

Towards Total-Body J-PET

with  **GATE** simulations :-)
opengatecollaboration.org

Wojciech Krzemień
On behalf of the J-PET collaboration

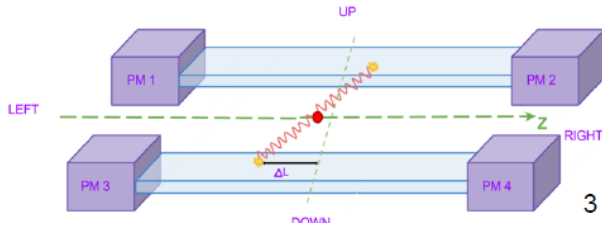
Jagiellonian Positron Emission Tomography



Cost-effective total body solution



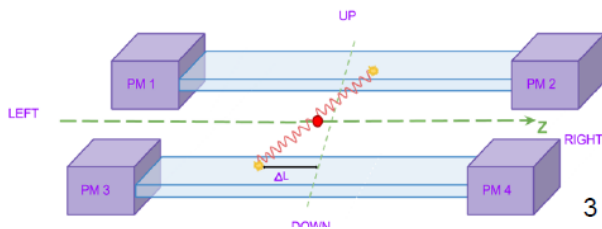
$$\Delta l = \frac{(t_2 - t_1) \cdot v}{2} \cong \frac{(t_2 - t_1) \cdot c}{4}$$



$$\Delta x = \frac{(t_l - t_r) \cdot c}{2} \implies \Delta x = \frac{\Delta t}{2} \cdot c$$

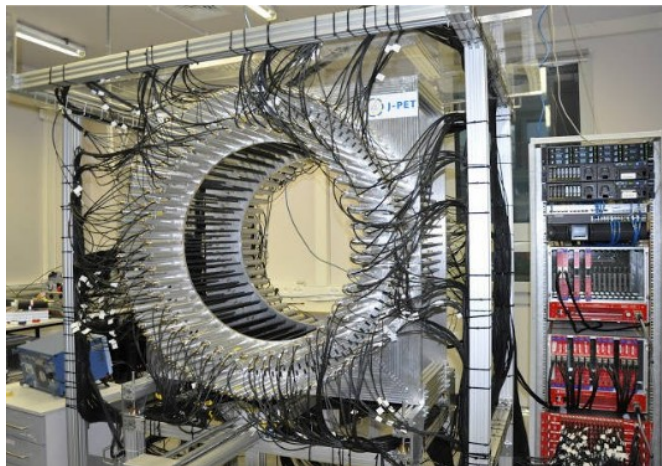
Cost-effective total body solution

$$\Delta l = \frac{(t_2 - t_1) \cdot v}{2} \cong \frac{(t_2 - t_1) \cdot c}{4}$$



$$\Delta x = \frac{(t_l - t_r) \cdot c}{2} \implies \Delta x = \frac{\Delta t}{2} \cdot c$$

First prototype

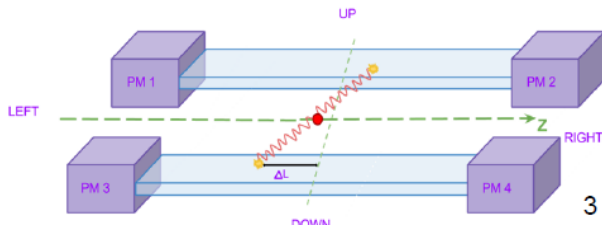


Acta Phys Pol. B 48 (2017) 1567

- 50 cm AFOV
- 192 plastic strips
- Readout → vacuum tube photomultipliers

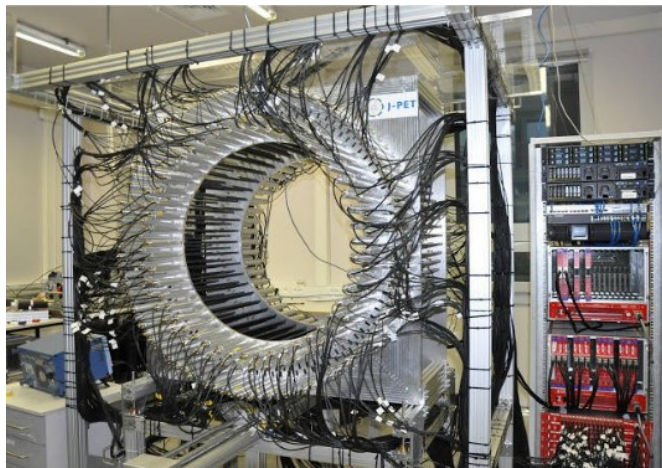
Cost-effective total body solution

$$\Delta l = \frac{(t_2 - t_1) \cdot v}{2} \cong \frac{(t_2 - t_1) \cdot c}{4}$$



$$\Delta x = \frac{(t_l - t_r) \cdot c}{2} \implies \Delta x = \frac{\Delta t}{2} \cdot c$$

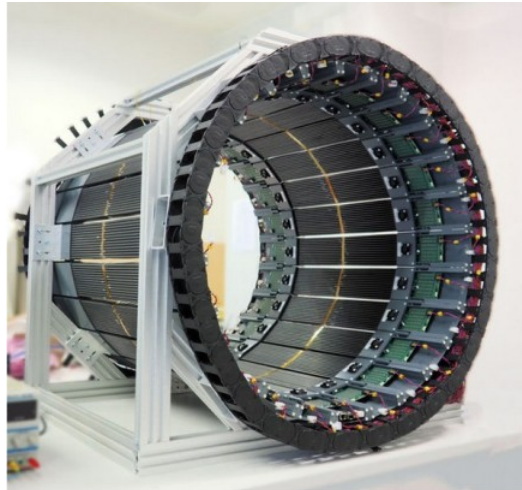
First prototype



Acta Phys Pol. B 48 (2017) 1567

- 50 cm AFOV
- 192 plastic strips
- Readout → vacuum tube photomultipliers

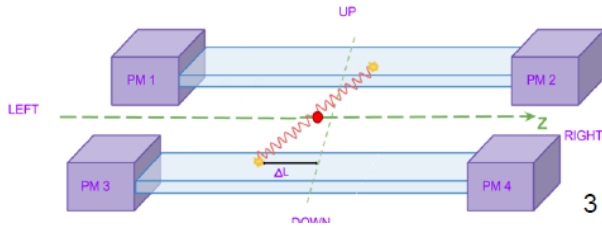
Modular J-PET



- 50 cm AFOV
- 24 modules x 13 strips
- Readout → silicon photomultipliers matrices

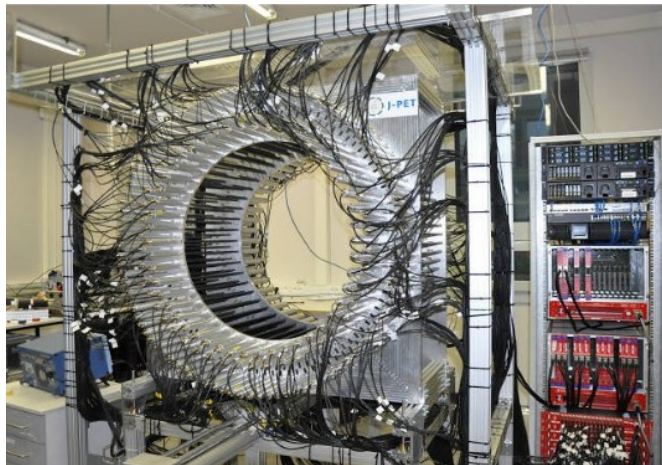
Cost-effective total body solution

$$\Delta l = \frac{(t_2 - t_1) \cdot v}{2} \cong \frac{(t_2 - t_1) \cdot c}{4}$$



$$\Delta x = \frac{(t_l - t_r) \cdot c}{2} \implies \Delta x = \frac{\Delta t}{2} \cdot c$$

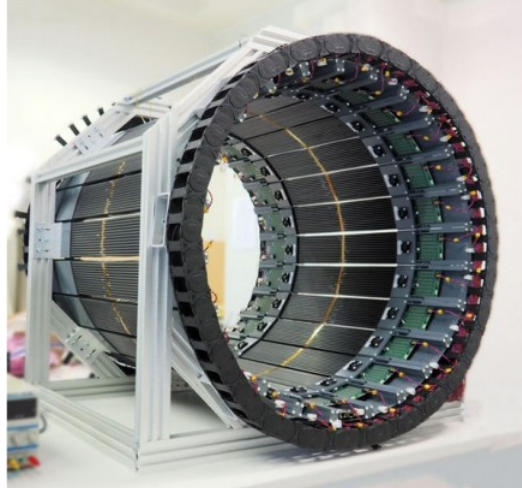
First prototype



Acta Phys Pol. B 48 (2017) 1567

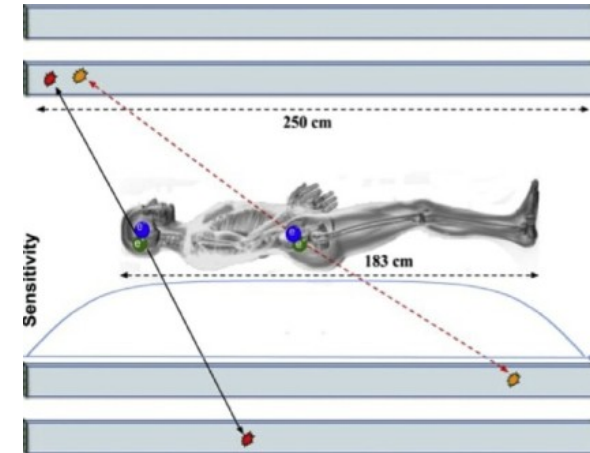
- 50 cm AFOV
- 192 plastic strips
- Readout → vacuum tube photomultipliers

Modular J-PET



- 50 cm AFOV
- 24 modules x 13 strips
- Readout → silicon photomultipliers matrices

Total-body

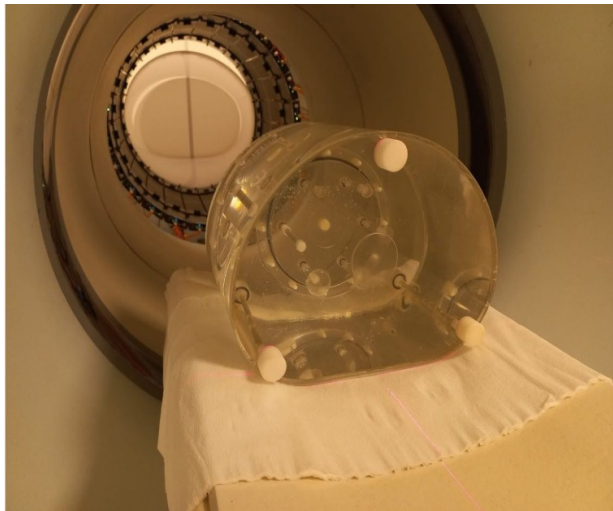
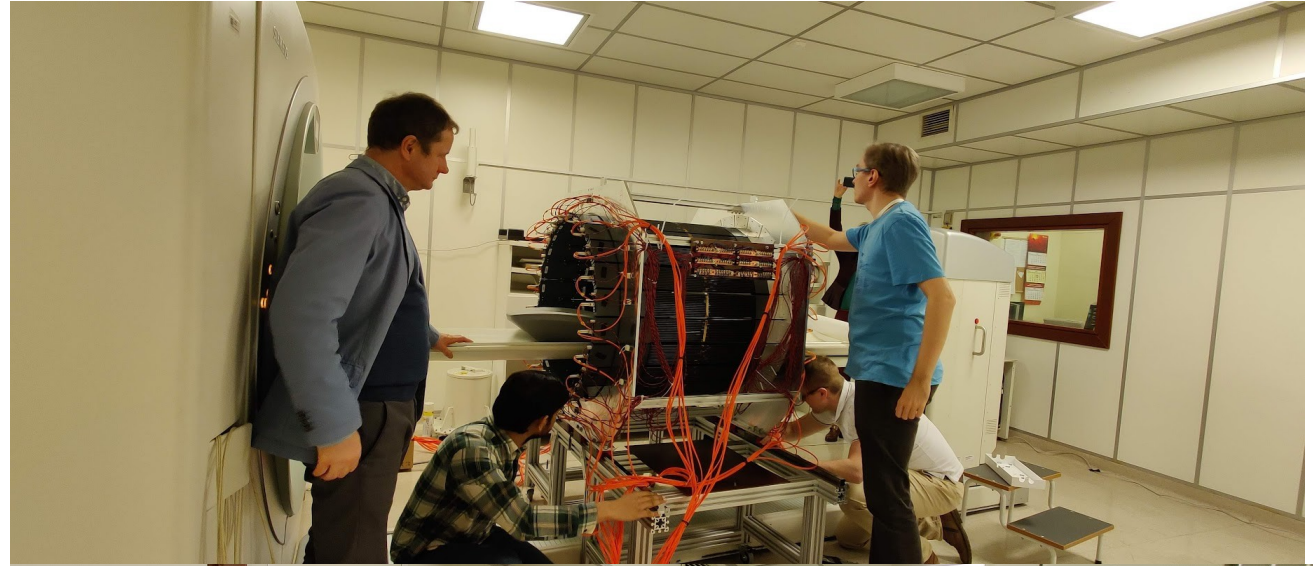
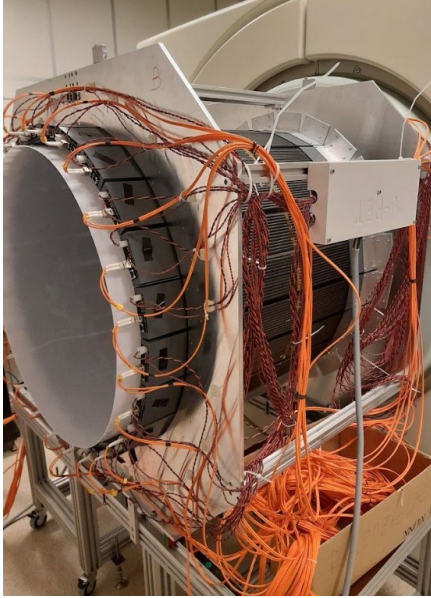


PET Clinics 15 (2020) 439
Phys. Med. Biol. 66 (2021) 175015

- 250 cm AFOV
- Additional layers of wavelength shifters → better axial resolution

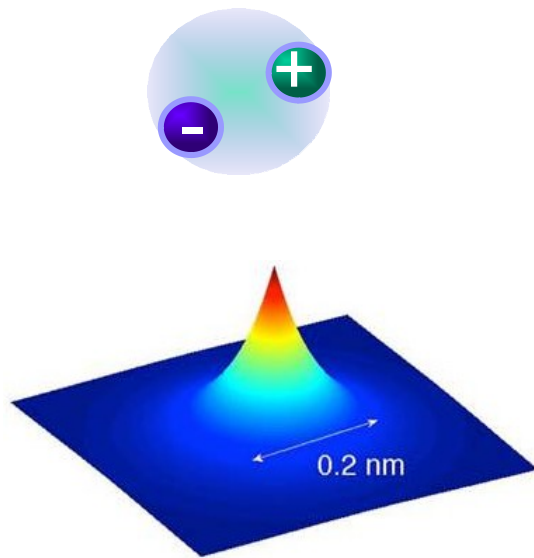


First test measurements with patients @Medical University of Warsaw

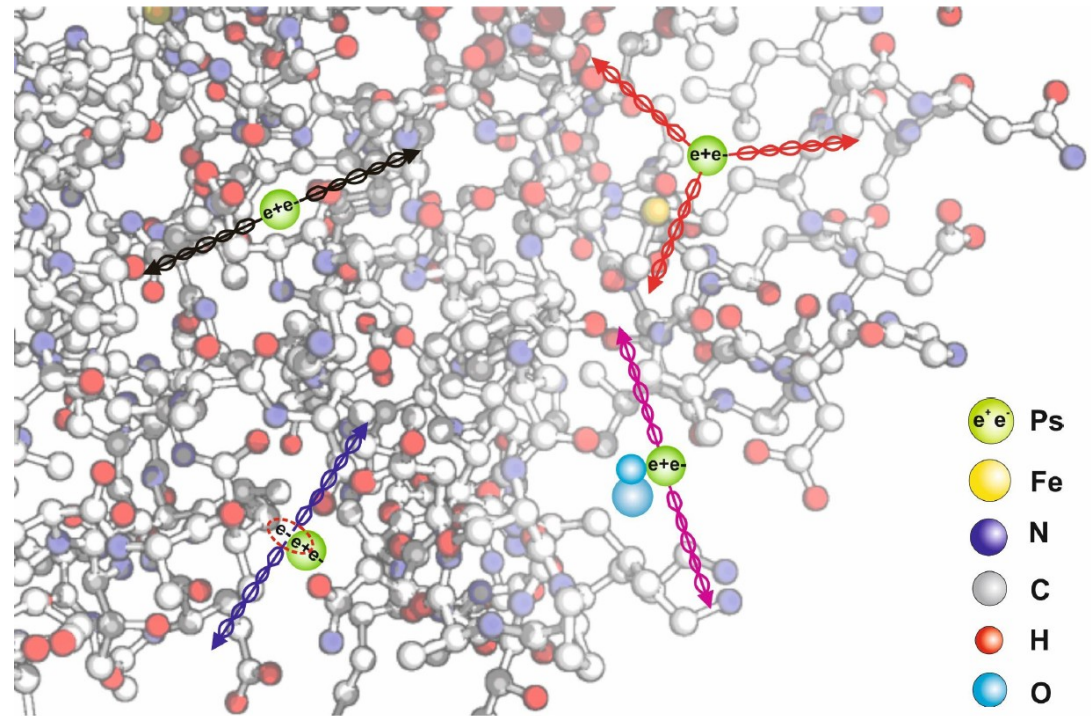


- ^{68}Ga and FDG – phantoms and patients
- Scandium 44 – phantoms
- data also taken with Biograph Truepoint PET-CT

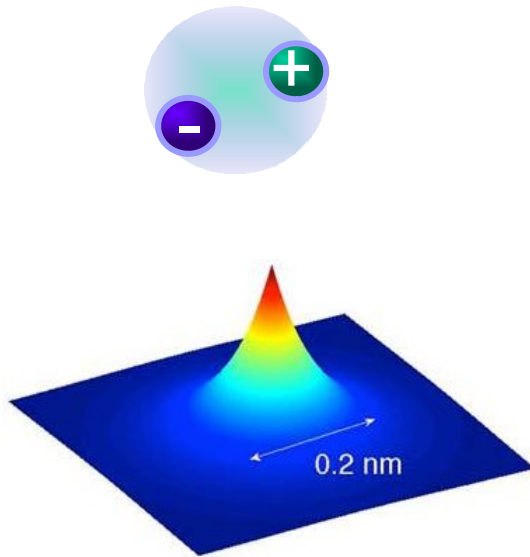
Multi-photon imaging



Model of the hemoglobin molecule



Positronium in PET



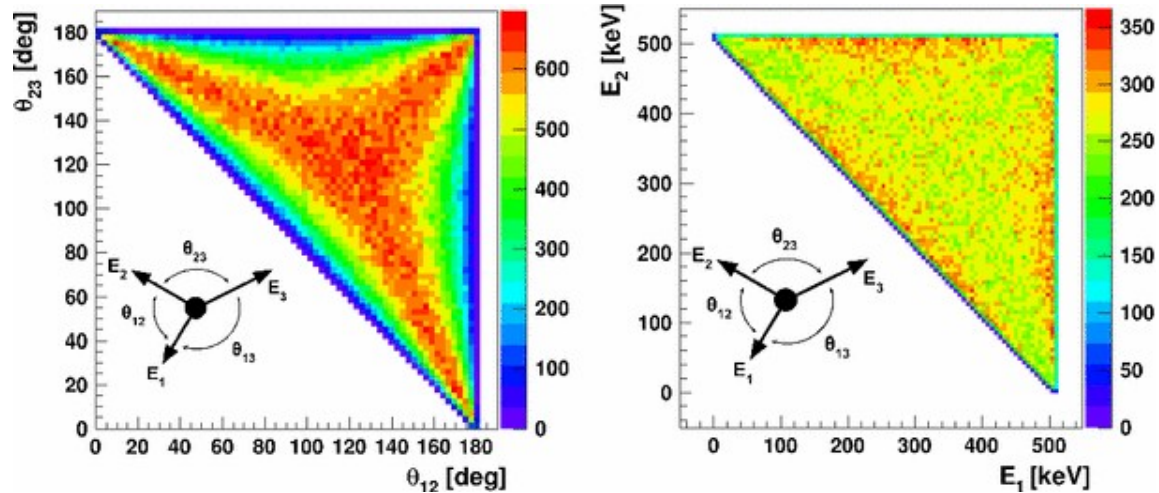
Para-positronium:

- lifetime ~125 ps
- two-photon decay

Ortho-positronium:

- lifetime ~142 ns
- three-photon decay

Daria Kisielewska



Implementation of QED-compliant description of ortho-positronium decay

- 1) P. Moskal et al., *Phys. Med. Biol.* 64 (2019) 055017
- 2) P. Moskal et al. *Eur. Phys. J. C* 78 (2018) 970
- 3) D. Kaminska et al., *Eur. Phys. J. C* (2016) 76:445

Source Extensions in GATE

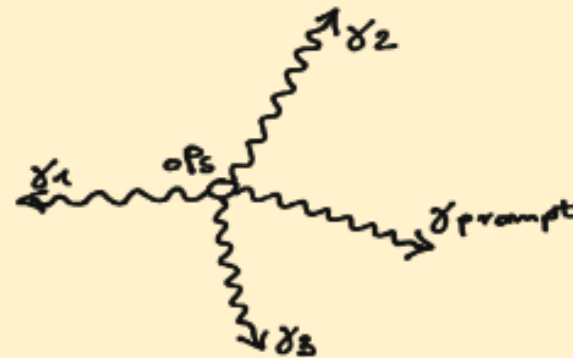
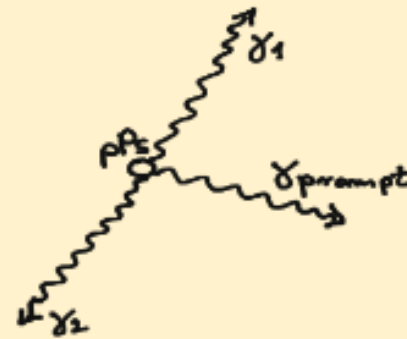
GateExtendedVSource

- Positronium decays (pPs, oPs, mixed)
- Polarization supported
- Configurable decay properties:
 - prompt gamma emission
 - prompt gamma energy
 - positronium life time
 - fraction of pPs and oPs decays

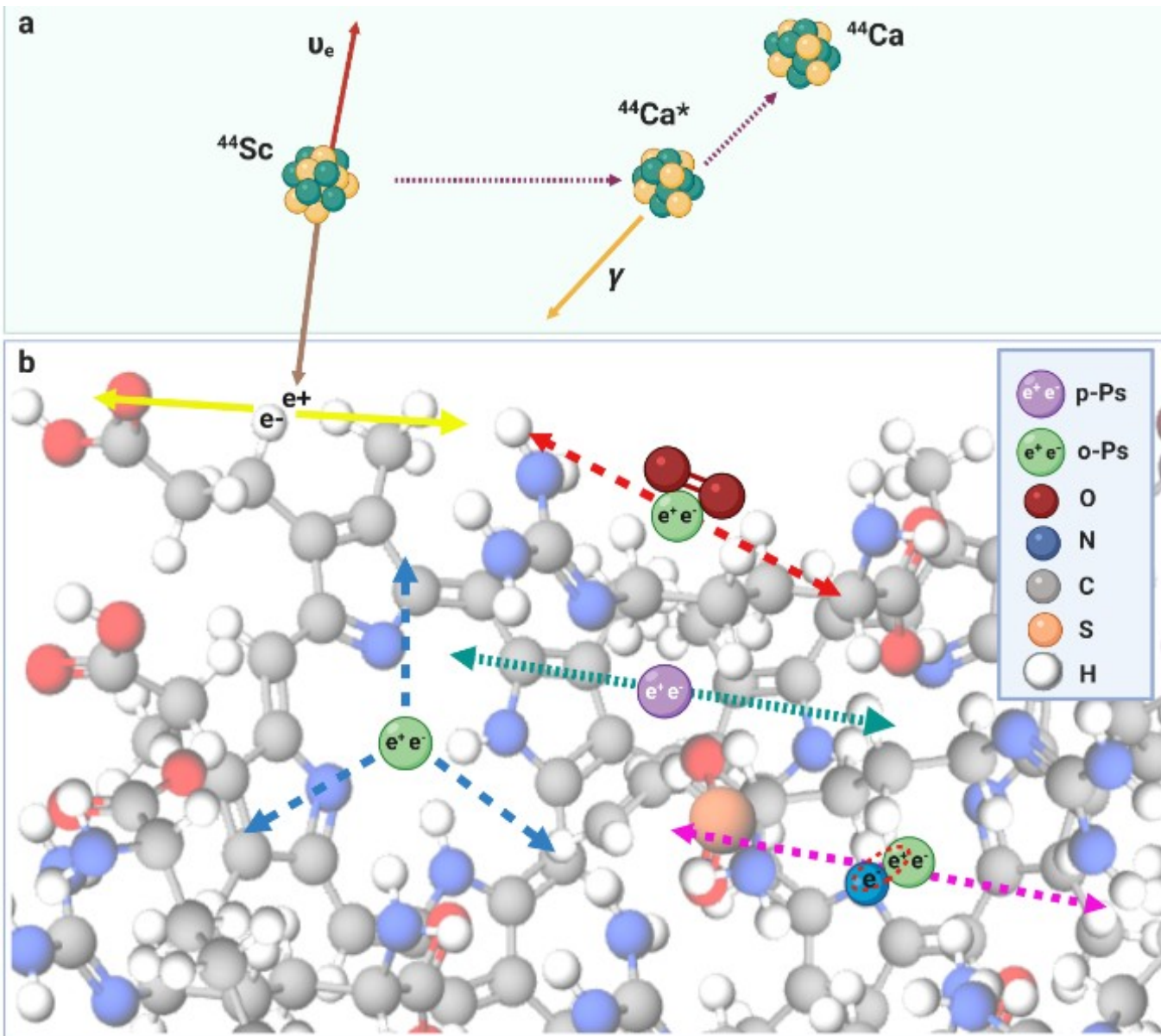
GateVSource

Inherited Gate Source class functionality

Positronium decays



available in GATE \geq v9.0



From article in Rev. Mod.Phys. S. Bass, S. Mariuzzi, P. Moskal, E. Stępień

<https://arxiv.org/pdf/2302.09246.pdf>

Accepted Paper

Colloquium: Positronium physics and biomedical applications

Rev. Mod. Phys.

Steven D. Bass, Sebastiano Mariuzzi, Pawel Moskal, and Ewa Stepień

Accepted 16 February 2023

ABSTRACT

ABSTRACT

Positronium is the simplest bound state, built of an electron and a positron. Studies of positronium in vacuum and its decays in medium tell us about Quantum Electrodynamics, QED, and about the structure of matter and biological processes of living organisms at the nanoscale, respectively. Spectroscopic measurements constrain our understanding of QED bound state theory. { Searches for rare decays and measurements of the effect of gravitation on positronium are used to look for new physics phenomena. In biological materials positronium decays} are sensitive to the inter- and intra-molecular structure and to the metabolism of living organisms ranging from single cells to human beings. This leads to new ideas of positronium imaging in medicine using the fact that during positron emission tomography (PET) as much as 40% of positron annihilation occurs through the production of positronium atoms inside the patient's body. A new generation of the high sensitivity and multi-photon total-body PET systems opens perspectives for clinical applications of positronium as a biomarker of tissue pathology and the degree of tissue oxidation.

Simultaneous scans = standard image + lifetime image

Positronium imaging with the novel multiphoton PET scanner

PAWEŁ MOSKAŁ, KAMIL DULSKI, NEHA CHUG, CATALINA CURCEANU, ERYK CZERWIŃSKI, MEYSAM DADGAR, JAN GAJEWSKI, ALEKSANDER GAJOS

GRZEGORZ GRUDZIEN, WOJCIECH WIŚLICKI +27 authors Authors Info & Affiliations

SCIENCE ADVANCES • 13 Oct 2021 • Vol 7, Issue 42 • DOI: 10.1126/sciadv.abh4394

3,485



Abstract

In vivo assessment of cancer and precise location of altered tissues at initial stages of molecular disorders are important diagnostic challenges. Positronium is copiously formed in the free molecular spaces in the patient's body during positron emission tomography (PET). The positronium properties vary according to the size of inter- and intramolecular voids and the concentration of molecules in them such as, e.g., molecular oxygen, O₂; therefore, positronium imaging may provide information about disease progression during the initial stages of molecular alterations. Current PET systems do not allow acquisition of positronium images. This study presents a new method that enables positronium imaging by simultaneous registration of annihilation photons and deexcitation photons from pharmaceuticals labeled with radionuclides. The first positronium imaging of a phantom built from cardiac myxoma and adipose tissue is demonstrated. It is anticipated that

Kamil Dulski

CURRENT ISSUE



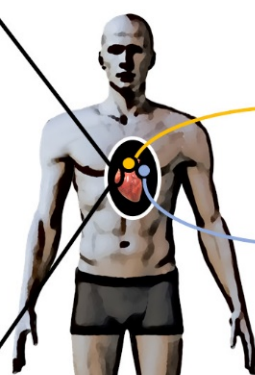
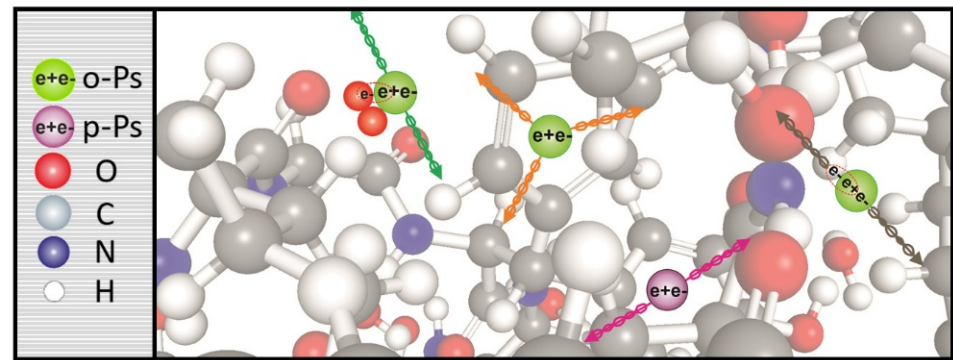
Control of lysosomal-mediated cell death by the pH-dependent calcium channel RECS1

BY PHILIPPE PIHAN, FERNANDA LISBONA, ET AL.

Epitope-preserving magnified analysis of proteome (eMAP)

BY JOHA PARK, SARIM KHAN, ET AL.

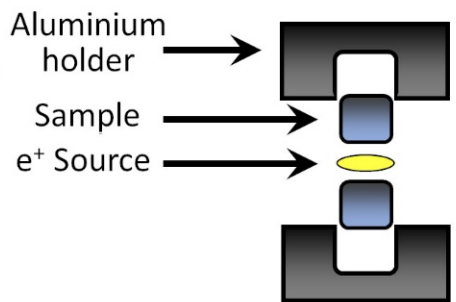
Speckle-free holography with partially coherent light



Adipose tissue
 Cardiac Myxoma

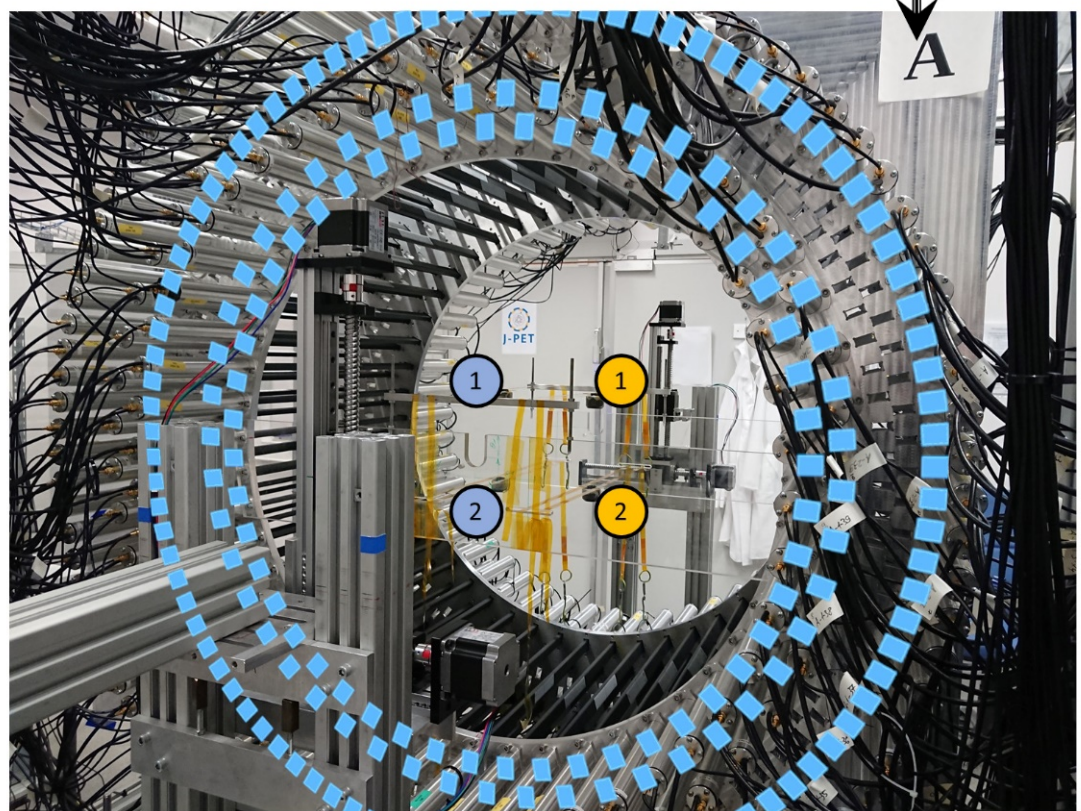
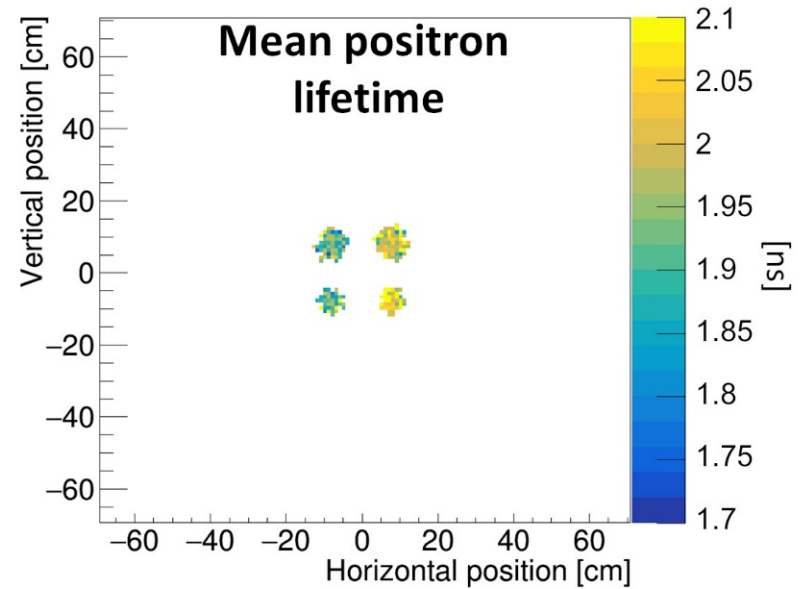
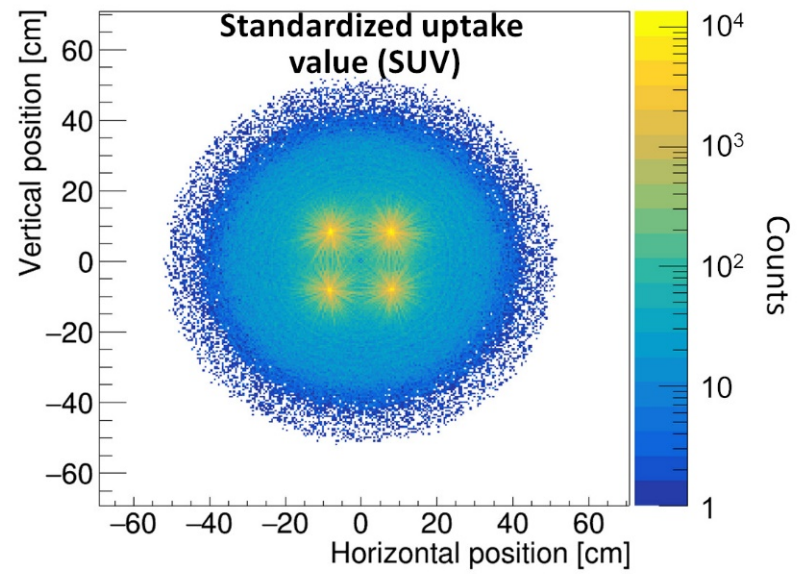


Sample preparation		
Patient 1	1	1
Patient 2	2	2

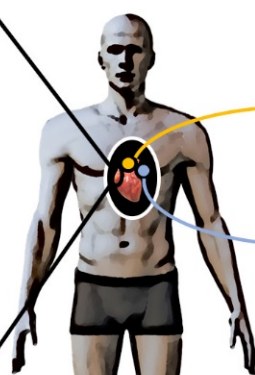
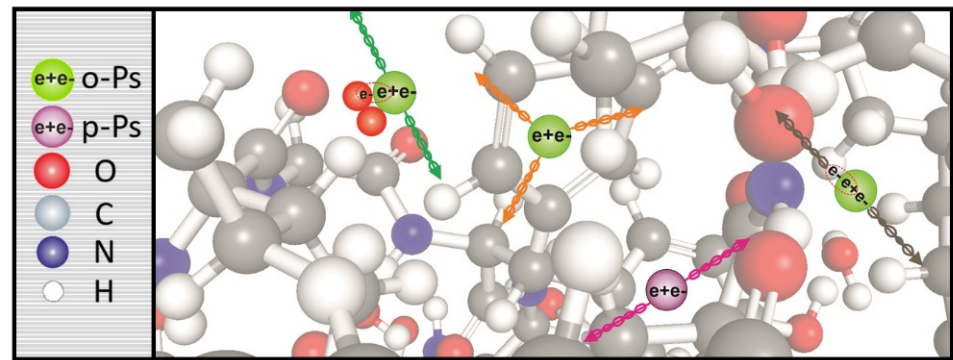


Placing samples in the chambers

Inserting setup to the detector



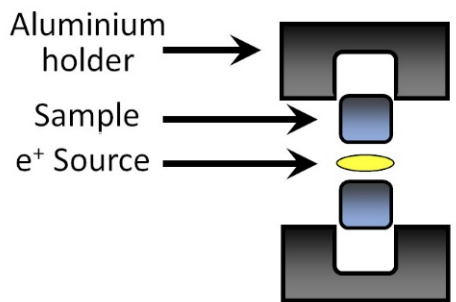
Kamil Dulski



Adipose tissue
Cardiac Myxoma

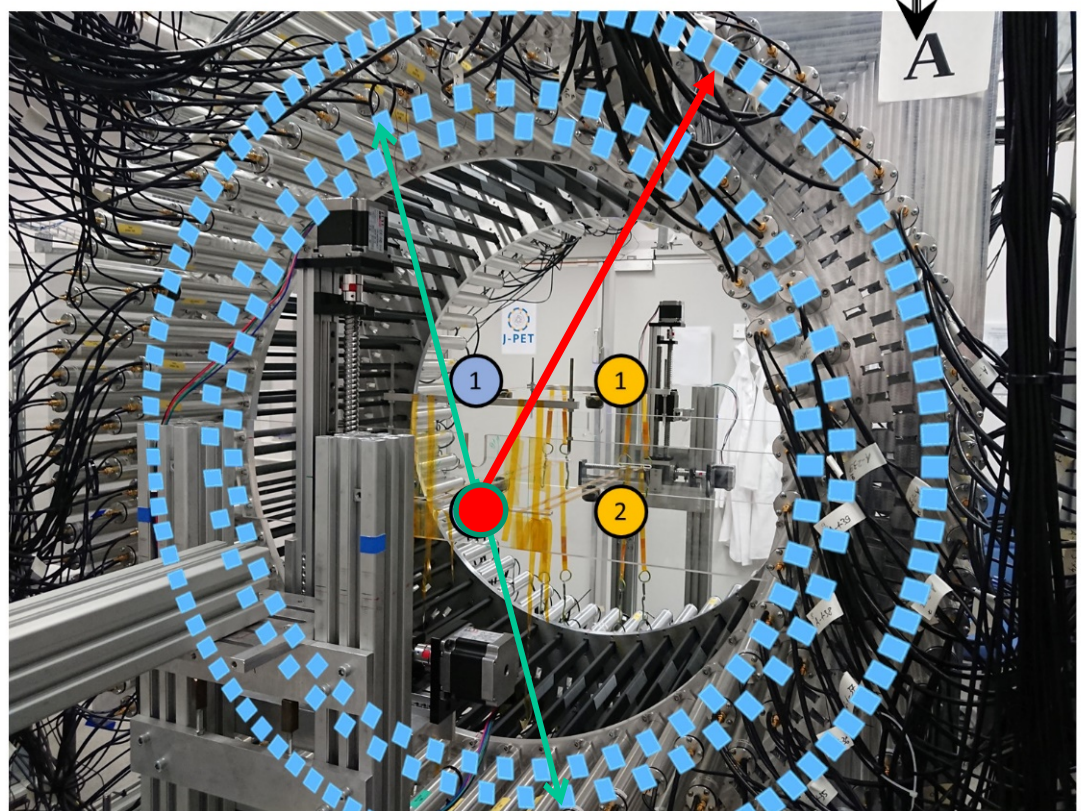
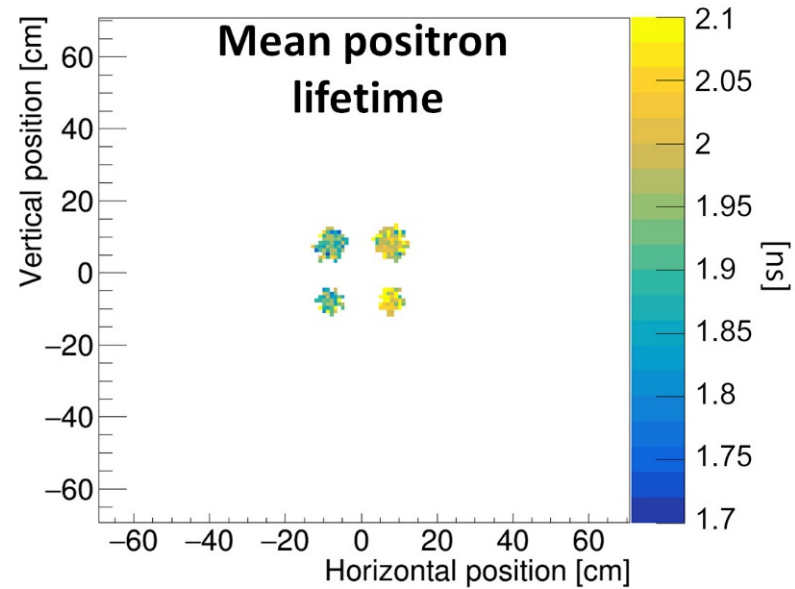
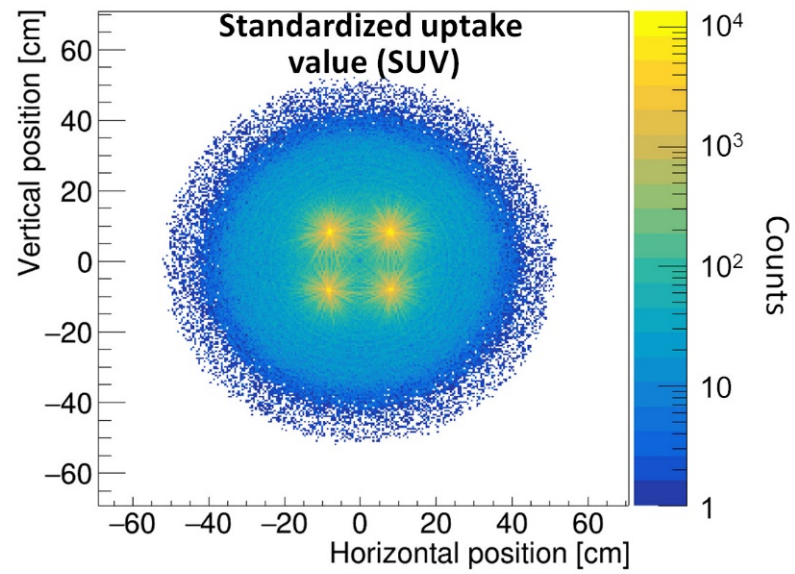


Sample preparation		
Patient 1	1	1
Patient 2	2	2



Placing samples in the chambers

Inserting setup to the detector



OPEN ACCESS

PAPER



Feasibility study of the positronium imaging with the J-PET tomograph

RECEIVED
31 May 2018REVISED
21 December 2018ACCEPTED FOR PUBLICATION
14 January 2019PUBLISHED
7 March 2019

Original content from this work may be used under the terms of the [Creative Commons Attribution 3.0 licence](#).

Any further distribution of this work must maintain attribution to the author(s) and the title of the work, journal citation and DOI.



P Moskal¹, D Kisielewska¹, C Curceanu², E Czerwiński¹, K Dulski¹, A Gajos¹, M Gorgol³, B Hiesmayr⁴, B Jasińska³, K Kacprzak¹, Ł Kapłon¹, G Korcyl¹, P Kowalski³, W Krzemień⁶, T Kozik¹, E Kubicz¹, M Mohammed^{1,7}, Sz Niedźwiecki¹, M Pałka¹, M Pawlik-Niedźwiecka¹, L Raczyński³, R Raj¹, S Sharma¹, Shivani¹, R Y Shopa³, M Silarski¹, M Skurzok¹, E Stępień¹, W Wiślicki³ and B Zgardzińska³

¹ Faculty of Physics, Astronomy and Applied Computer Science, Jagiellonian University, 30-348 Cracow, Poland

² INFN, Laboratori Nazionali di Frascati, 00044 Frascati, Italy

³ Institute of Physics, Maria Curie-Skłodowska University, 20-031 Lublin, Poland

⁴ Faculty of Physics, University of Vienna, 1090 Vienna, Austria

⁵ Department of Complex Systems, National Centre for Nuclear Research, 05-400 Otwock-Świerk, Poland

⁶ High Energy Physics Division, National Centre for Nuclear Research, 05-400 Otwock-Świerk, Poland

⁷ Department of Physics, College of Education for Pure Sciences, University of Mosul, Mosul, Iraq

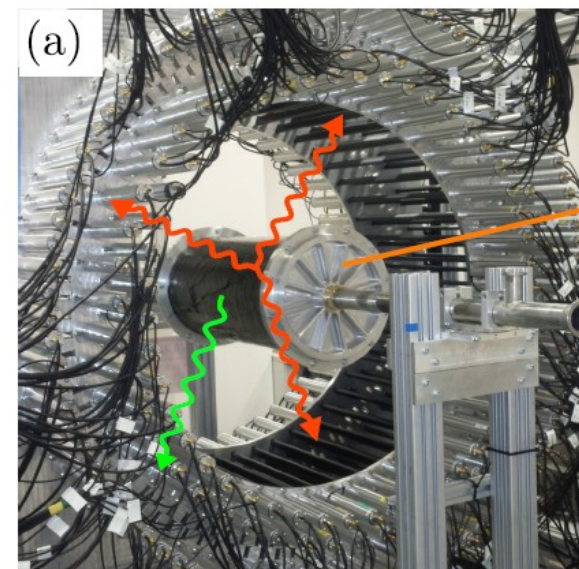
E-mail: daria.kisielewska@uj.edu.pl

Keywords: positron emission tomography, positronium atom, J-PET

Abstract

A detection system of the conventional PET tomograph is set-up to record data from e^+e^- annihilation into two photons with energy of 511 keV, and it gives information on the density distribution of a radiopharmaceutical in the body of the object. In this paper we explore the possibility of performing the three gamma photons imaging based on ortho-positronium

First in the world ortho-positronium image of the object



nature communications

[View all journals](#) [Search Q](#) [Login](#)

[Explore content](#) [About the journal](#) [Publish with us](#)

[Sign up for alerts](#) [RSS feed](#)

[nature](#) > [nature communications](#) > [articles](#) > [article](#)

Article | [Open Access](#) | [Published: 27 September 2021](#)

Testing CPT symmetry in ortho-positronium decays with positronium annihilation tomography

[P. Moskal](#), [A. Gajos](#), [...](#) [W. Wiślicki](#)

Nature Communications **12**, Article number: 5658 (2021) | [Cite this article](#)

3124 Accesses | 1 Citations | 40 Altmetric | [Metrics](#)

Abstract

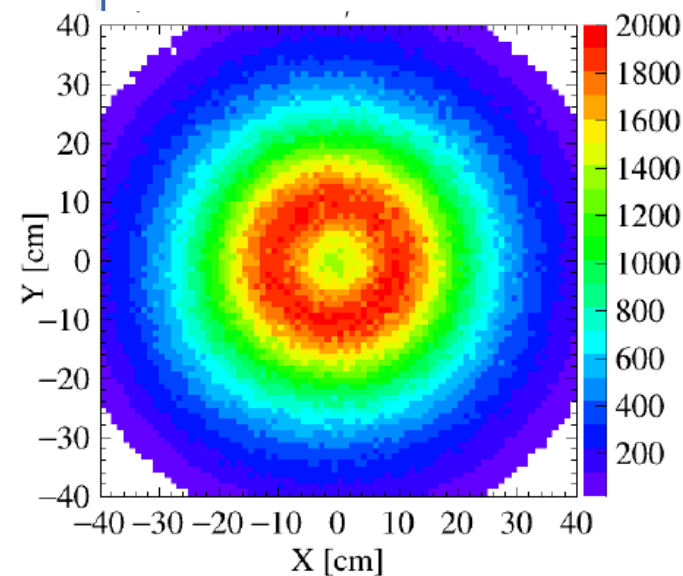
Charged lepton system symmetry under combined charge, parity, and time-reversal transformation (CPT) remains scarcely tested. Despite stringent quantum-electrodynamic limits, discrepancies in predictions for the electron-positron bound state (positronium atom) motivate further investigation, including fundamental symmetry tests. While CPT noninvariance effects could be manifested in non-vanishing angular correlations between final-state photons and spin of annihilating positronium, measurements were previously limited by knowledge of the latter. Here, we demonstrate tomographic reconstruction techniques applied to three-photon annihilations of ortho-positronium atoms to estimate their spin polarisation without magnetic field or polarised positronium source. We use a plastic-scintillator-based positron-emission-tomography scanner to record ortho-

Aleksander Gajos

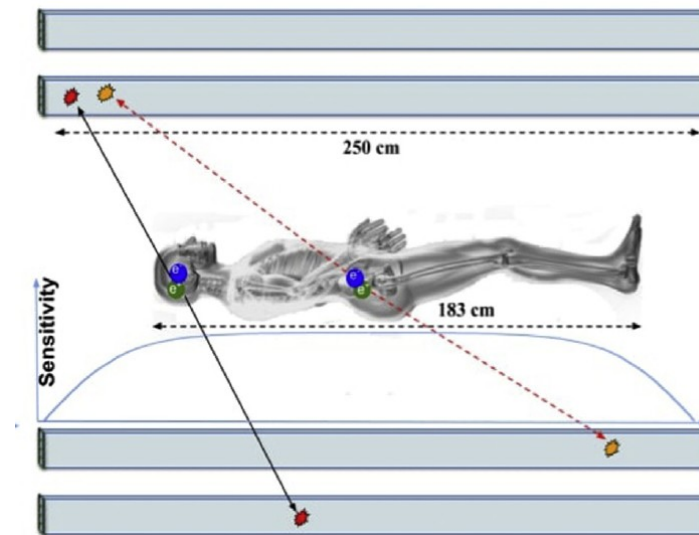
[Download PDF](#)

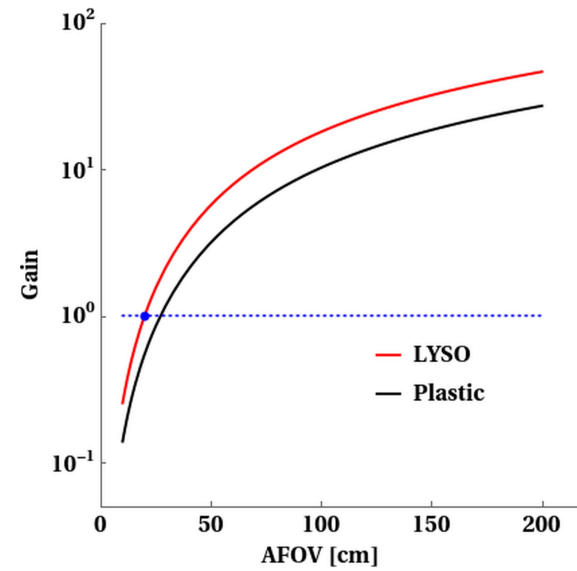
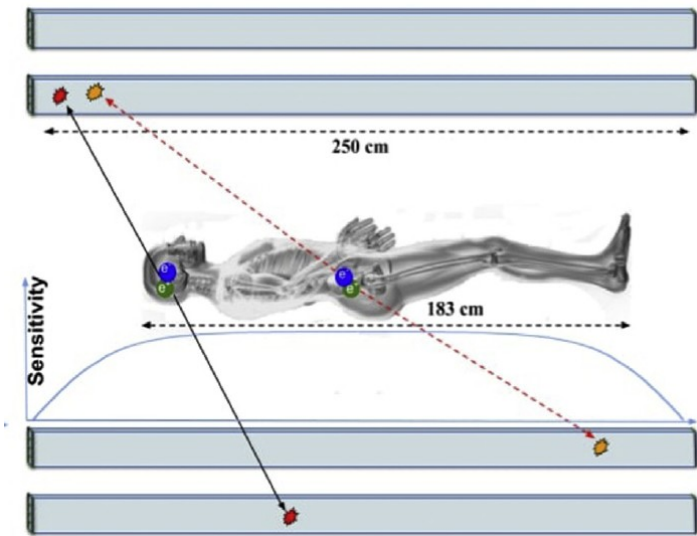
[Sections](#) [Figures](#) [References](#)

[Abstract](#)
[Introduction](#)
[Results](#)
[Discussion](#)
[Methods](#)
[Data availability](#)
[References](#)
[Acknowledgements](#)
[Author information](#)
[Ethics declarations](#)
[Additional information](#)
[Supplementary information](#)
[Rights and permissions](#)
[About this article](#)

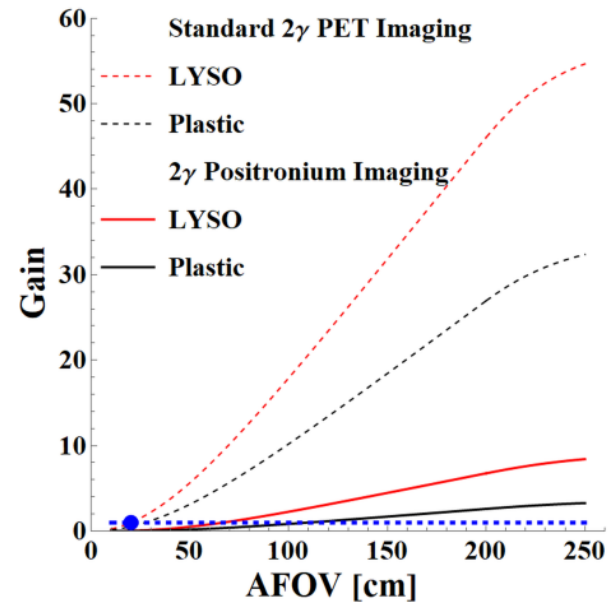
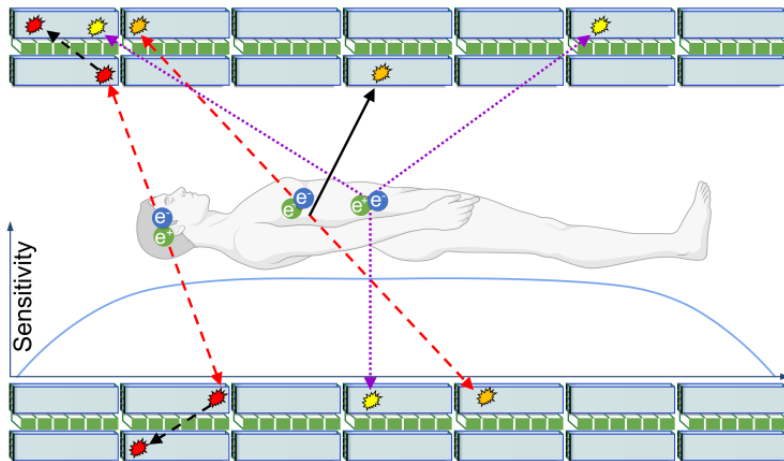


Towards Total Body J-PET





P. Moskal, E. Ł. Stępień,
PET Clinics 15 (2020) 439



Software for total-body J-PET

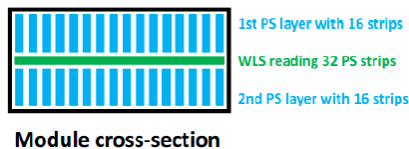
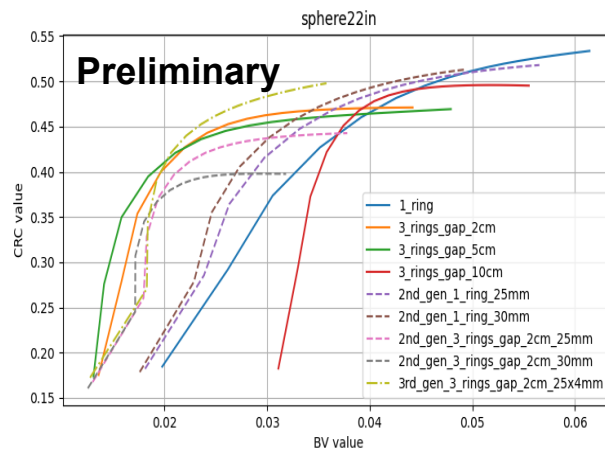
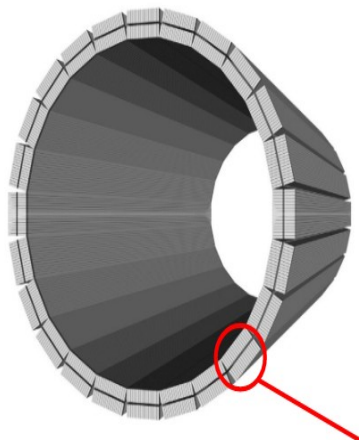
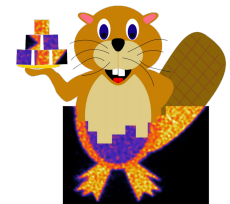
- scatter and random correction for total-body scanners
(see **Szymon Parzych talk tomorrow**)
- Normalization corrections
(see **A. Coussat's talk this afternoon**)
- point-spread functions
- system matrix parametrization
- Multi-photon + conventional PET reco. algorithms
- **Machine learning techniques for background reduction**
- Various software tools

Coordinator: W. Krzemien

- Jakub Baran
- Lech Raczynski
- Szymon Parzych
- Mateusz Bała
- Paweł Kowalski
- Aurelien Coussat
- Damian Trybek



Extensive usage of GATE simulations



Python

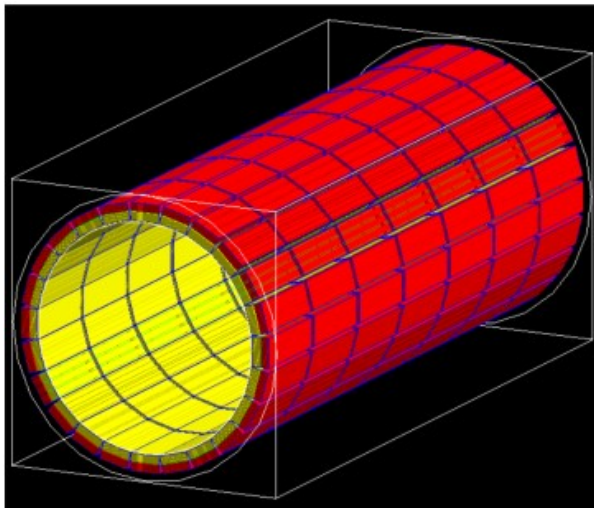
C++



GitHub

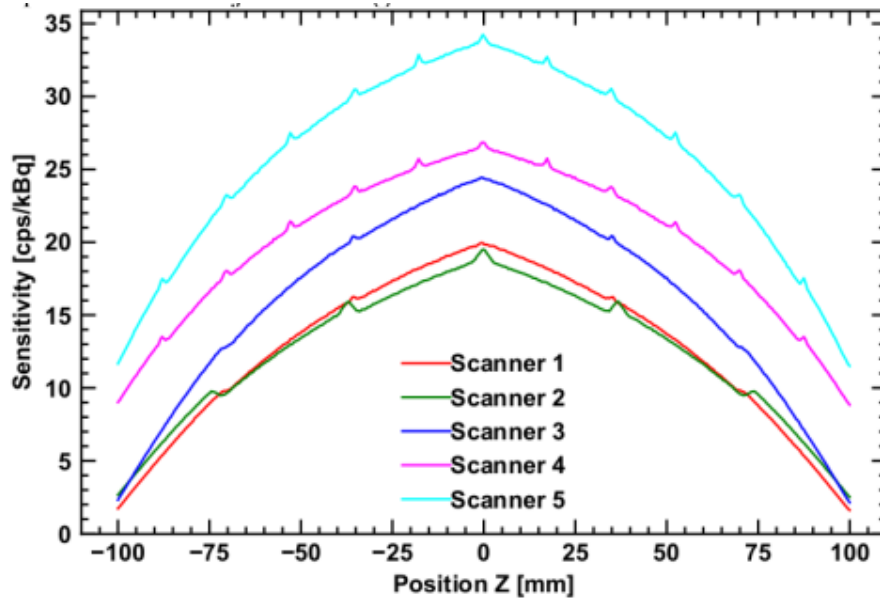


Total-Body J-PET Geometry Optimization

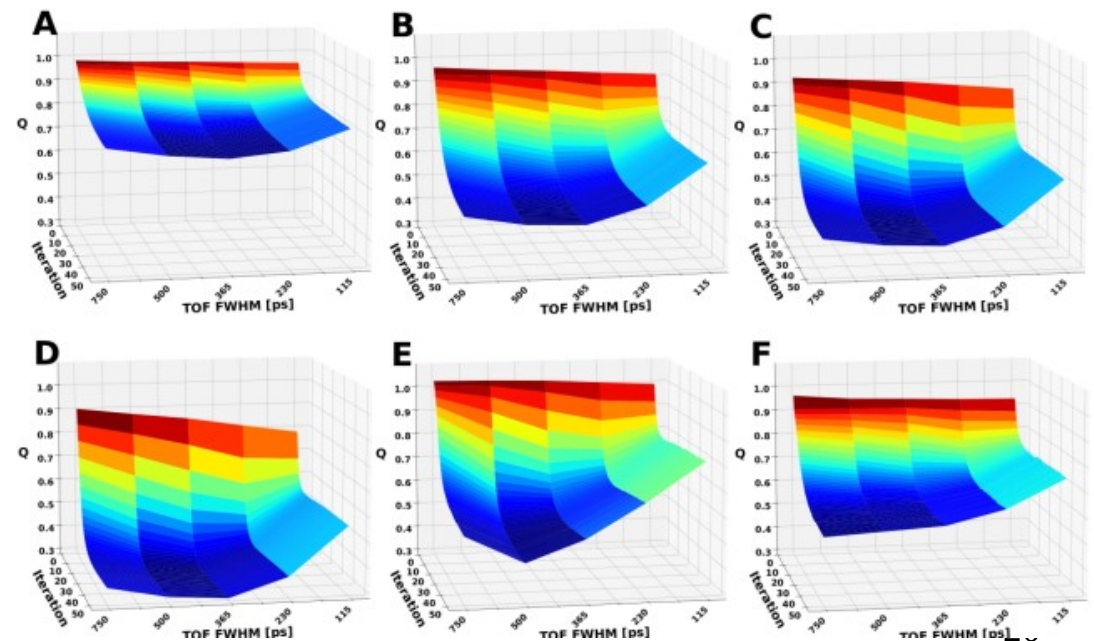


Property	Scanner geometry				
	<i>S1</i>	<i>S2</i>	<i>S3</i>	<i>S4</i>	<i>S5</i>
Radius [mm]	506	506	425	414.65	414.65
Axial FOV [mm]	2099.2	2159.2	2099.2	2430	2430
Scintillator length [mm]	686.4	686.4	686.4	330	330
Scintillator cross-section [mm]	25x5.7	25x5.7	25x5.7	25x6.0	30x6.0
No of adjacent rings	3	3	3	7	7
Gap between adjacent rings [mm]	20	50	20	20	20

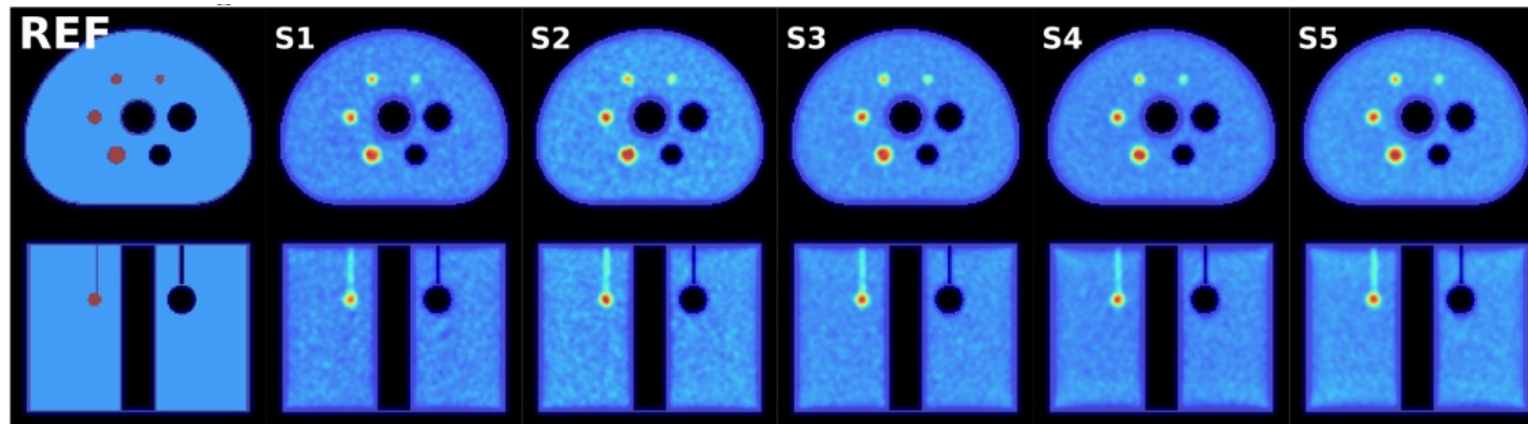
preliminary Sensitivity



TOF kernel choice

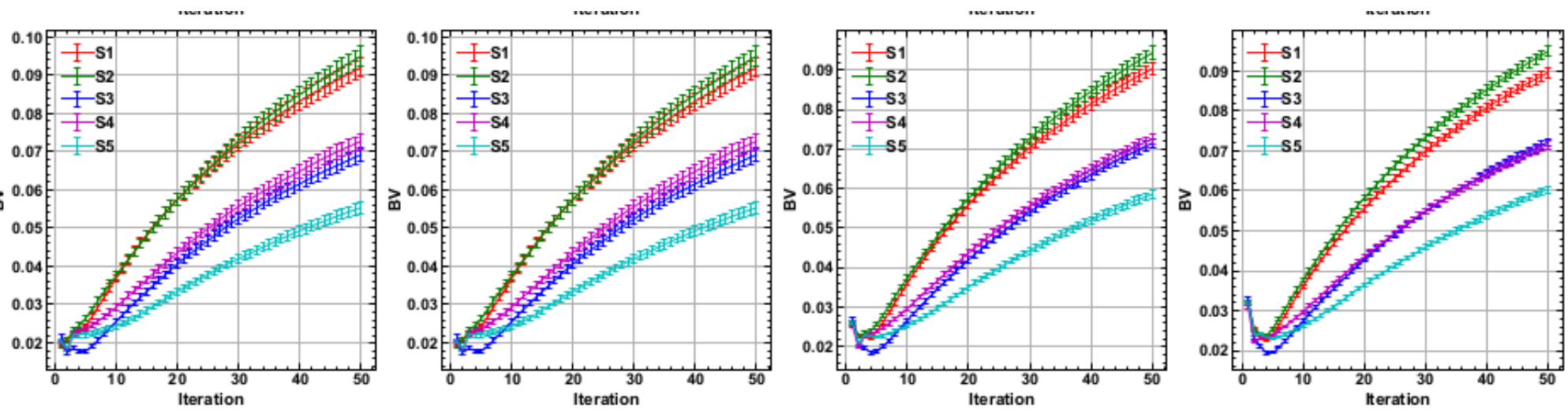


Total-Body J-PET Geometry Optimization – NEMA IEC



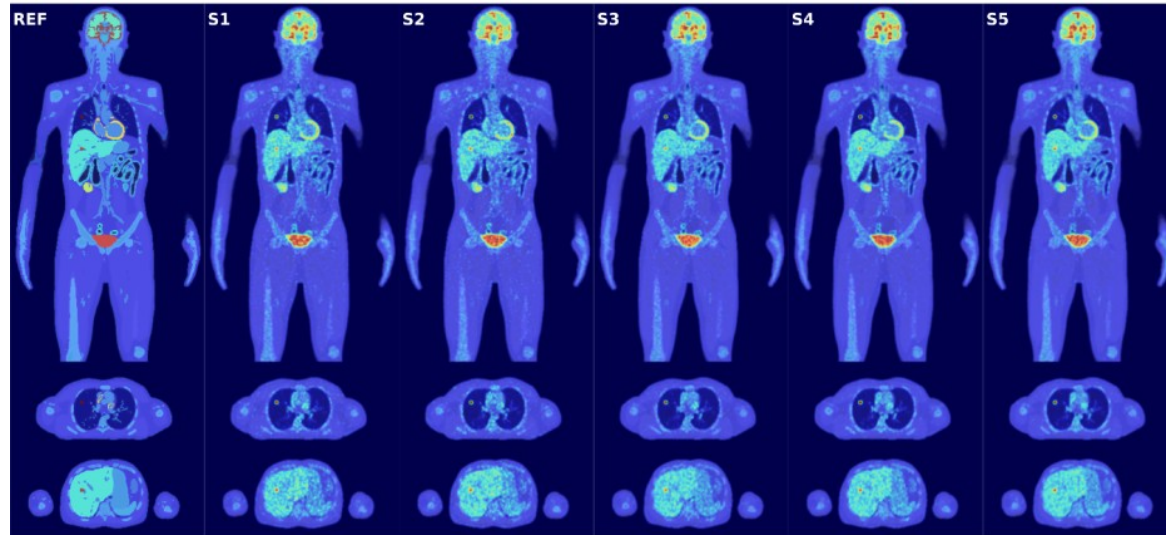
preliminary

Background variability



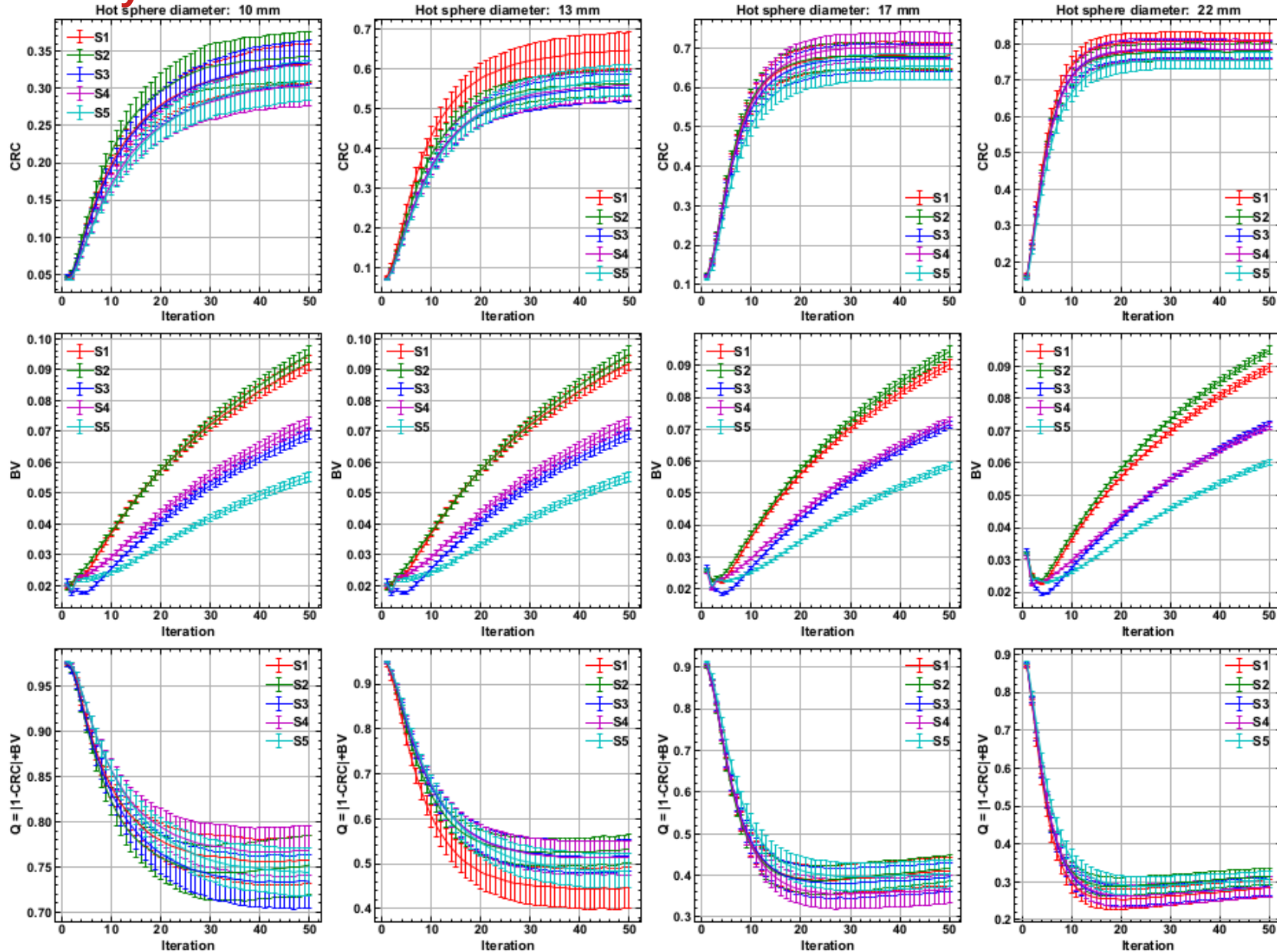
Total-Body J-PET Geometry Optimization – XCAT phantom

preliminary



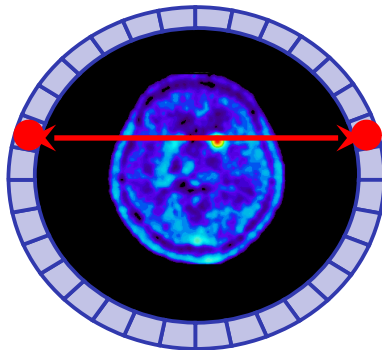
Total-Body J-PET Geometry Optimization – XCAT phantom

preliminary

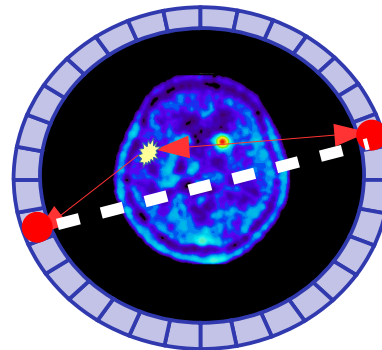


Coincidence classification for total-body J-PET

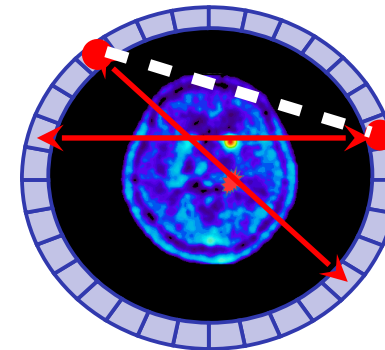
True events



Scattered events

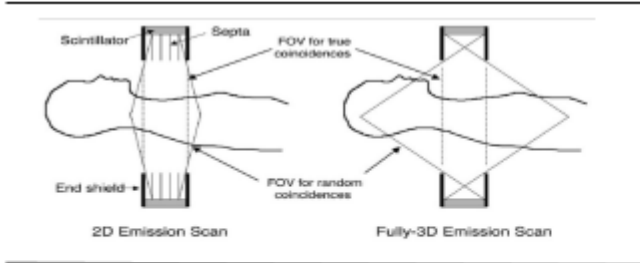


Random events



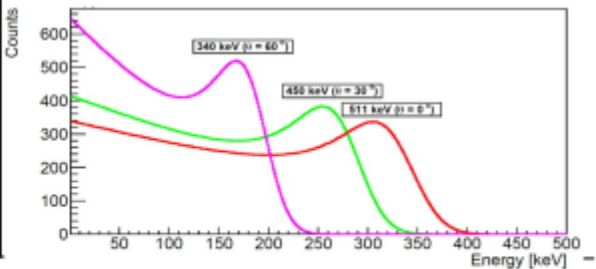
Coincidence classification for total-body J-PET

For total-body J-PET scanner we expect higher background level from non-genuine coincidences



Multiple scattering in the phantom is not negligible

In J-PET

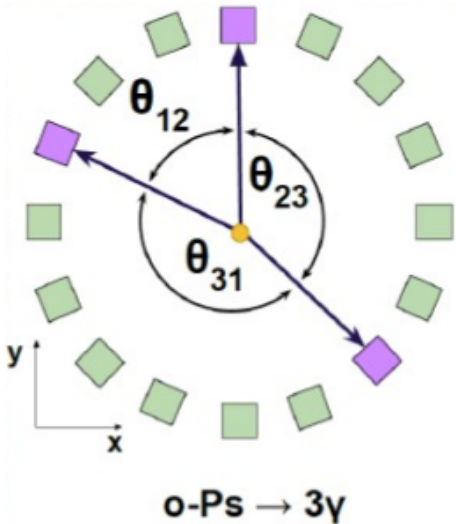


D. Brasse et al. J Nucl Med 2005; 46:859–867

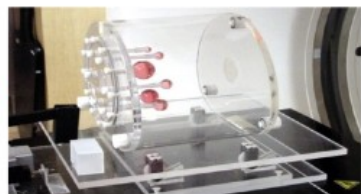
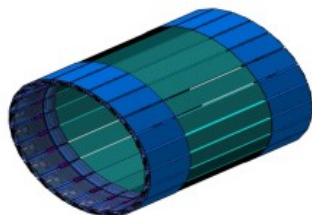
Situation much more complicated for multi-photon coincidences...

- More photons \rightarrow More combinations
- Less strictly defined geometry
- Photon energies have a distribution

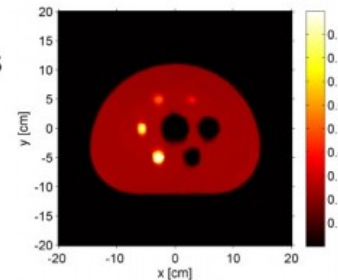
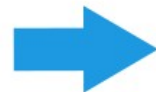
Idea: apply ML techniques to reduce background (ACCIDENTAL, SCATTER)



Training data generation



Monte Carlo Simulations



Modular J-PET

- 50 cm AFOV
- 24 modules x 13 strips
- 24 x 6 x 500 mm strips

NEMA IEC Phantom

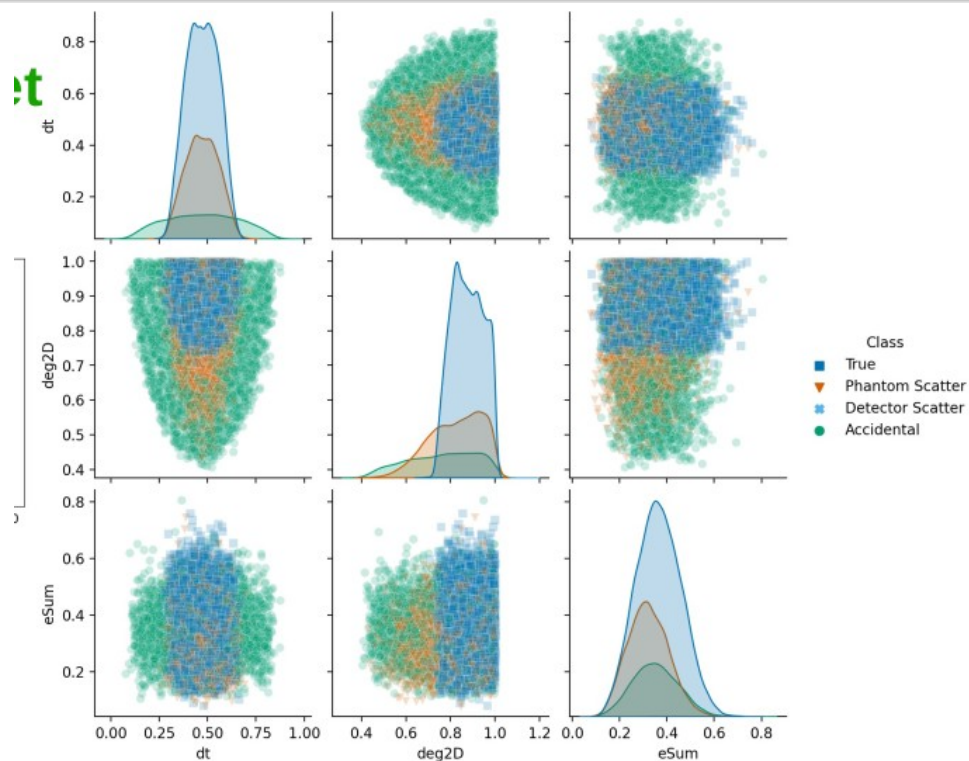
- 4 hot spheres
- 2 cold spheres
- Activity - 59 Mbq
- acquisition time - 500 seconds
- contrast between hot and cold regions – 4:1

GATE MC Simulation

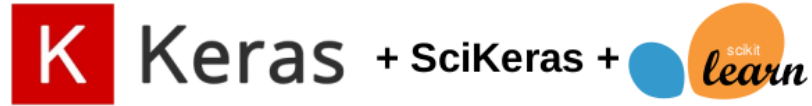
- 30M coincidences
- Phenomenological time, energy and positional resolution
- Geometry cuts → reduce accidental fraction



21



- Feedforward Neural Network



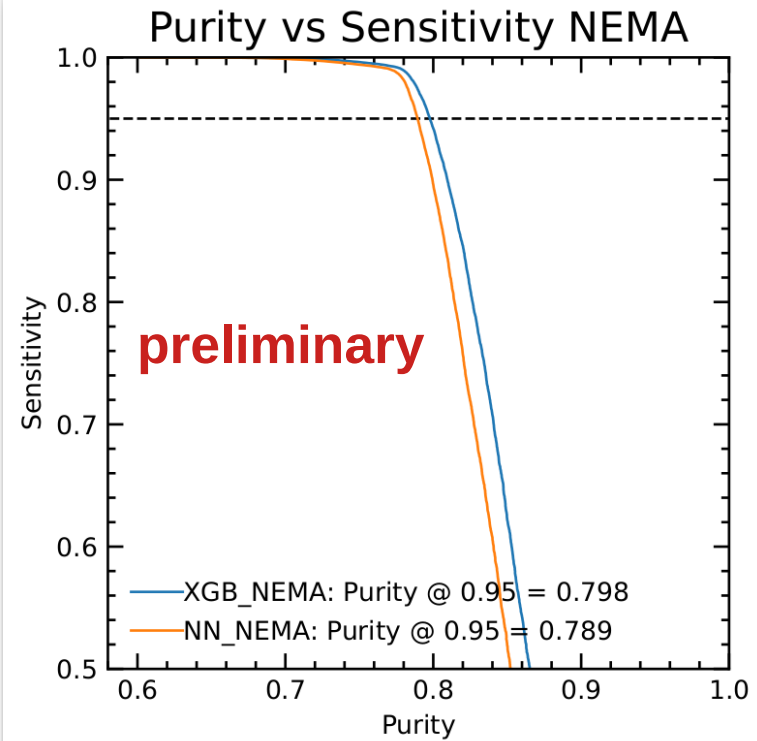
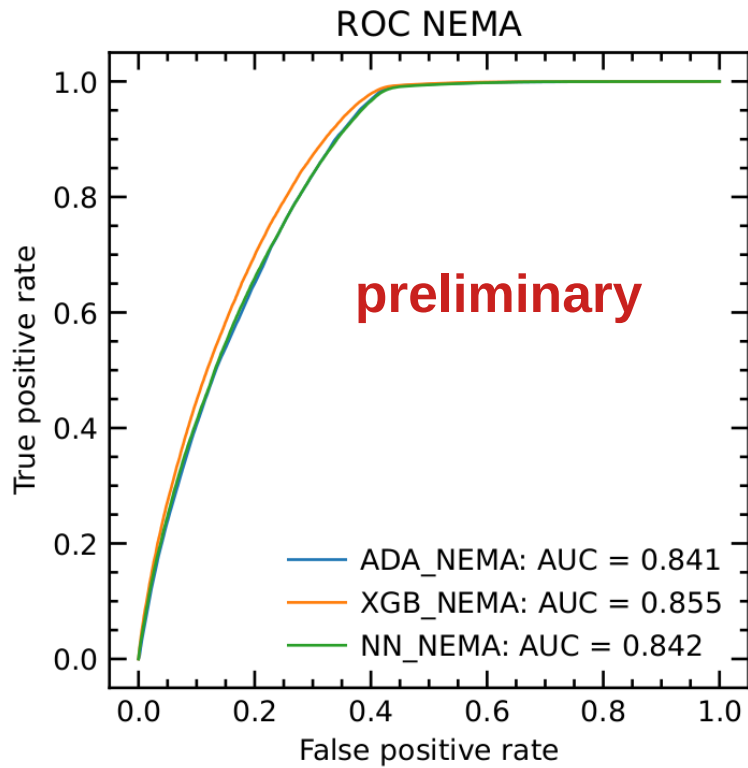
- ADABOOST



- XGBoost



Base line: 65%



Quantum simulations and medical imaging software platform

Group:

- Wojciech Krzemień
- Konrad Klimaszewski
- Mateusz Bała
- Oleksander Fedoruk
- Lech Raczyński
- Tobiasz Jarosiewicz

Services



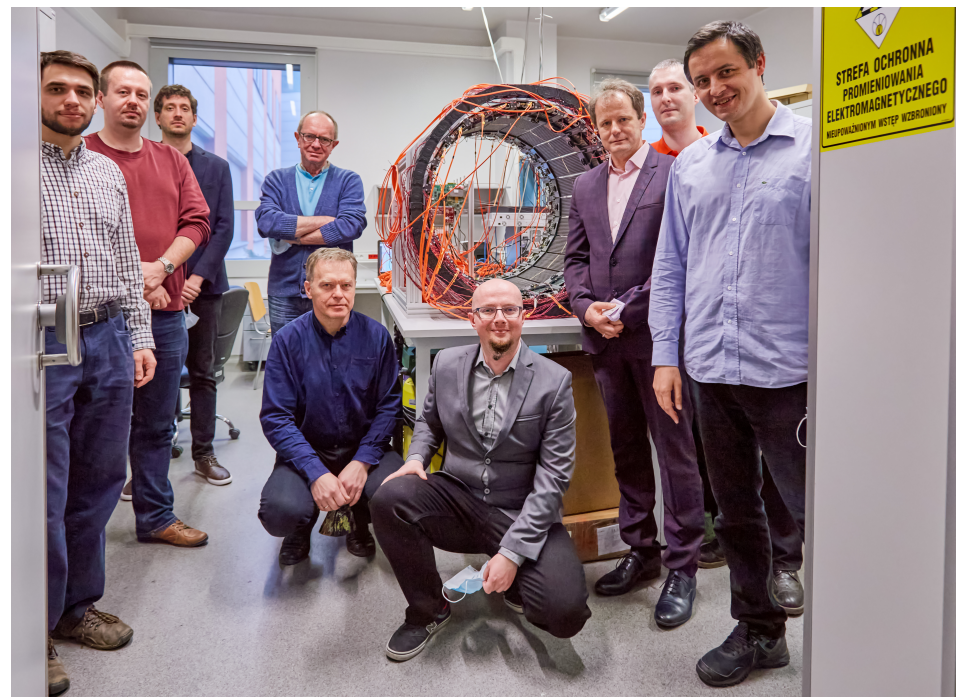
Quatum emulators/
Quantum computer



Libraries



Thank you for attention



More materials available at:
<http://koza.if.uj.edu.pl/pet/>