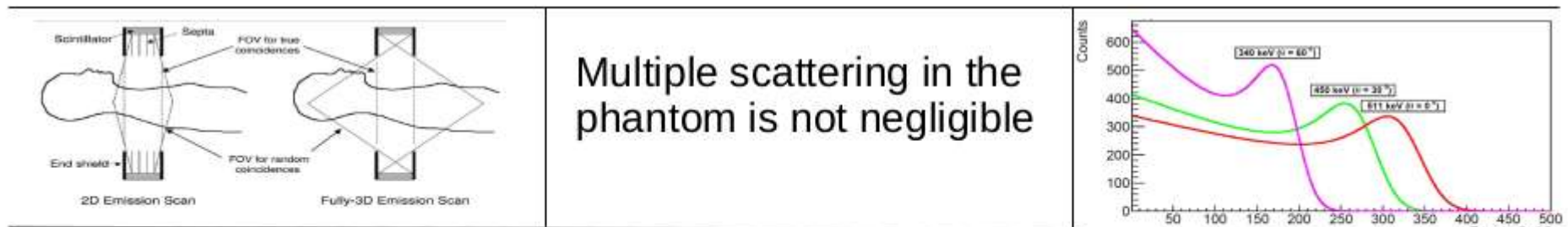


Random events



Coincidence classification for total-body J-PET

For total-body J-PET scanner we expect higher background level from non-genuine coincidences

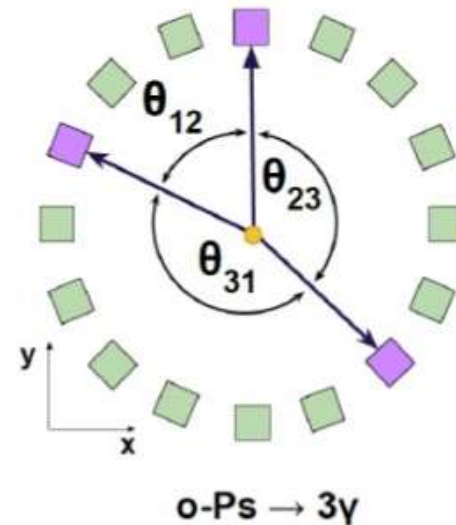


D. Brasse et al. J Nucl Med 2005; 46:859–867

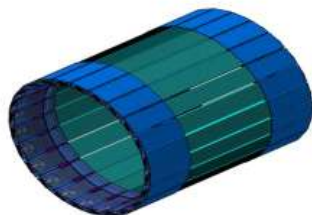
Situation much more complicated for multi-photon coincidences...

- More photons → More combinations
- Less strictly defined geometry
- Photon energies have a distribution

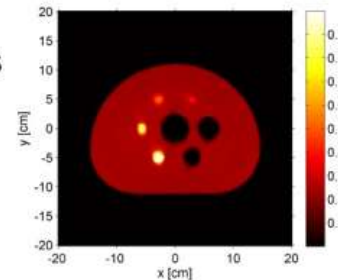
Idea: apply ML techniques to reduce background (ACCIDENTAL, SCATTER)



Training data generation



Monte Carlo Simulations



Modular J-PET

- 50 cm AFOV
- 24 modules x 13 strips
- 24 x 6 x 500 mm strips

NEMA IEC Phantom

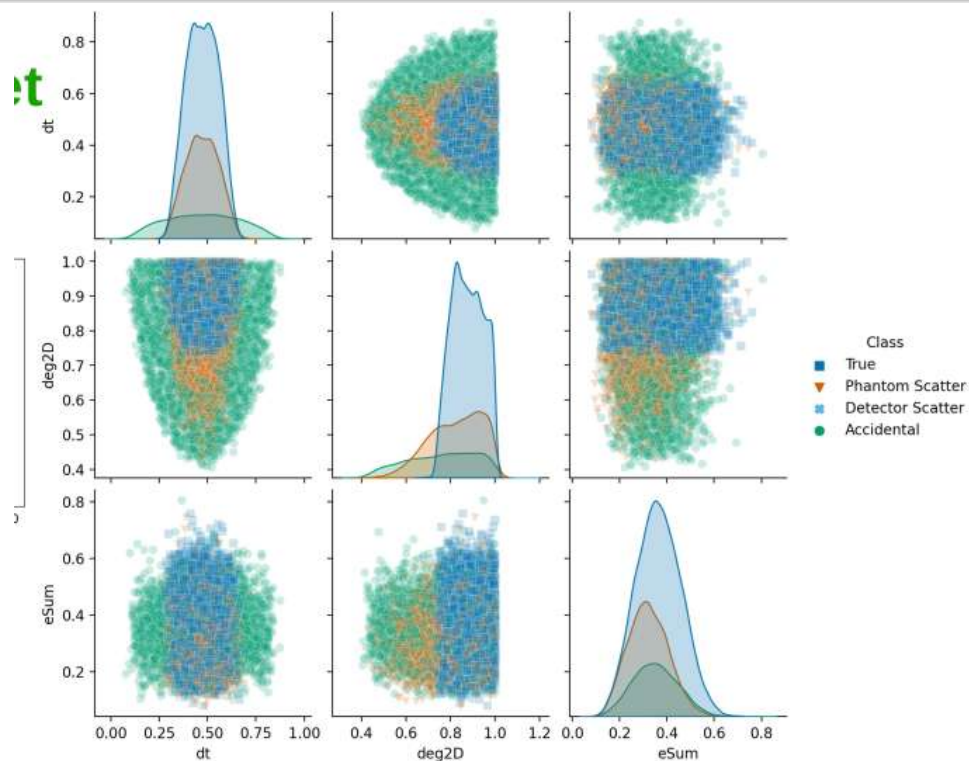
- 4 hot spheres
- 2 cold spheres
- Activity - 59 Mbq
- acquisition time - 500 seconds
- contrast between hot and cold regions – 4:1

GATE MC Simulation

- 30M coincidences
- Phenomenological time, energy and positional resolution
- Geometry cuts → reduce accidental fraction



21



- Feedforward Neural Network



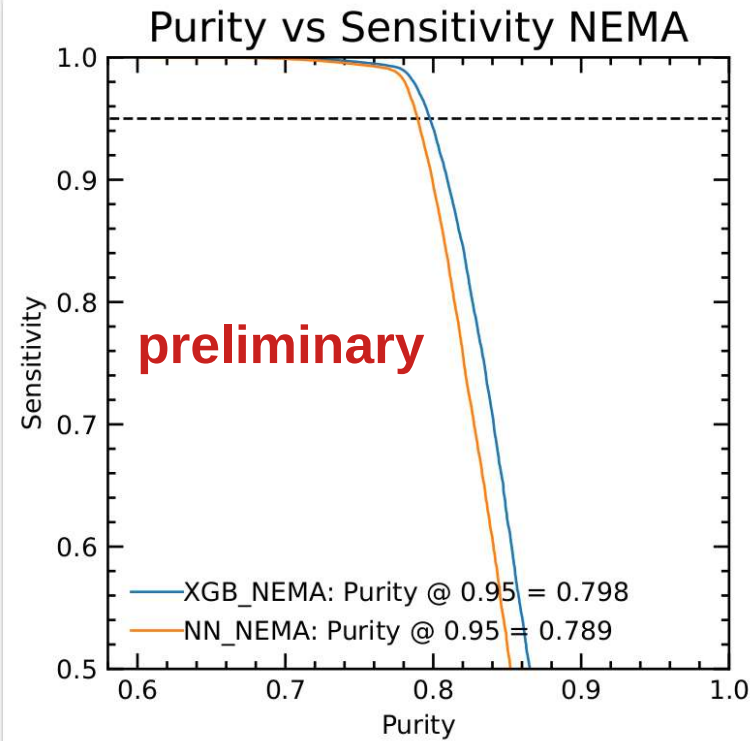
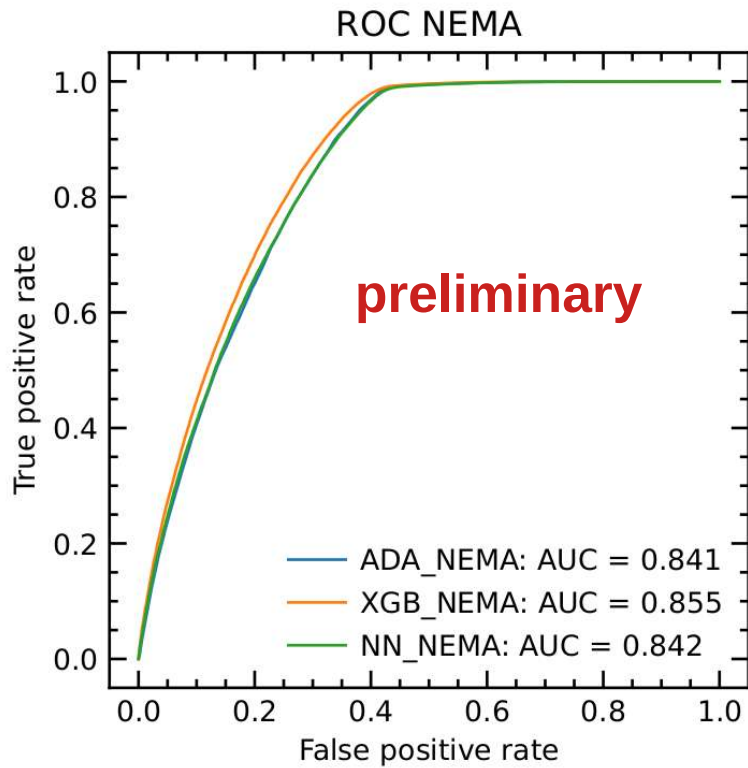
- ADABOOST



- XGBoost



Base line: 65%





Summary 2

- Two applications of ML to data filtering in (J-PET) tomography:
 - reduction of the scatter/random fractions in two-photon case
 - No visible bias observed in reconstructed images
- First trial to apply ML to multiphoton case
- S/B $\sim 10x$ improvement
- First positronium lifetime spectra obtained



OPEN ACCESS

PAPER



Feasibility study of the positronium imaging with the J-PET tomograph

RECEIVED
31 May 2018

REVISED
21 December 2018

ACCEPTED FOR PUBLICATION
14 January 2019

PUBLISHED
7 March 2019

Original content from this work may be used under the terms of the [Creative Commons Attribution 3.0 licence](#).

Any further distribution of this work must maintain attribution to the author(s) and the title of the work, journal citation and DOI.



P Moskal¹, D Kisielewska¹, C Curceanu², E Czerwiński¹, K Dulski¹, A Gajos¹, M Gorgol¹, B Hiesmayr⁴, B Jasińska³, K Kacprzak¹, Ł Kapłon¹, G Korcyl¹, P Kowalski³, W Krzemień⁶, T Kozik¹, E Kubicz¹, M Mohammed^{1,7}, Sz Niedźwiecki¹, M Pałka¹, M Pawlik-Niedźwiecka¹, L Raczyński², J Raj¹, S Sharma¹, Shivani¹, R Y Shopa³, M Silarski¹, M Skurzok¹, E Stępień¹, W Wiślicki¹ and B Zgardzińska³

¹ Faculty of Physics, Astronomy and Applied Computer Science, Jagiellonian University, 30-348 Cracow, Poland

² INFN, Laboratori Nazionali di Frascati, 00044 Frascati, Italy

³ Institute of Physics, Maria Curie-Skłodowska University, 20-031 Lublin, Poland

⁴ Faculty of Physics, University of Vienna, 1090 Vienna, Austria

⁵ Department of Complex Systems, National Centre for Nuclear Research, 05-400 Otwock-Świerk, Poland

⁶ High Energy Physics Division, National Centre for Nuclear Research, 05-400 Otwock-Świerk, Poland

⁷ Department of Physics, College of Education for Pure Sciences, University of Mosul, Mosul, Iraq

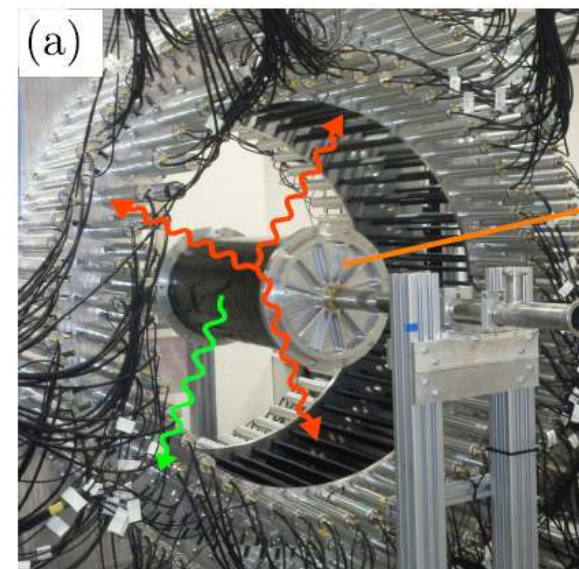
E-mail: daria.kisielewska@uj.edu.pl

Keywords: positron emission tomography, positronium atom, J-PET

Abstract

A detection system of the conventional PET tomograph is set-up to record data from e^+e^- annihilation into two photons with energy of 511 keV, and it gives information on the density distribution of a radiopharmaceutical in the body of the object. In this paper we explore the possibility of performing the three gamma photons imaging based on ortho-positronium

First in the world orthopositronium image of the object



nature communications

[View all journals](#) [Search Q](#) [Login](#)

[Explore content](#) [About the journal](#) [Publish with us](#)

[Sign up for alerts](#) [RSS feed](#)

[nature](#) > [nature communications](#) > [articles](#) > [article](#)

Article | [Open Access](#) | [Published: 27 September 2021](#)

Testing CPT symmetry in ortho-positronium decays with positronium annihilation tomography

P. Moskal, A. Gajos, [...] W. Wiślicki

Nature Communications 12, Article number: 5658 (2021) | [Cite this article](#)

3124 Accesses | 1 Citations | 40 Altmetric | [Metrics](#)

Abstract

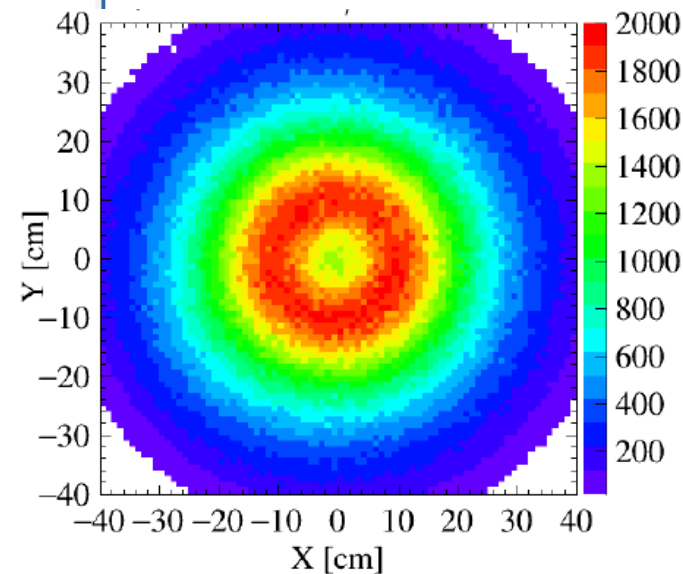
Charged lepton system symmetry under combined charge, parity, and time-reversal transformation (CPT) remains scarcely tested. Despite stringent quantum-electrodynamic limits, discrepancies in predictions for the electron-positron bound state (positronium atom) motivate further investigation, including fundamental symmetry tests. While CPT noninvariance effects could be manifested in non-vanishing angular correlations between final-state photons and spin of annihilating positronium, measurements were previously limited by knowledge of the latter. Here, we demonstrate tomographic reconstruction techniques applied to three-photon annihilations of ortho-positronium atoms to estimate their spin polarisation without magnetic field or polarised positronium source. We use a plastic-scintillator-based positron-emission-tomography scanner to record ortho-

Aleksander Gajos

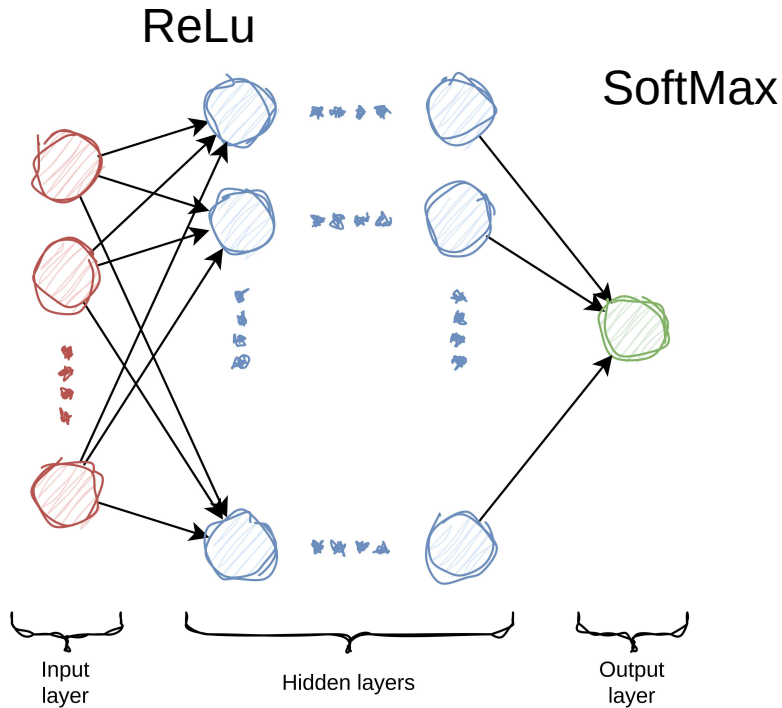
[Download PDF](#)

[Sections](#) [Figures](#) [References](#)

[Abstract](#)
[Introduction](#)
[Results](#)
[Discussion](#)
[Methods](#)
[Data availability](#)
[References](#)
[Acknowledgements](#)
[Author information](#)
[Ethics declarations](#)
[Additional information](#)
[Supplementary information](#)
[Rights and permissions](#)
[About this article](#)



Feedforward Neural Network



- Optimizer: Adam
- Loss: Customized loss function
- Size and number of hidden layers optimized using Cross Validation
- Optimization: Tree-Structure Parzen Estimation
- Input data normalized to (0, 1) range

Training/Validation/Test : 70%/15%/15%





Considered Features

Maximum feature space dimensions 46

- Deposited energies
- spatial hit coordinates
- registration time
- relative distance between hits
- relative time between hits
- total energy sum
- total energy of the annihilation photon candidates
- opening angles between photons after the preliminary vertex reconstruction
- interdetector scatter metric



New CASToR toolkits

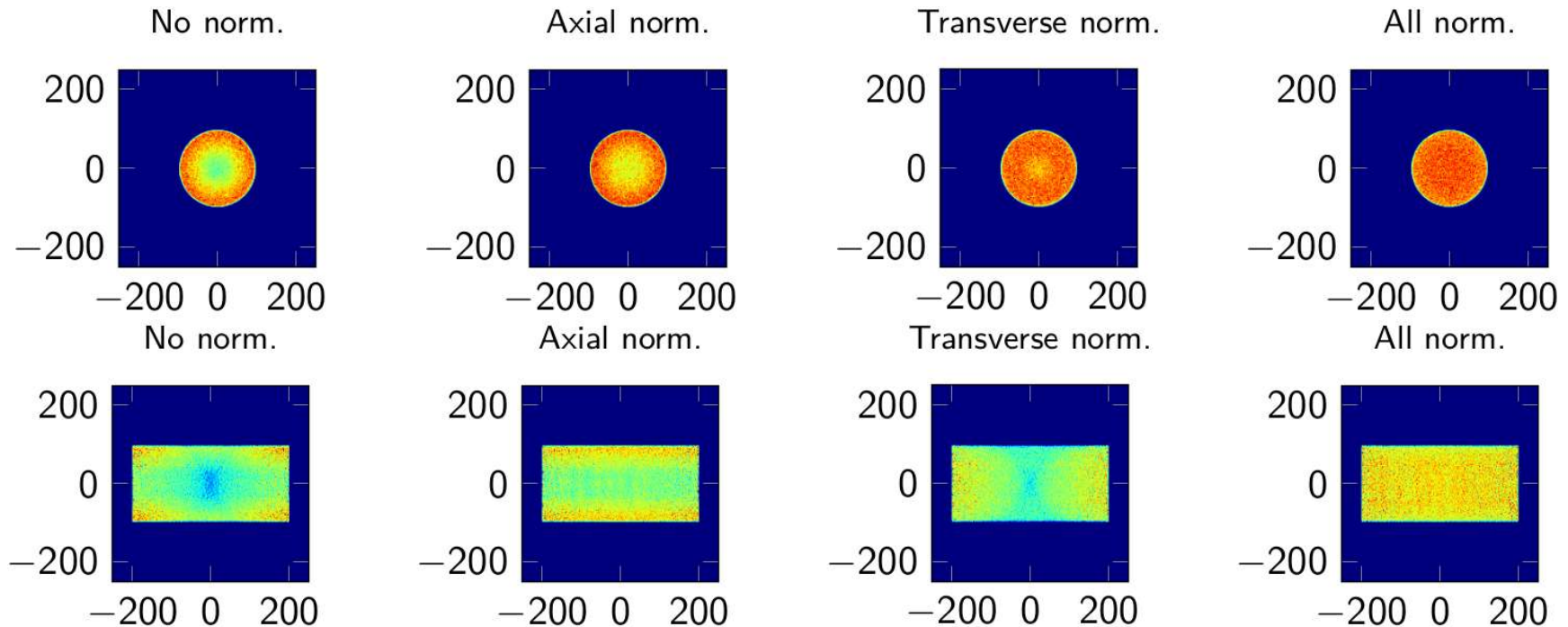
- `castor-norm`
- Compute direct normalization factors
- `castor-datafileMerger`
- Merge several datafiles into one

```
castor-norm \  
-df normalization_scan.Cdh \  
-img normalization_phantom.img \  
-sc Scanner \  
-fout output
```

```
castor-datafileMerger \  
-df input.Cdh \  
-norm with_normalization.Cdh \  
-fout output
```

Component-based normalization

- We developed a collection of scripts that compute, from GATE output, component-based normalization factors



Decrease efficiency of GATE dataset

- We developed a tool to decrease the efficiency of a GATE dataset, post-simulation, to assess efficiency normalization

