

Revue calorimétrie et photodétecteur pour l'imagerie médicale

Sara Marcatili

LPSC – Laboratoire de Physique Subatomique et Cosmologie

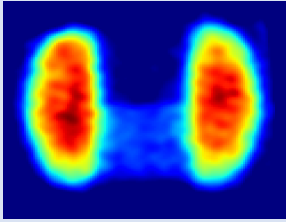


Imaging instrumentation at IN2P3

Nuclear imaging

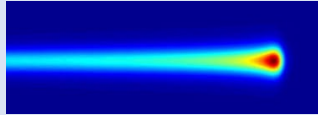
X-ray Imaging

γ camera and SPECT
Single Photon Emission Computed Tomography



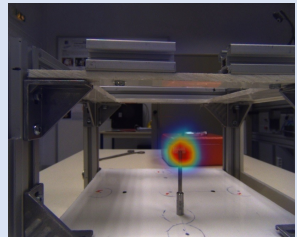
$E_\gamma = 0.1 \div 1$ MeV
Photoelectric

Prompt Gamma Imaging



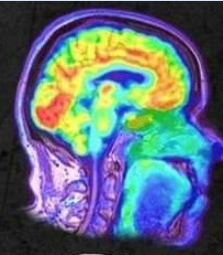
$E_\gamma = 1 \div 10$ MeV
Compton + Pair P.

Environmental applications



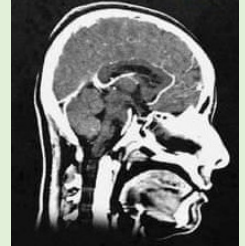
$E_\gamma > 1$ MeV
Compton

PET
Positron Emission Tomography

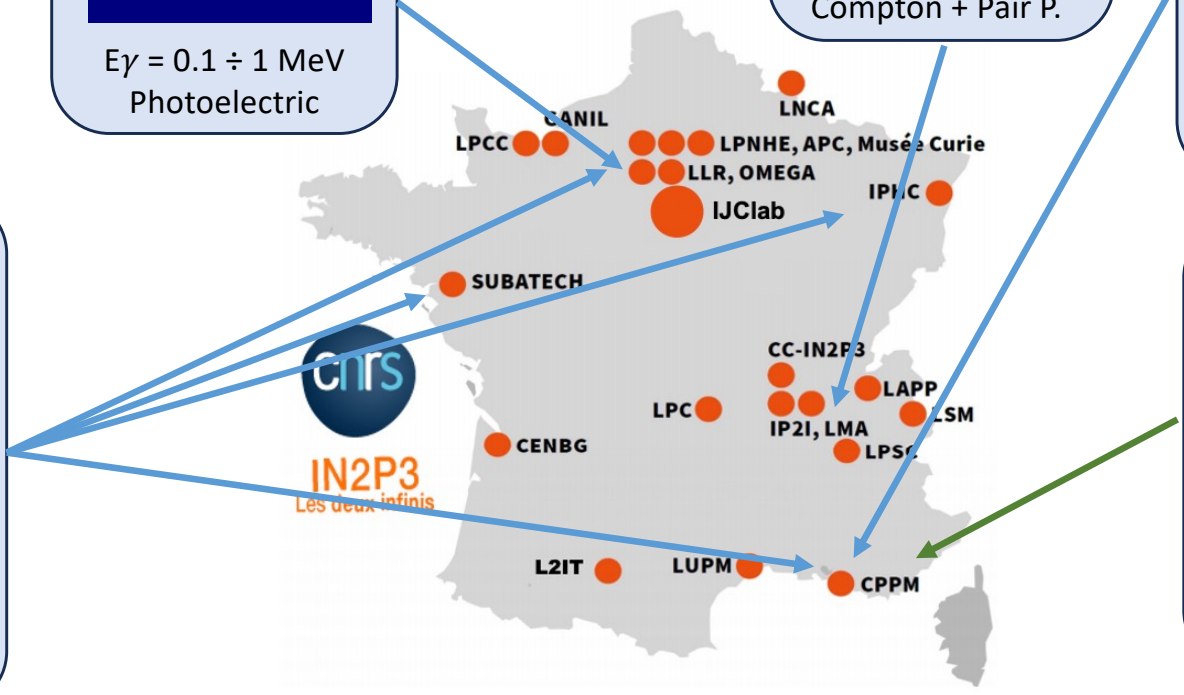


$E_\gamma = 511$ keV
Photoelectric

X-ray imaging

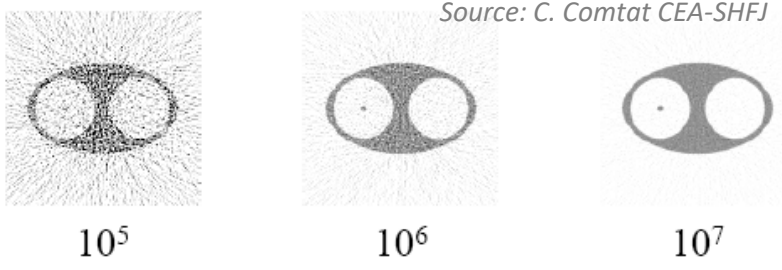
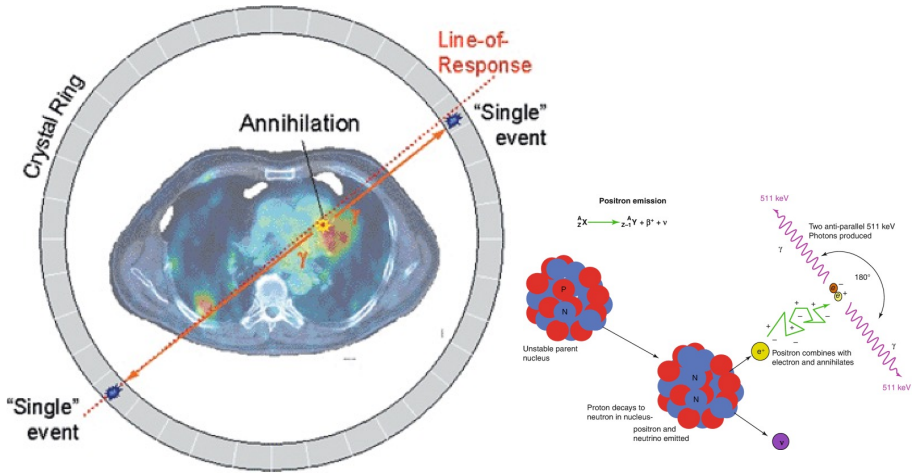


$E_x < 200$ keV
Photoelectric



Positron Emission Tomography

More events, better images... higher dose !



Many strategies to increase sensitivity

10 ps – PET

- <1.5 spatial resolution on the LOR
- No need for tomographic back-projection
- 14-fold improvement in SNR
- or 20-fold dose reduction

The diagram shows an 'Annihilation' event within a 'Crystal Ring'. Two 'LOR' lines are drawn from the event to the detectors. Time-of-flight (TOF) is measured as the difference in arrival times $t_2 - t_1$. Two histograms are shown: 'without TOF' (broad distribution) and 'with TOF' (narrow distribution), demonstrating improved spatial resolution.

3 γ PET

- ^{44}Sc : β^+ emitter + 1.157 MeV γ
- LOR / Compton cone intersection
- Shorter scans or lower dose

The diagram shows a 'Liquid xenon Compton Telescope' (LXCT) setup. A ^{44}Sc source emits a positron (β^+) and a 1.157 MeV γ ray. The positron annihilates, producing two 511 keV γ rays. The LXCT consists of 'Crystals + PM' (Photomultiplier) layers. The γ rays interact via Compton scattering, creating a 'Compton cone'. The intersection of the LOR and the Compton cone determines the event location. The formula $\Delta l = f(\sigma_E, \sigma_x, \sigma_y, \sigma_z)$ is shown. A box specifies: ^{44}Sc (β^+ ; $E_{\text{max}} = 1,474$ MeV, γ : $E_0 = 1,157$ MeV).

Whole body PET

- Currently < 1% of available signal collected
- Lower dose
- Study of systemic disease

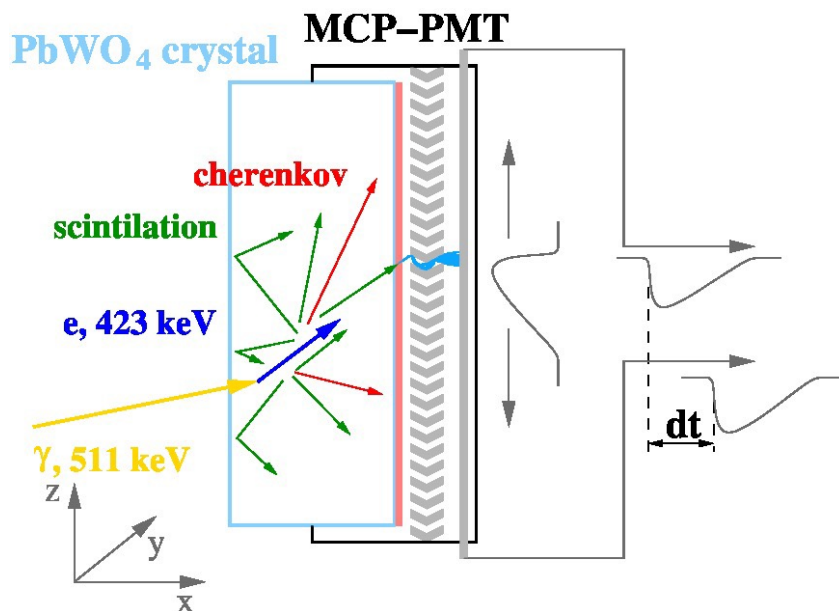
A 3D rendering of a whole-body PET scanner, showing a long cylindrical ring of detectors. Source: Explorer project, S. Cherry

Hybrid imaging (PET/CT – PET MRI)

Combining functional and morphological information

A PET/CT scan image showing a cross-section of a patient's chest. The PET image (color) is overlaid on the CT image (grayscale), showing functional information combined with anatomical structure.

Development of scintronic MCP-PMT detection modules for fast timing



- Detection of scintillation and Cherenkov photons emitted in PWO
- Direct deposition of a photocathode ($n \sim 2,7$) on the crystal surface ($n \sim 2,3$)
- Encapsulation within a Micro-Channel Plate Multiplier Tube (MCP-MT)
- Coincidence Time resolution (CTR) ~ 20 ps FWHM (excluding MCP-MT)

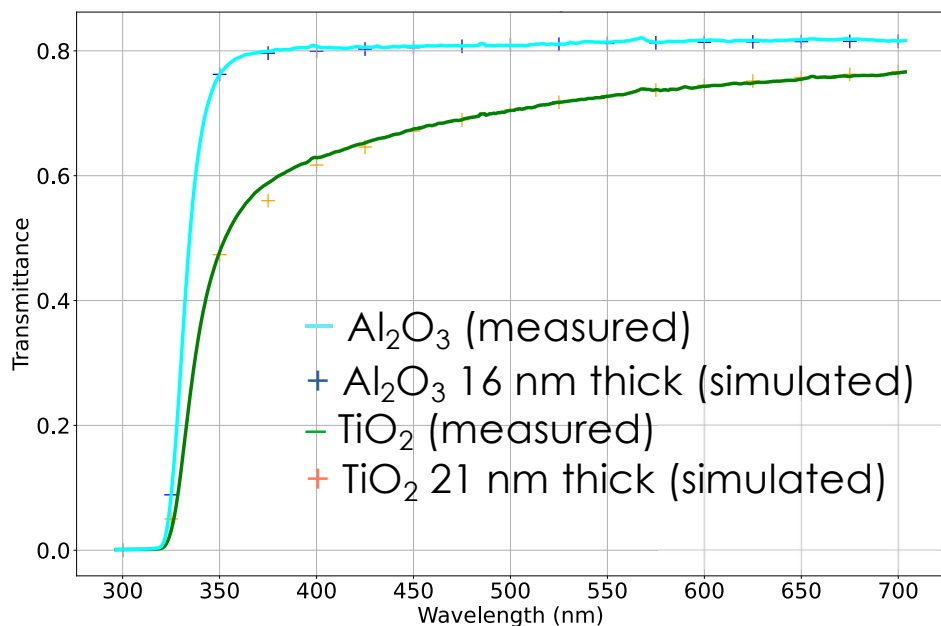
D. Yvon *et al.* JINST 15 (2020) P07029

Modelisation of light transmission through surfaces with thin film optical coating in Geant4

L. Cappellugola *et al.* in Conf. Rec. IEEE NSS/MIC'2021
C.-H. Sung, L. Cappellugola *et al.* accept. in NIMA 2023

Update of the optical light transport of Geant4 version 11.1 to model optical coating

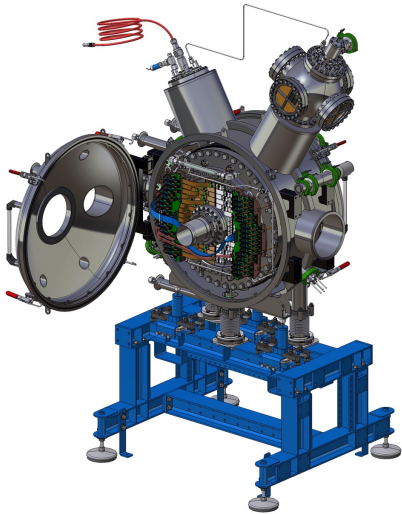
L. Cappellugola *et al.* Technical Forum Geant4, 2022



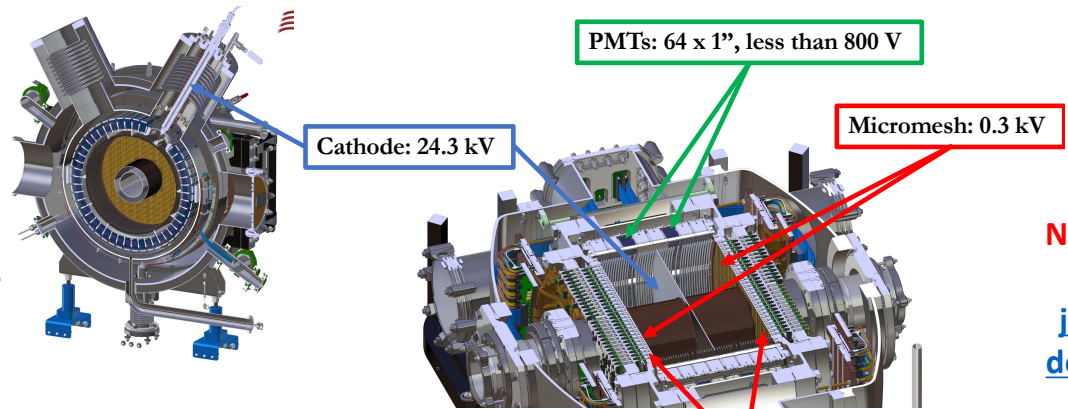
3 γ PET: XEMIS2 (Xenon Medical Imaging Systems)



XEMIS prototypes are made of single phase LXe TPC 



Charge and light generated by LXe γ interactions
Very Large acceptance for small animal : 24 cm axial FOV
Thickness : 12 cm LXe in radius
Very precise : 0.1 mm 3D resolution on Compton interactions



Around 10 FTE/year since 5 years in Subatech Tech teams and Xénon group

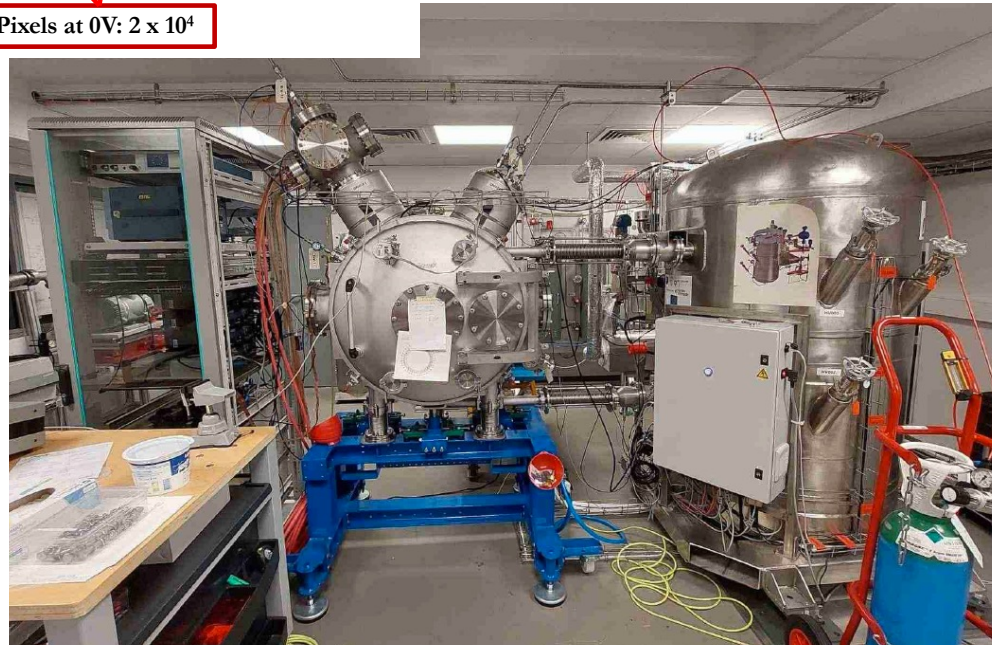
New In2p3 colleagues very welcome
Contacts :
jean-luc.beney@subatech.in2p3.fr
dominique.thers@subatech.in2p3.fr

20000 analogical electronics channels for charge read-out
Working conditions : LXe@-100 °C, P@1,2 bars, LXe density : 3

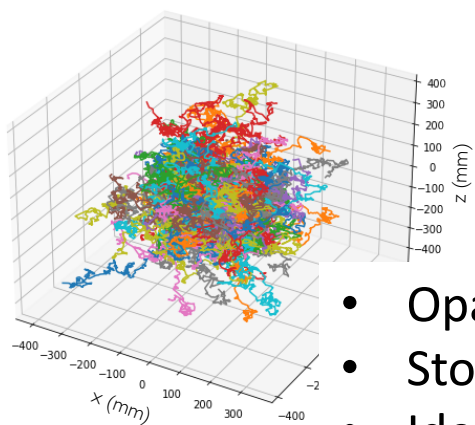
First LXe Compton Telescope designed for small animal Medical Imaging

Installed at "Nantes Centre" CHU in the CIMA Building

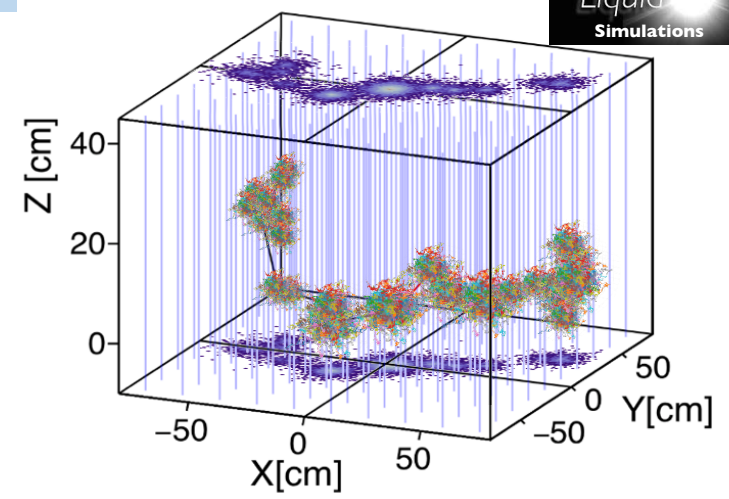
XEMIS2 construction scheduled : closing this year



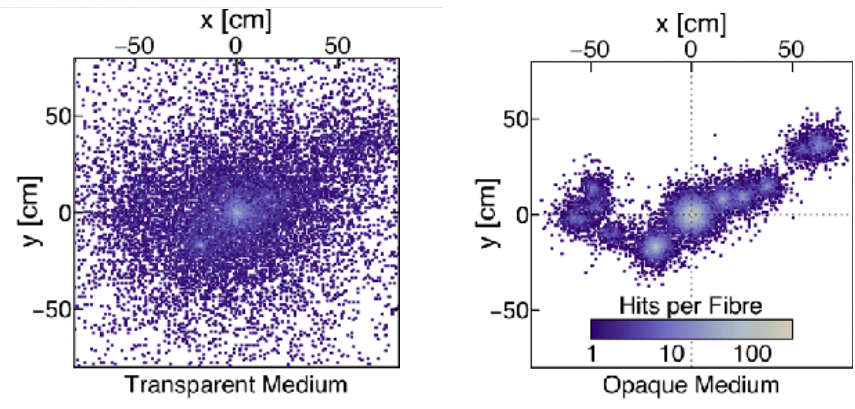
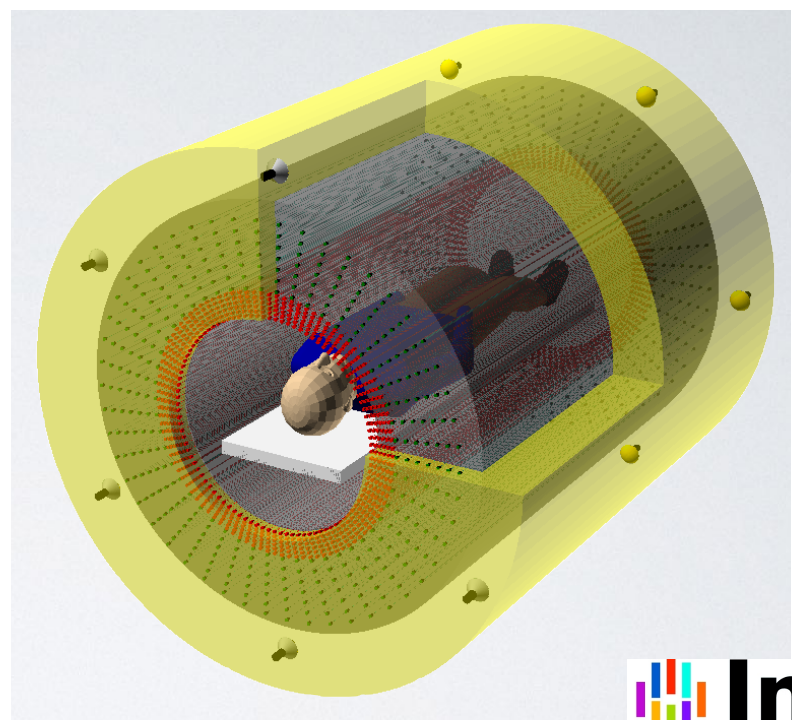
Whole Body PET with LiquidO



- Opaque scintillator
- Stochastic light confinement
- Identify each γ interaction point



Goal



LPET-OTech Consortium

M. Bongrand^d, C. Bourgeois^{aa}, D. Brasse^{*b}, D. Breton^{aa}, M. Briere^{aa}, A. Cabrera^{†aa}, V. Chaumat^{aa}, A. Dahmane^b, R. Gazzini^{aa}, D. Giovagnoli^b, F. Haddad^d, A. Hourlier^b, G. Hull^{aa}, P. Lanièce^{ab}, F. Lefevre^d, P. Loaiza^{aa}, J. Maalmi^{aa}, Y. Mellak^c, T. Merlin^c, R. Mastrippolito^{ab}, C. Marquet^{‡aa}, L. Ménard^{ab}, D. Navas-Nicolás^{aa}, P. Pillot^d, L. Simard^{aa}, D. Stocco^d, M.-A. Verdier^{ab}, D. Visvikis^c, and F. Yermia^d



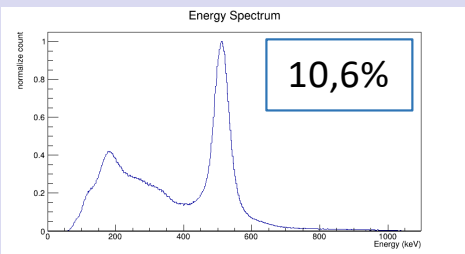
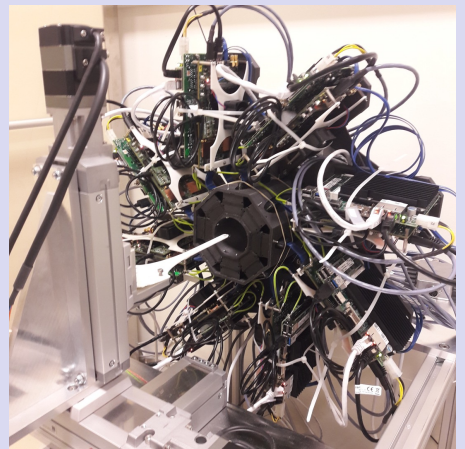
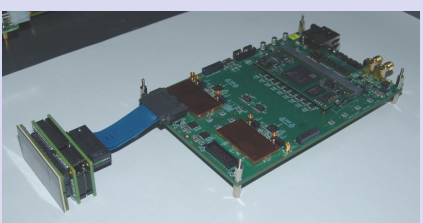


Imagerie TEP/CT

Projet région/BPI
Collab. Inviscan, Streb&Weil
Labelisé pôle Biovalley

Module de détection (25x50mm²):
23x96 LYSO:Ce, 0.98x0.98x8mm³
32 voies électroniques

Système:
2 anneaux de 8 modules chacun



Base commune de développement

Matrice SiPM de type S13361-3050
ASIC Imotep2
Système de mesure multivoies (charge & temps)
Multiplexage par réseau de résistances
Virtex 5 / Gbit Ethernet

D Brasse (david.brasse@iphc.cnrs.fr)
V Bekaert, F Boisson, N Chevillon, C Fuchs,
X Fang, J Sahr,
R Sefri

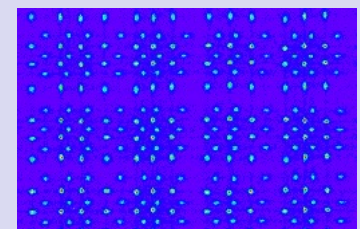
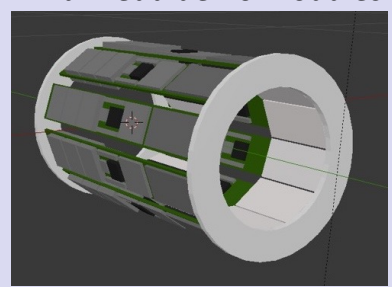
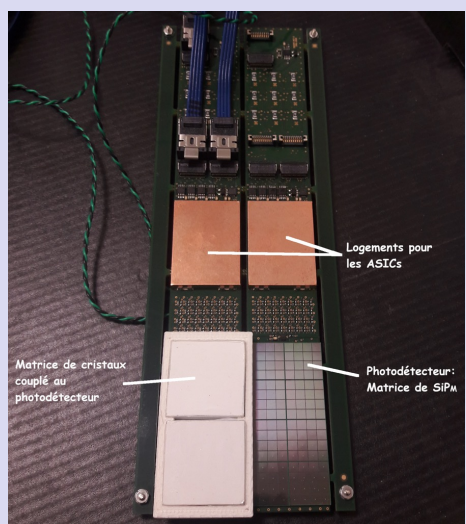
Imagerie TEP/IRM

Projet CPER I2MT
Collab. Laboratoire Icube

Contraintes:
compacité & champ magnétique

Module de détection (25x50mm²):
Double couche
33x68 LYSO:Ce, 0.66x.66x4mm³
32 voies électroniques

Système:
1 anneau de 10 modules



Base commune de développement

PMT H9500 256 voies

ASIC Imotep1

Système de mesure multivoies (charge & temps)

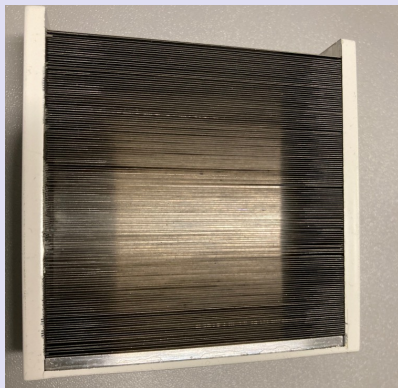
Virtex 5 / Gbit Ethernet

F Boisson (frederic.boisson@iphc.cnrs.fr)

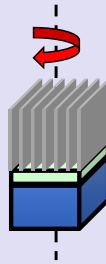
V Bekaert, D Brasse, N Chevillon,

C Fuchs, X Fang, J Sahr, R Sefri

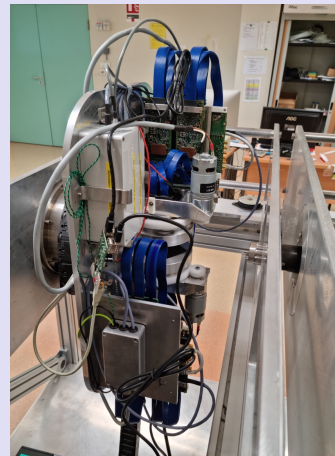
De trous à lames parallèles



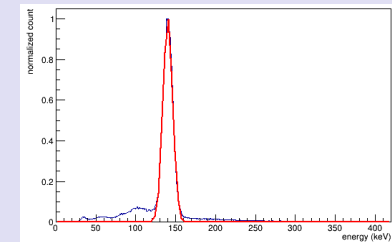
Amélioration de l'efficacité
de 0,02 to 1%



Spin-rotation



1D -> 2D : nécessité
de reconstruction dédiée



Efficacité : 0,6 % (@25mm)

R_E : 10,3 % (@140 keV)

FOV: 50x50 mm²

Vers l'information 3D

Etude des performances intrinsèques : 2 cristaux CeBr₃ (avec réflecteur ou revêtement noir)

Utilisation de réseau de CNN pour la correction de linéarité

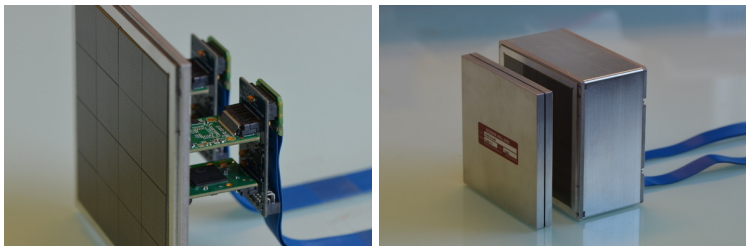
Mise en place d'algorithmes et de protocoles dédiés aux acquisitions et reconstructions 3D

OBJECTIFS

- THIDOS : proposer de nouvelles approches instrumentales (caméra ambulatoire) et méthodologiques (analyse des incertitudes liées au calcul de la dose, système expert) visant à renforcer le contrôle de la dose délivrée lors du traitement à l'iode radioactif des maladies thyroïdiennes

MATERIELS & METHODES

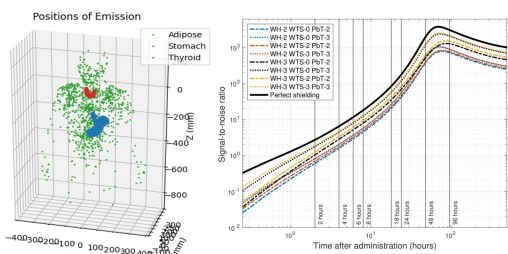
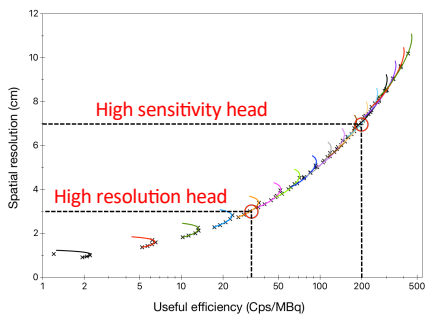
Optimisation de l'ensemble scintillateur/photodétecteur



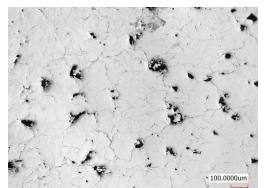
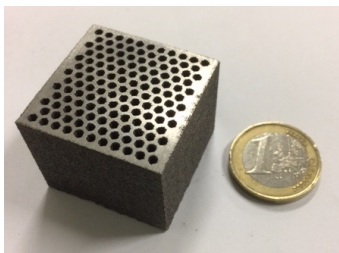
Matrice de SiPMs et électronique miniaturisée (PETSys Electronics) - Scintillateur monolithique CeBr3 - Méthodes de reconstruction avancées

Optimisation du collimateur haute-énergie et du blindage

Simulation Monte-Carlo (GATE)



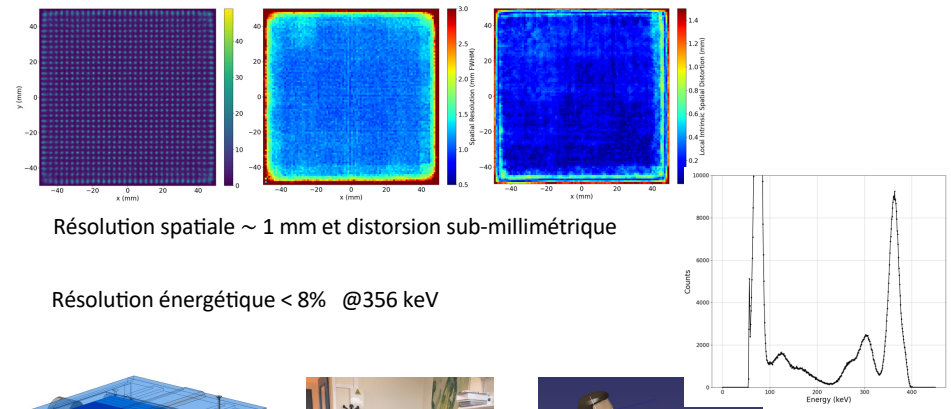
Etude des paramètres d'impression 3D tungstène par fusion laser sélective (collaboration UTBM, ICB, Belfort)



RESULTATS

- Développement du prototype clinique de la caméra ambulatoire (10x10 cm²)
- Conception et validation d'un réseau Bayésien pour l'estimation de l'incertitude sur la dose absorbée (IRSN)

Reconstruction par réseau de neurones convolutif profond



Résolution spatiale ~ 1 mm et distorsion sub-millimétrique

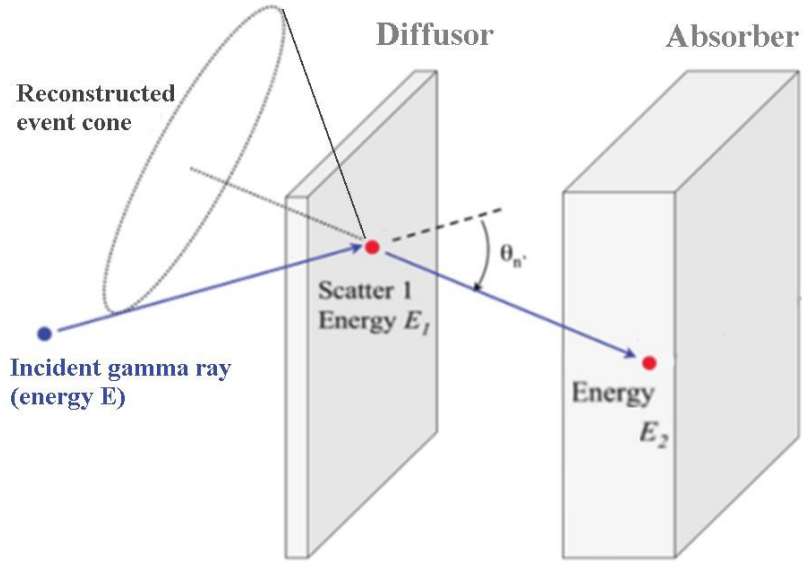
Résolution énergétique < 8% @356 keV



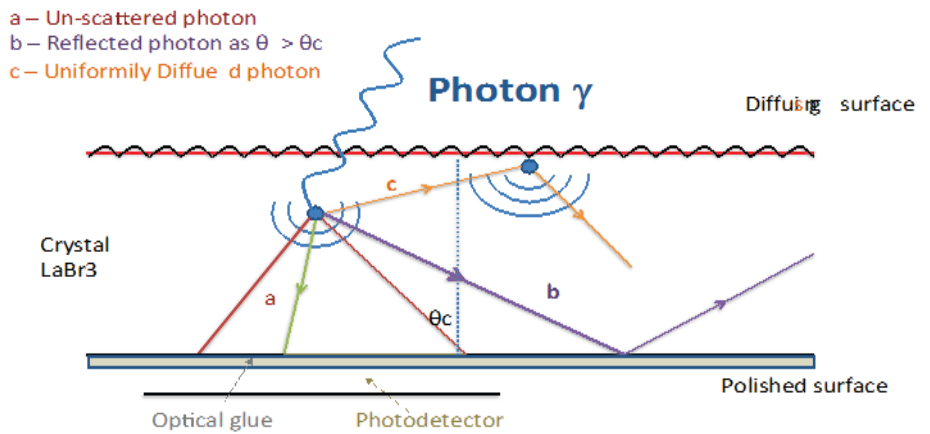
Support financier

Plan Cancer (AAP Physicancer, INSERM, 296 k€, 2019-2022) et AP-IN2P3

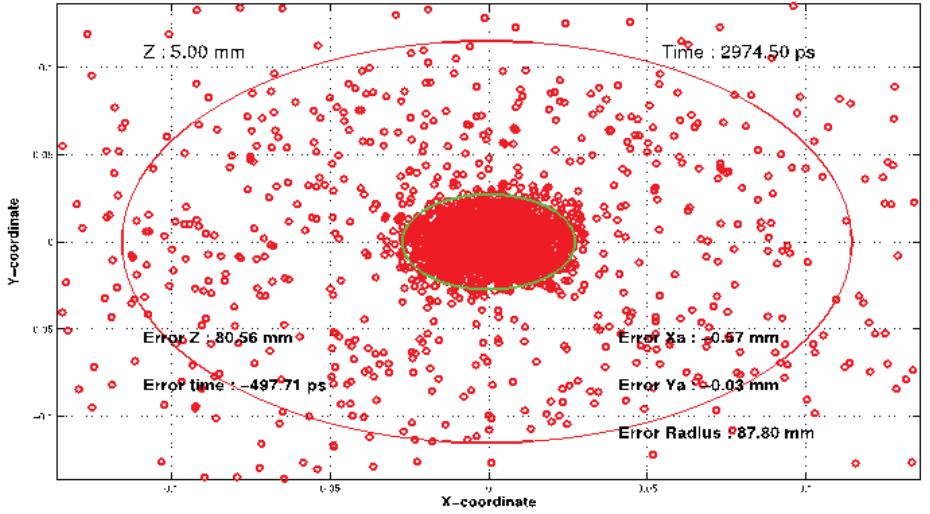
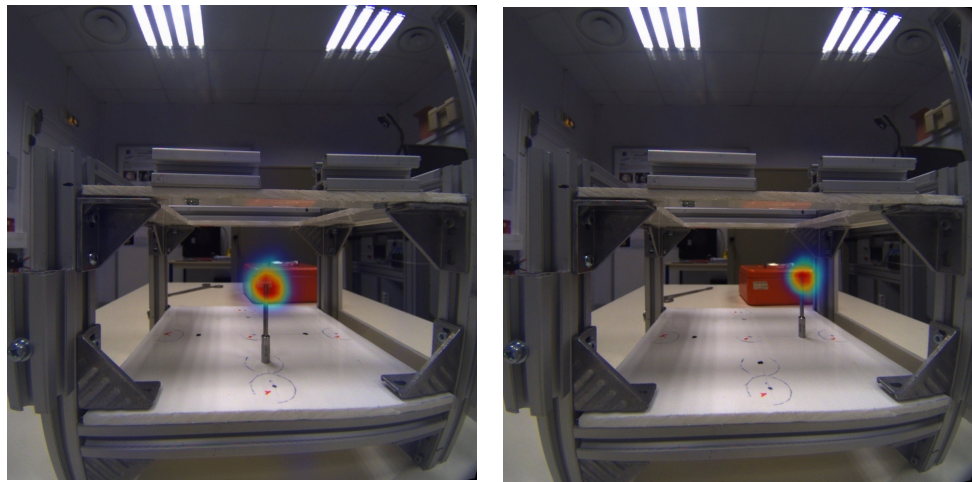
Detectors: monolithic LaBr_3 detectors readout by digital SiPM matrices (Philips)



Depth of Interaction

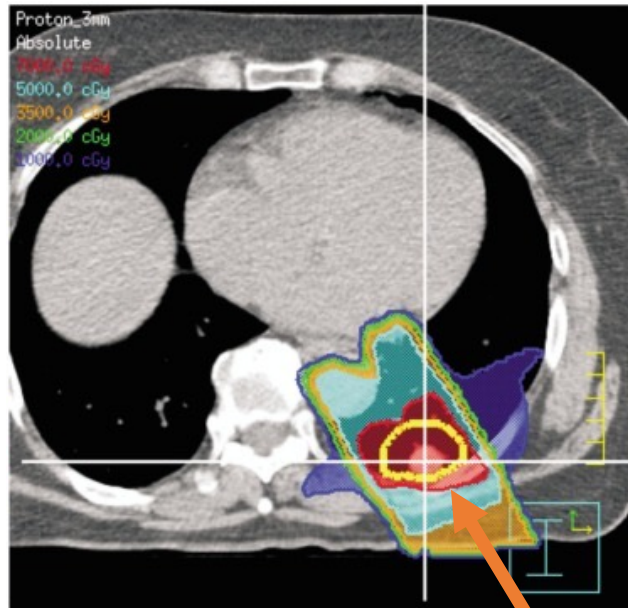


Detection of a Germanium source

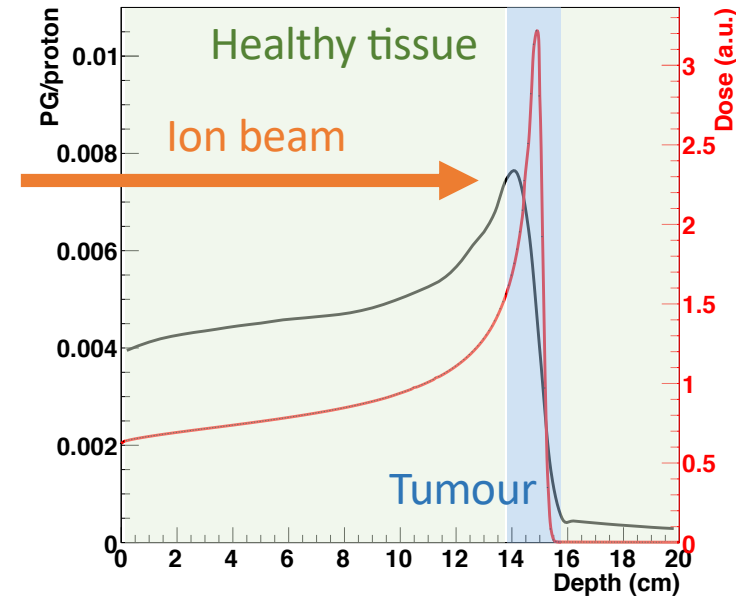


A. Iltis and H. Snoussi. J. Imaging 1 (2015) 45-59

PG Imaging for Proton therapy monitoring



Ion beam



Many source of errors (patient's positioning, anatomical changes...) impose the use of safety margins

=> Reduced treatment efficacy

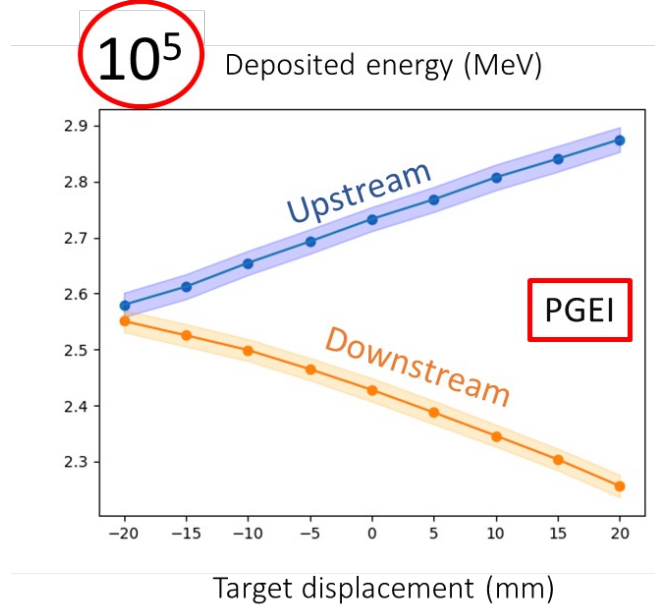
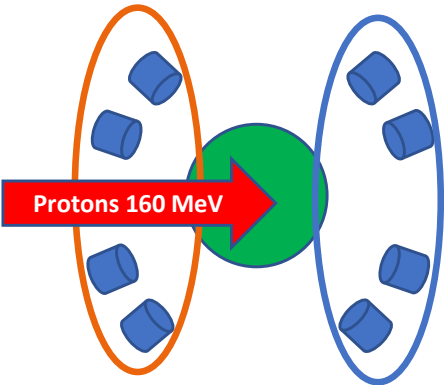
Prompt Gamma Energy Integral (PGEI)

- Detection of many simultaneous photons by large scintillators
- Integral of detected energy: PGEI method
- Fast scintillators : PbWO_4 , to keep linear response at high energy deposit



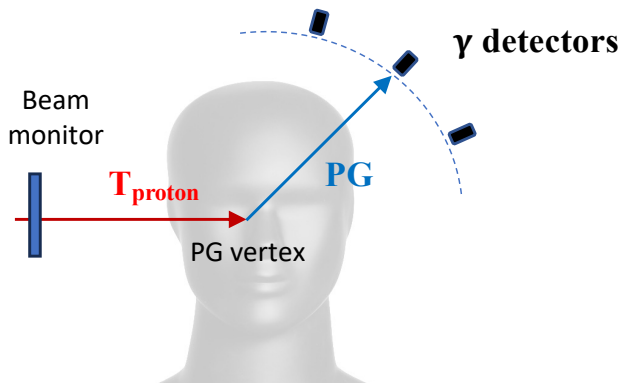
GATE simulation

- Spot of 1.5×10^7 protons
- 5 cm radius LaBr3 detectors



Experiment

(68 MeV pulsed alpha beam, 2 μA)



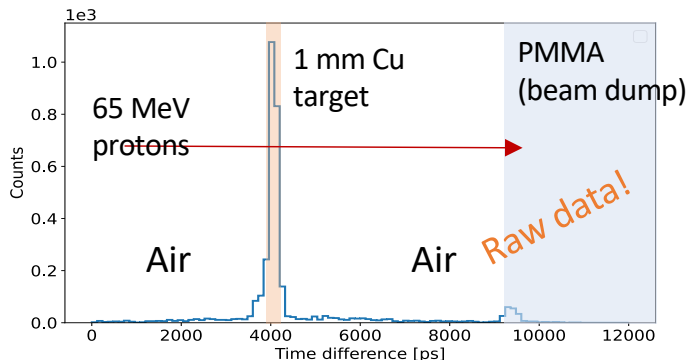
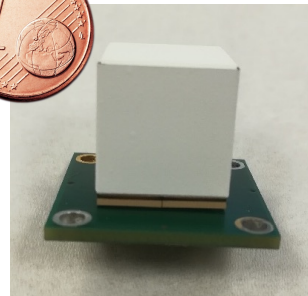
GOAL

- 30 γ detectors to achieve a uniform target coverage
- Detection efficiency $\sim 0.5\%$
- Targeted coincidence time resolution ~ 100 ps RMS
- Dedicated reconstruction for PG vertex

$$TOF = T_{proton}(r_v) + \frac{1}{c} \|r_d - r_v\|$$

TIARA γ module (Cherenkov)

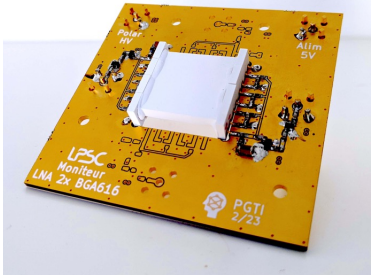
(1.5 cm)³ PbF₂ coupled to SiPMs



Prototype v.4: Time resolution ~ 100 ps RMS

Beam monitor

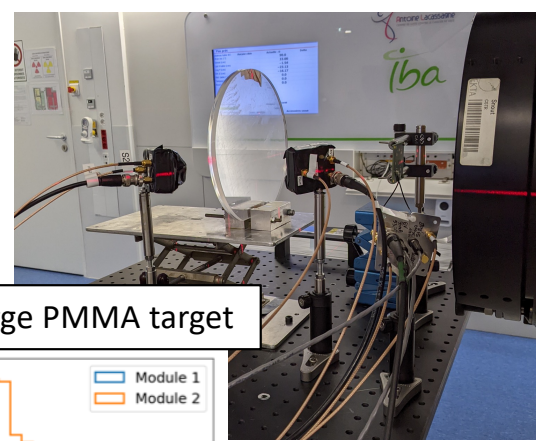
$\sim 4\text{cm}^2$ plastic scintillator readout by SiPMs



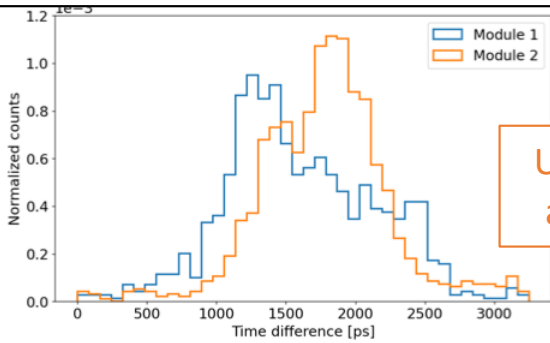
Prototype v.0 (test with 148 MeV)
Time resolution = 52 ps RMS
Spatial resolution = 2.5 mm RMS

Experiment on clinical accelerator

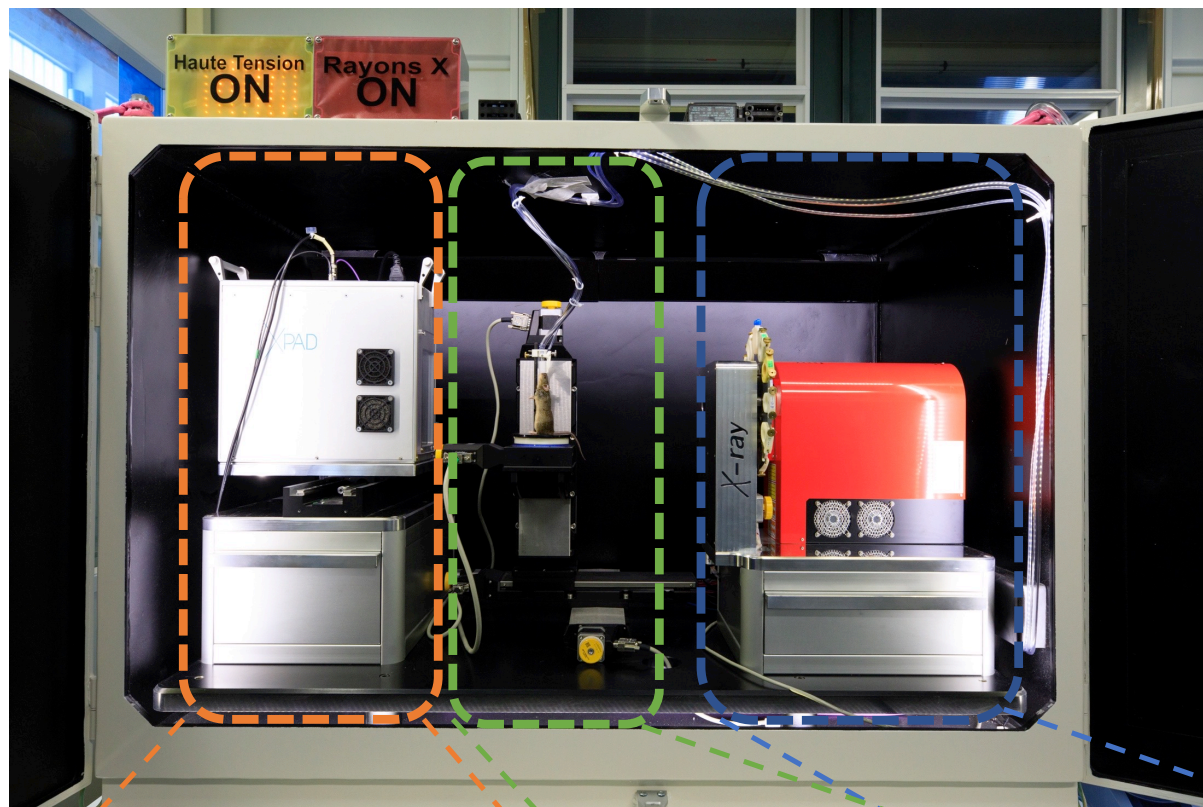
CTR = 112 ps RMS at 148 MeV, SPR



PG TOF profile from large PMMA target



Uniform sensitivity all over the range

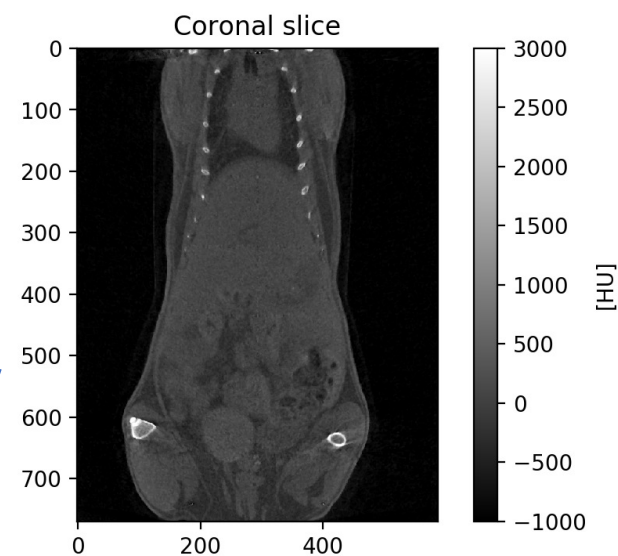


F. Cassol *et al.* BPEX 2 (2016) 025003

- ✓ A. Dawiec (2011) PhD
- ✓ H. Ouamara (2013) PhD
- ✓ M. Dupont (2014) PhD
- ✓ C. Kronland-Martinet (2015) PhD
- ✓ M. Hamonet (2016) PhD
- ✓ F. Cassol (2018) HDR

F. Cassol *et al.* iScience 21 (2019) 68-83

- ✓ L. Portal (2018) PhD



Detector (imXPAD)

- 500,000 XPAD3/Si hybrid pixels $130 \times 130 \mu\text{m}^2$
- 500 μm thick

Animal support

- 3-axis motion + rotation
- Minerva gas anesthesia system

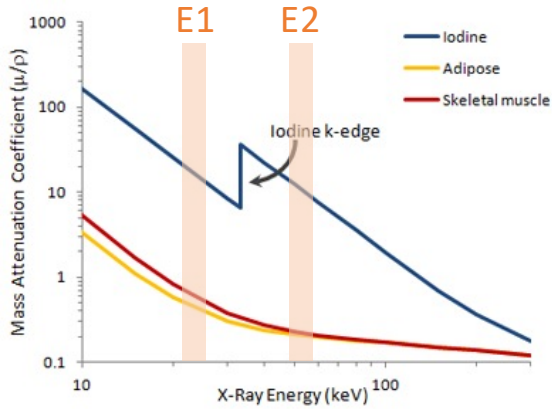
X-ray tube (Hamamatsu)

- 40 to 150 kV
- filter wheel

K-edge X ray imaging

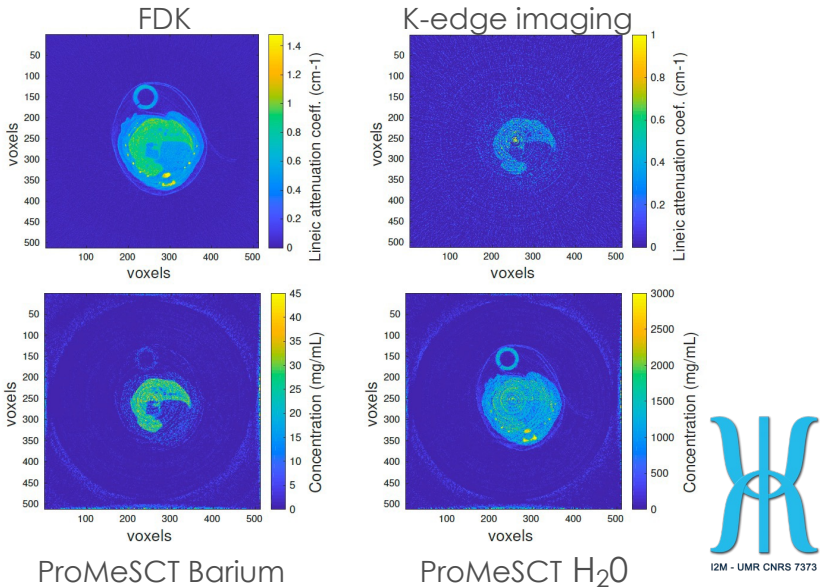
K-edge imaging:

Dual energy acquisition below and above the k-edge



Detector (imXPAD)

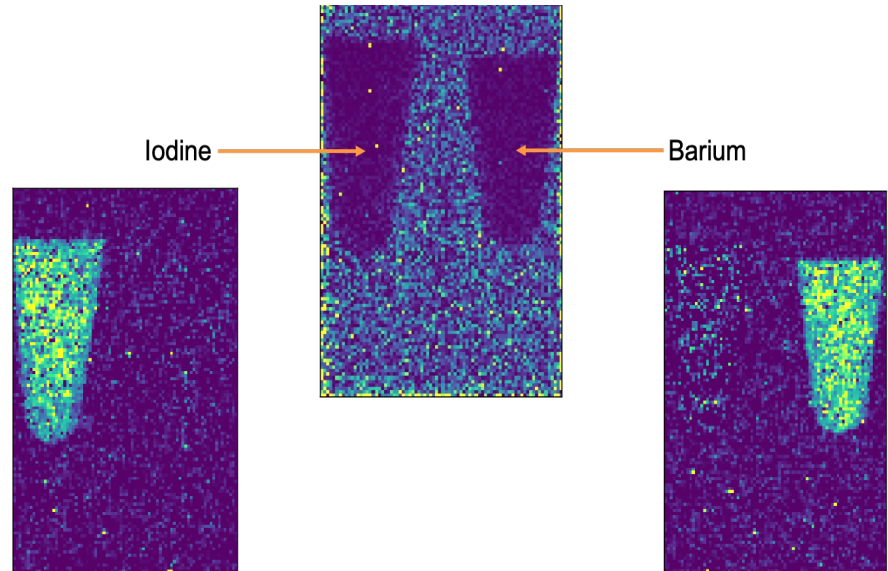
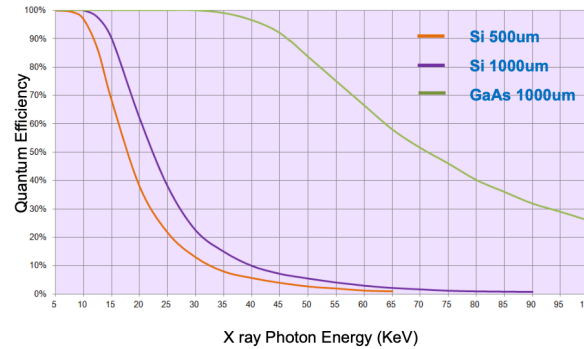
- 70,000 **XPAD3/CdTe** hybrid pixels
- 130 x 130 μm^2 , 700 μm thick
- **ProMeSCT** dedicated reconstruction



S. Tairi et al. IEEE TRPMS 5 (2021) 548-558

Detector (Cegitek <- imXPAD)

- 9600 **XPAD3/GaAs** hybrid pixels
- 130 x 130 μm^2
- 1000 μm thick



Questions ?