

# A review of unsupervised anomaly detection models for neuroimaging applications

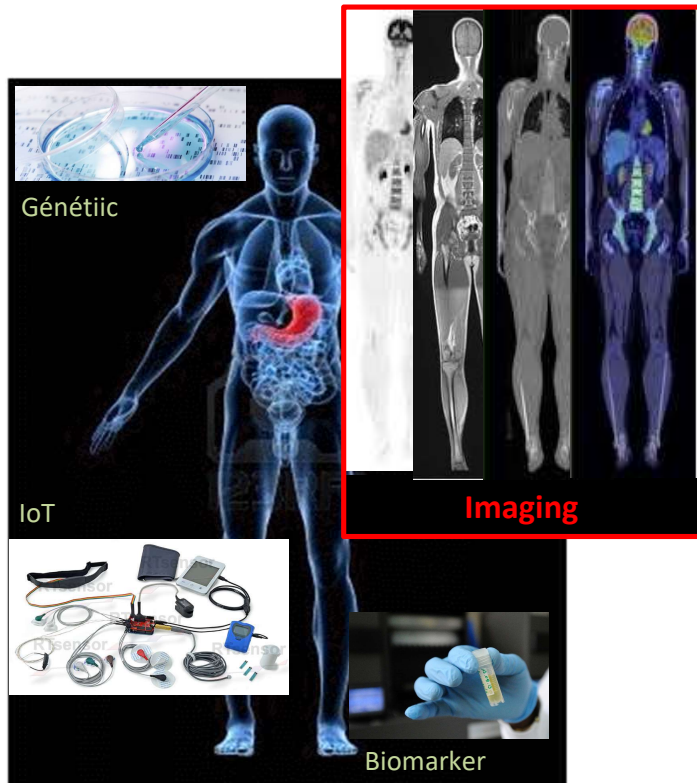
Carole Lartizien

[carole.lartizien@creatis.insa-lyon.fr](mailto:carole.lartizien@creatis.insa-lyon.fr)

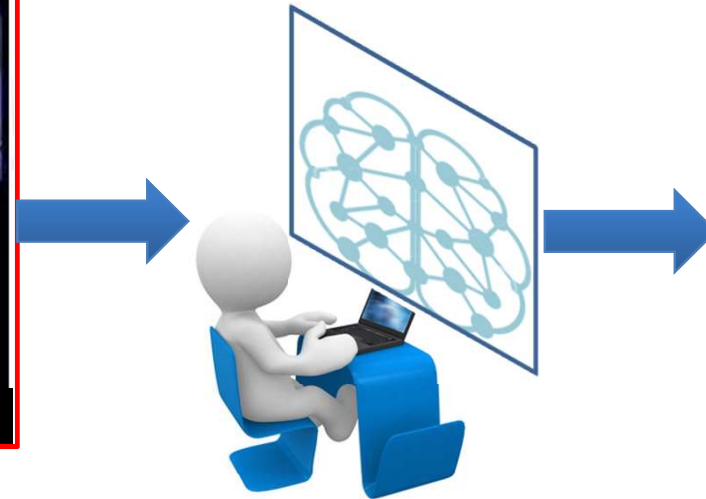
- AI for medical image analysis
- AI for neuroimaging analysis
- Basics of machine learning for image analysis
- Supervised semantic segmentation : use case #1
- Unsupervised anomaly detection : use cases #2 and #3.
- Conclusion

## AI for medical image analysis

## Data



## AI – assisted physicians

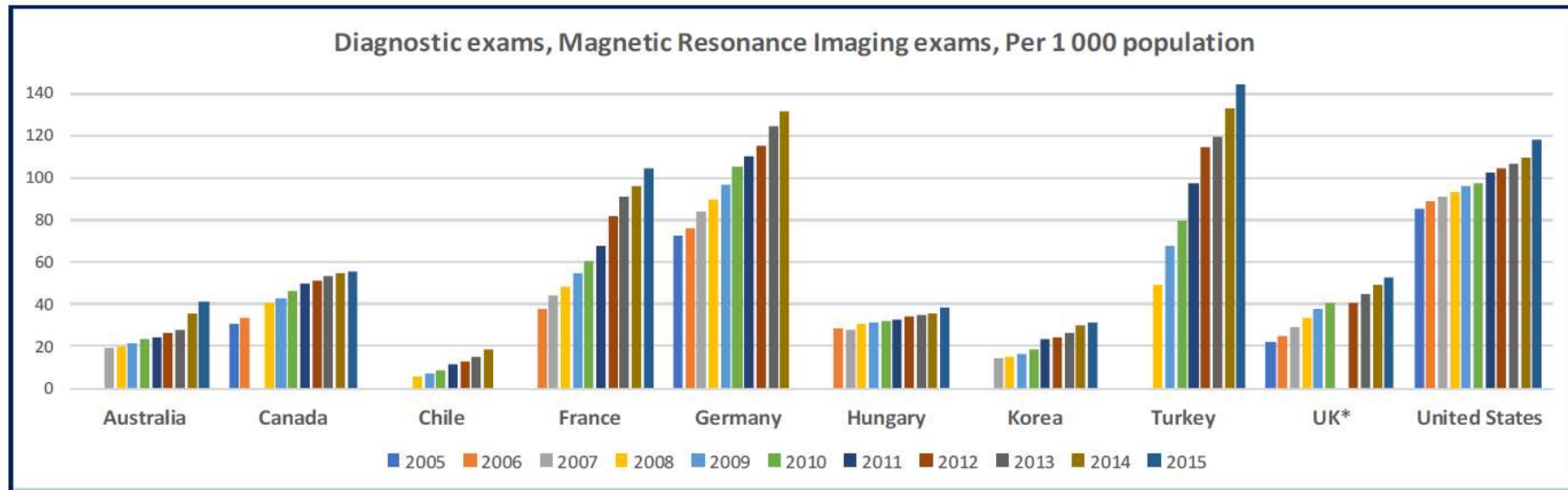


## Precision medicine

- Refine Diagnosis
- Improve therapy planning
- Predict therapy outcome
- Develop preventive medicine

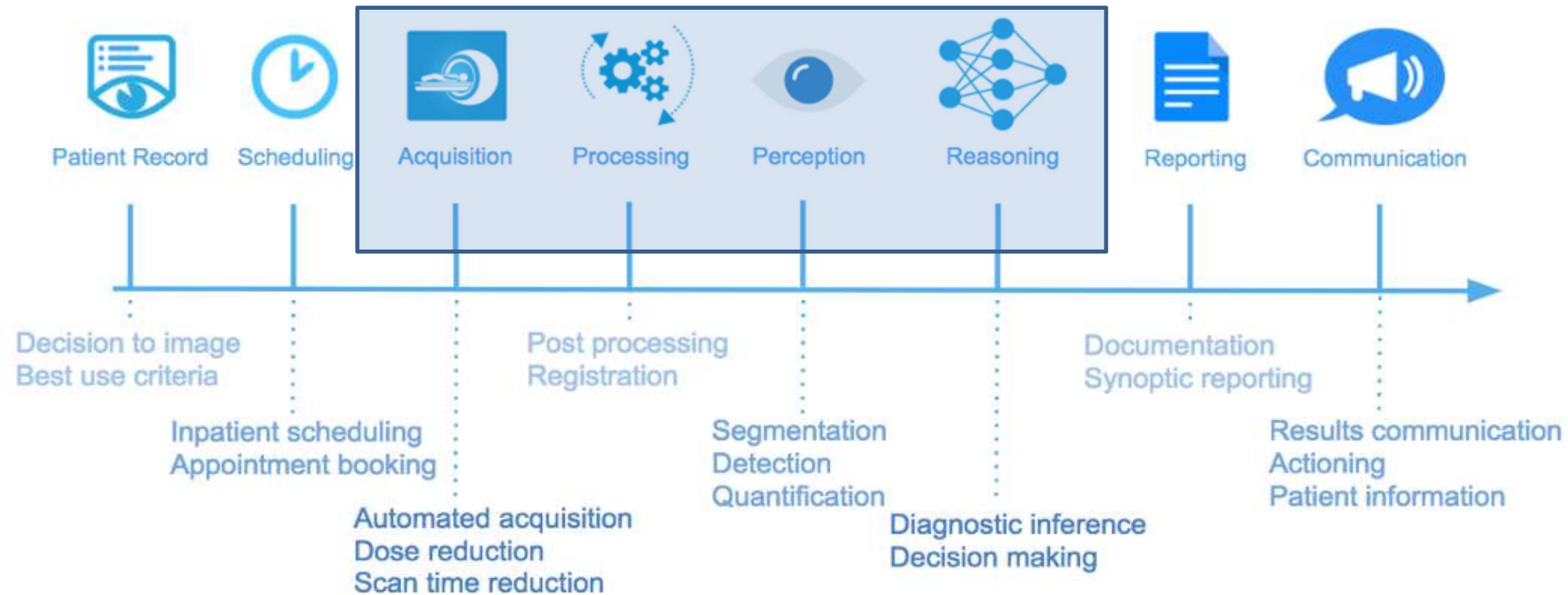


Figure 2: Diagnostic exams and MRI exams per 1,000 population



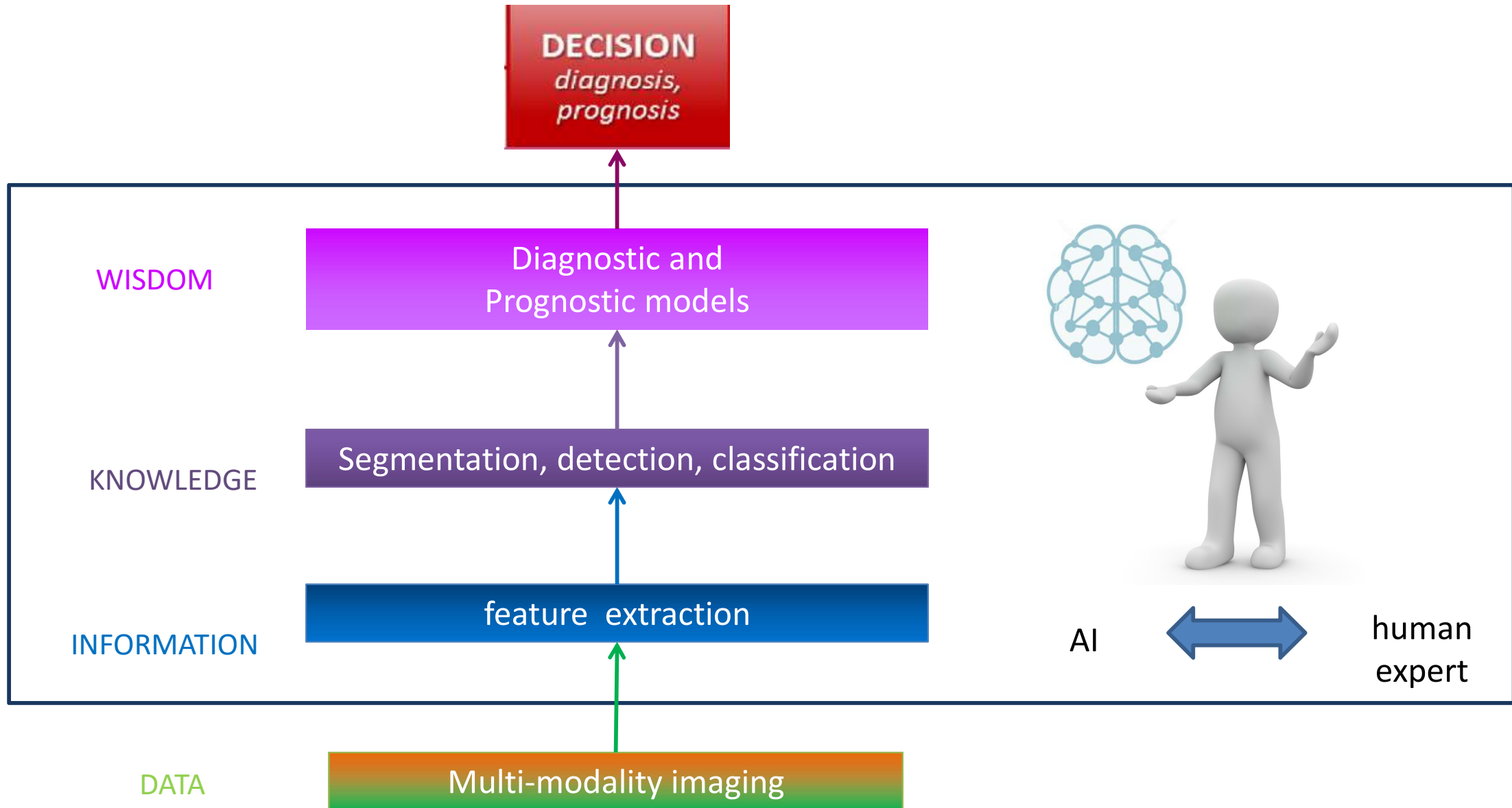
<https://emea.gehealthcarepartners.com/images/pdfs/Rapid-Review--Radiology-Workforce-Review-FINAL.pdf>

# AI in clinical practice



<https://towardsdatascience.com/why-ai-will-not-replace-radiologists-c7736f2c7d80>

# From imaging data to wisdom

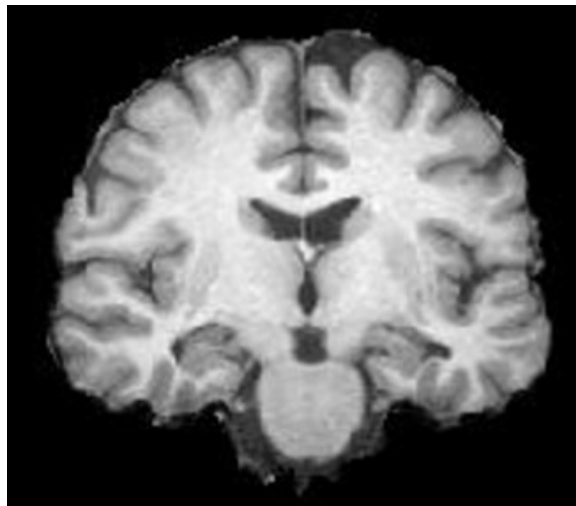


## AI for neuroimaging analysis

## AI for neuroimaging data analysis

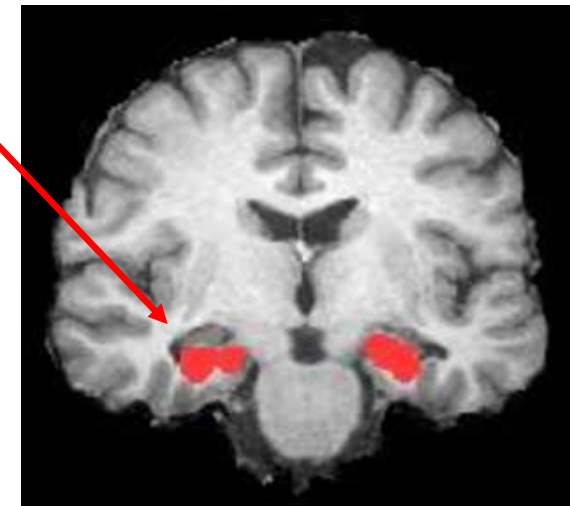
Is this patient affected by preliminary symptoms of the Alzheimer disease (AD) ?

Are there **imaging biomarkers** of the pathology ?



Hippocampus atrophy  
 is one imaging  
 biomarkers of AD

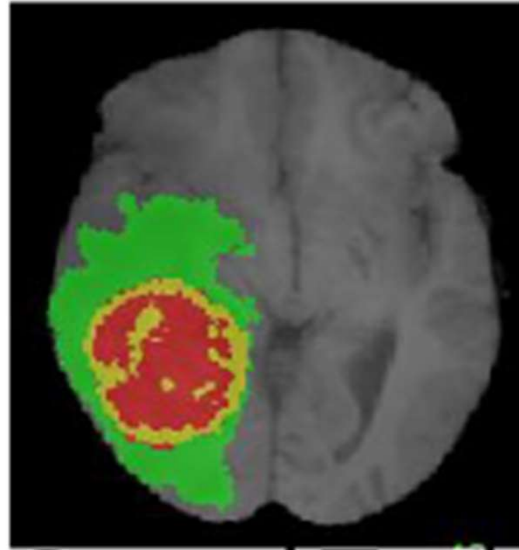
**Pathological  
 classes** : Normal,  
 Mild cognitive  
 impairment, AD



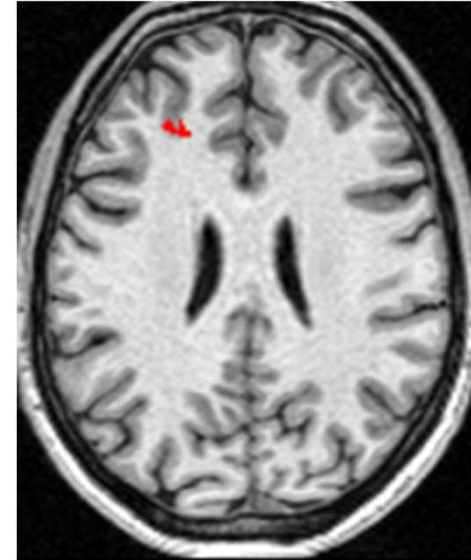
**Prediction of a patient-level  
 malignancy score**

**Segmentation of anatomical  
 structures of interest**

## AI for neuroimaging data analysis



Segmentation of the different components of a brain tumor

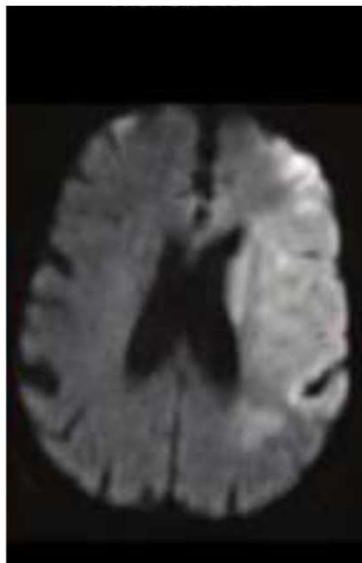


Detection of subtle abnormalities in cortical gyration leading to epileptogenic seizures

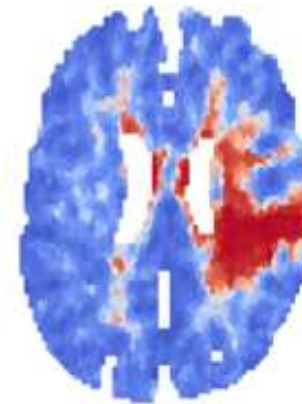
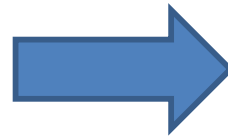
## Localisation of suspicious area

## AI for neuroimaging data analysis

Will this patient who has just had a stroke benefit from a surgical thrombectomy ?



MRI image at ICU

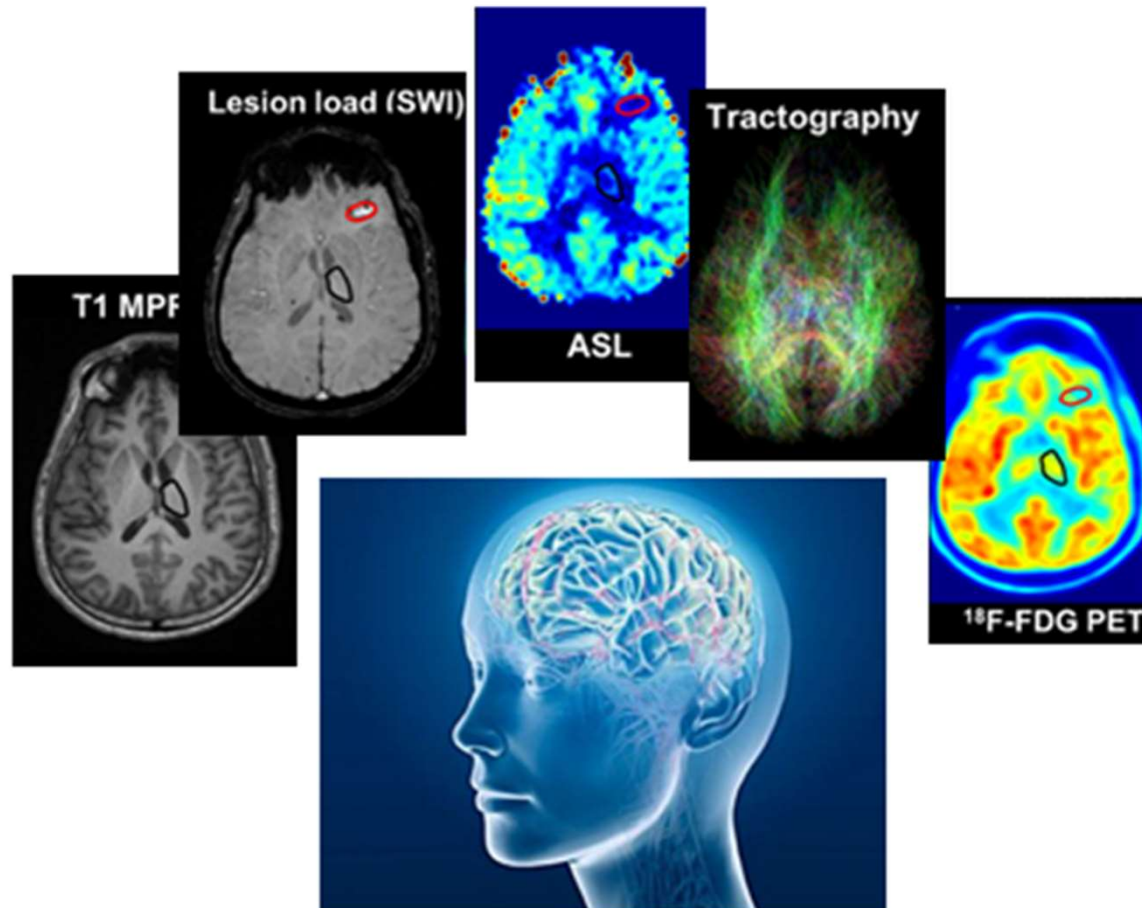


Predicted lesion 6 months after thrombectomy

**Prediction of outcome from surgery or therapy**



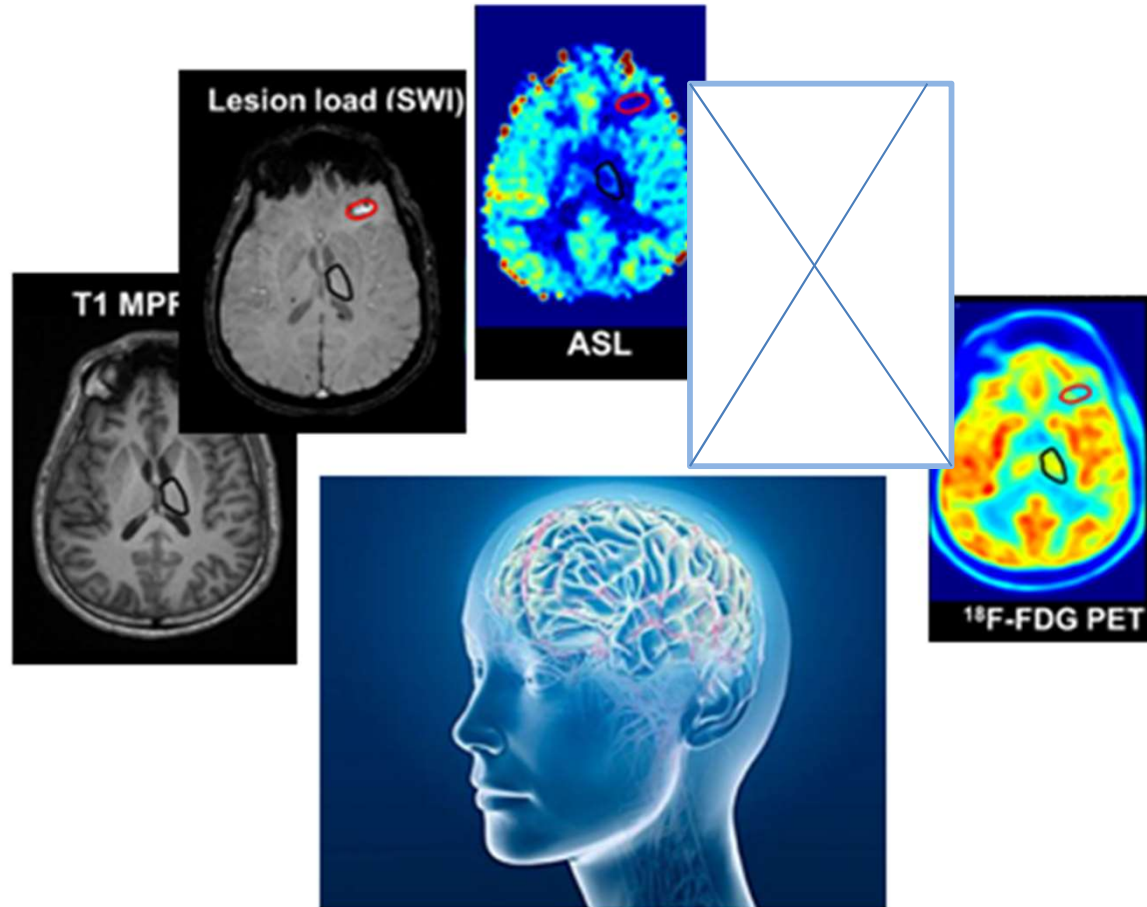
# AI for neuroimaging data analysis



**Multimodal heterogenous data analysis....**



# AI for neuroimaging data analysis

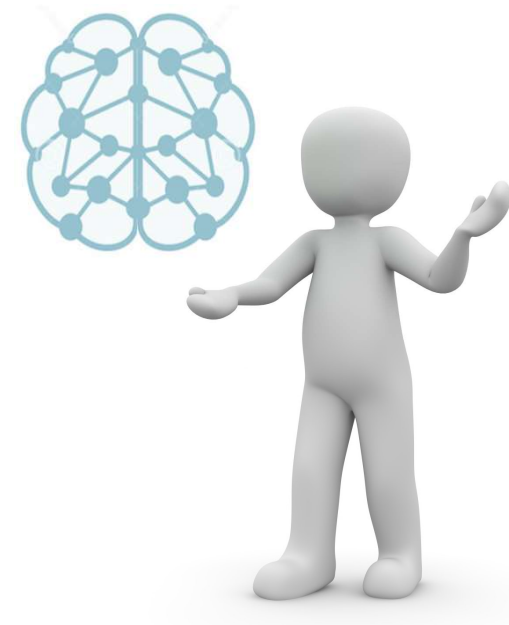


with missing data....

# Basics of machine learning for image analysis (in a few seconds)

## Basics of machine learning

1. Define a **task**
2. Formulate this task as a **decision model**
3. Learn the hyperparameters of the decision model based on samples **data** and a **performance metric**
4. Infer decision from this model on new samples



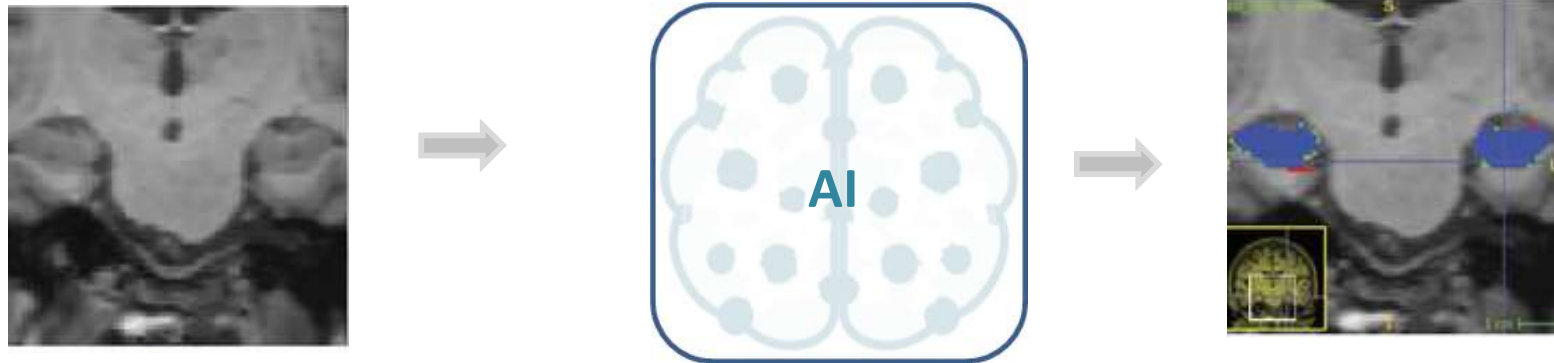
## Design your AI algorithm

### 1. Task definition

Detect lesions on brain T1 MRI

### 2. Problem formulation as a decision task

Decide whether each voxel is a 'lesion' or 'normal tissue'



- Binary classification problem
- At the voxel level

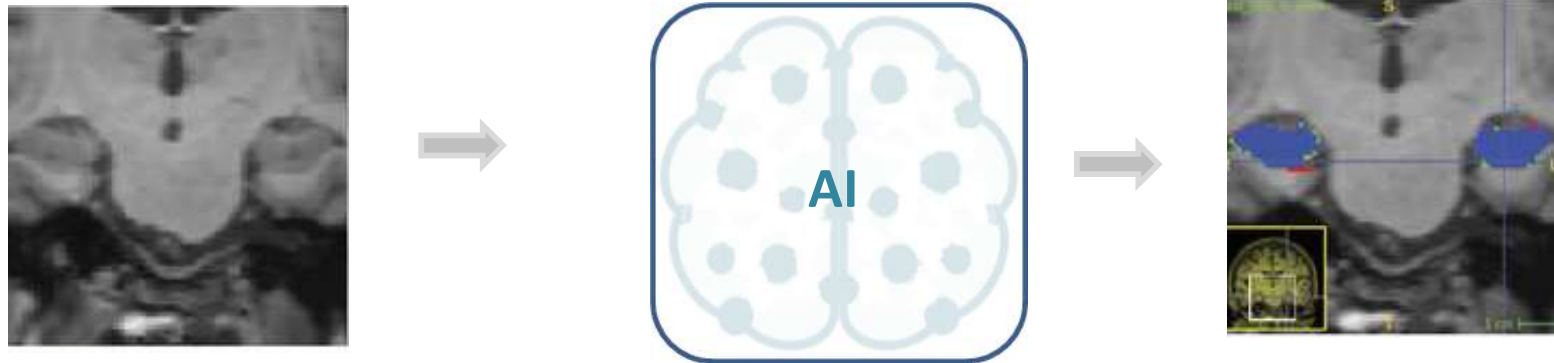
## Design your AI algorithm

### 3. Characteristic of the database

How many samples?  
 Are they annotated?  
 ...

### 4. Expert knowledge

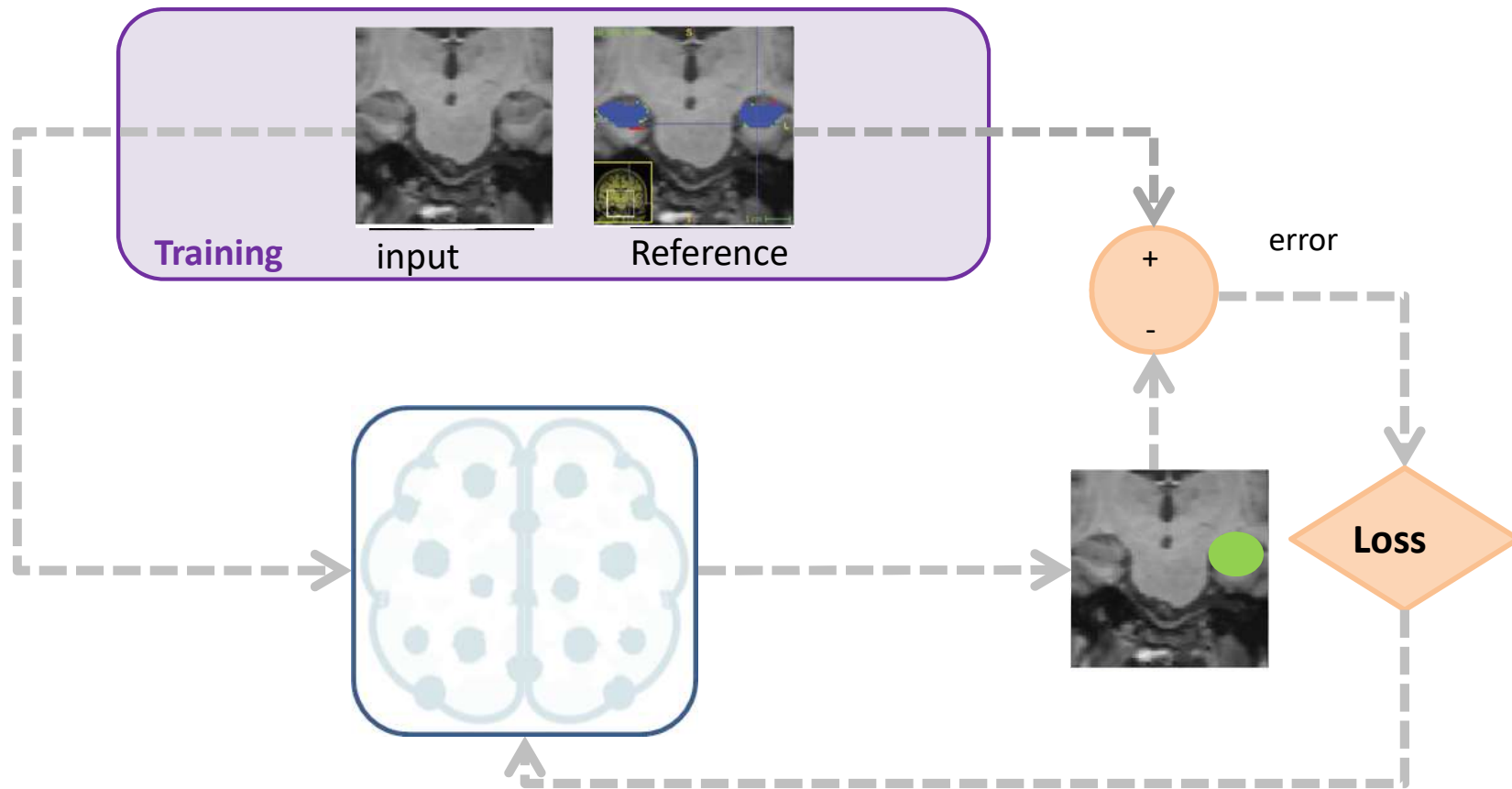
Insert manually engineered features? Priors on the expected output etc...



- Binary classification problem
- At the voxel level
- Supervised learning
- Clinically driven feature maps

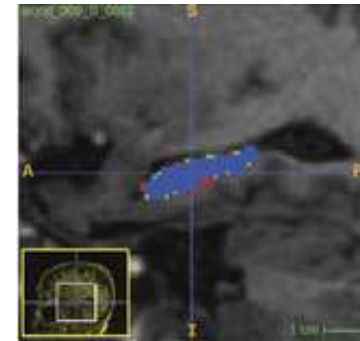
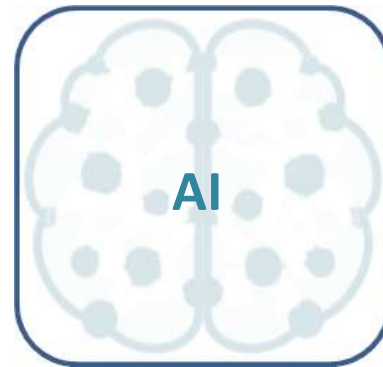
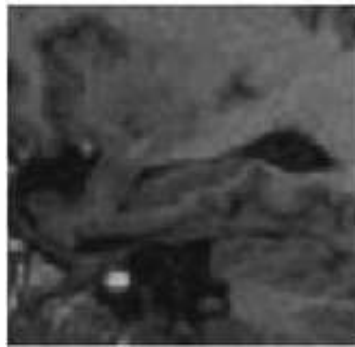
# Design your AI algorithm

## 3. Learn the decision mode based on training samples and performance metric

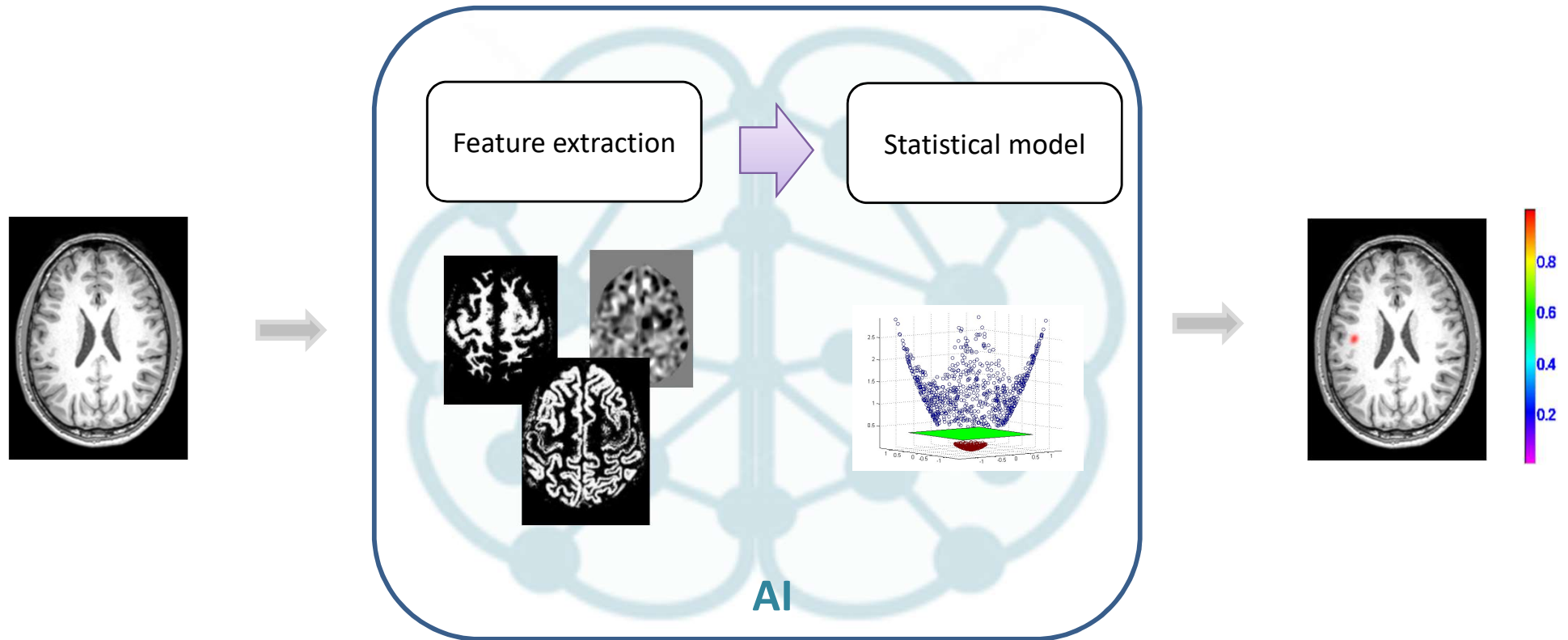


## Design your AI algorithm

## 4. Infer decision on new samples

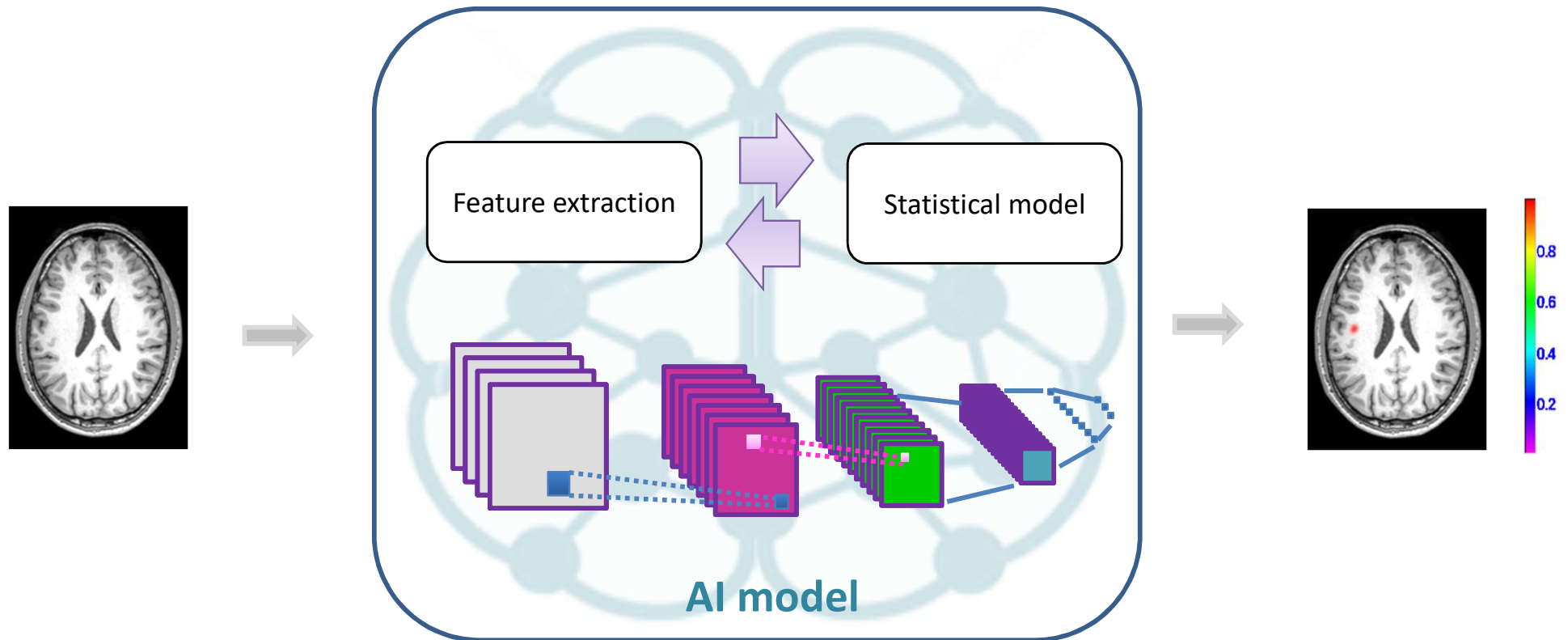


From standard machine learning...





...to deep learning

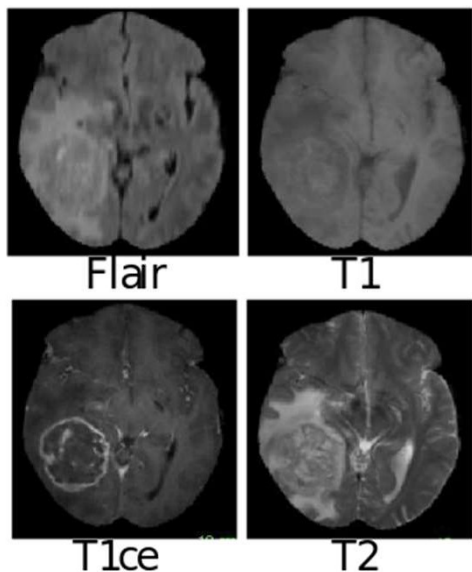


## USE CASE # 1

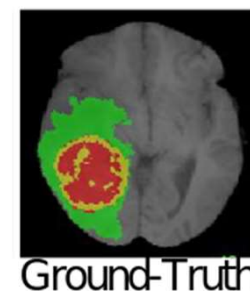
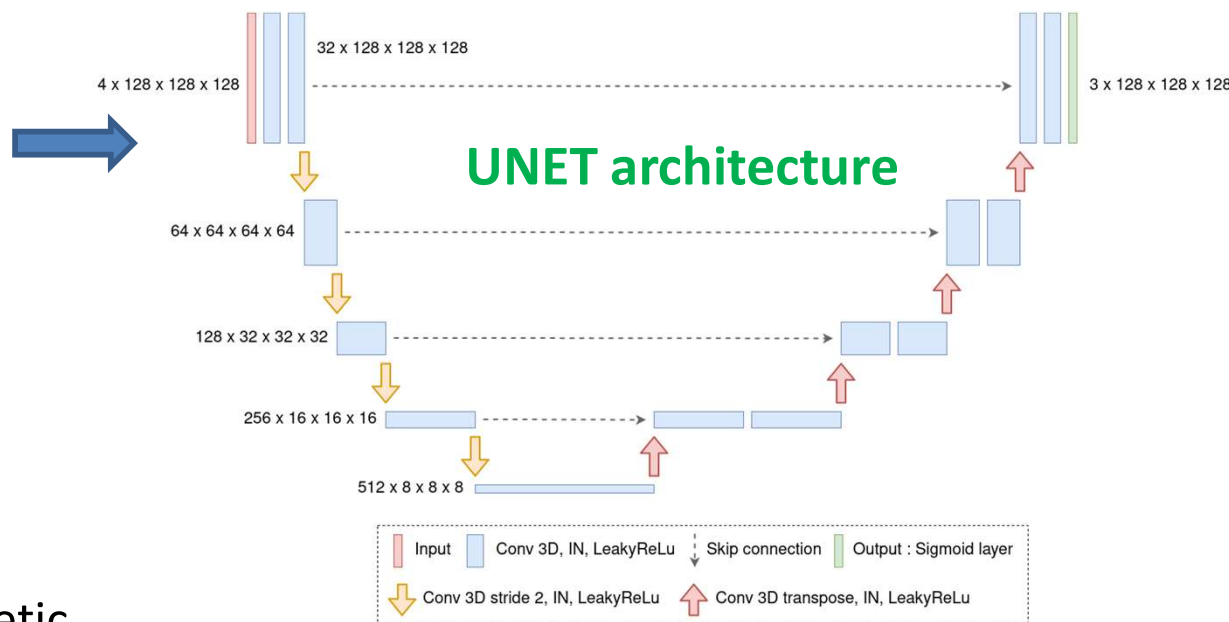
Automatic multi-class segmentation of brain tumors

**Supervised learning**

# Automatic multi-class segmentation of brain tumors



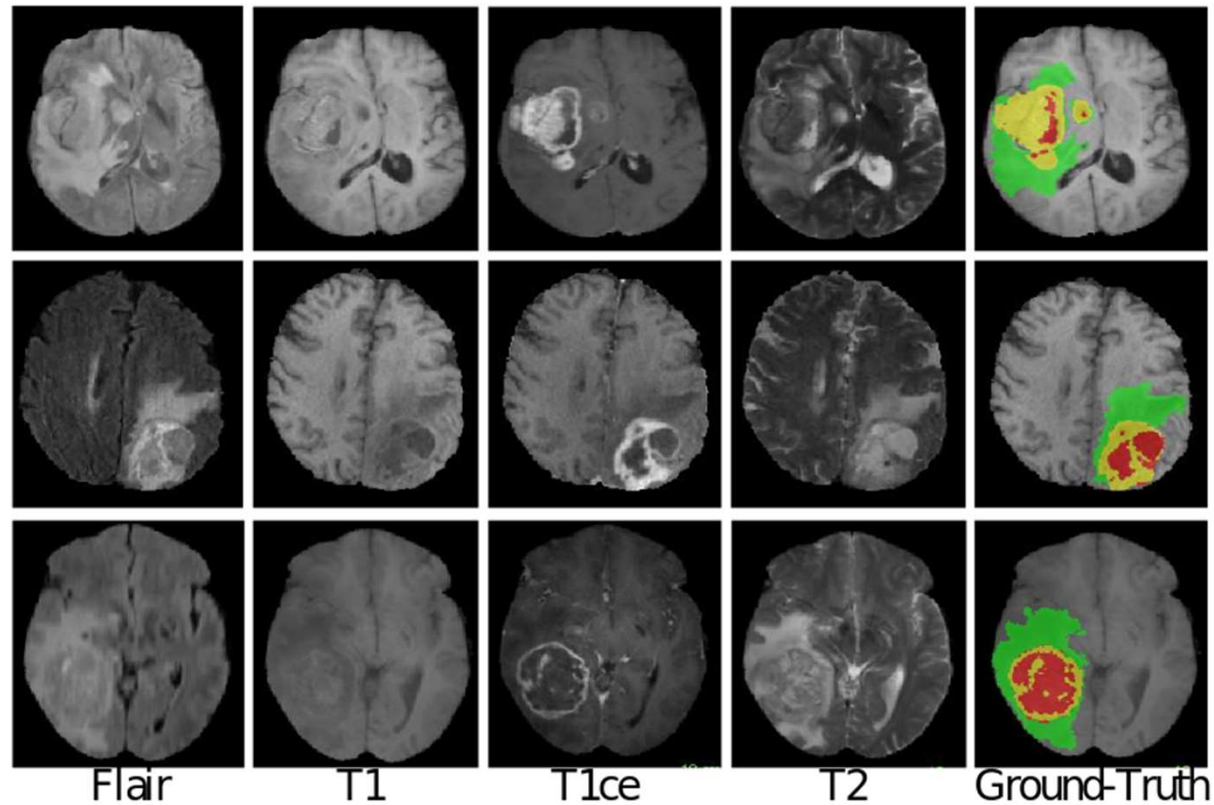
Multiparametric Magnetic Resonance Imaging (MRI)



Whole Tumor  
Tumor core  
Enhancing Tumor

→ Segmentation of the brain tumor is valuable at each step of the patient care : from diagnosis to prognosis, treatment planning and follow-up up to outcome prediction

## Automatic multi-class segmentation of brain tumors



Manual annotation by expert clinicians on 3D image of dimension :  
~240 x 240 x 155 with  
1mm<sup>3</sup> isotropic voxels

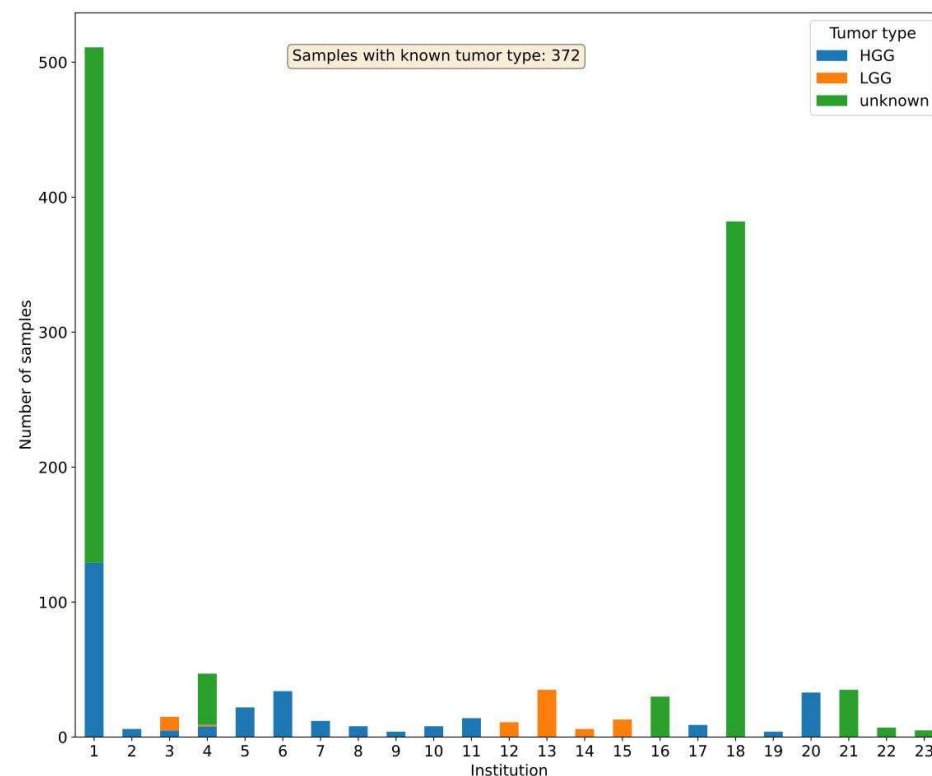
Manual annotations are time consuming but « feasible »

→ International initiatives to gather large datasets

## Automatic multi-class segmentation of brain tumors

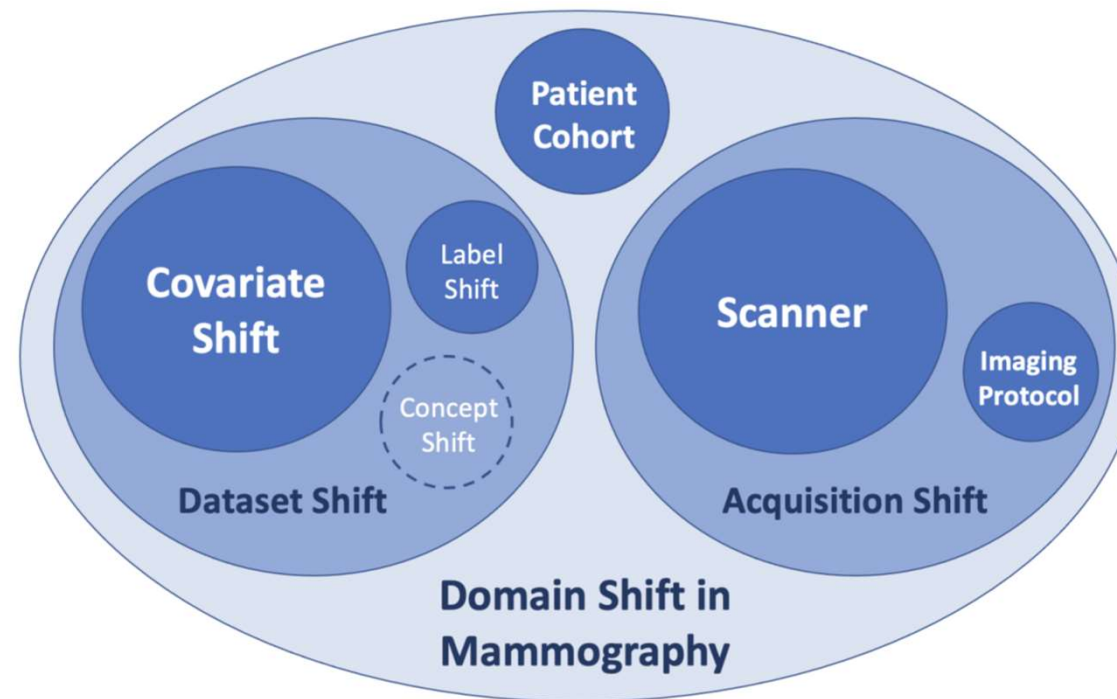
## Federated Brain Tumor Segmentation (FeTS2022) Challenge Dataset

- **Dataset size** : 1251 patients,
- **MRI scan**
  - **voxel size** : 240 x 240 x 155 of 1mm<sup>3</sup>
  - 4 modalities : *Flair, T1, T1ce, T2*,
- **Partitioning** : original, institution-wise
  - 23 institutions, heterogeneous distributions.
- **Manual annotations** : 3D multi labels
  - *Whole Tumor, Tumor core, Enhancing Tumor*



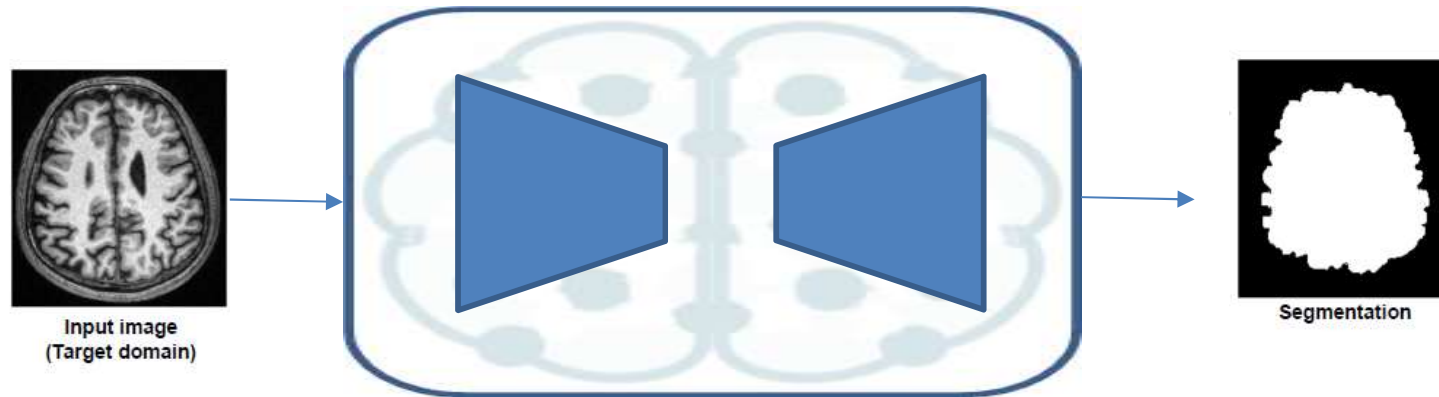
## Performance generalization and domain shift

- The **generalization** of a model measures its ability to make good predictions on new unseen data
- These new data come potentially from different "populations" (domain) than those to train the model → **domain shift**



[Garrucho et al, arxiv 2022]

# Performance generalization and domain shift



Task : brain Segmentation  
(skull stripping)

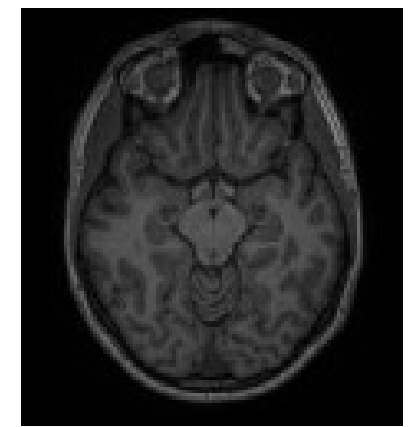
Database : CC359\* : 359  
T1 MRI of healthy  
subjects acquired on 6  
different scanners



Philips 1.5 T



GE 1.5 T



Siemens 3T

\*<https://www.ccdataset.com/download>

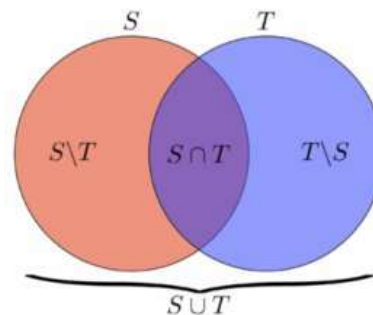
[Zakazov, MICCAI21]



## Performance generalization and domain shift

|          | Sm, 1.5T         | Sm, 3T           | GE, 1.5T         | GE, 3T           | Ph, 1.5T         | Ph, 3T           |
|----------|------------------|------------------|------------------|------------------|------------------|------------------|
| Sm, 1.5T | <b>.86 (.04)</b> | .61 (.14)        | .70 (.08)        | .66 (.13)        | .69 (.10)        | .78 (.06)        |
| Sm, 3T   | .70 (.07)        | <b>.87 (.04)</b> | .63 (.08)        | .73 (.07)        | .65 (.08)        | .72 (.06)        |
| GE, 1.5T | .36 (.12)        | .11 (.10)        | <b>.84 (.06)</b> | .36 (.14)        | .62 (.16)        | .55 (.11)        |
| GE, 3T   | .74 (.07)        | .66 (.15)        | .58 (.11)        | <b>.89 (.03)</b> | .59 (.10)        | .74 (.05)        |
| Ph, 1.5T | .58 (.07)        | .40 (.11)        | <b>.81 (.05)</b> | .52 (.07)        | <b>.88 (.04)</b> | .74 (.09)        |
| Ph, 3T   | .55 (.13)        | .37 (.15)        | .63 (.11)        | .36 (.11)        | .53 (.12)        | <b>.86 (.05)</b> |

Table 1: columns - source domains for training, rows - target domains for testing. Metric: surface dice, tolerance=1.



$$Dice(S, T) = \frac{2|S \cap T|}{|S| + |T|}$$

[Zakazov, MICCAI21]



# Performance generalization and domain shift

## Data harmonization

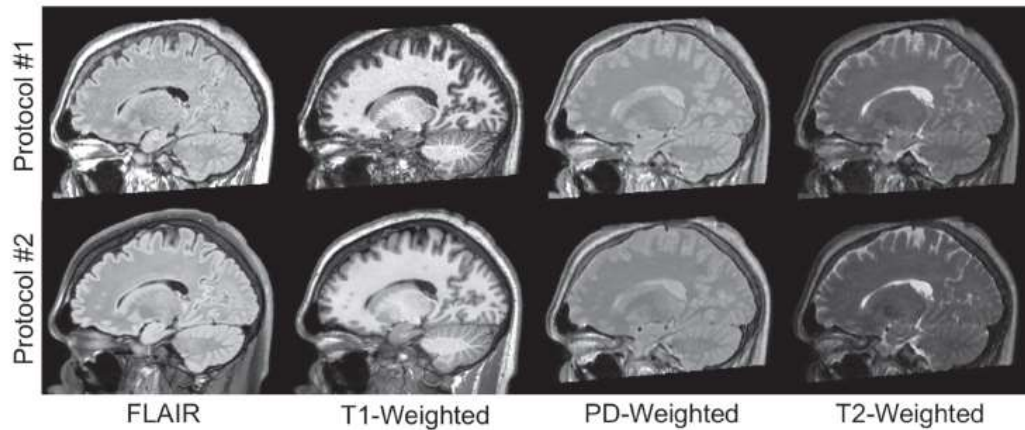
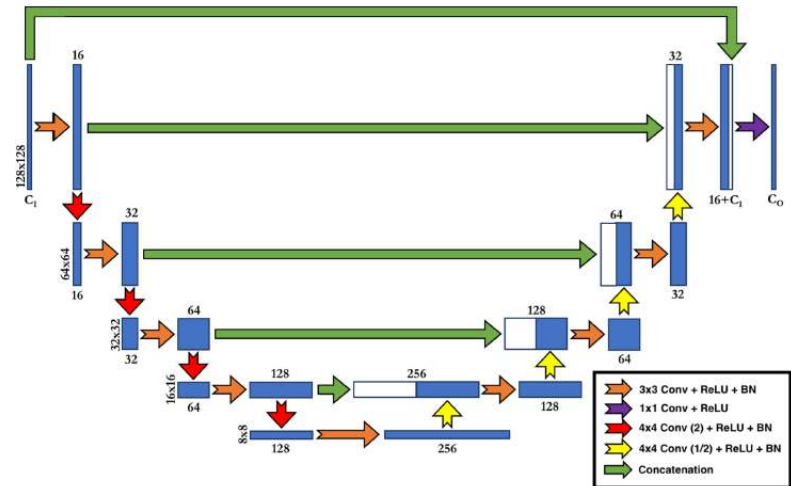


Fig. 1. Preprocessed images from one subject from the overlap cohort depicting the four input (Protocol #1) and four target (Protocol #2) contrasts.



DeepHarmony: A deep learning approach to contrast harmonization across scanner changes

- UNET
- 1 UNET per view (coronal, axial, sagittal)
- 2 versions :
  - O2O one-to-one : 1 input modality → 1 output modality
  - MO2 many-to-one : 4 input modalities → 1 output modalities

[Dewey, Mag Res Imag 19]

# Performance generalization and domain shift

## Data harmonization

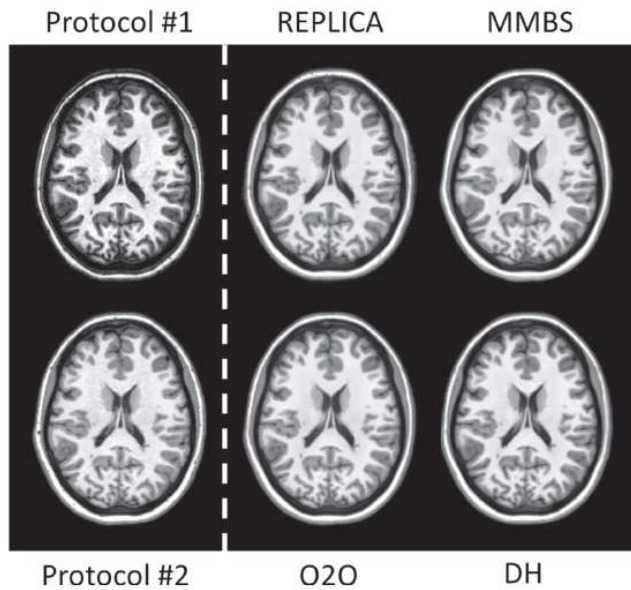


Fig. 4. Harmonized Protocol #1 T1-weighted images using REPLICA, MMBS, O2O, and DeepHarmony (DH). For comparison, the input contrast (Protocol #1) and the target contrast (Protocol #2) are displayed on the left side of the white, dashed line.

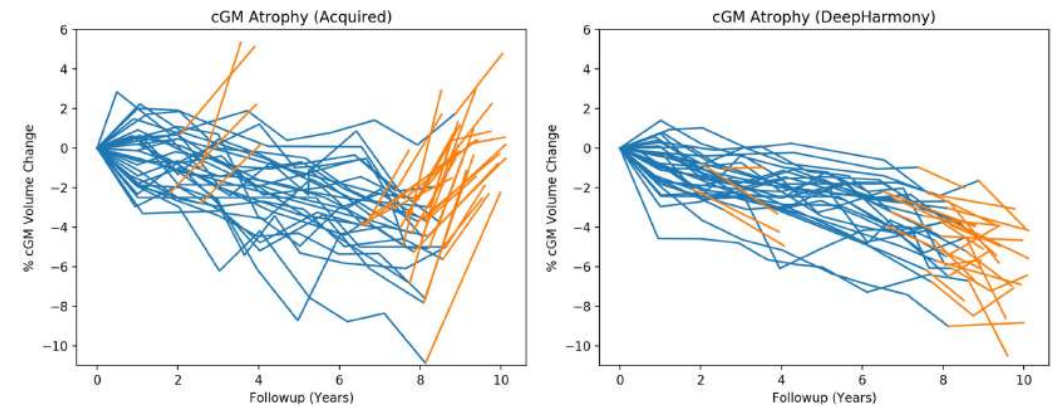
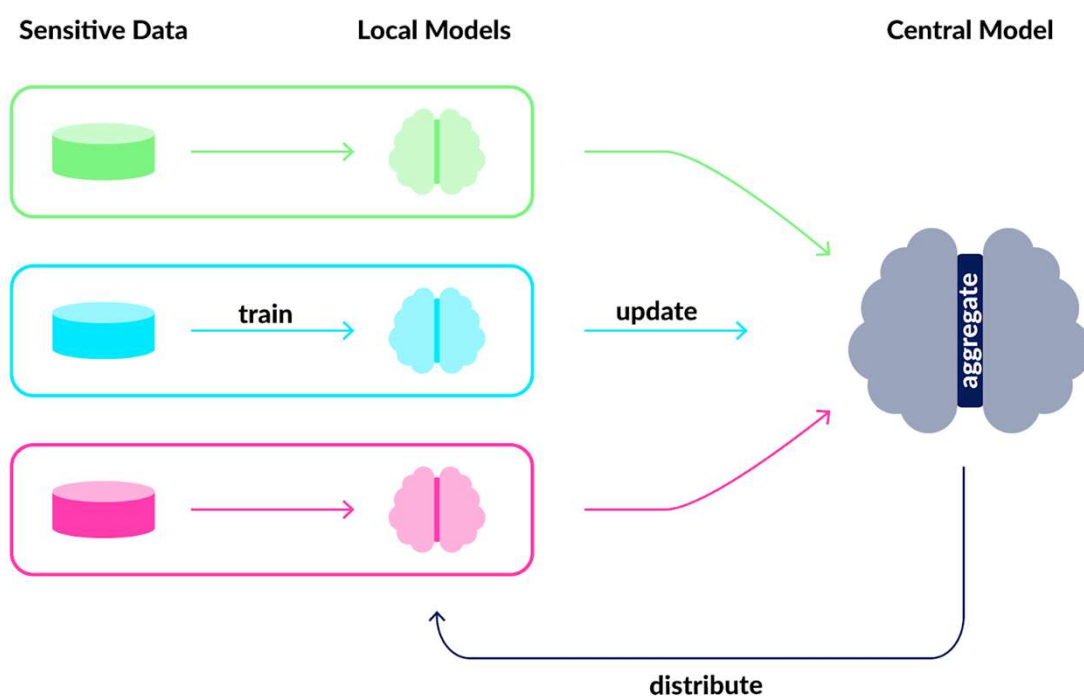


Fig. 8. Longitudinal trajectories for cortical grey matter (in % from baseline). Protocol #1 is shown in blue and Protocol #2 is shown in orange. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)

[Dewey, Mag Res Imag 19]

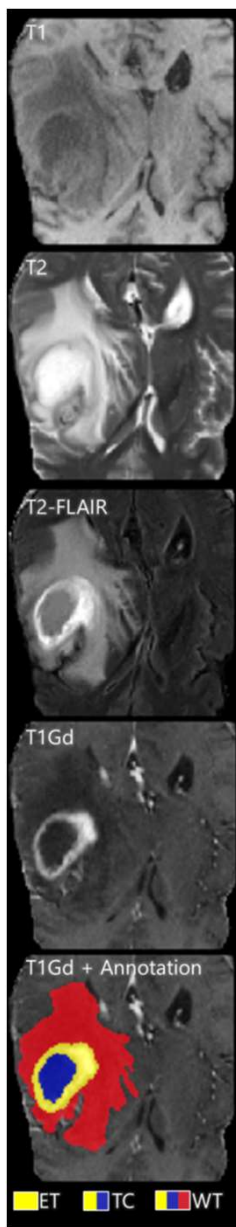
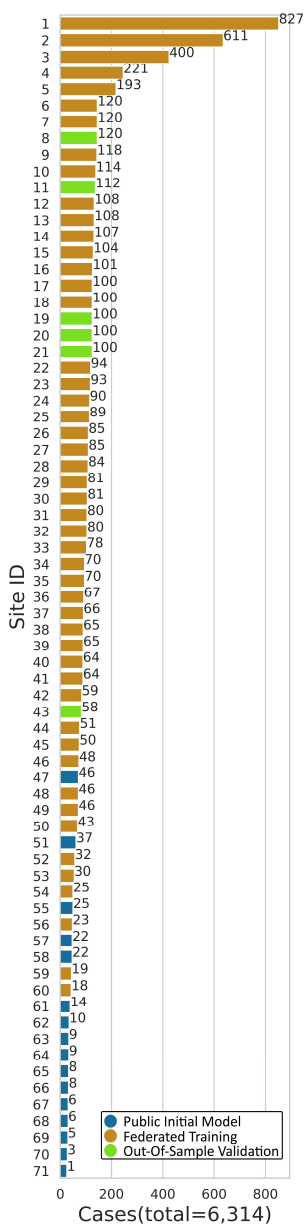
# Federated learning

A privacy-preserving decentralized training paradigm

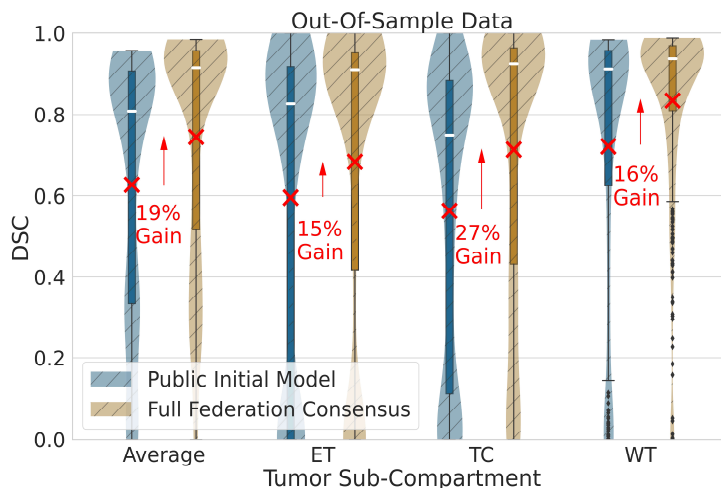


- **First algorithm** : Federated Averaging (FedAvg, **2016**).
- A growing interest in the medical community
- Many open questions regarding FL in the context of heterogeneous data : fairness, personalization ,....

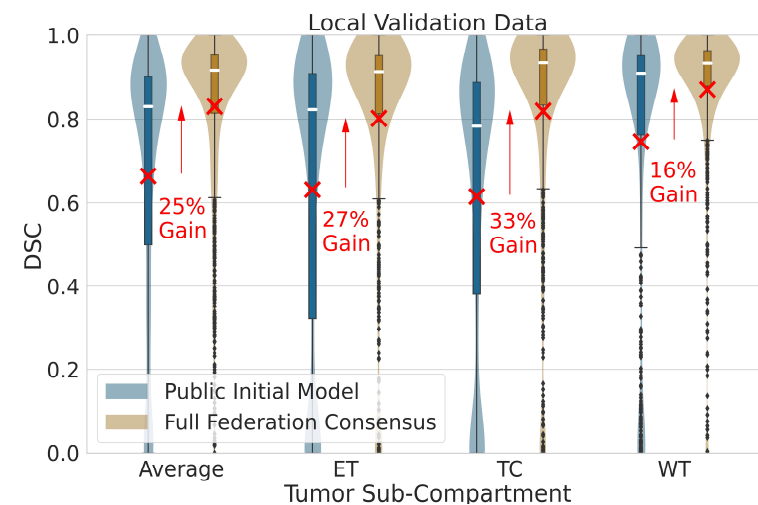
# Federated learning



## Federated Brain Tumor Segmentation (FeTS)



- **public initial model** : trained on 231 cases from 16 sites
- **Out-of-sample site** : did not participate in model training



[Pati et al arxiv 22]

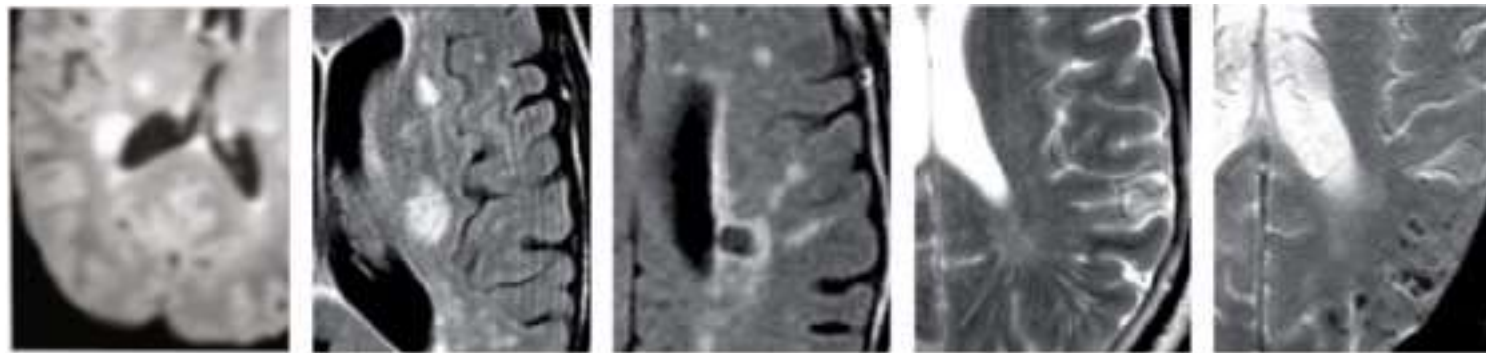
## USE CASE # 2

Detection and localisation of subtle brain anomalies

## Unsupervised anomaly detection

## Learning with no annotation

Annotations are time consuming and sometimes hard/impossible to generate



multiple  
sclerosis

white matter  
hyperintensity

lacune

perivascular  
space

cerebral  
microbleed

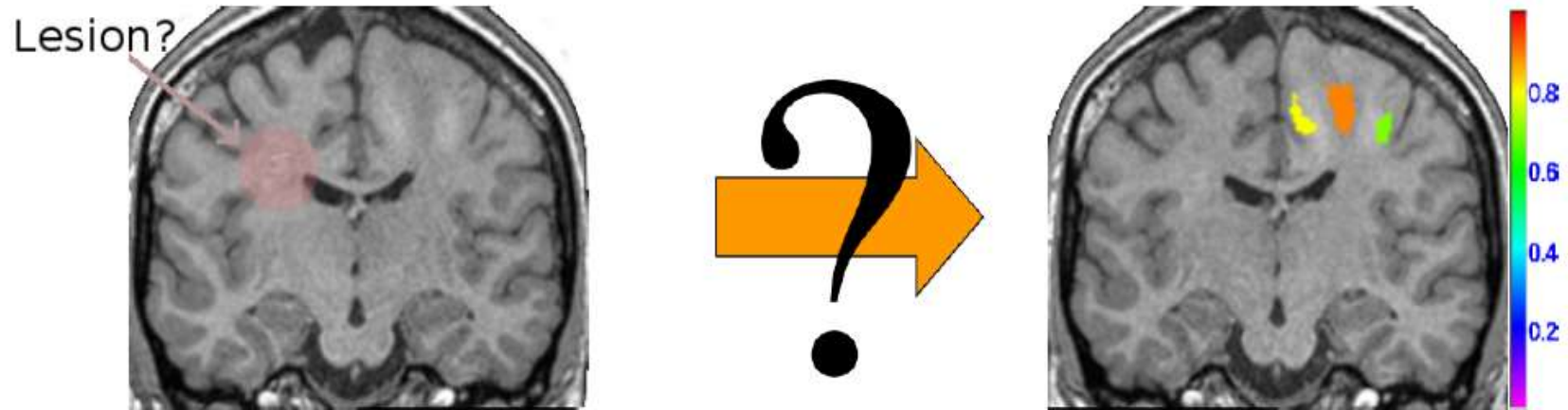
Exemple neuropathologies with subtle lesions

 **Unsupervised anomaly detection (UAD)**

Illustration from [Wardlaw et al. , 2012](#)



## Problem formulation: objectives & challenges



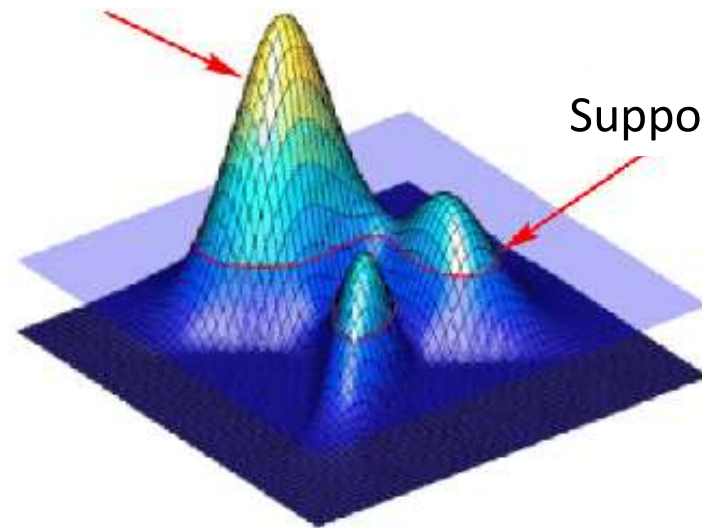
- Multi-modality data (MRI, PET)
- High dimensional data
- No pathological examples
- Noisy images

- Labelled cluster map
- Probabilistic outputs

## Problem formulation

- Formulate the problem as an anomaly detection problem
- Model the distribution of the normal class
- Detect outliers from the normative distribution

Normative distribution

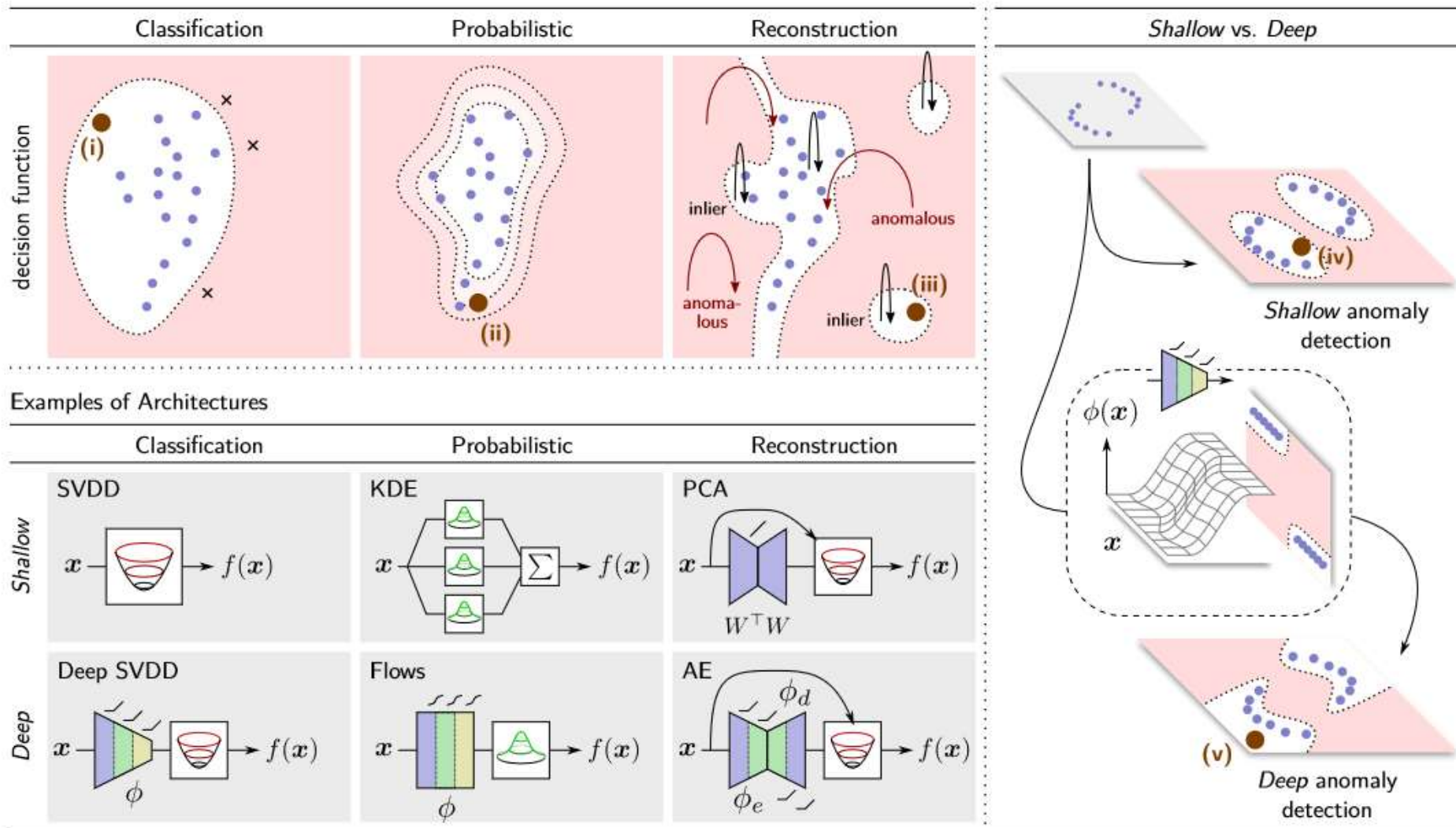


Support of the normative distribution



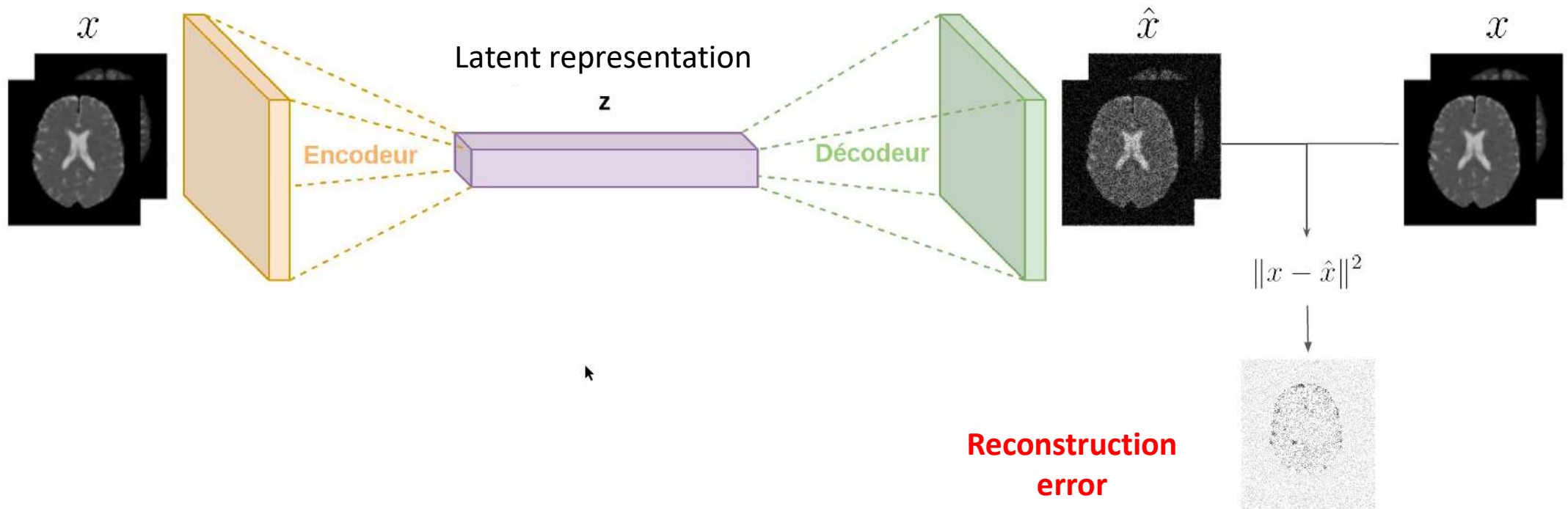
# A Unifying Review of Deep and Shallow Anomaly Detection

Lukas Ruff, Jacob R. Kauffmann, Robert A. Vandermeulen, Grégoire Montavon, Wojciech Samek, *Member, IEEE*,  
Marius Kloft\*, *Senior Member, IEEE*, Thomas G. Dietterich\*, *Member, IEEE*,  
Klaus-Robert Müller\*, *Member, IEEE*.

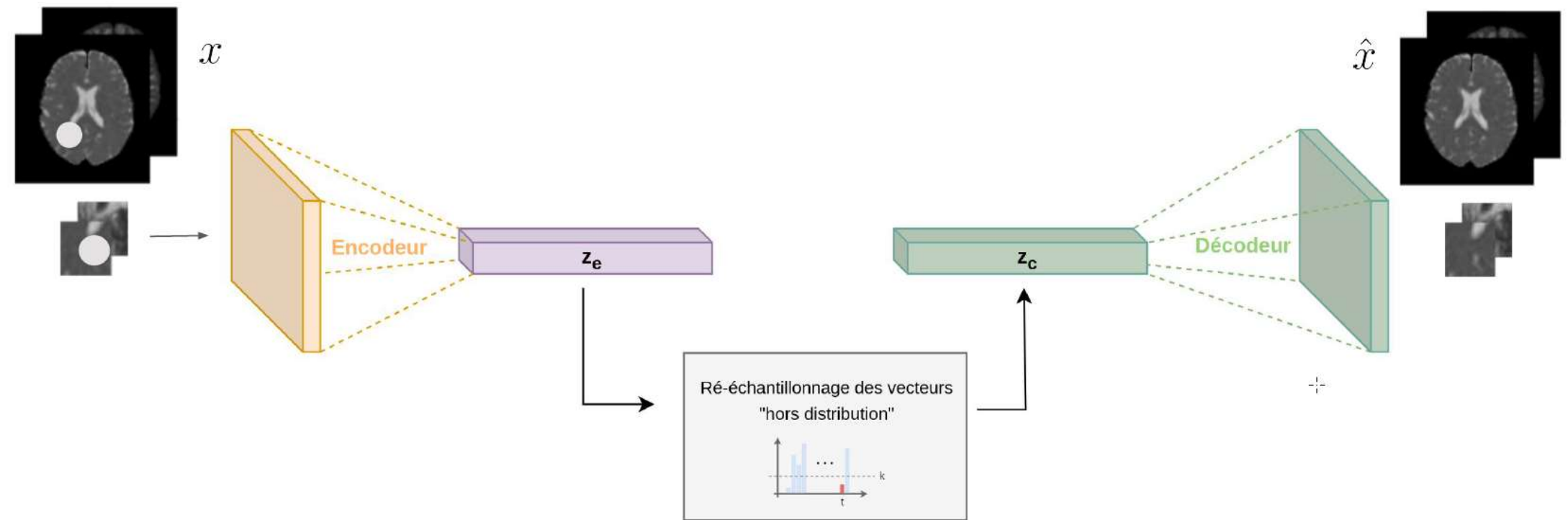


Proceedings of the IEEE (2021) 1-40

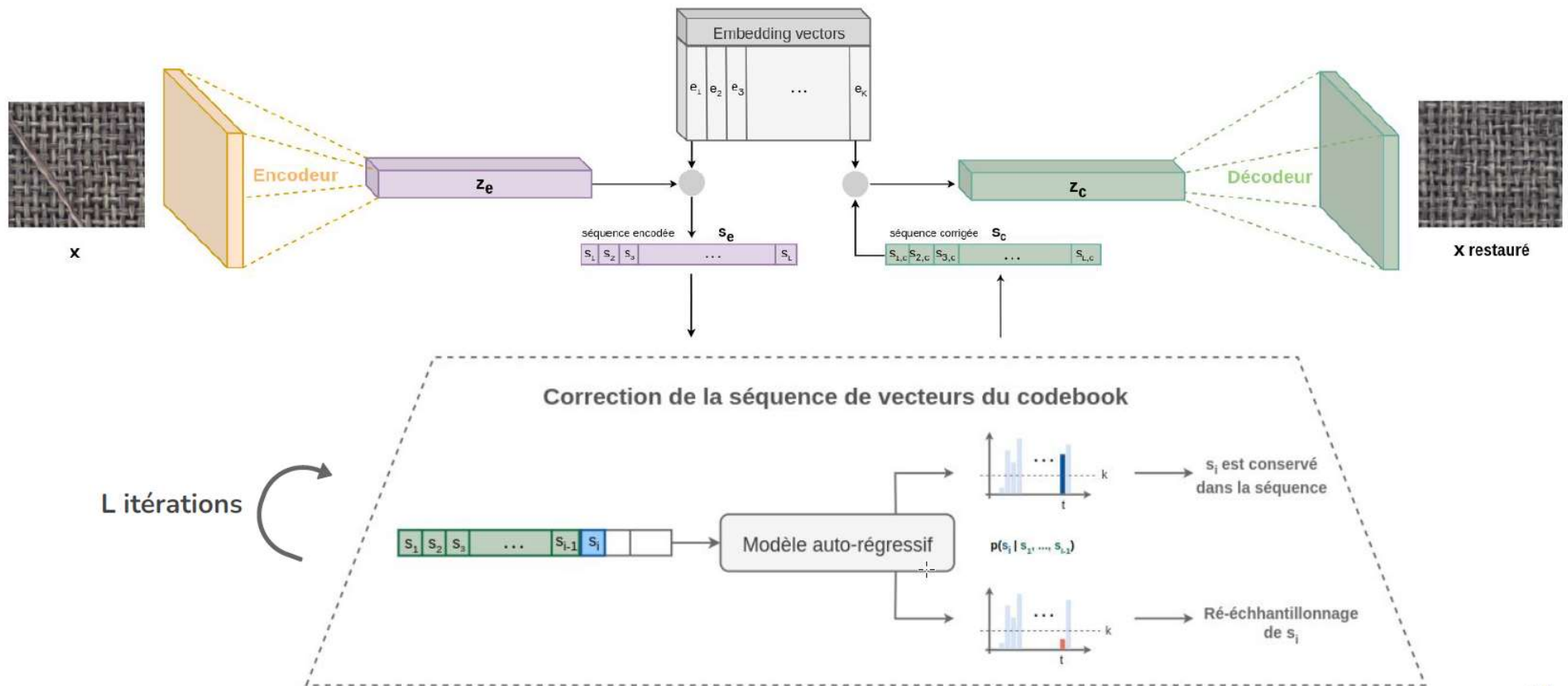
Anomaly detection based on reconstruction error



# Anomaly detection based on reconstruction error after restauration of the latent representation



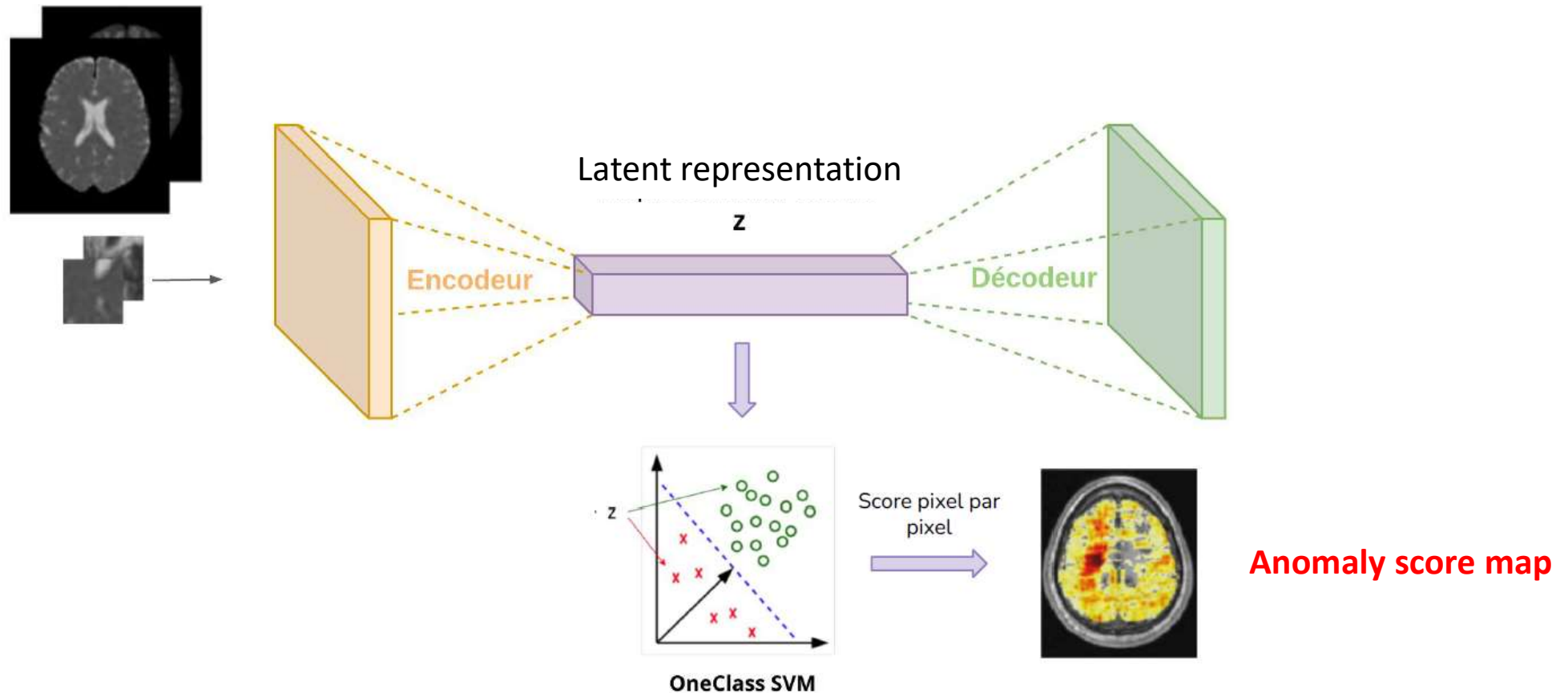
# Vector quantized –variational auto-encoder (VQ-VAE)



21

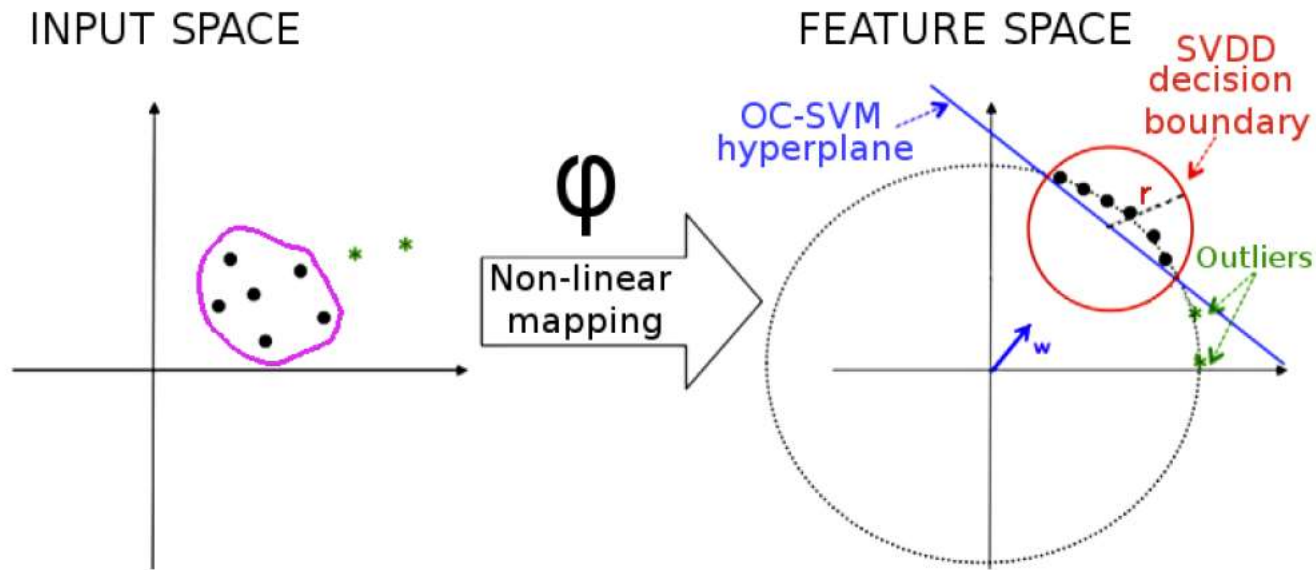
[Oord et al, 2017]

Anomaly detection based on **estimation of the support of the normative distribution in the latent space**



[Alaverdyan MEDIA 2020]





### One class-SVM

### Support Vector Data Description

$$\begin{cases} \min_{\mathbf{w}, \rho} & \frac{1}{2} \|\mathbf{w}\| - \rho \\ \text{with} & \mathbf{w}^T \mathbf{x}_i \geq \rho + \frac{1}{2} \|\mathbf{x}_i\|^2 \end{cases}$$

$$\begin{cases} \min_{R \in \mathbb{R}, \mathbf{c} \in \mathbb{R}^d} & R^2 \\ \text{with} & \|\mathbf{x}_i - \mathbf{c}\|^2 \leq R^2, \quad i = 1, \dots, n \end{cases}$$

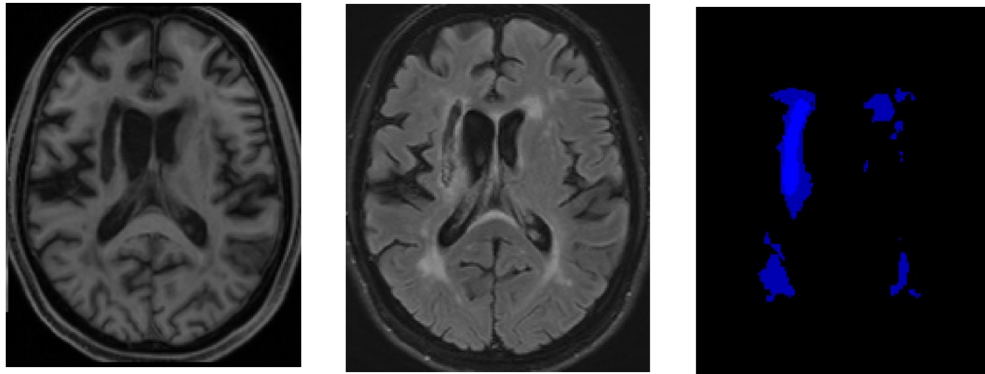
with  $\rho = \frac{1}{2} (\|\mathbf{c}\|^2 - R)$  and  $\mathbf{w} = \mathbf{c}$ .

# Benchmarking UAD models on the challenge WMH dataset



## The WMH challenge dataset

## White Matter Hyperintensities (WMH)



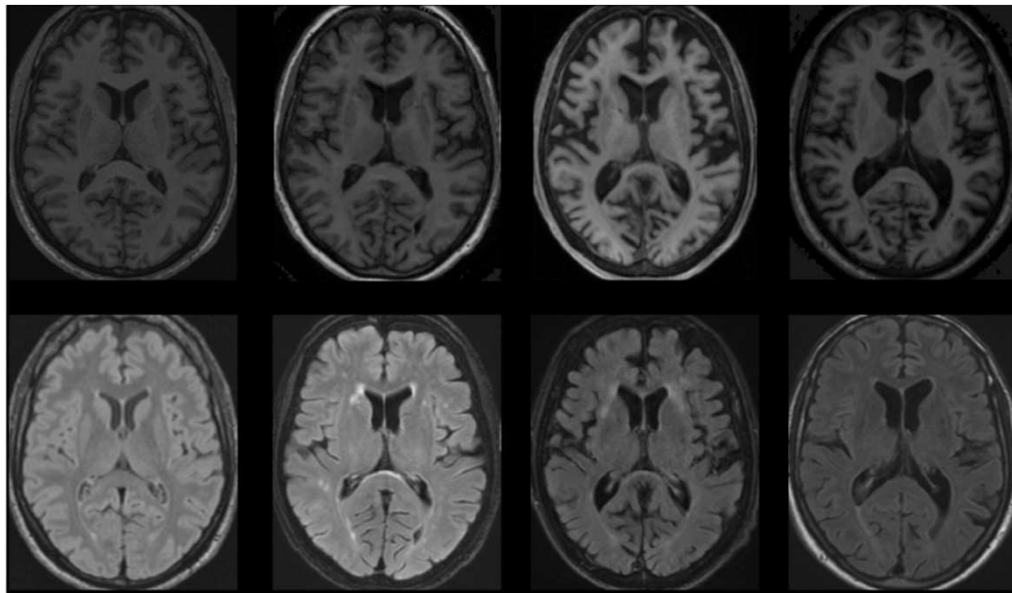
T1

FLAIR

GT

- The **control private dataset** :
  - 75 paired T1w and FLAIR MRI scans of healthy subjects
  - Acquired on a 1.5T Siemens Sonata scanner.
- The **WMH Challenge dataset**:
  - 60 T1w and FLAIR images
  - acquired on 3 different hospitals with 3 scanners of different manufacturers,
  - each image as its associated 3D lesion mask.

T1

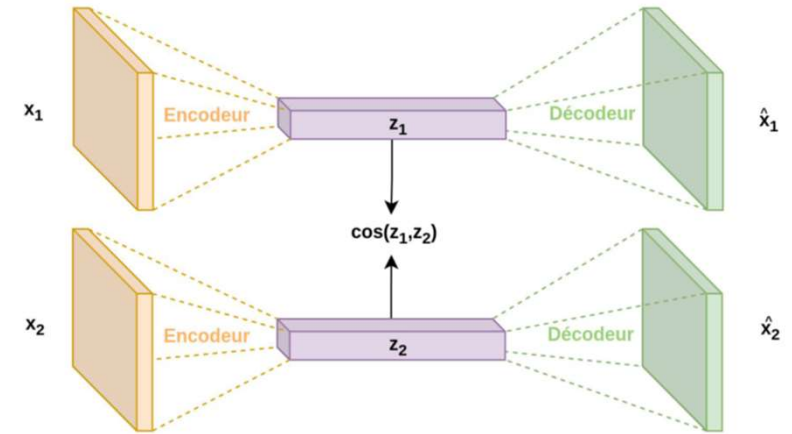
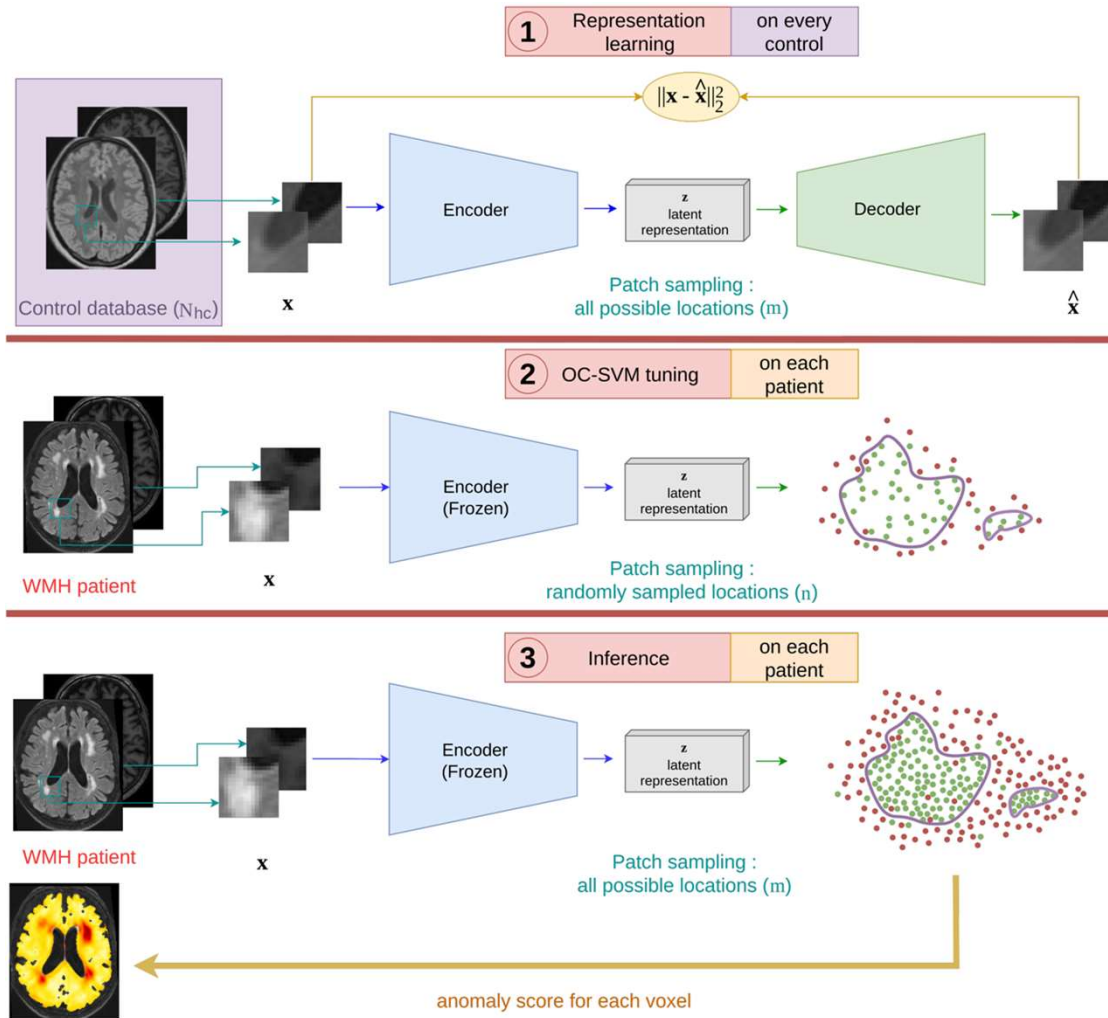


Control

Amsterdam

Singapore

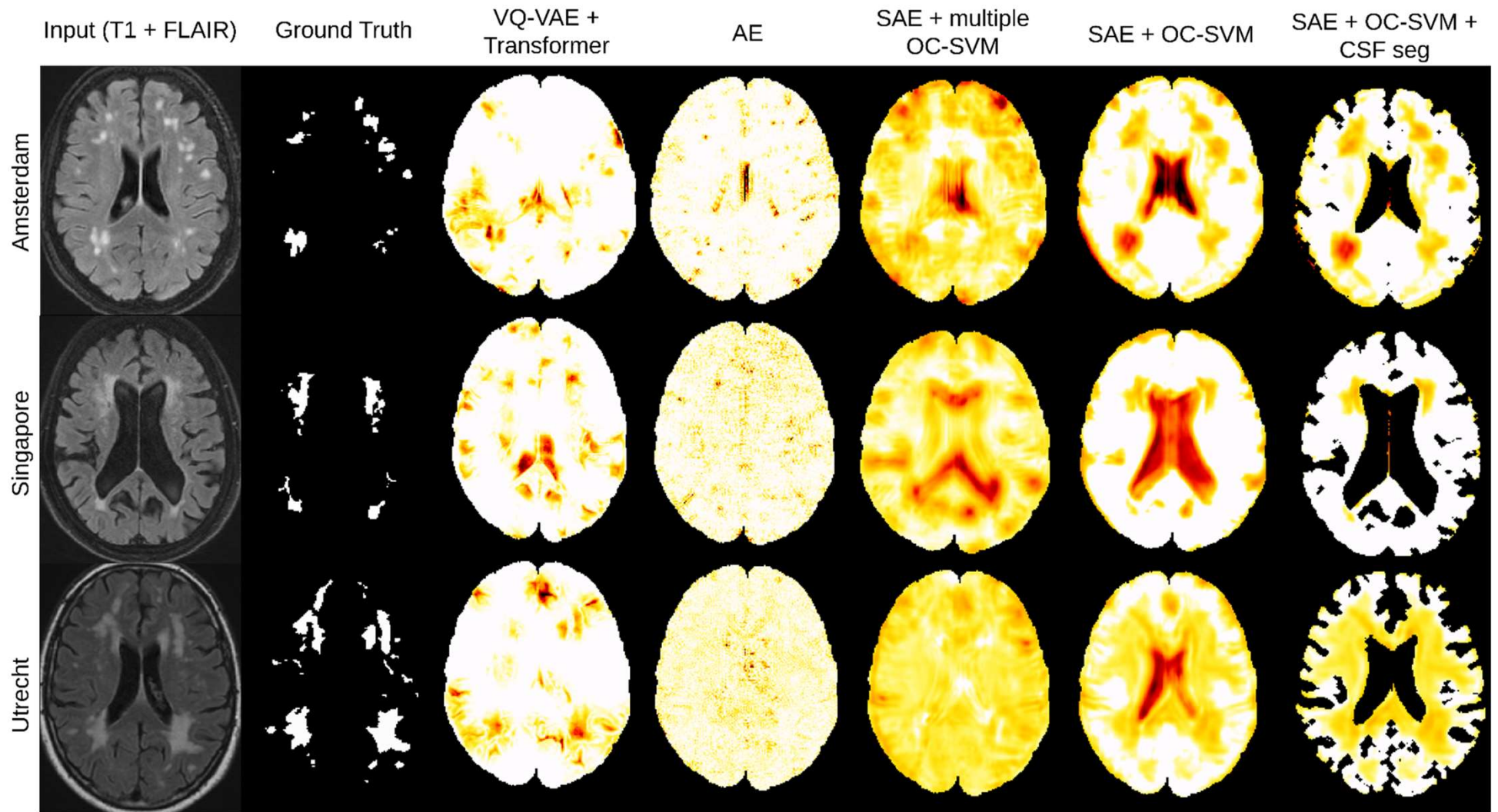
Utrecht



Siamese autoencoder

$$L_{SAE}(x_1, x_2) = \sum_{t=1}^2 \|x_t - \hat{x}_t\|_2^2 - \alpha \cdot \cos(z_1, z_2)$$

[Pinon MIDL 2023]



[Pinon MIDL 2023]



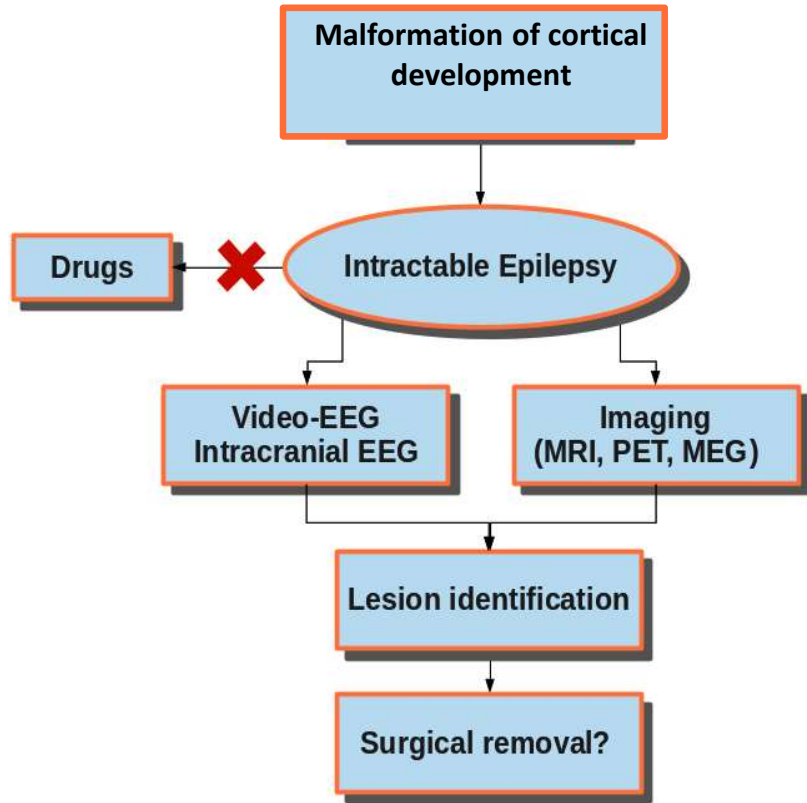
| 3 hospitals | VQ-VAE<br>+ Transformer<br>(Pinaya) | AE<br>(Baur)  | SAE<br>+ multiple<br>OC-SVM<br>(Alaverdyan) | SAE<br>+ OC-SVM<br>(Ours) | SAE<br>+OC-SVM<br>+CSF seg<br>(Ours) |
|-------------|-------------------------------------|---------------|---------------------------------------------|---------------------------|--------------------------------------|
| AU ROC      | 0.69 ± 0.13                         | 0.53 ± 0.09   | 0.52 ± 0.19                                 | <b>0.80</b> ± 0.09        | <b>0.81</b> ± 0.10                   |
| AU ROC 30   | 0.40 ± 0.20                         | 0.20 ± 0.12   | 0.19 ± 0.16                                 | <b>0.48</b> ± 0.20        | <b>0.59</b> ± 0.17                   |
| AU PRC      | 0.065 ± 0.079                       | 0.028 ± 0.030 | 0.023 ± 0.031                               | <b>0.084</b> ± 0.099      | <b>0.165</b> ± 0.168                 |
| AU PRO      | 0.55 ± 0.10                         | 0.50 ± 0.08   | 0.43 ± 0.17                                 | 0.71 ± 0.11               | <b>0.80</b> ± 0.07                   |
| AU PRO 30   | 0.19 ± 0.13                         | 0.15 ± 0.07   | 0.09 ± 0.13                                 | 0.33 ± 0.18               | <b>0.48</b> ± 0.13                   |
| [ Dice ]    | 0.11 ± 0.10                         | 0.06 ± 0.05   | 0.05 ± 0.05                                 | <b>0.14</b> ± 0.13        | <b>0.22</b> ± 0.17                   |

[Pinon MIDL 2023]

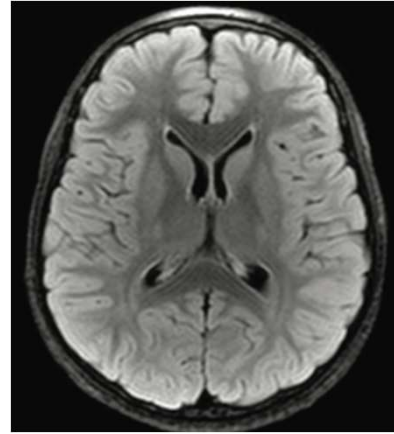
- The proposed SAE+ OC-SVM model performs on par with the state of the art UAD model on the WMH dataset
- Limits of the WMH dataset as a reference dataset for UAD benchmarking :
  - Anomaly are ‘easy’ to detect on FLAIR images
  - Anomaly are not visible on T1 images
  - Median age of the population is high → physiological normal anomalies due to brain aging process (cortex shrinkage..)

# Unsupervised anomaly detection of the epileptogenic zone (EZ)

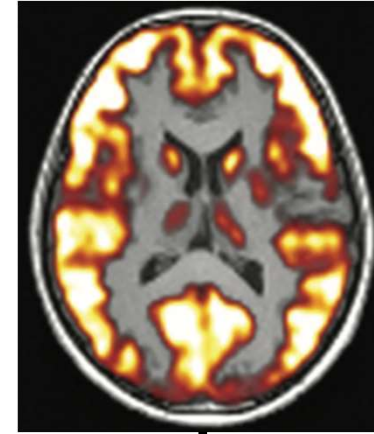
# Management of the patient with medically refractory epilepsy



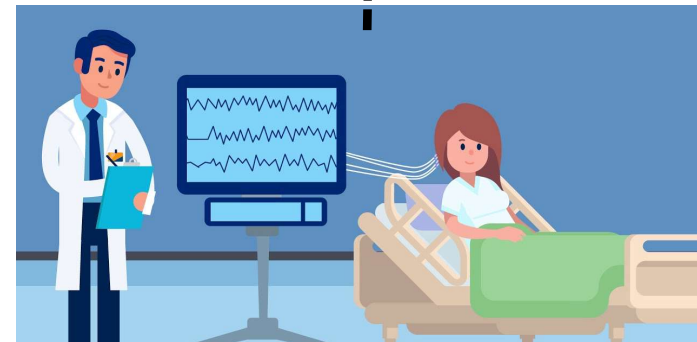
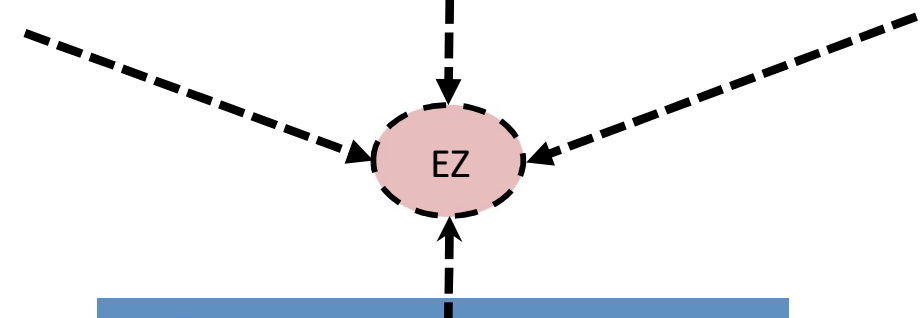
anatomical MRI



FDG PET



MEG

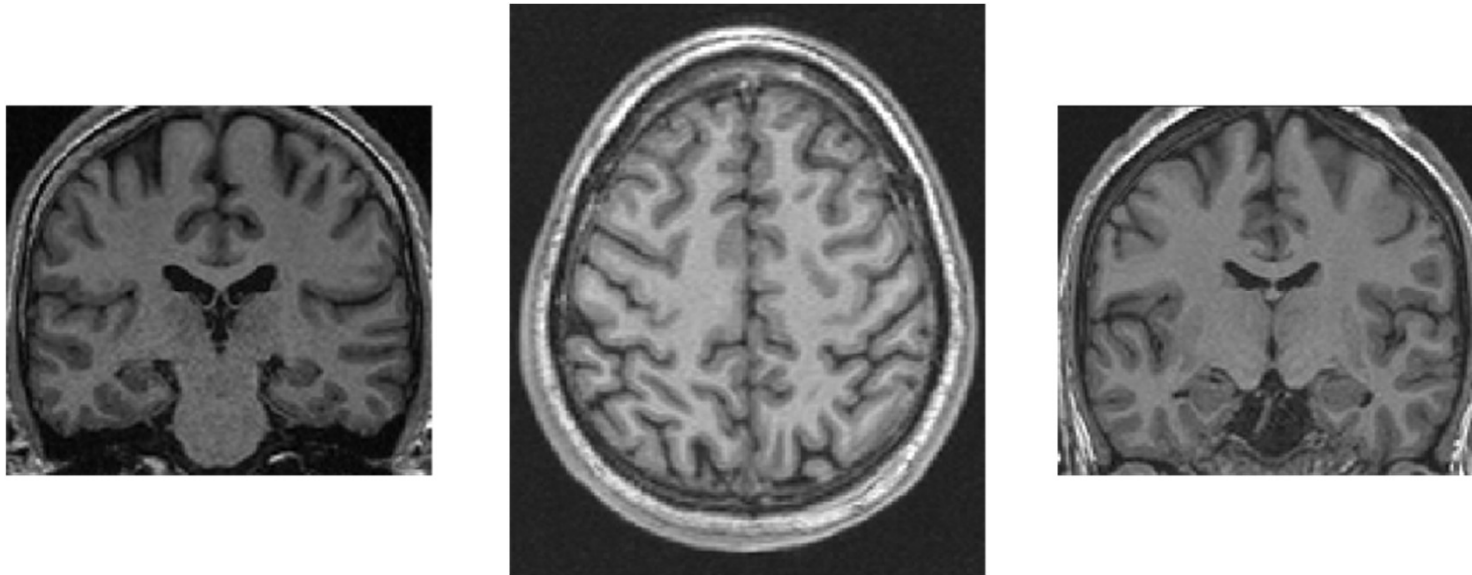


Long-Term Video EEG

**EZ = Epileptogenic Zone**



- Imaging plays a crucial role in the surgical planning



- But the detection task is hard

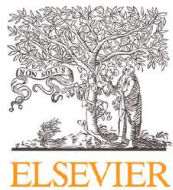
- 20-30% of patient MRI are « negative » meaning the physician considered the exam as « non pathological »



- Detecting and localizing the epileptogenic zone → significant improvement of good surgery outcome

[Nagae et al. 2016]

Medical Image Analysis 60 (2020) 101618



Contents lists available at ScienceDirect

## Medical Image Analysis

journal homepage: [www.elsevier.com/locate/media](http://www.elsevier.com/locate/media)



### Regularized siamese neural network for unsupervised outlier detection on brain multiparametric magnetic resonance imaging: Application to epilepsy lesion screening



Zaruhi Alaverdyan<sup>a</sup>, Julien Jung<sup>b</sup>, Romain Bouet<sup>b</sup>, Carole Lartizien<sup>a,\*</sup>

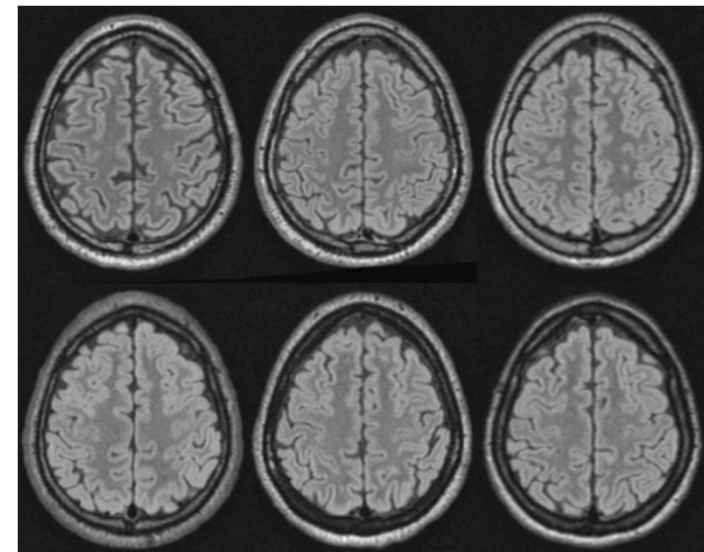
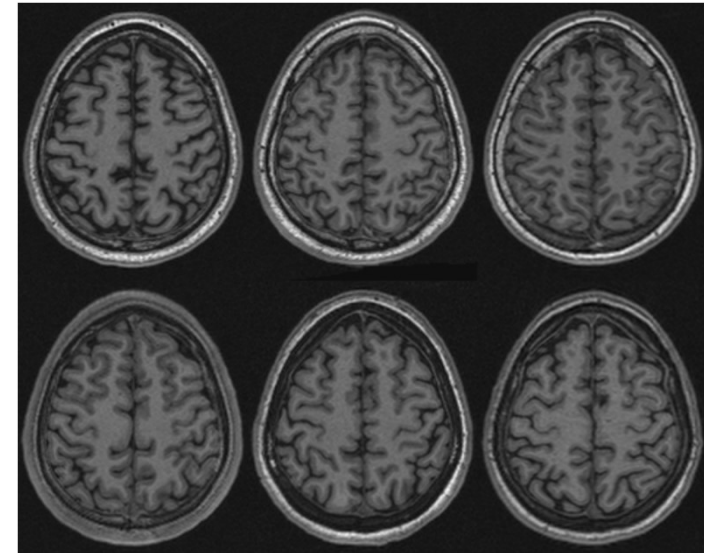
<sup>a</sup> Univ Lyon, INSA-Lyon, Université Claude Bernard Lyon 1, UJM-Saint Etienne, CNRS, Inserm, CREATIS UMR 5220, U1206, F69621, Lyon, France

<sup>b</sup> Lyon Neuroscience Research Center, CRNL, INSERM U1028, CNRS UMR5292, University Lyon 1, Lyon, France

| References               | Subjects    | Imaging modality | Imaging features | Classifiers | Main outcomes                         |
|--------------------------|-------------|------------------|------------------|-------------|---------------------------------------|
| Alaverdyan et al. (2020) | 21 FE, 75HC | T1, FLAIR        | Signals          | SVM, RSN    | Sens. = 0.62 to detect anomaly lesion |

## Dataset

- The **private control dataset** :
  - 75 paired T1w and FLAIR MRI scans of healthy subjects
  - Acquired on a 1.5T Siemens Sonata scanner.
- The **private epilepsy dataset**:
  - 21 T1w and FLAIR images
  - Acquired on a 1.5T Siemens Sonata scanner
  - Référence of EZ localization is based on
    - Post-surgery Engel score
    - Manual annotation of the lesion on the MRI based on clinical report and sEEG analysis

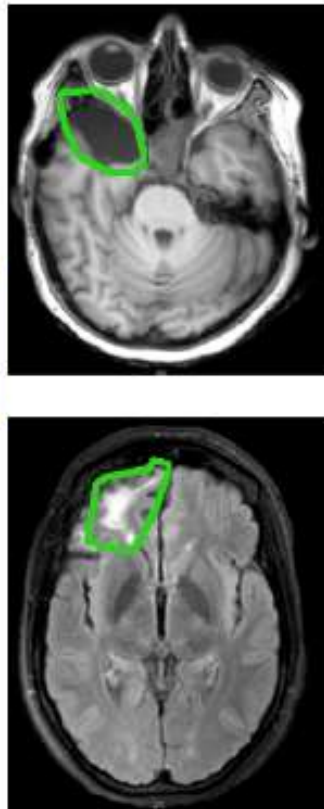


Example T1 and FLAIR images of patients

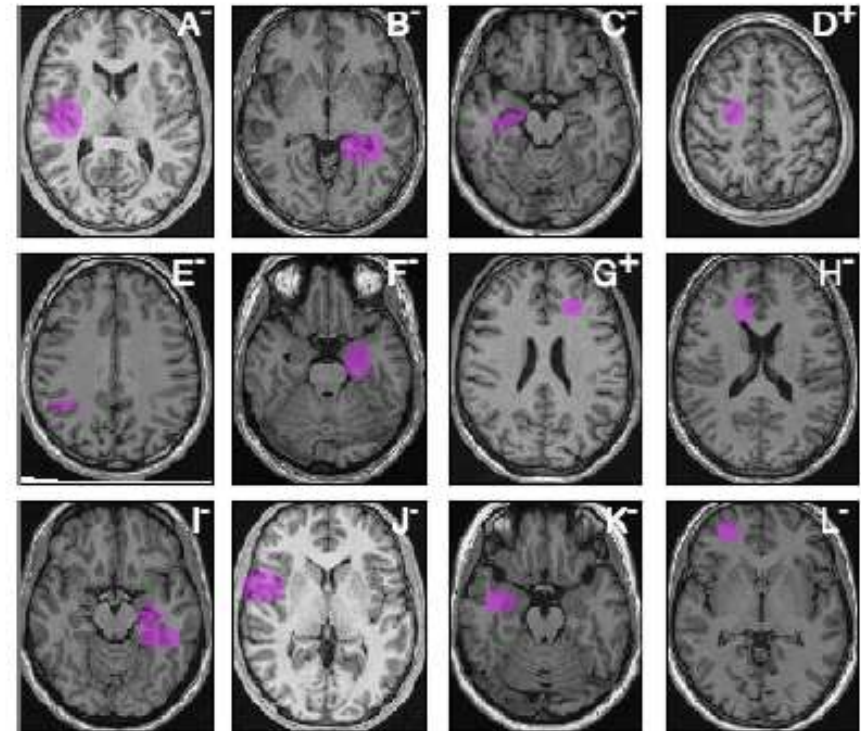


Post-surgical scans  
thermocoagulation reports

Positive outcome :  
seizure-free patients



Ground truth : 18 MRI-negative patients



*Lesion annotations obtained in collaboration with Dr J. Jung*

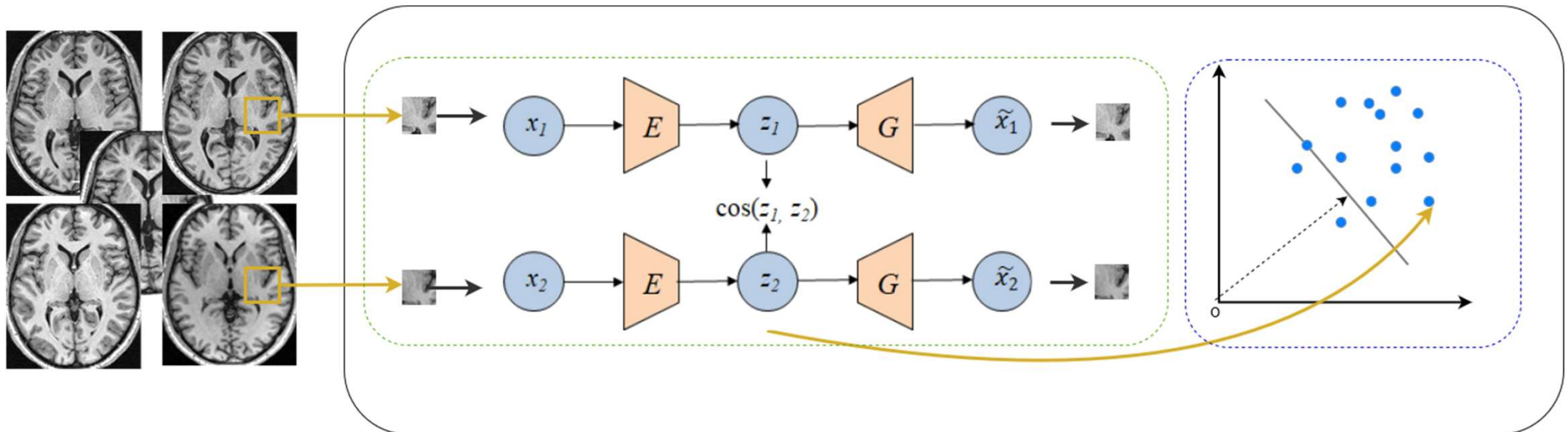
# Unsupervised anomaly detection

Step 1 : train a self-supervised model on healthy control data

Healthy control database

Deep siamese autoencoder for representation learning

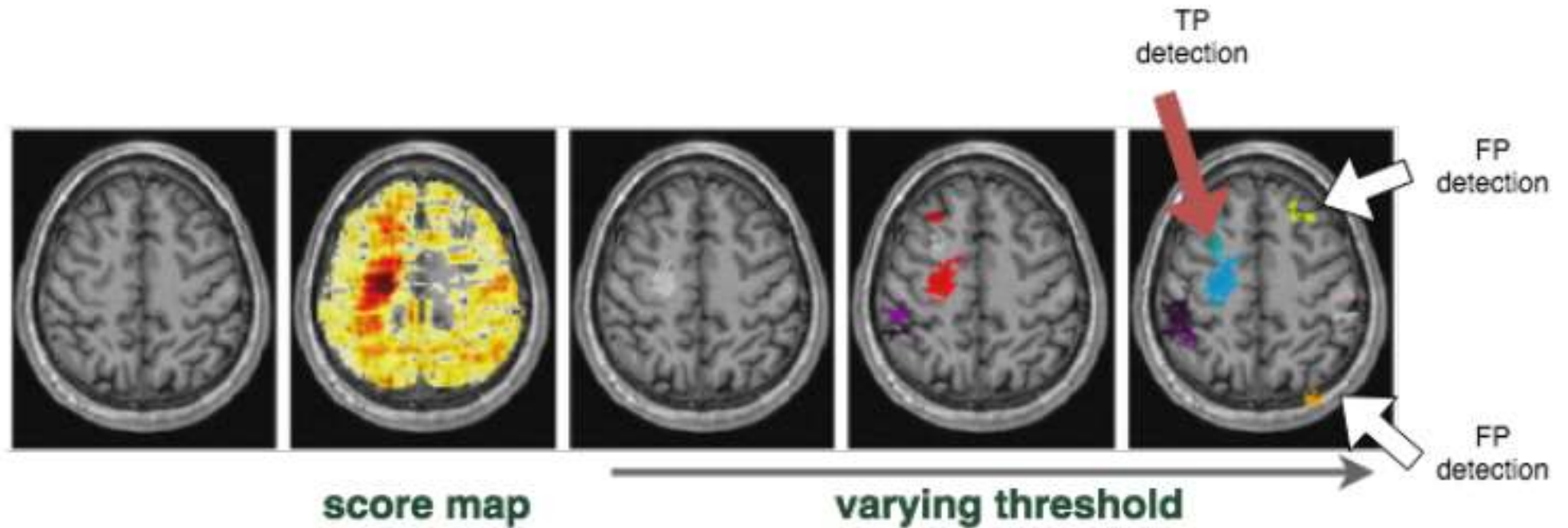
Outlier detection with oc-SVM in the latent space



[Alaverdyan et al MEDIA 2020]

# Unsupervised anomaly detection

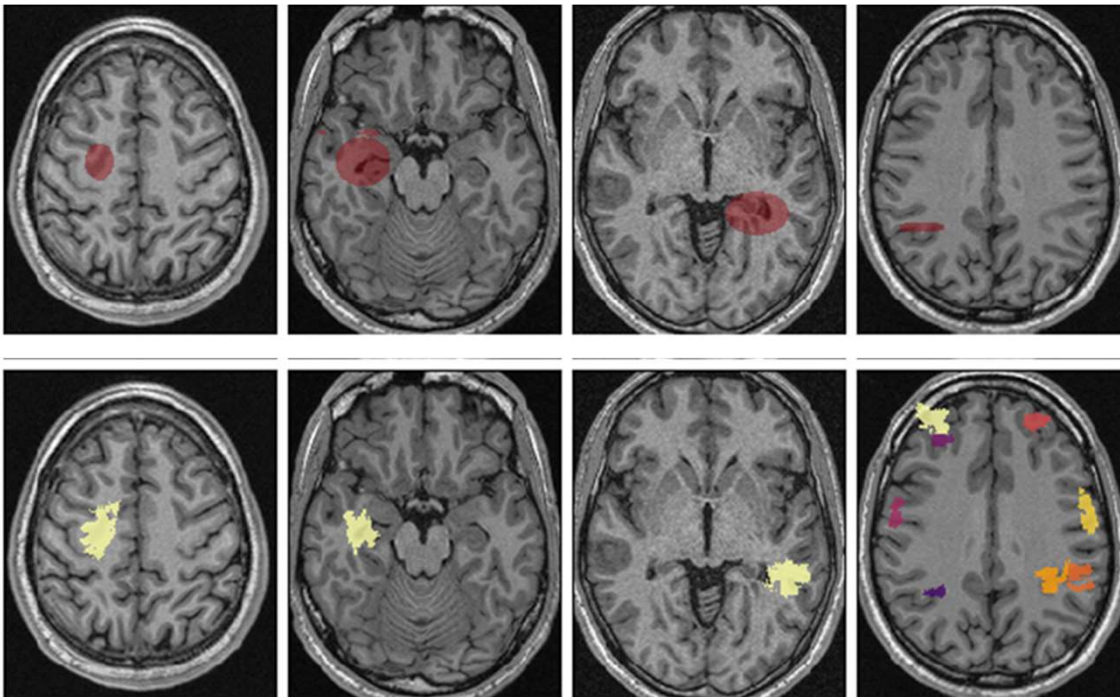
Step 2 : detect anomalous pattern in epilepsy patients



**Predicted lesion map (MIP).**  
The brighter colour, the most suspicious the clusters

[Alaverdyan et al MEDIA 2020]





### Predicted lesion map (MIP).

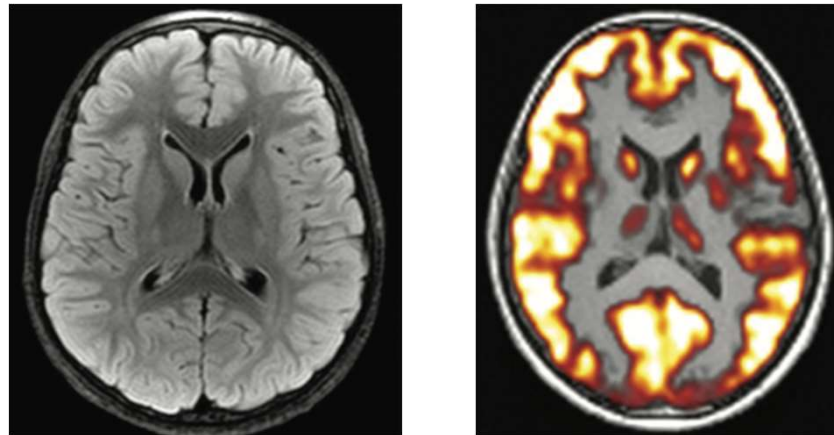
The brighter colour, the most suspicious the clusters

- **Sensitivity :**
  - 62% on 21 negative MRI negative exams of epilepsy patients
- **Specificity**
  - Mean rank of the detected clusters : 3.5

[Alaverdyan et al MEDIA 2020]

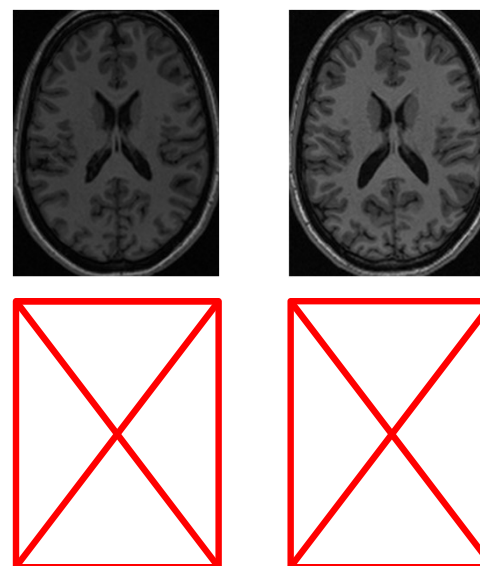
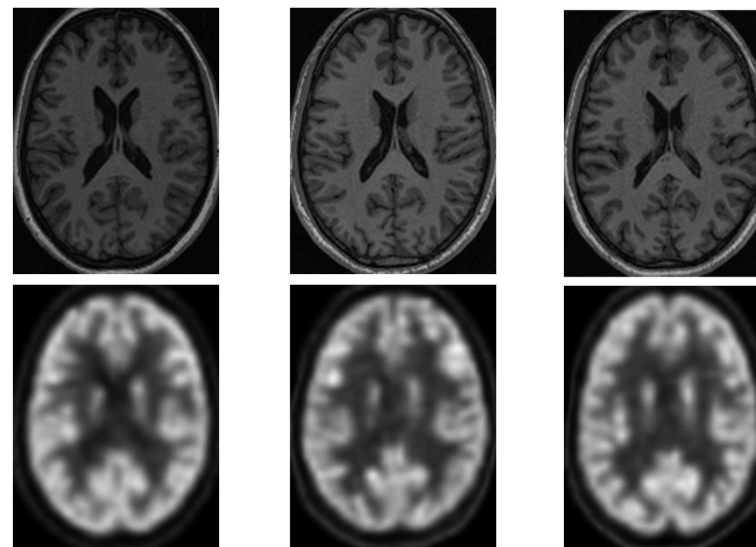
## Dataset

- How to improve ?
- Include PET modality → complementary information



## Dataset

- The **private control dataset** :
  - **35 paired** T1w MRI and FDG scans of healthy subjects
  - Acquired on a 1.5T Siemens Sonata scanner.
  - 40 T1w MRI of healthy subject with NO paired FDG PET examen
  
- The **private epilepsy dataset**:
  - 21 T1w and PET images
  - Acquired on a 1.5T Siemens Sonata scanner
  - Référence of EZ localization is based on
    - Post-surgery Engel score
    - Manual annotation of the lesion on the MRI based on clinical report and sEEG analysis



Challenge :  
Missing data in  
the control  
population



## GAN-based synthetic FDG PET images from T1 brain MRI can serve to improve performance of deep unsupervised anomaly detection models

Daria Zotova<sup>1</sup>, Julien Jung<sup>2</sup>, and Carole Lartizien<sup>1</sup>[0000-0001-7594-4231]

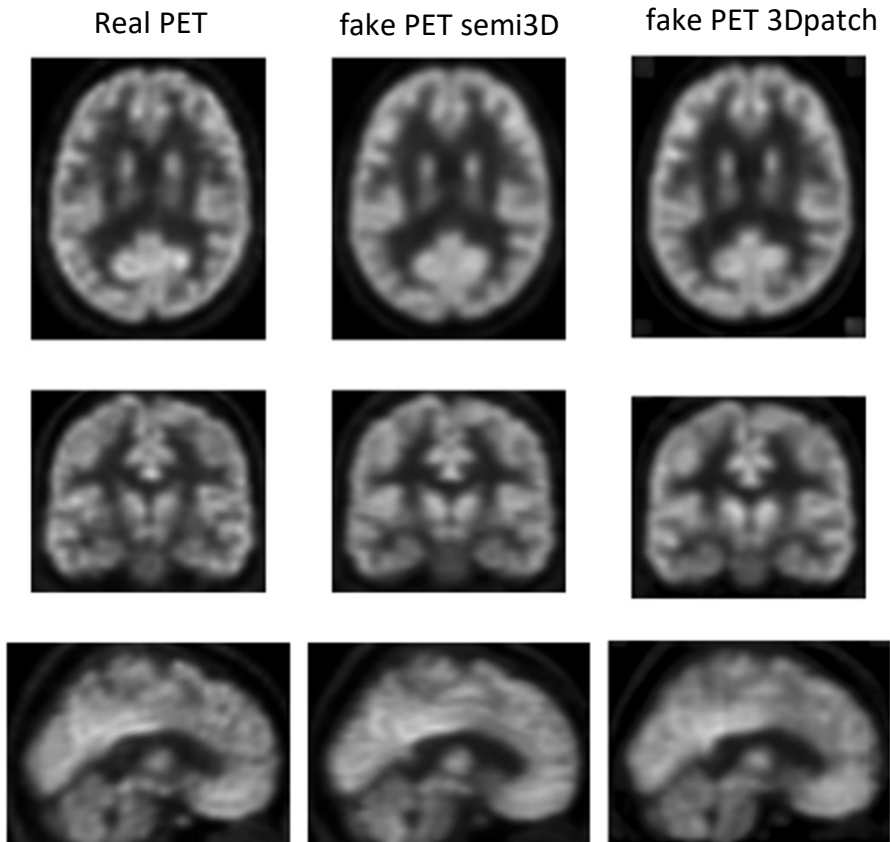
<sup>1</sup> Univ Lyon, CNRS, Inserm, INSA Lyon, UCBL, CREATIS, UMR5220, U1206,  
F-69621, Villeurbanne, France

{Daria.Zotova,Carole.Lartizien}@creatis.insa-lyon.fr

<sup>2</sup> Lyon Neuroscience Research Center, CRNL, INSERM U1028, CNRS UMR5292,  
University Lyon 1, Lyon, France







Qualitative analysis of the synthetic normative PET data

|               | 35 T1+PET real | 35 T1+fake PET semi3d | 35 T1+fake PET 3dpatch | Color code      |
|---------------|----------------|-----------------------|------------------------|-----------------|
| Patient A     | -              | -                     | -                      | lobe temporal L |
| Patient B     | x (5)          | x (4)                 | x (1)                  | lobe temporal R |
| Patient C     | x (3)          | x (4)                 | x (2)                  | pole temporal R |
| Patient D     | x (8)          | -                     | x (1)                  | insula          |
| Patient E     | -              | -                     | -                      | other           |
| Patient F     | -              | x (4)                 | x (5)                  |                 |
| Patient G     | x (1)          | x (1)                 | x (3)                  |                 |
| Patient H     | -              | x (3)                 | x (5)                  |                 |
| Patient I     | x (7)          | x (1)                 | x (1)                  |                 |
| Patient J     | x (4)          | x (3)                 | -                      |                 |
| Patient K     | -              | -                     | -                      |                 |
| Patient L     | -              | -                     | x (2)                  |                 |
| # of detected | 6              | 7                     | 8                      |                 |
| mean rank     | 4,7            | 2,9                   | 1,9                    |                 |

Performance of the UAD model trained with real or synthetic normative PET data

[Zotova et al MICCAI SASHIMI 2021]

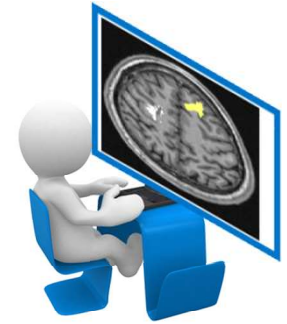




**From  
Research..**

## Unsupervised anomaly detection

**Some methodological challenges to  
address ..**



**..to clinic**

- **Improve performance**
  - Inject some priors → toward weak supervision
  - Efficiently fuse multi-modality imaging and non imaging data, accounting for missing modalities -> unsupervised representation modeling (couplage LLM and CV modeling..)
- **Generalize well**
  - Same level of performance regardless of data origin and quality
- Provide some **confidence level** on predictions
- Be **respectful of privacy**

# Thank you for your attention!

## Acknowledgments

Most of the illustrations and the reported results of this talk were produced by PhD students of my group, Meriem El Azami, Zaruhi Alaverdyan, Daria Zotova, Nicolas Pinon, Matthis Manthe, Robin Trombetta.

## More on our work

<https://scholar.google.fr/citations?user=na6f2dQAAAAJ&hl=fr>