

**POLITECNICO**  
MILANO 1863

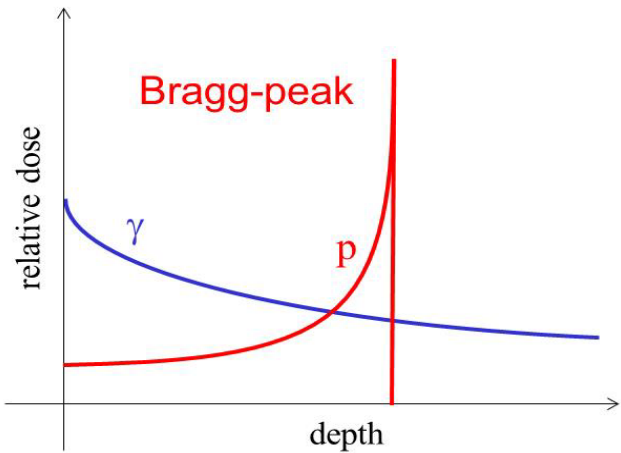
# Gamma-ray detectors for range and dose verification

**Carlo Fiorini**

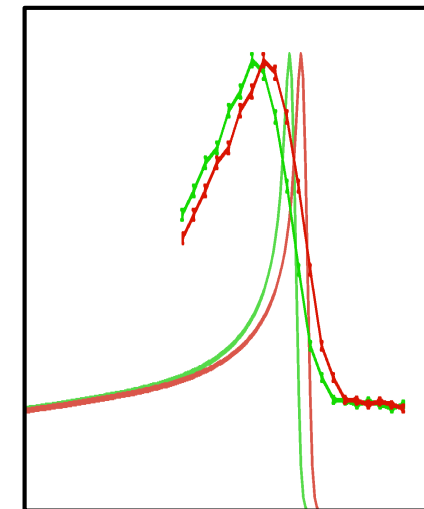
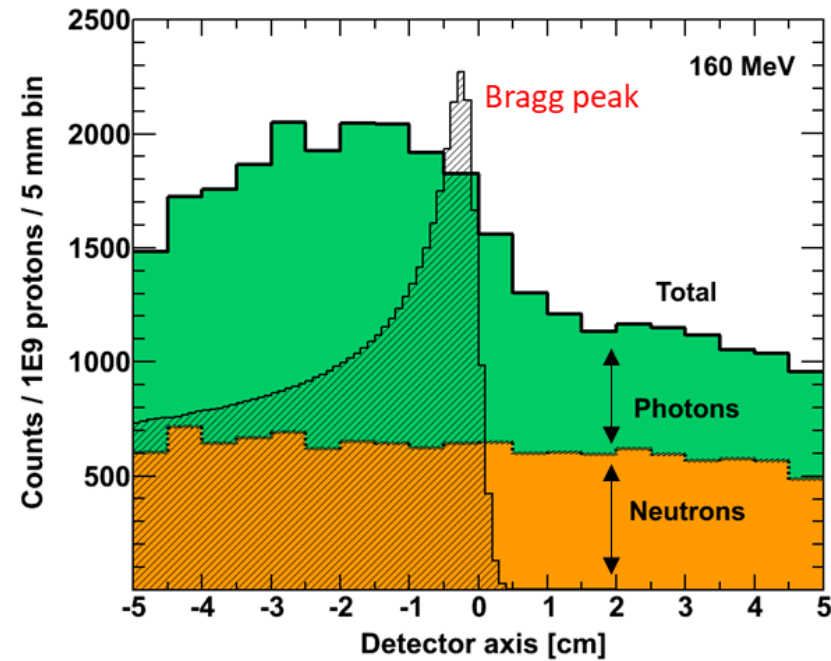
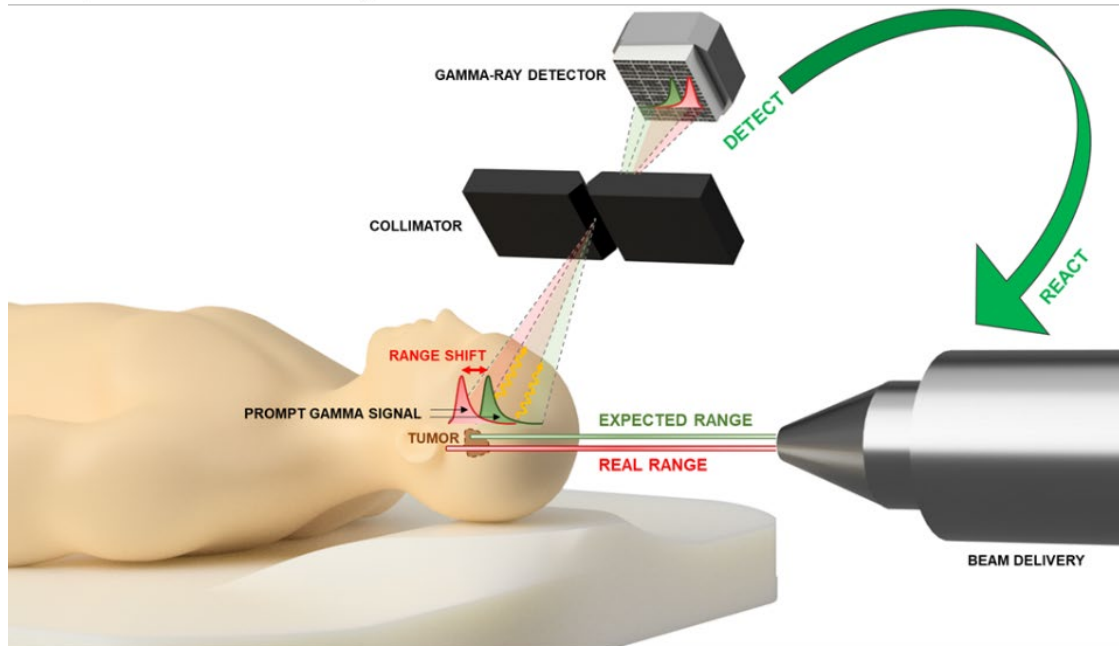
*Dipartimento di Elettronica, Informazione e Bioingegneria  
Politecnico di Milano, Italy*

- **Range verification by prompt-gammas detection in C-ions radiotherapy**
- **Dose measurements by gamma detection in BNCT (Boron Neutron Capture Therapy)**

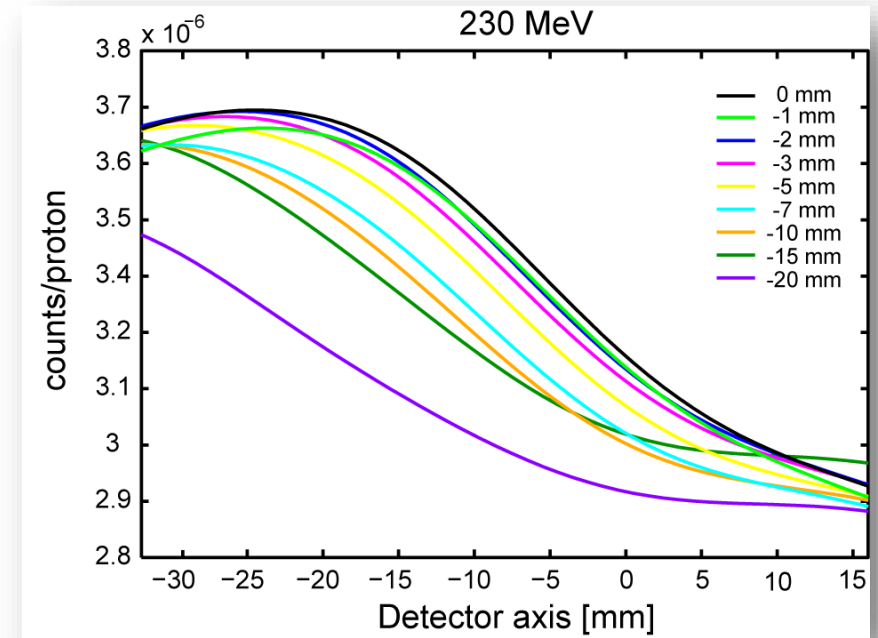
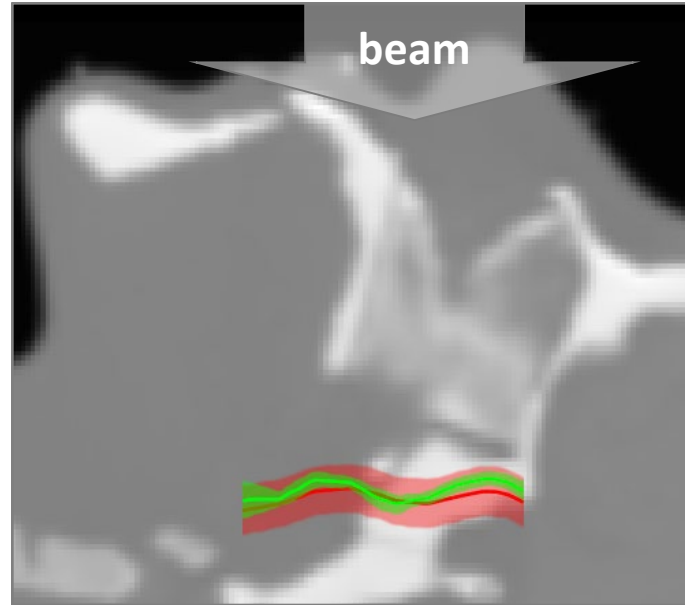
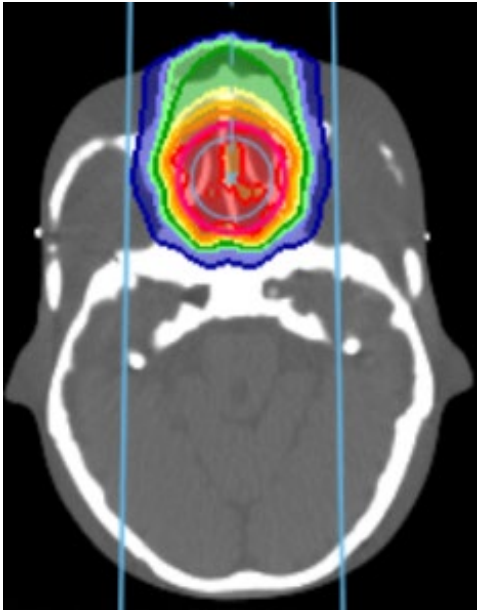
# Prompt Gamma Imaging (PGI) for Range Verification in Hadrontherapy



The measurement of the **particle beam range** in the target is very important: real range of proton beams in patients may contain **uncertainties** of up to 10-15 mm (uncertainties on tissue composition, density, organ motions, patient positioning, etc).



# Range Verification with protons



Shift measurements

Planning uncertainty > 5 mm  
(margin of 3.5% + 2 mm)

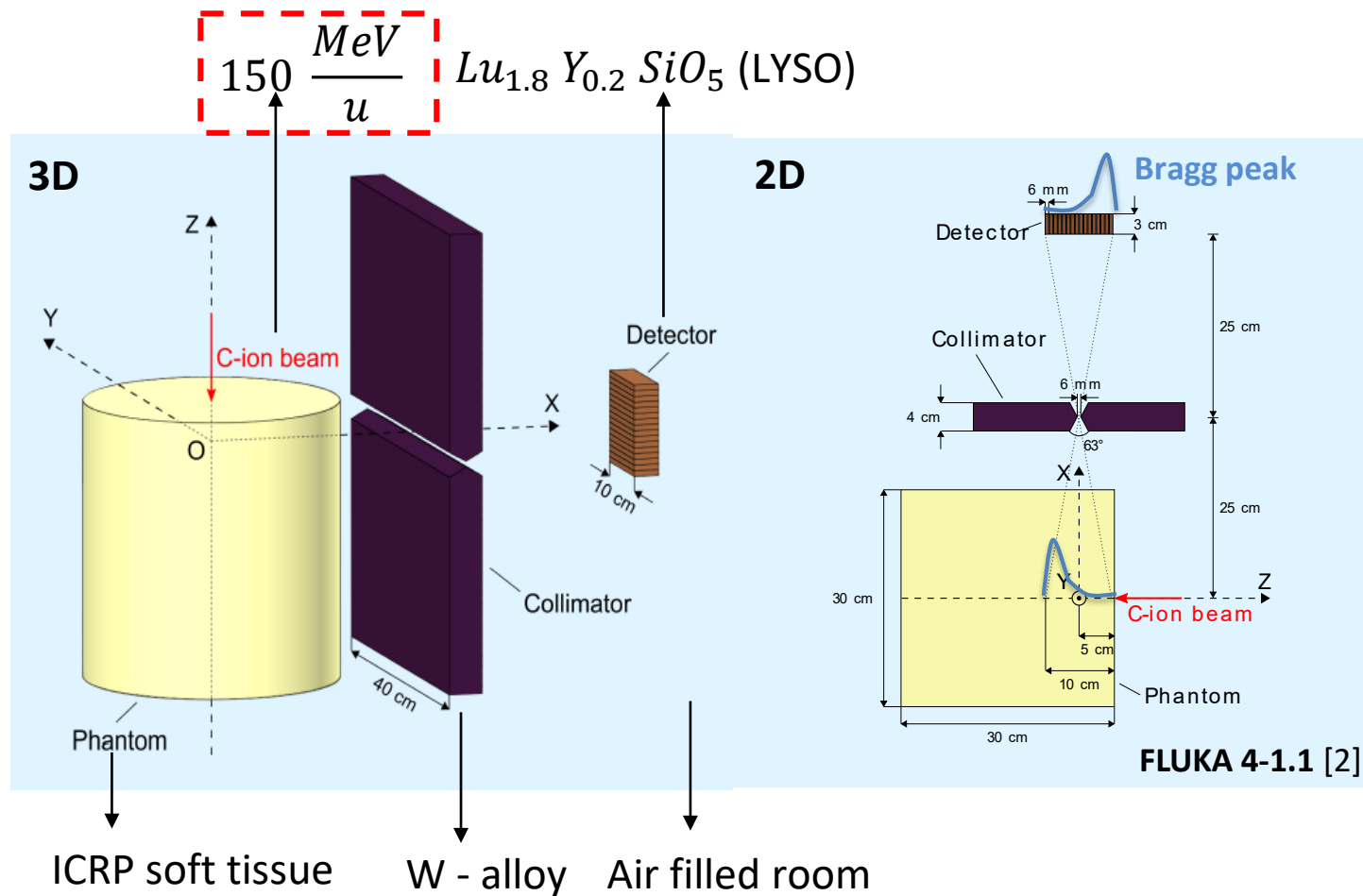
Measurement uncertainty ( $1.5\sigma$ )  
 $\approx$  2.0 mm

Clinical trial of PG camera  
for Proton irradiation

- C.Richter, et al., "First clinical application of a prompt gamma based in vivo proton range verification system", Radiother Oncol 2016;118:232–7.
- Y.Xie, et al., "Prompt gamma imaging for in vivo range verification of pencil beam scanning proton therapy", Int J Radiat Oncol Biol Phys 2017;99:210–8.

# Feasibility Study for Range Verification with C-ions (MC study)

Considered beam energy range of **120÷400 MeV/u** for C-ions (CNAO)



## Challenges for PGI with Carbon irradiation:

- Two orders of magnitude less carbon ions than protons used for irradiation (issue partially compensated by higher PG yield of carbon vs. proton)
- Secondary gammas reduces the range-end falloff
- Higher neutron background (vs. proton irradiation)

Scoring of the response of a **pixelated knife-edge slit camera** to the secondary particles emitted by a **ICRP soft tissue phantom**.

Energy interval: **3-7 MeV**

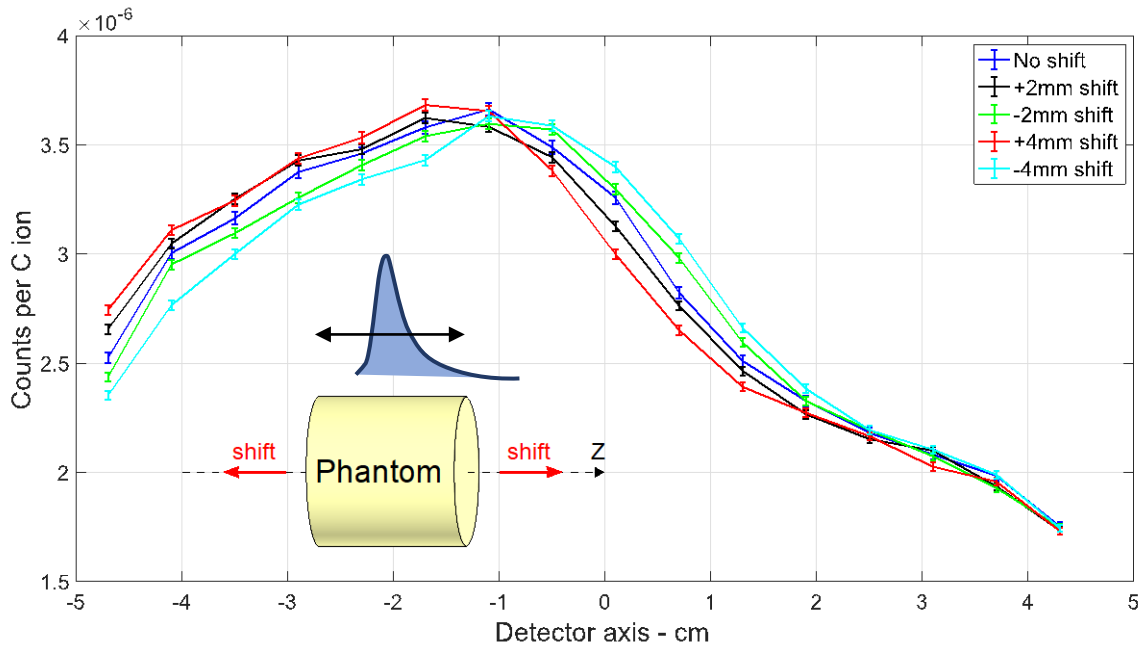
A.Missaglia, et al., **Prompt-gamma fall-off estimation with C-ion irradiation at clinical energies, using a knife-edge slit camera: a Monte Carlo Study**, Physica Medica 107, art. no. 102554, 2023.

# Reconstructed PGI profiles

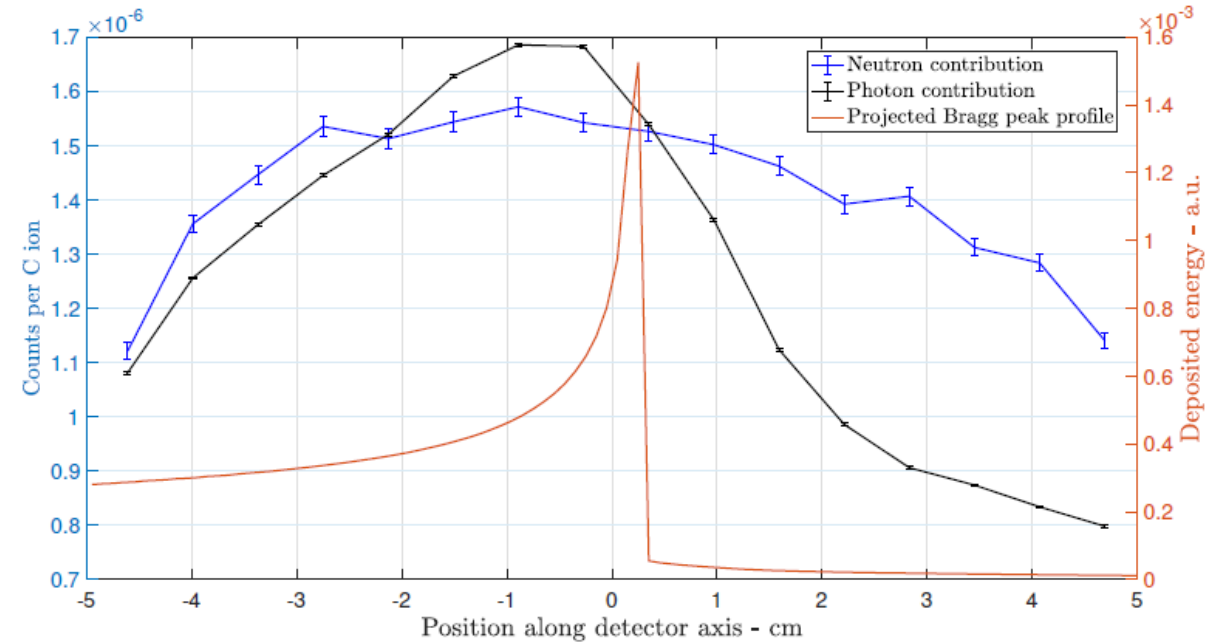
## Particle range sensitivity determination by target longitudinal shifts

- Spatial **correlation** between the **Bragg peak** and the **secondary gamma emission** in the high neutron background of CIRT.

Simulated primary particles for each shift of the phantom:  $4 \times 10^9$  carbon ions



Distinguishable PGI signal curves for different phantom shifts



Prompt-gamma component over an almost **uniform neutron background**

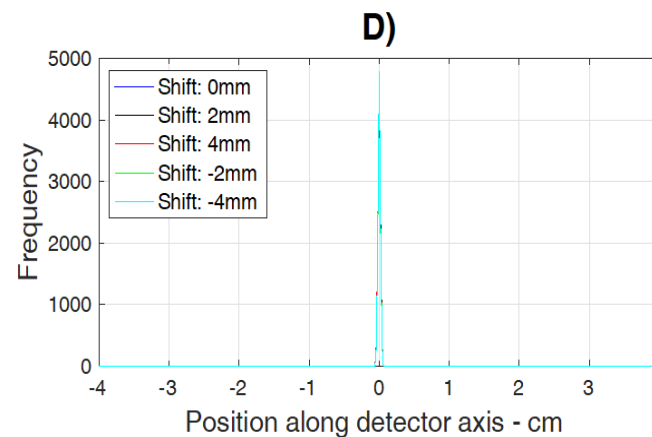
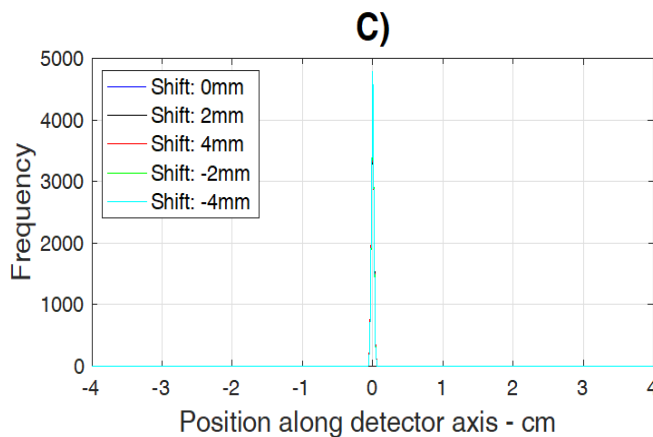
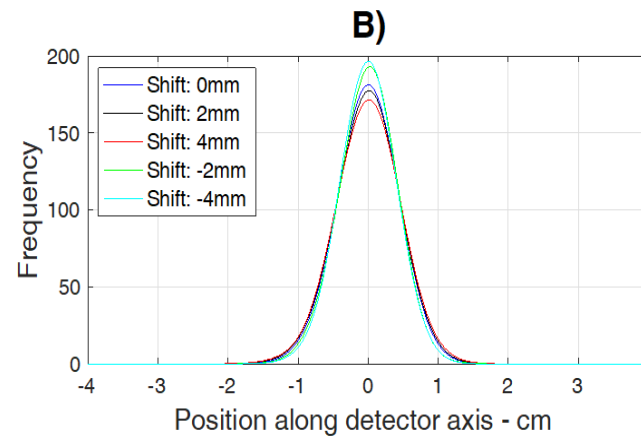
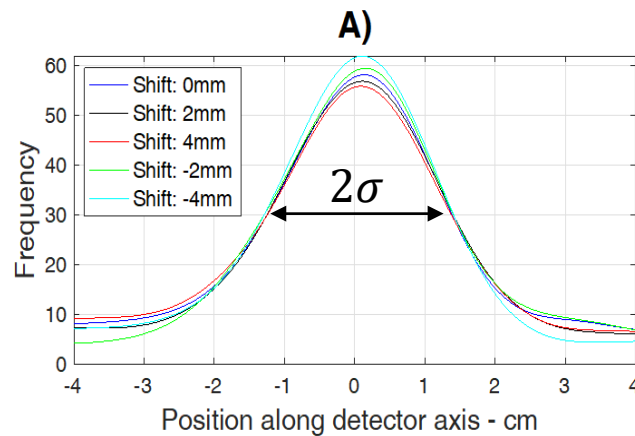
# Particle Range Precision Determination – Spot and Spill irradiations

Graphical representation of the **precision ( $2\sigma$ )** in retrieving the Bragg peak fall-off for **different phantom shifts and number of C-ions** : A)  $10^6$  , B)  $10^7$  , C)  $10^8$  , D)  $10^{10}$

irradiation **spot**

irradiation **spill**

upper bound (e.g. FLASH therapy)

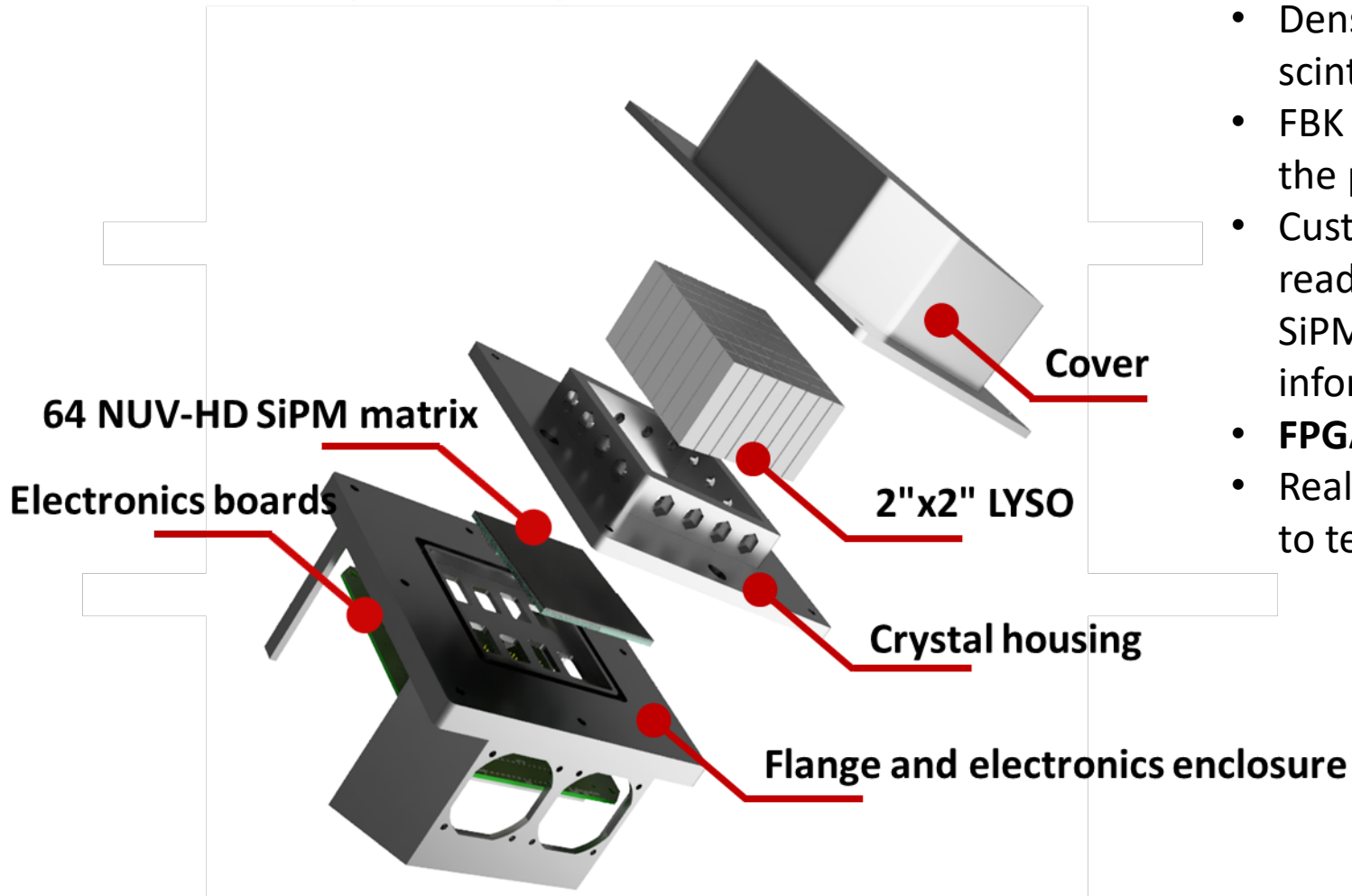


➤ **Spot irradiation** to the phantom for different number of incident carbon ions ( $10^6$ ,  $10^7$ ,  $10^8$  and  $10^{10}$ ) → **~ 10 mm.**

➤ **spill irradiation**, namely  **$5 \times 10^7$  ions** → From *range retrieval analysis*: **4.2 mm** precision.

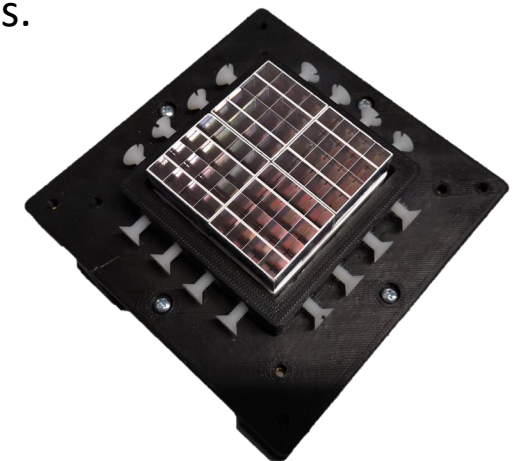
# Toward the Development of a PGI System for CIRT

## FIRST PROTOTYPE (64 channel)



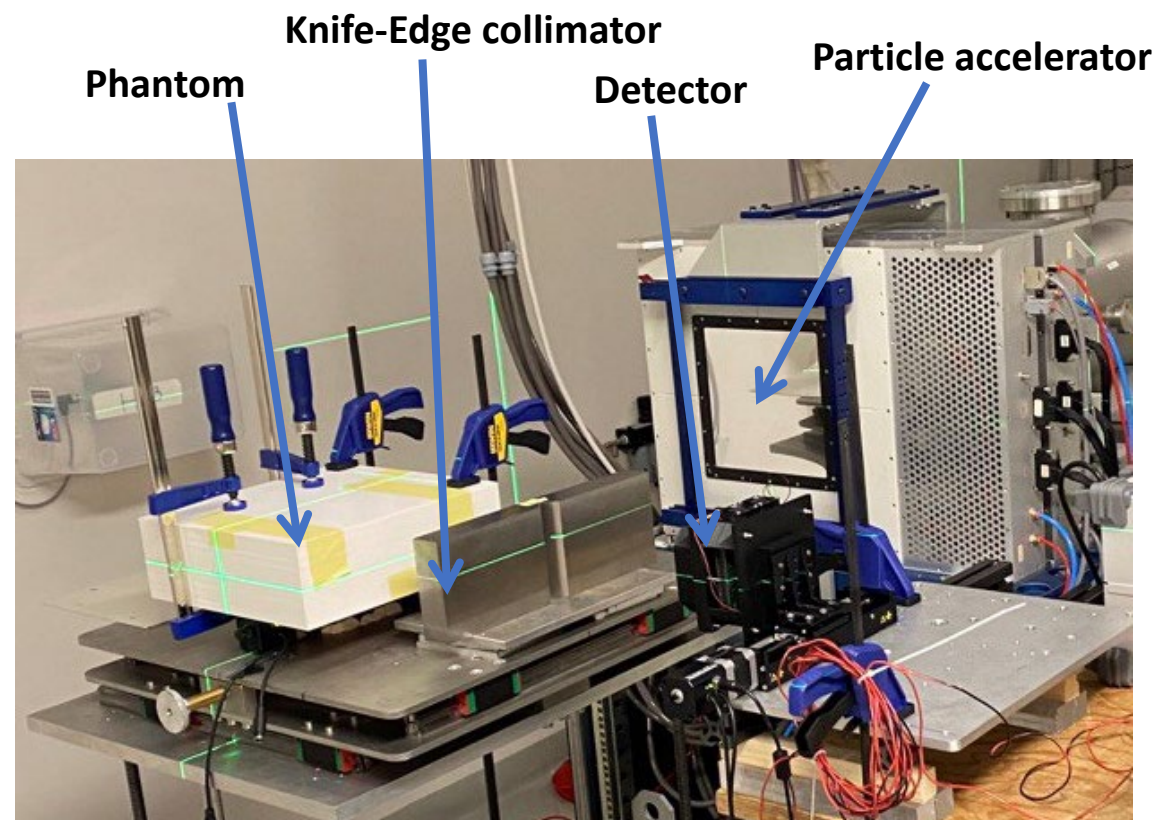
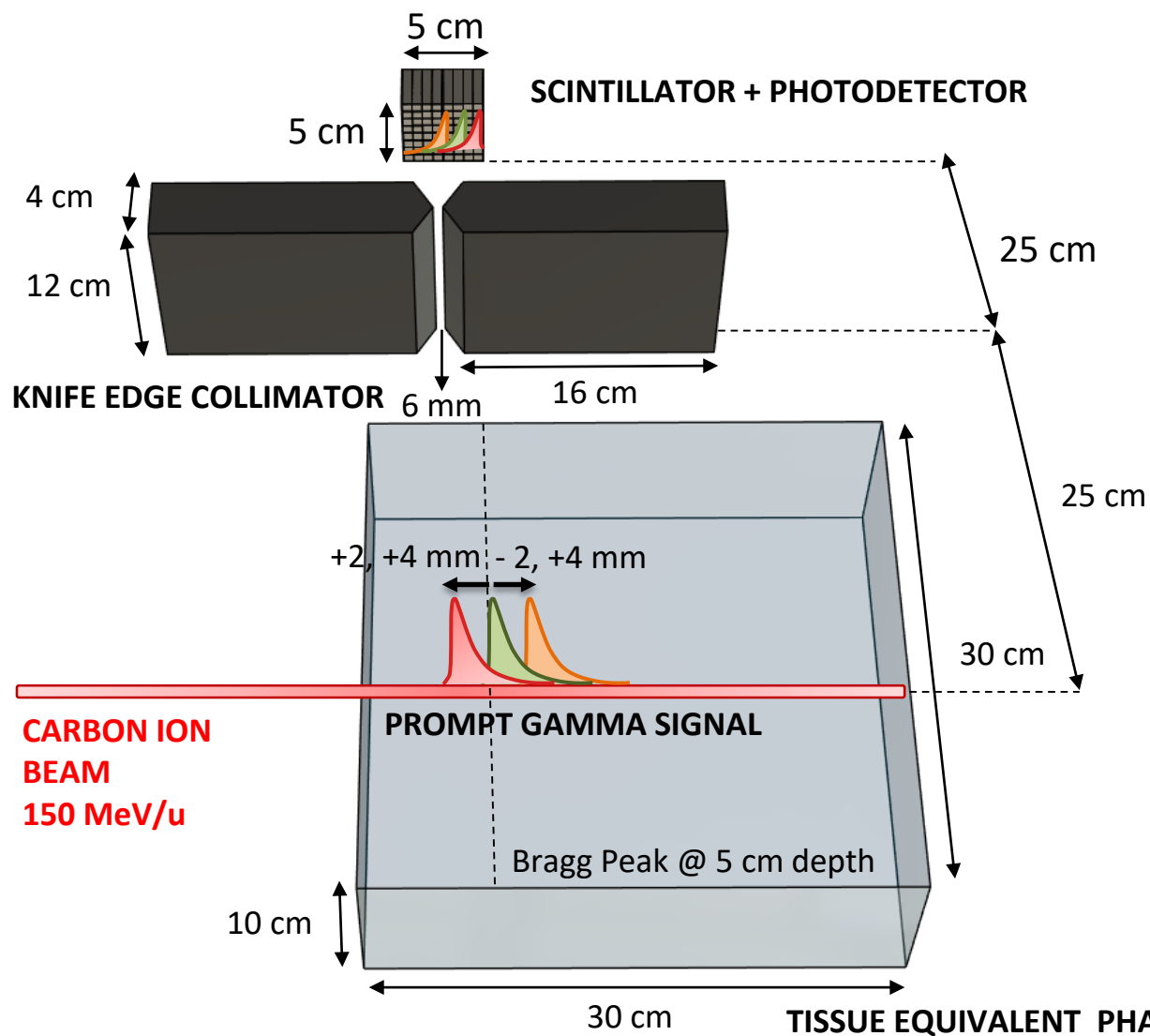
## SYSTEM FEATURES

- Dense, fast, high light yield pixelated **LYSO** scintillator.
- FBK **NUV-HD SiPMs** suitable for **1:1 coupling** with the pixelated scintillator.
- Custom **16-ch GAMMA ASIC** that has the goal to read monolithically the current supplied by each SiPM and to provide in output the energy information of the gamma ray.
- **FPGA-based DAQ system**.
- Real-time **compensation of SiPM gain drifts** due to temperature variations.





# Knife Edge Slit Camera Setup Configuration at CNAO

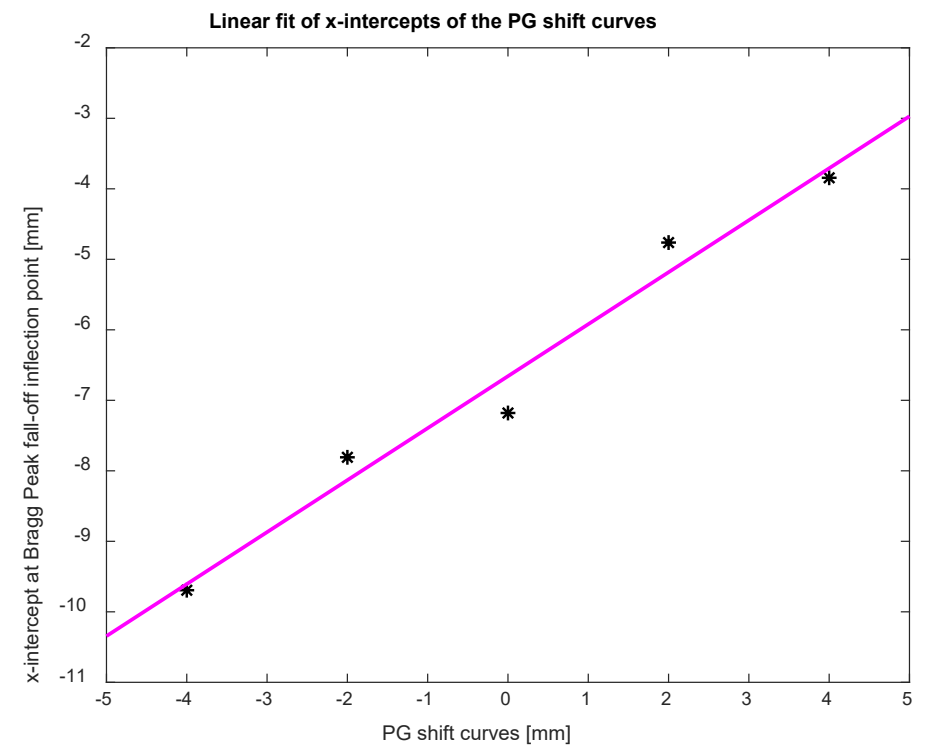
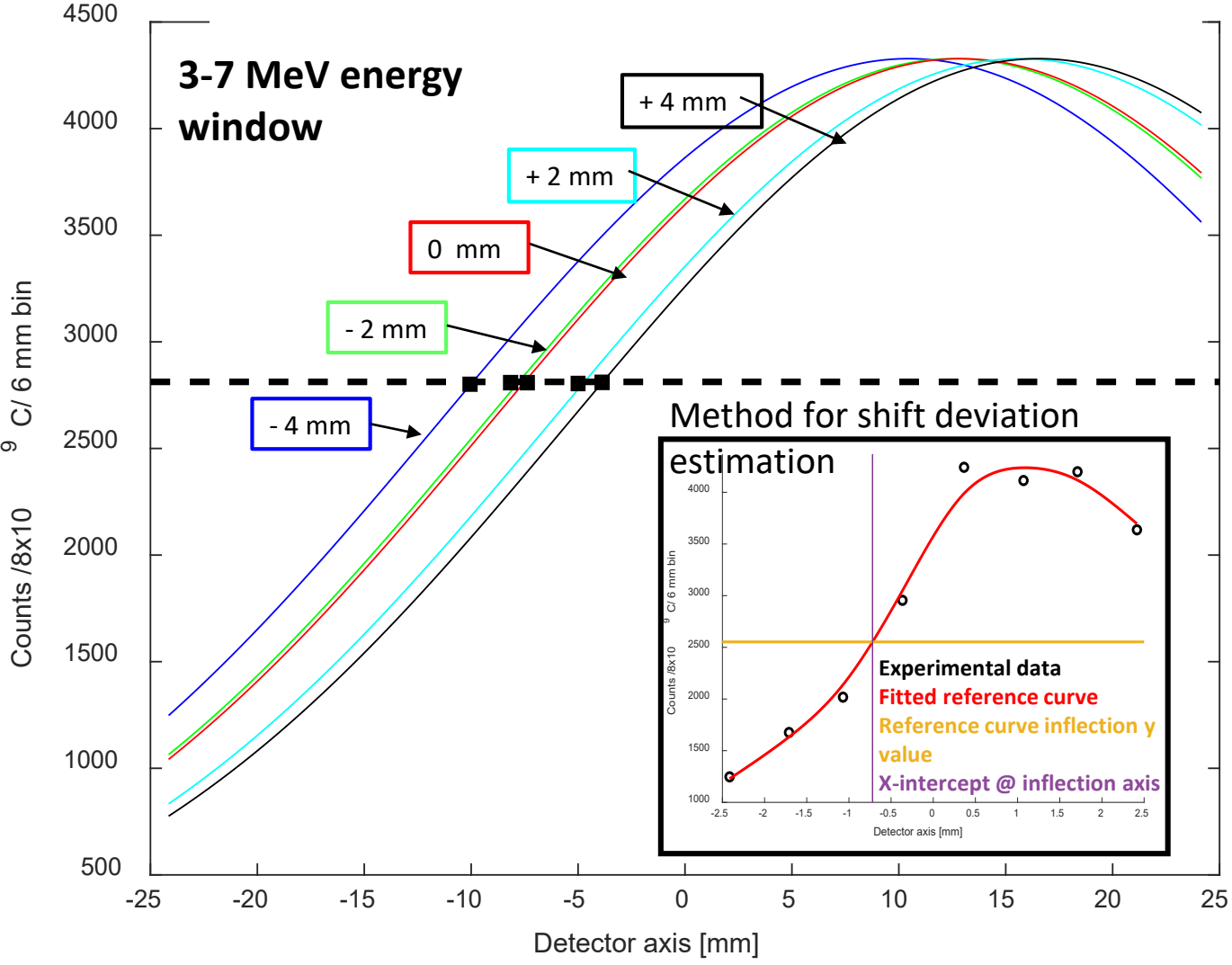


**Particle beam structure:**

100 spills of  $8 \times 10^7$  carbon ions =  $8 \times 10^9$  carbon ions

# Analysis of Experimental Data: Curve Shifts (preliminary)

$$N_{C-ions} = 8 \times 10^9$$

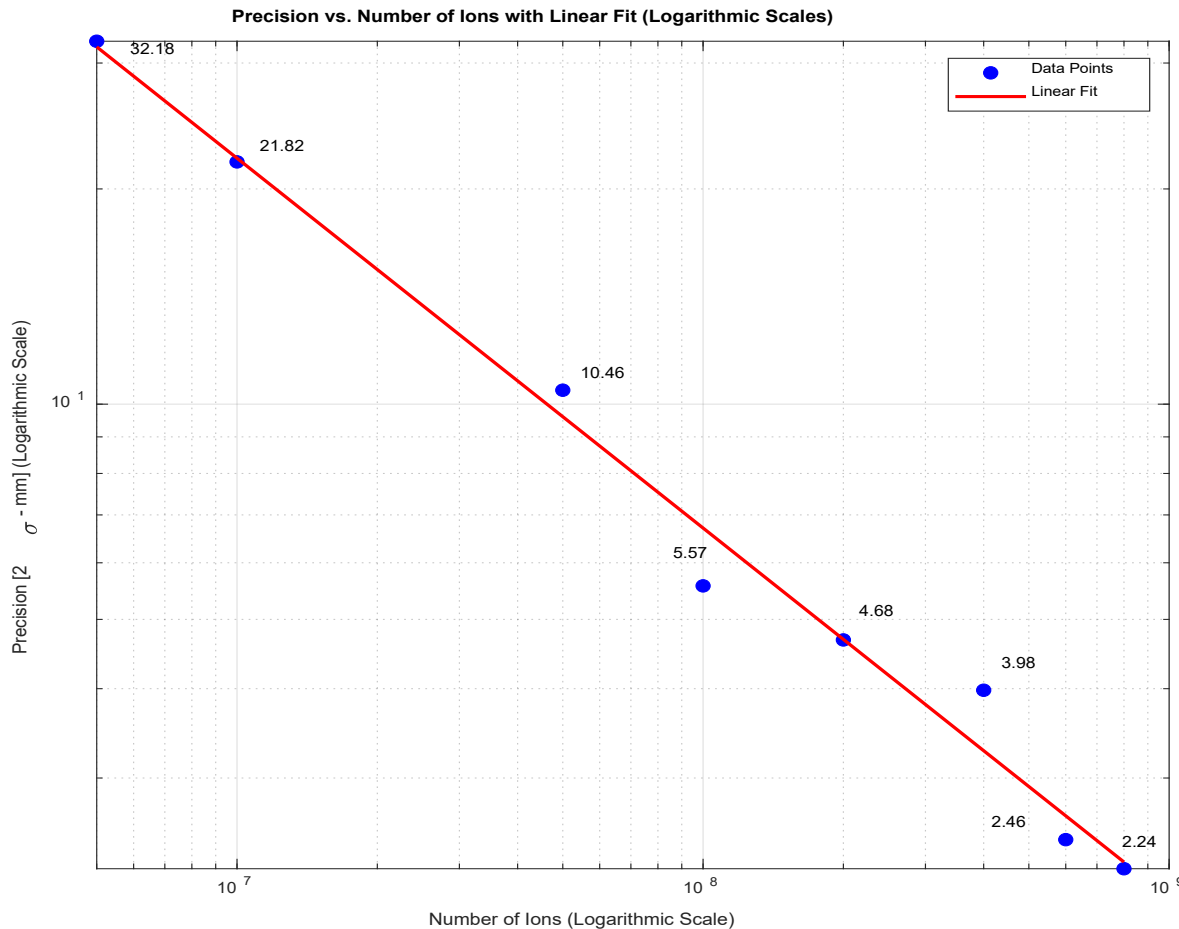


**Mean deviation from the expected shift positions: ~0.24mm**

# Range retrieval precision vs. number of Carbon ions (preliminary)

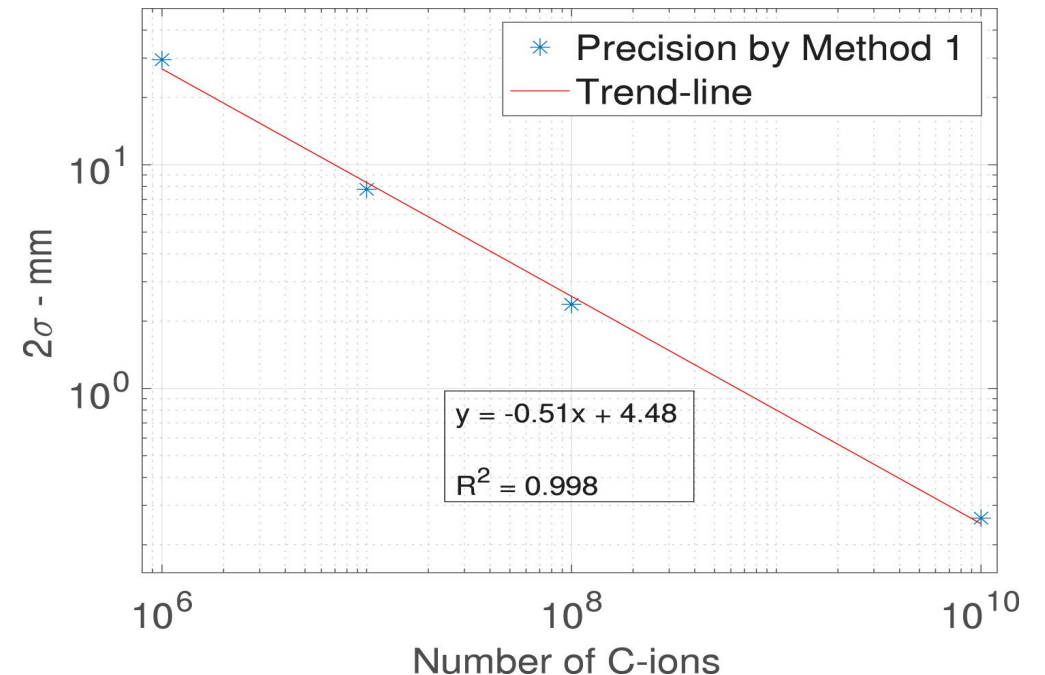
Linear interpolation of the double logarithmic data log(precision) VS log(Number of carbon ions).

The precision is proportional to  $N_{ions}^{-1/2} = \frac{1}{\sqrt{N_{ions}}}$



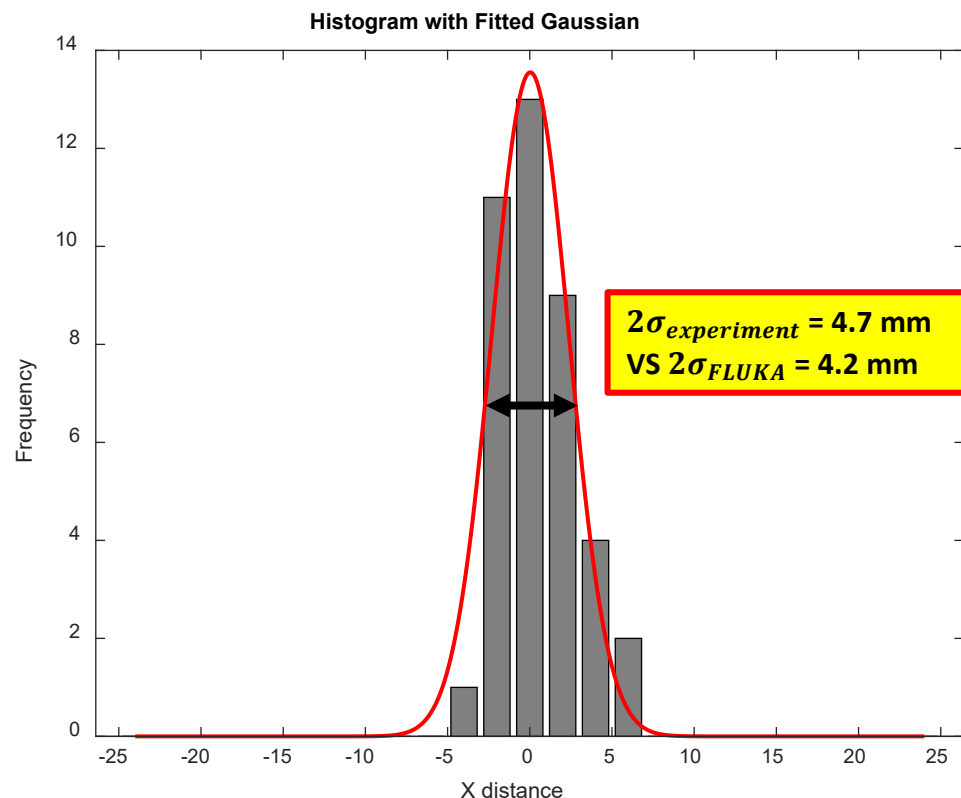
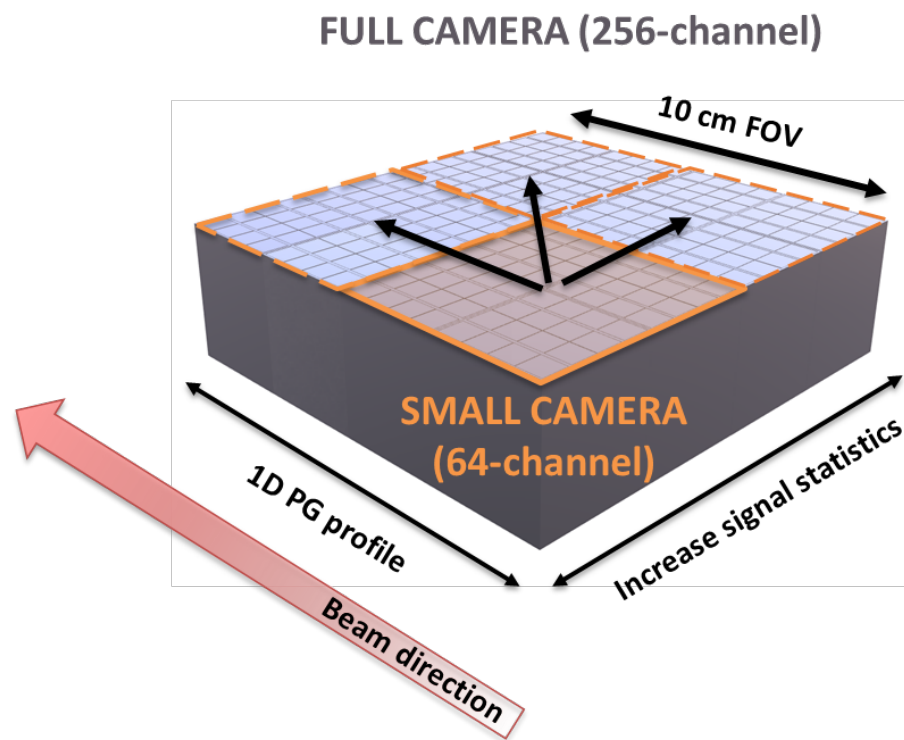
Estimated Slope (m): -0.5172  
Residual Sum of Squares (RSS): 2.9724  
R-squared (R<sup>2</sup>): 0.9964

## FLUKA SIMULATIONS



# Measured vs. simulated precision (preliminary)

$$N_{C\text{-ions}} = 2 \times 10^8$$

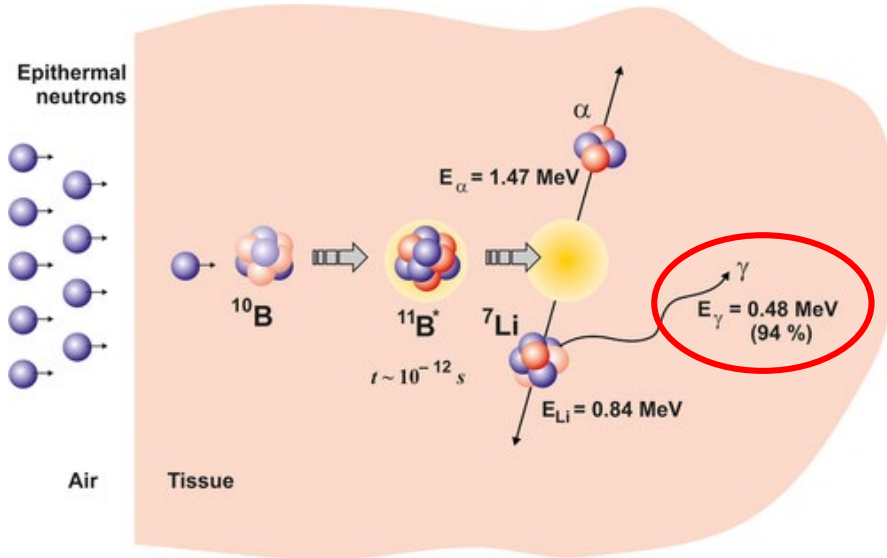


In order to achieve the desired statistics as for the 256 channel camera, we assume to multiply x4 the number of carbon ions of the measurement corresponding to a spill:

$$4 \times 5 \times 10^7 \text{ ions} = 2 \times 10^8 \text{ ions}$$

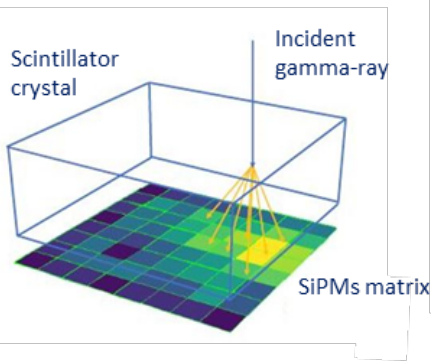
Plot of the histogram of distances between the reference and noisy curve peaks distances between their x value at the y inflection of the reference curve

# Gamma-ray detectors for BNCT (Boron Neutron Capture Therapy)

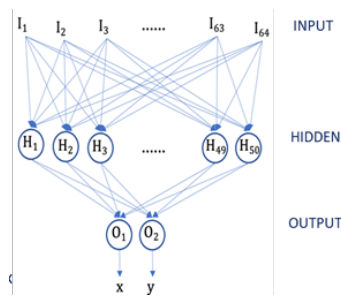


Detection of emitted **478keV gamma photons** may let to estimate  $^{10}\text{B}$  neutron captures and support therapeutic outcome (personalized dosimetry).

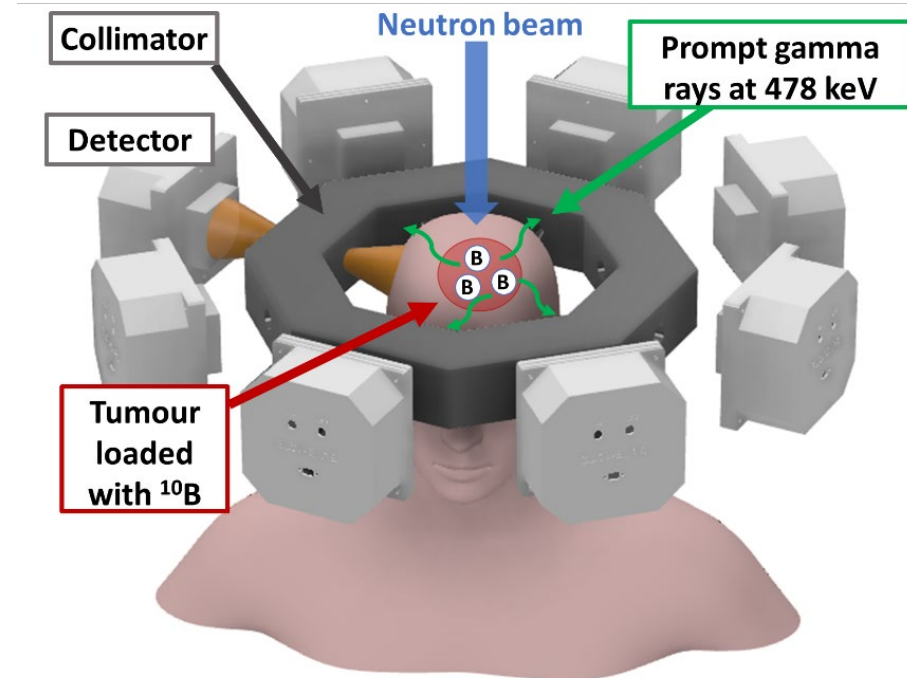
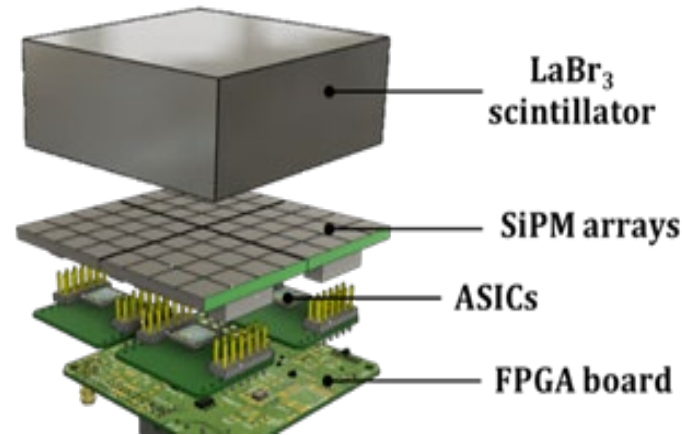
**Goal:** Development of a SPECT (Single Photon Emission Tomography) system) for BNCT



Scintillator/SiPMs-based gamma-ray detector



Neural-Network for event reconstruction



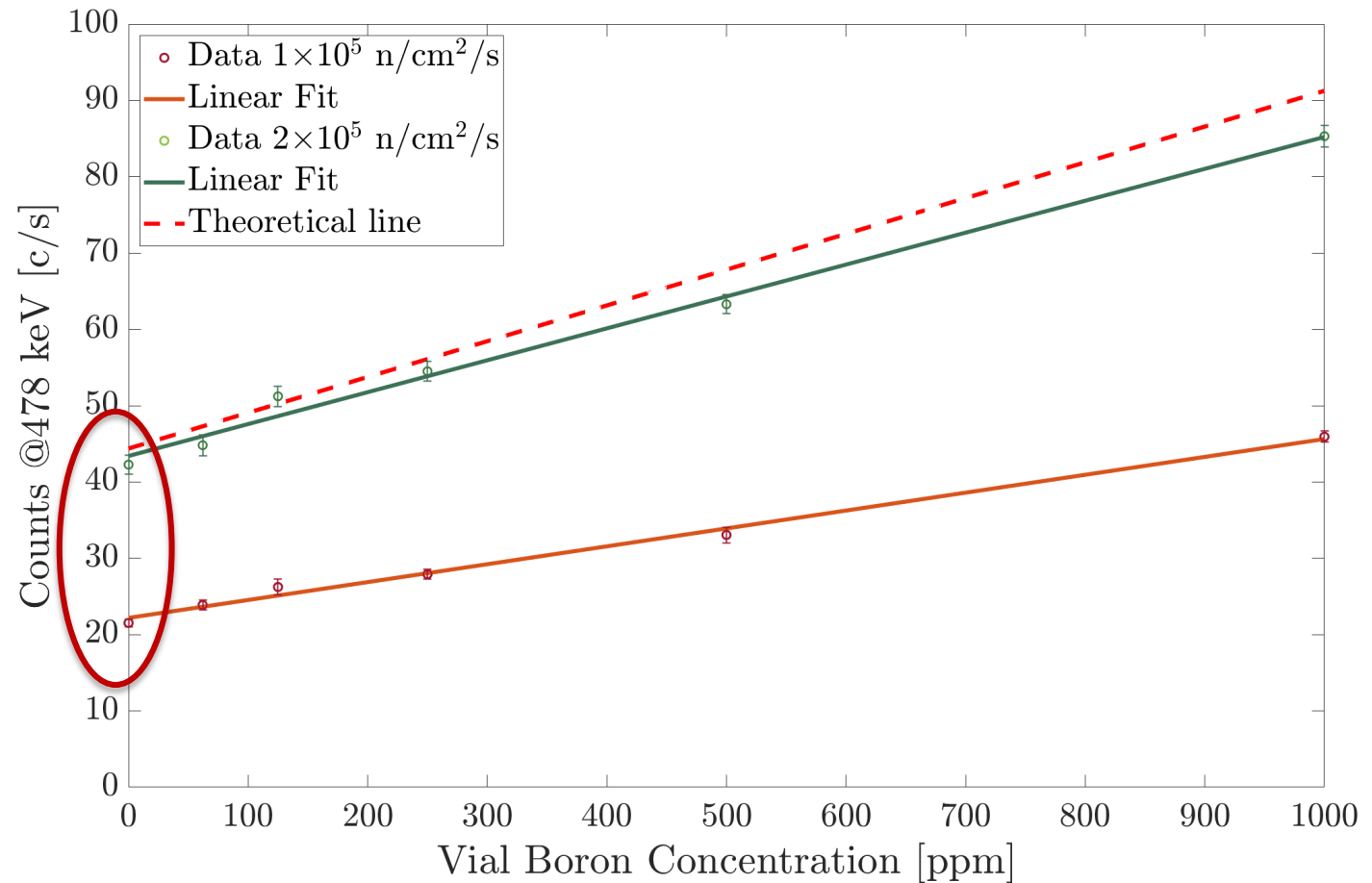
# Linearity Measurements

Measurements performed at the **TRIGA Mark II** reactor of Pavia University (Italy).

Six vials at different concentrations taken at different reactor power (4 kW and 8 kW)

✓ Good **linear correlation** between the boron concentration and the detected events at 478 keV.

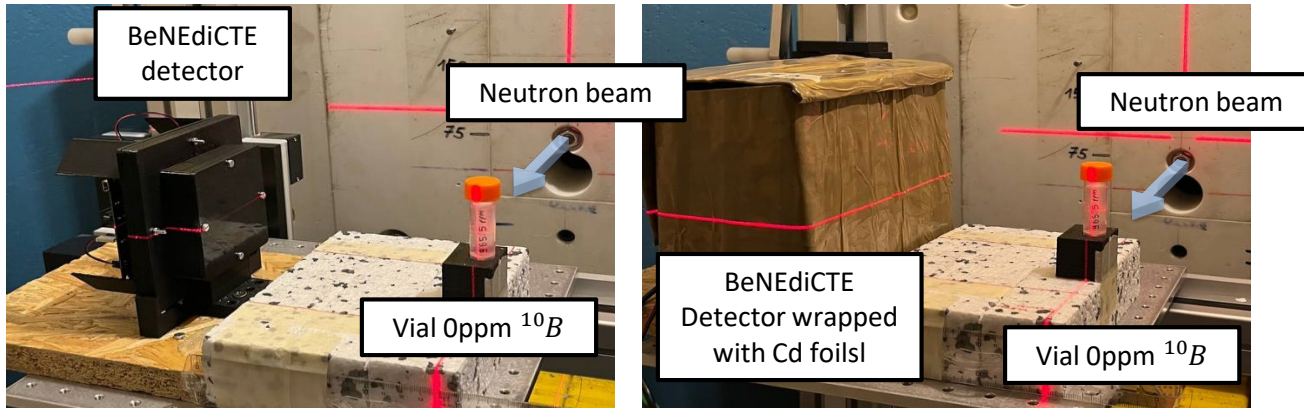
✗ Events at **478 keV** detected during the 0ppm measurement



# Shielding study

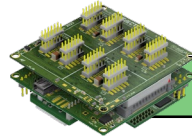
**✗** FLUKA simulations showed a high 478 keV contribution given by the presence of boron in the electronics.

Cd housing to shield thermal neutrons.



**✓** Almost complete reduction of the boron peak coming from the electronics.

**✗** Background radiation enhancement.

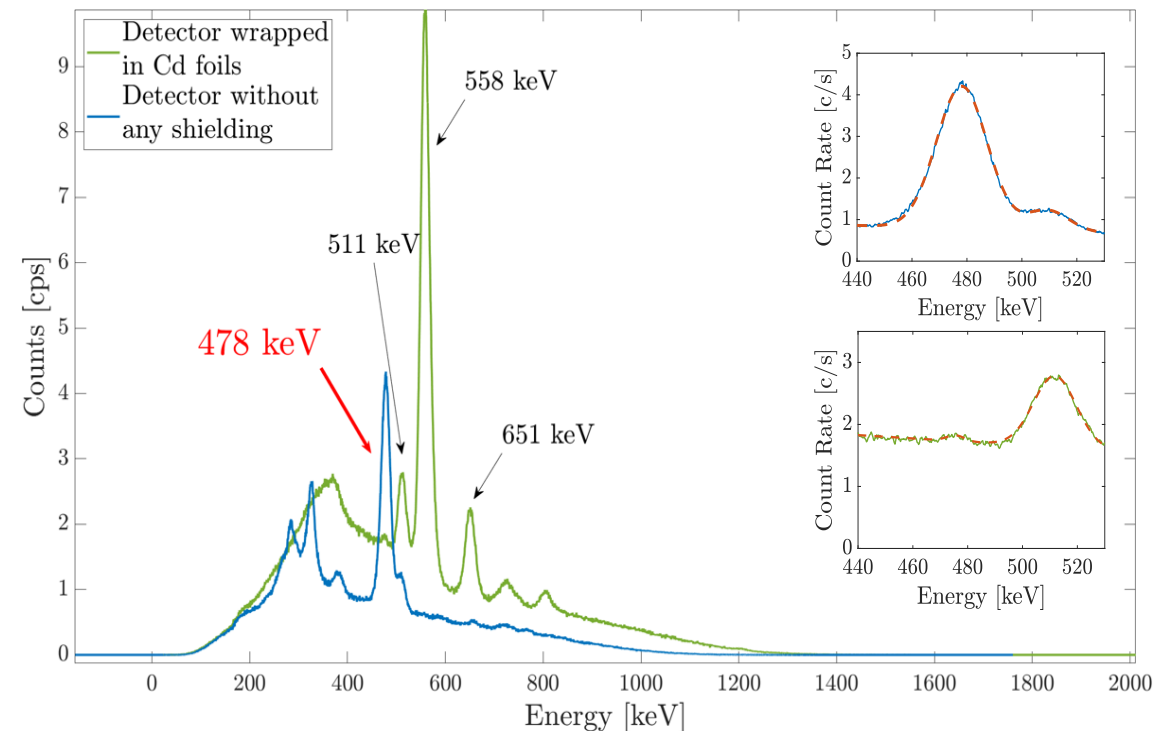


Flame Retardant (FR4) substrate

Epoxy resin 40%

"E"-grade glass fiber 60%

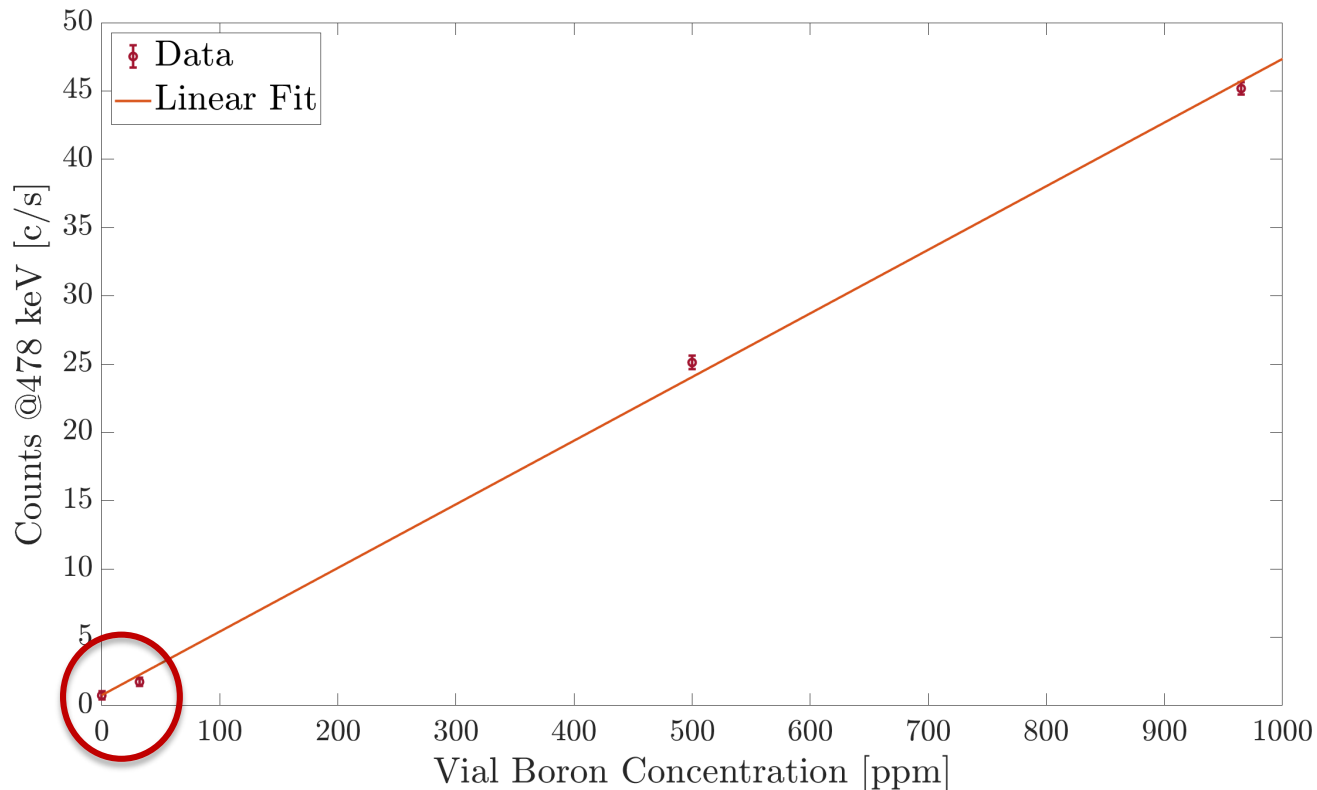
**0.2 – 0.3 %  $^{10}B$  by weight**



# New Linearity Measurements

Measurements performed at the **TRIGA Mark II** reactor of Pavia University (Italy).

**4 vials at different concentrations** (0 ppm, 32 ppm, 500 ppm, 1000 ppm) and **Neutron flux of  $10^5$  n/cm<sup>2</sup>/s**.



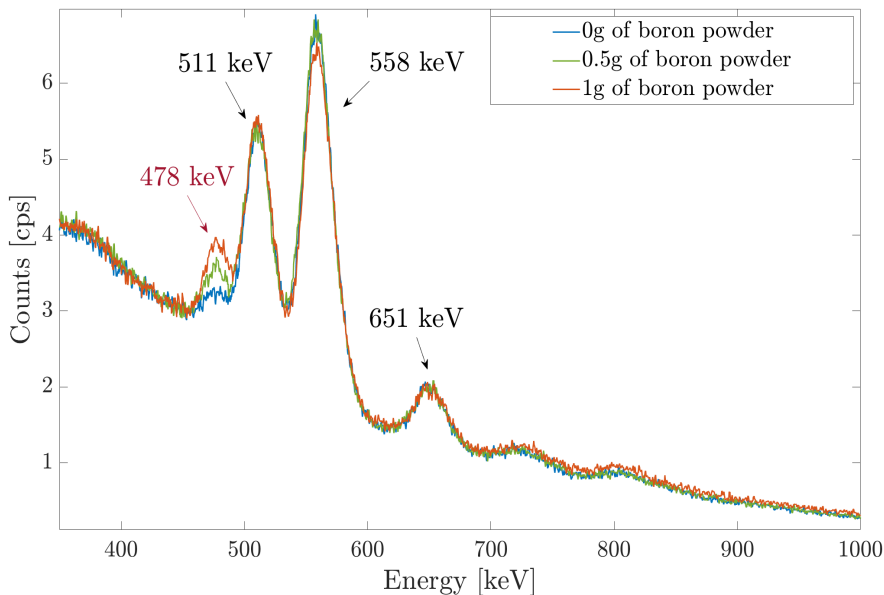
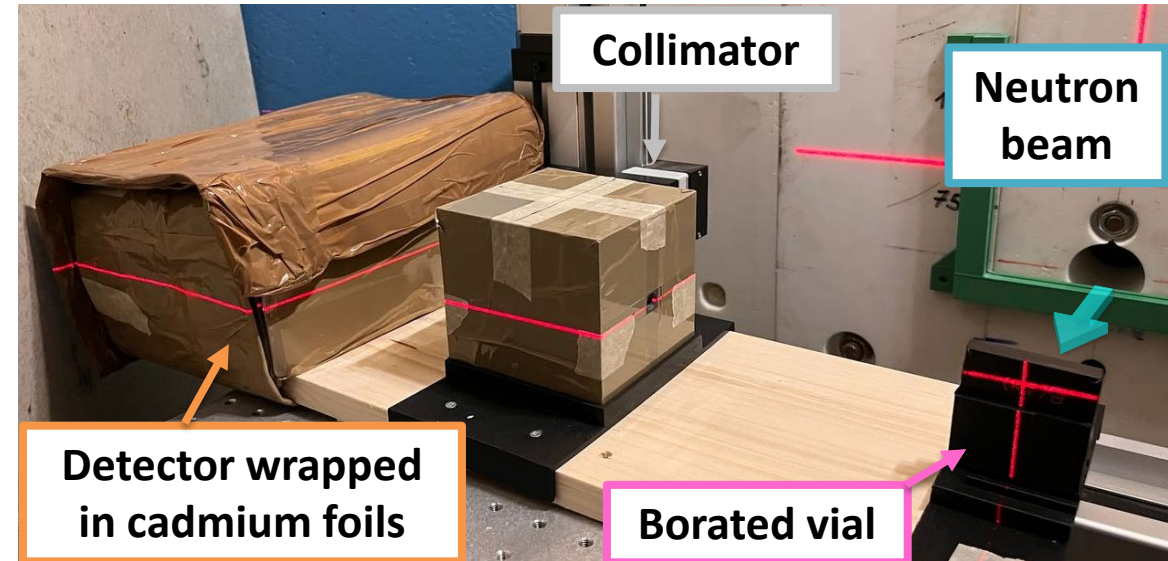
- ✓ Good **linear correlation** between the boron concentration and the detected events at 478 keV.
- ✓ Almost zero events at **478 keV** detected during the 0 ppm measurement.



# Spectroscopy/Imaging Measurements at TRIGA MARK II nuclear reactor

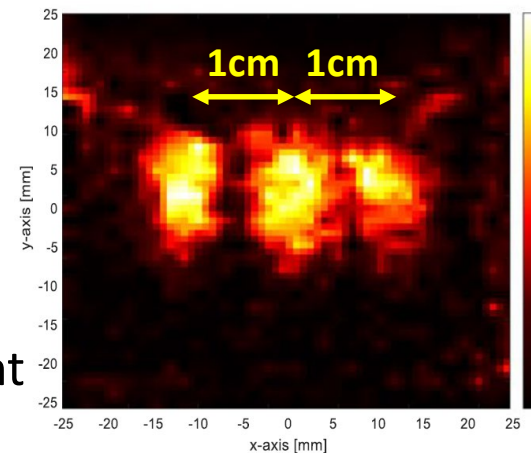
## Experimental setup at nuclear reactor of Pavia:

- Neutron flux of  $2 \times 10^6$  n/cm<sup>2</sup>/s
- Sample  $4 \times 0.3 \times 1.6$  cm<sup>3</sup> filled with boron powder
- 40 cm distance between the sample and the detector
- **Pinhole collimator**



## ➔ Spectroscopic Results

Identification of the BNCT photopeak at 478 keV and linear response at different boron quantities



## ➔ Imaging Results

The ANN algorithm is able to track shifts of 1 cm of the borated sample