

Journées thématiques du Réseau Semi-conducteurs IN2P3-IRFU

Luc HEBRARD
[*luc.hebrard@unistra.fr*](mailto:luc.hebrard@unistra.fr)

Microcapteurs magnétiques intégrés sur CMOS et applications

Laboratoire ICube

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CMOS compatible magnetic sensors

Hall effect magnetometers : from 1D to 3D sensing

Magnetic tracking of medical tools under MRI

Conclusion

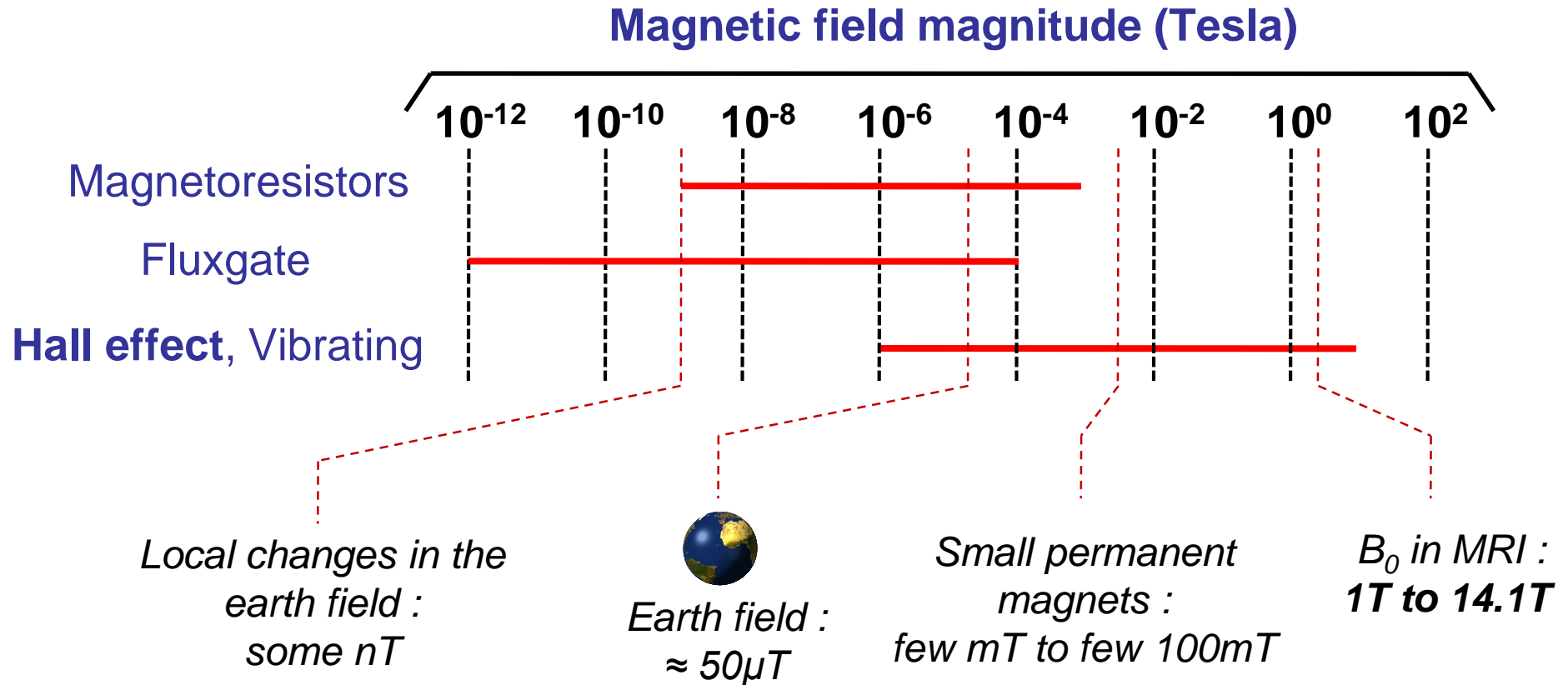
CMOS compatible sensors, **even fully compatible (no post-process)**

Sensing device + specific electronics = micro-sensor
 ↗ simple post-process if required

Applied projects :

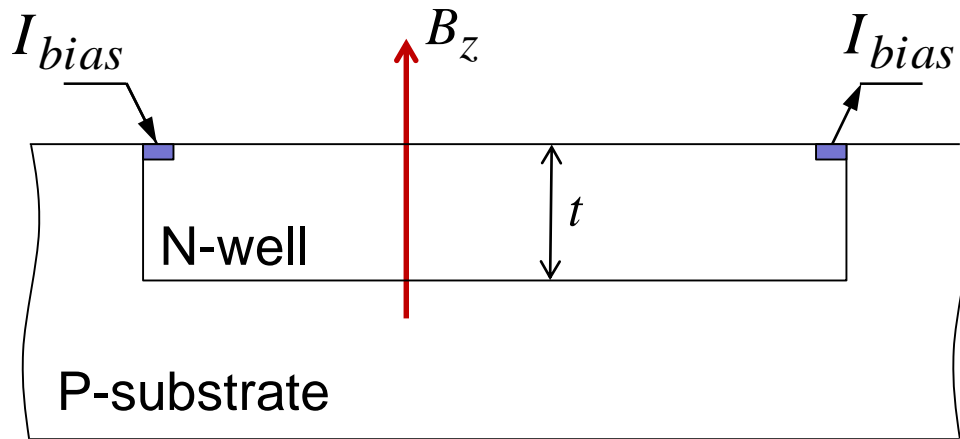
- Contactless current sensors
- Magnetic navigation of catheter
- ECG in MRI
- **Medical tool tracking/positioning in MRI**
- NMR microprobe

Medical applis → **3D sensor**



→ DC to a few kHz bandwidth magnetometers

- ➔ Fully compatible with CMOS processes → no post-processing
- ➔ Easy industrial outlets → the most produced micro-magnetometer (1D)
- ➔ Wide range of measurement : few $10\mu\text{T}$ to several Tesla
- ➔ Two types of Hall devices :
 - HHD : Horizontal Hall device → for B_z measurement
 - VHD : Vertical Hall device → for B_x and B_y measurement
- ➔ 3D Hall probe = 1 HHD + 2 VHD



$$V_H = \frac{G \cdot r}{n \cdot q \cdot t} \cdot I_{bias} \cdot B_z = S_I \cdot I_{bias} \cdot B_z$$

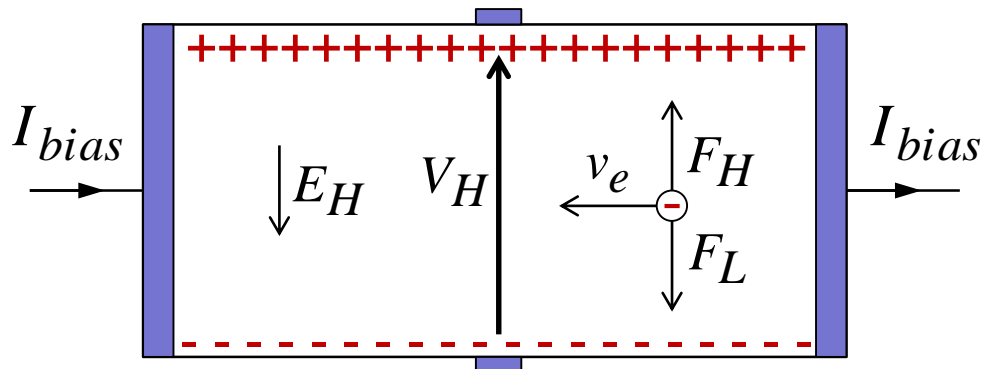
S_I : current relative sensitivity

$G < 1$: geometrical factor

r : scattering factor ≈ 1.15 for Si

n : doping of the plate

t : plate thickness



Biassing current flowing « horizontally » \Rightarrow **HHD**

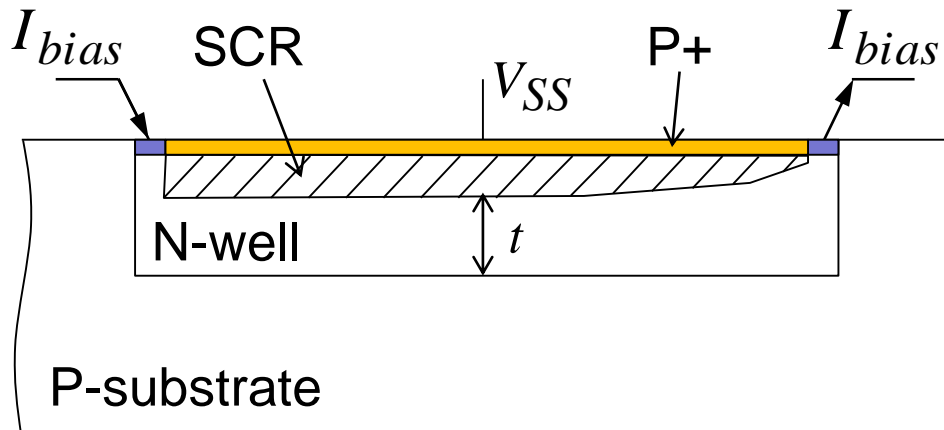
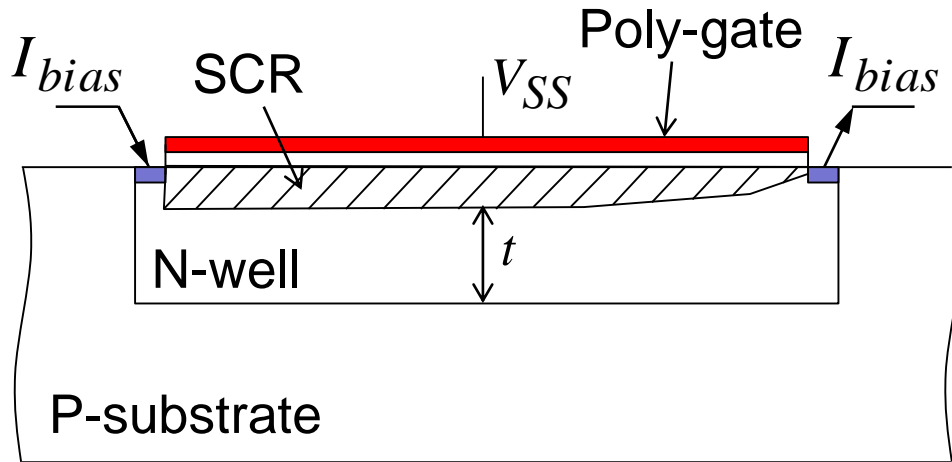
➔ Accurate processing of the fluctuation of the mean free transit time τ

$$V_H = \frac{G \cdot r}{n \cdot q \cdot t} \cdot I_{bias} \cdot B_z = S_I \cdot I_{bias} \cdot B_z + S_{IPHE} \cdot I_{bias} \cdot B_x \cdot B_y$$

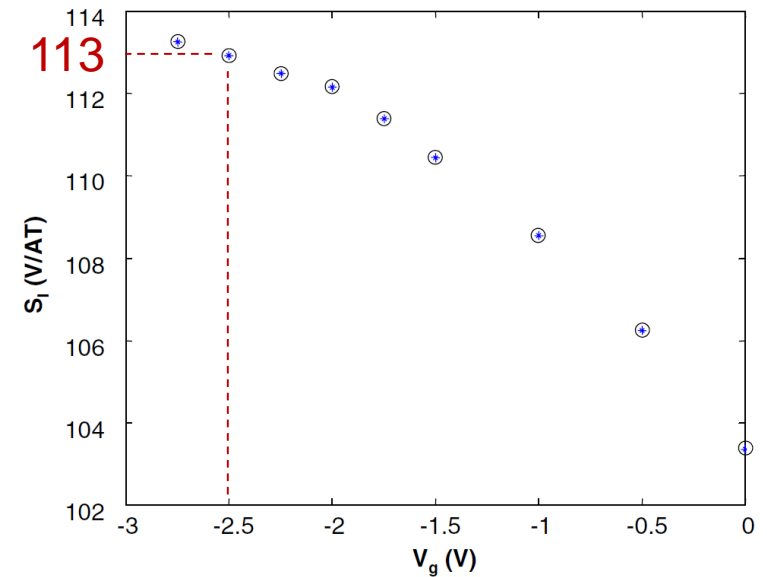
$$S_I = \frac{G \cdot r}{n \cdot q \cdot t} = \frac{G \cdot \langle \tau^2 \rangle}{n \cdot q \cdot t} \quad S_{IPHE} = \frac{\mu_n}{n \cdot q \cdot t} \cdot \left[\frac{\langle \tau^3 \rangle}{\langle \tau \rangle^3} - \frac{\langle \tau^2 \rangle^2}{\langle \tau \rangle^4} \right]$$

$S_{IPHE}/S_I \approx 8\%$ → not an issue when $B_x \approx B_y \approx B_z \approx$ a few mT

➔ Be careful when you measure a few mT over a few Teslas !



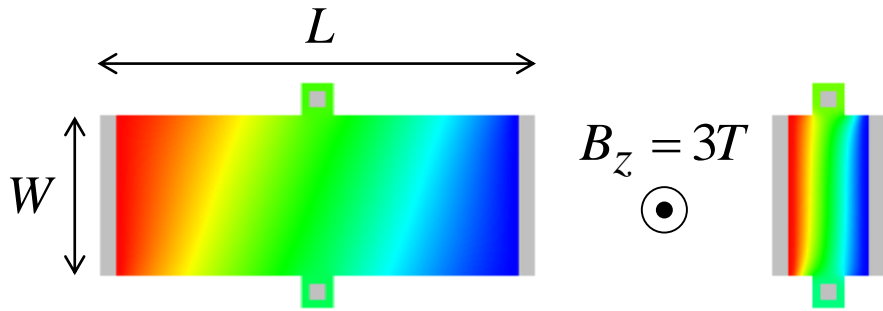
S_I improvement:



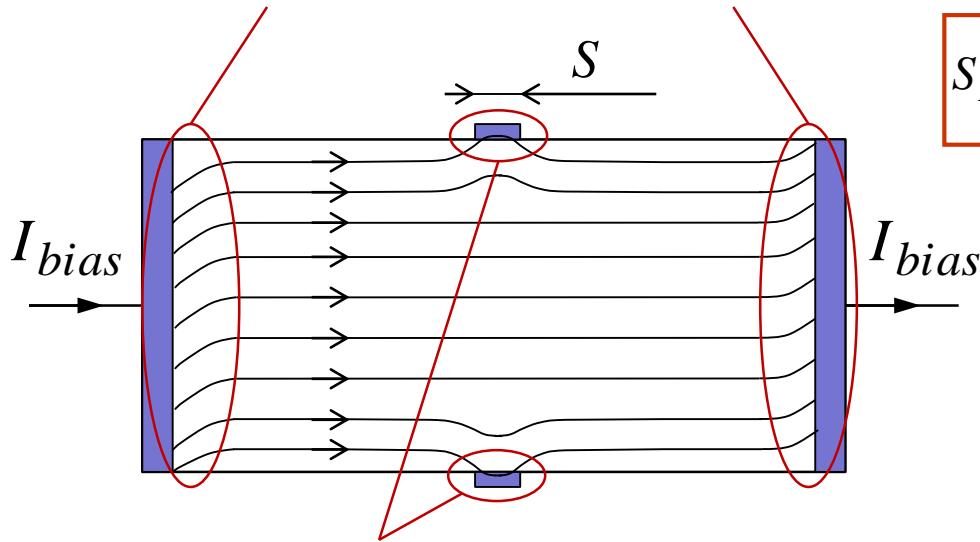
HHD in CMOS 0.6 μ m

without any gate $S_I = 80$ V/(A·T)

$V_g = V_{SS} = -2.5$ V : $S_I = 113$ V/(A·T)

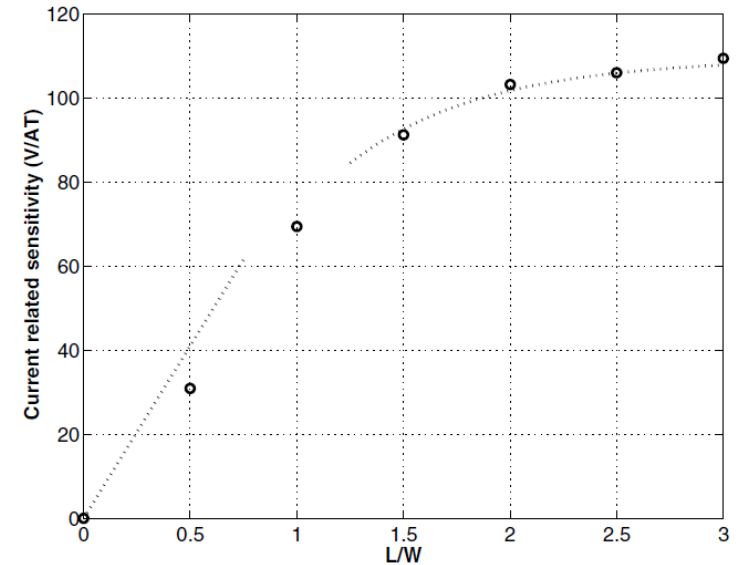


Short circuit by the biasing contacts



Short circuit by the sensing contacts

$$S_I = \frac{G \cdot r}{n \cdot q \cdot t}$$



$$G \approx 1 \text{ for } \begin{cases} L/W > 2 \\ W/S > 10 \end{cases}$$

$$L = 20\mu\text{m and } W = 10\mu\text{m}$$

Voltage biasing for highest I_{bias} ?

$$V_H = \frac{G \cdot r}{n \cdot q \cdot t} \cdot I_{bias} \cdot B_z$$

$$R_{in} = \frac{1}{n \cdot q \cdot \mu_n} \cdot \frac{L}{W \cdot t}$$

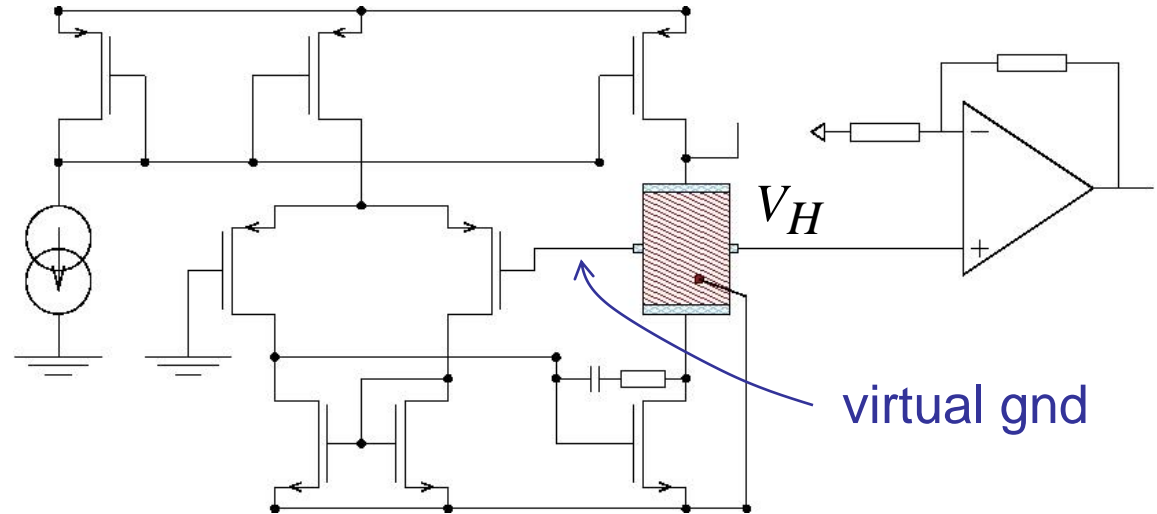


$$V_H = G \cdot r \frac{W}{L} \cdot \mu_n \cdot V_{bias} \cdot B_z$$



Very sensitive to temperature!

Current biasing is better



Easy to design I_{bias} insensitive to T



Low thermal drift of the sensor sensitivity

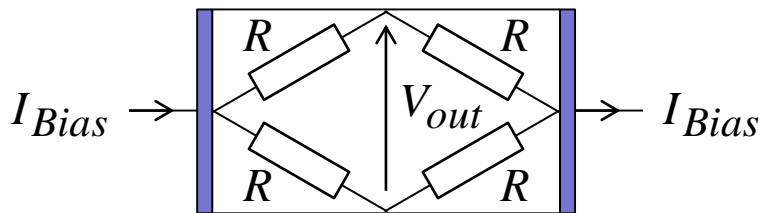
Three sources :

Sensing contact misalignment

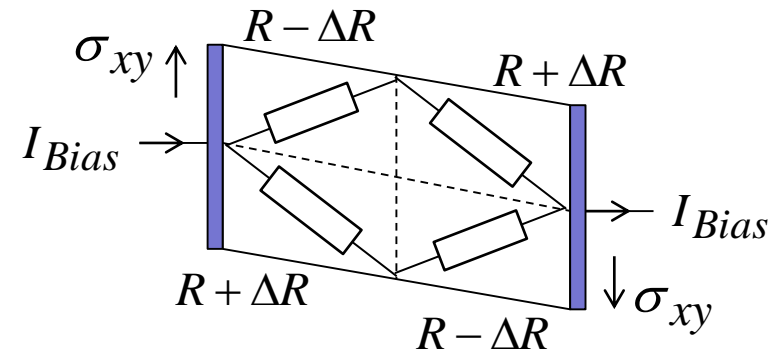
Doping gradients

Shear stress

→ Unbalanced equivalent Wheatstone bridge



$$V_{out} = 0$$



$$V_{out} = \Delta R \cdot I_{bias} = V_{off}$$

Typical output $V_{off} = 1$ to 2 mV

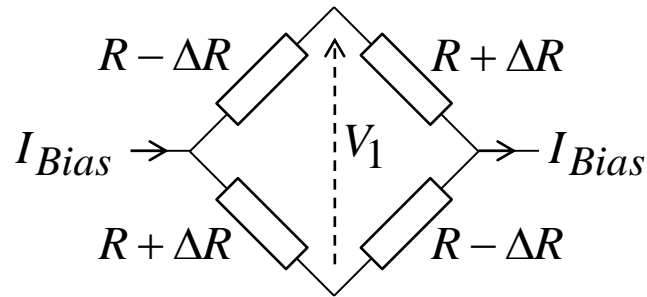
Typical sensitivity $S_A = 100$ mV/T

→ Equivalent input offset of **10mT to 20mT !!!**

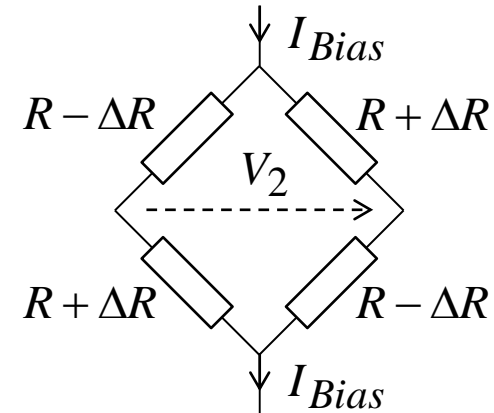
Symmetrical HHD by a 90° rotation
 Sensing and biasing contacts swap

\longrightarrow

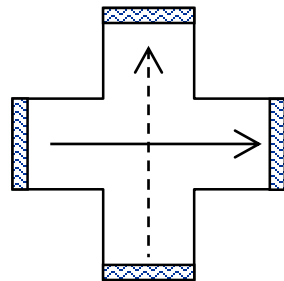
V_H is unchanged
 V_{off} is reversed



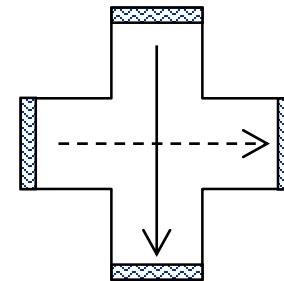
Phase 1: $V_1 = V_H + V_{off}$

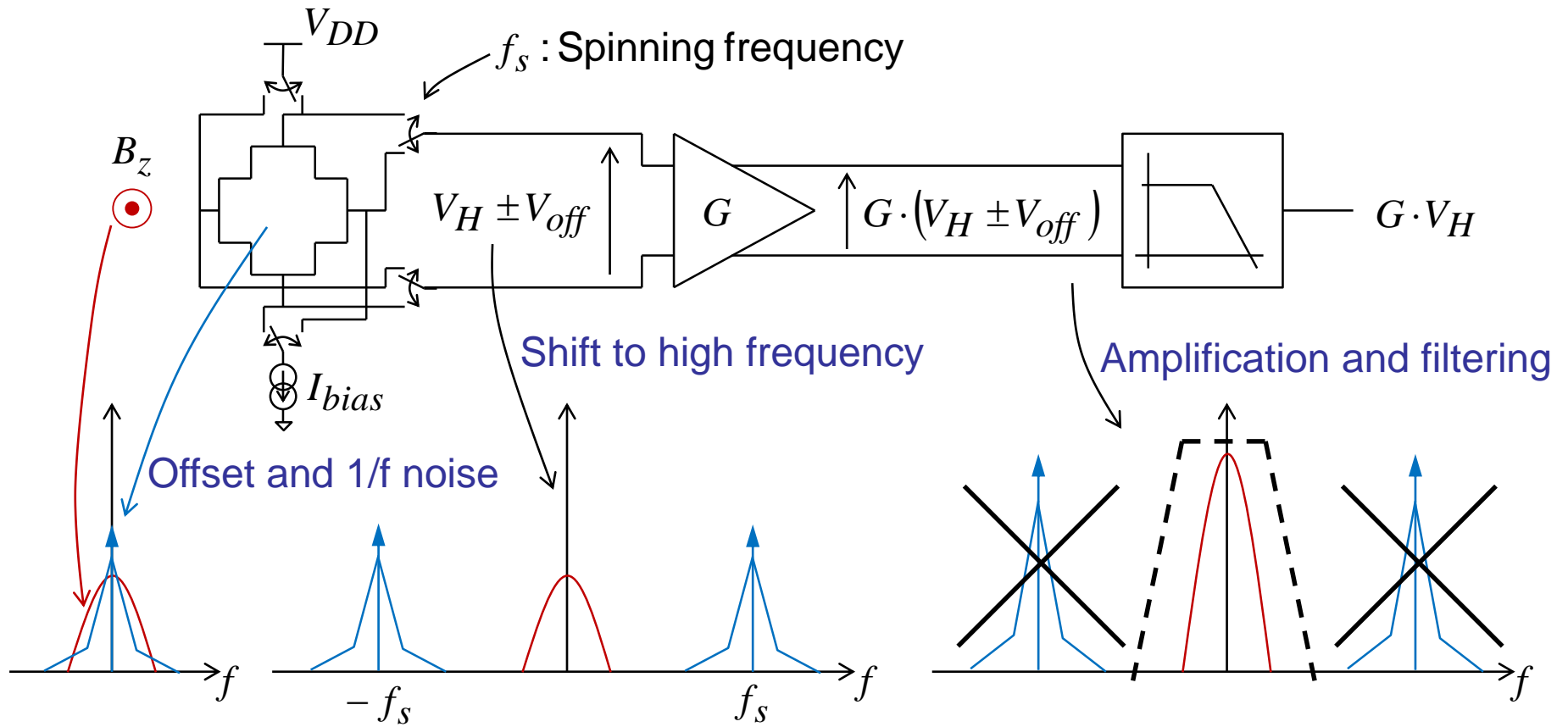


Phase 2: $V_2 = V_H - V_{off}$

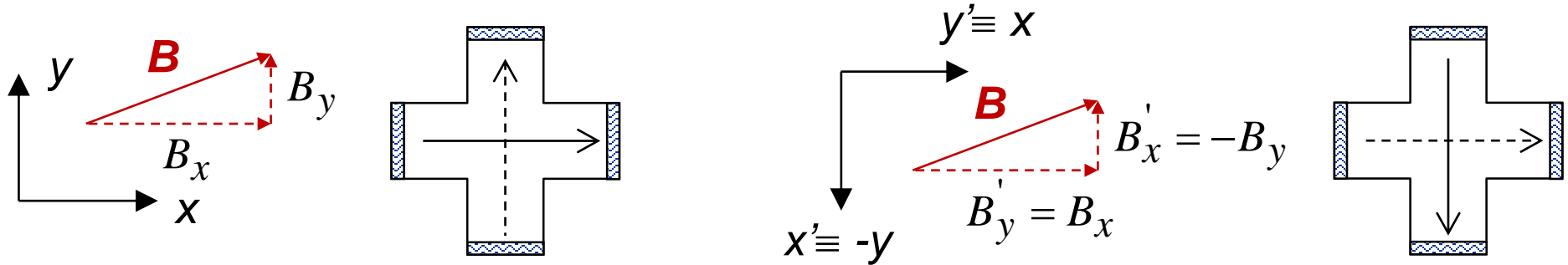


Cross-shaped HHD





➔ 1/f noise cancelling → resolution of **10 μ T over a few kHz bandwidth**

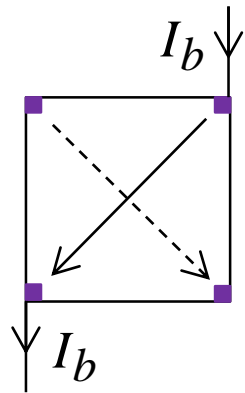


$$V_{PHE1} = S_{IPHE} \cdot I_{bias} \cdot B_x \cdot B_y$$

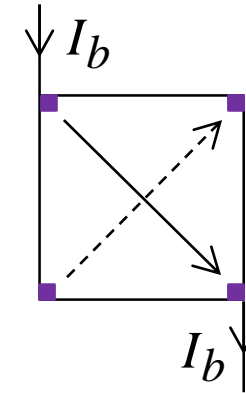
$$V_{PHE2} = S_{IPHE} \cdot I_{bias} \cdot \underbrace{B'_x \cdot B'_y}_{-B_x \cdot B_y}$$

$$V_{PHE2} = -V_{PHE1}$$

➡ Spinning current is magic !



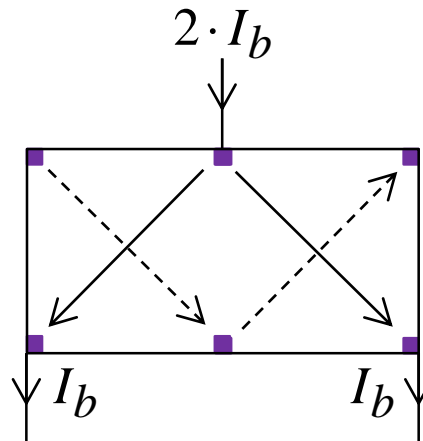
Two separate devices



$$V_1 = V_H + V_{off} + V_{PHE} + V_{1/f1}$$

$$V_2 = V_H - V_{off} - V_{PHE} + V_{1/f2}$$

Two HHD in series



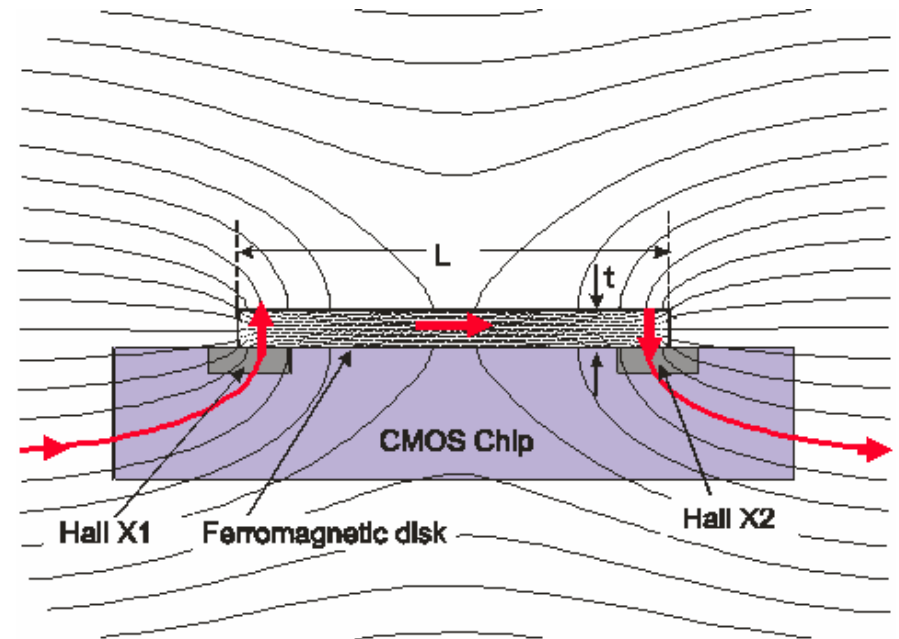
$$V_{out} = 2 \cdot V_H + V_{1/f1} + V_{1/f2}$$

$$V_{out} = 2 \cdot V_H + V_{1/f}$$

Reproduced from C. Schott, and al., CMOS Three Axis Hall Sensor and Joystick Application, IEEE Sensor Conference, 2004

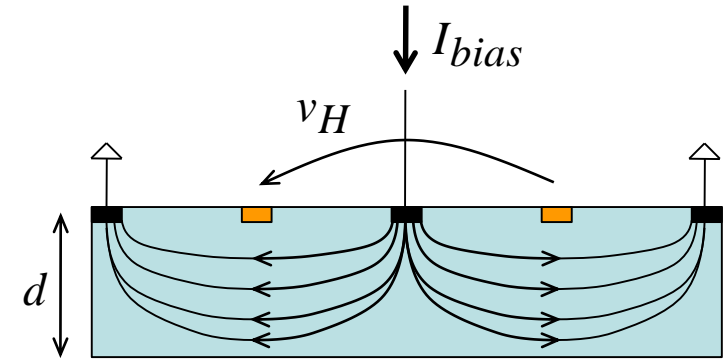
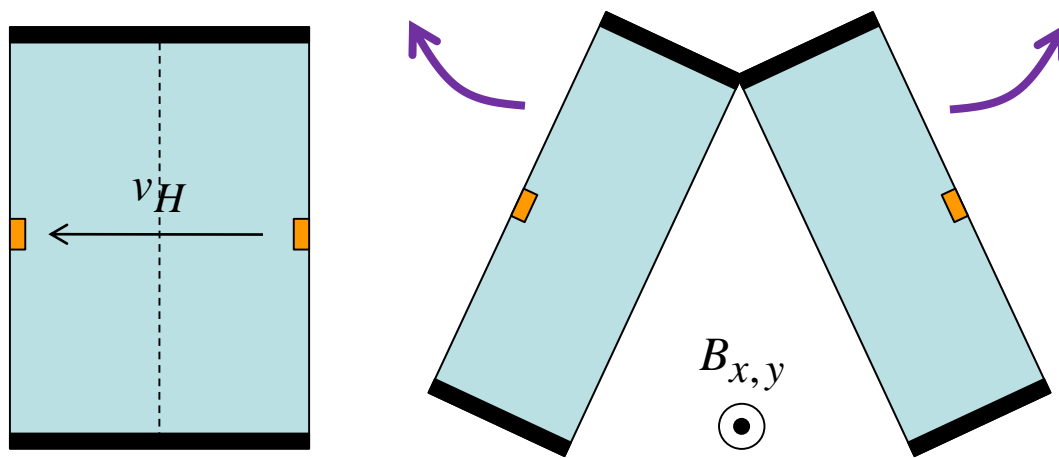
2001/2002 : Introduction of Integrated Magnetic Concentrators (ICM) – (EPFL)

- Magnetic amplification by a factor of 10
- Soft magnetic material above CMOS
- Low hysteresis...
- Commercial product from Melexis



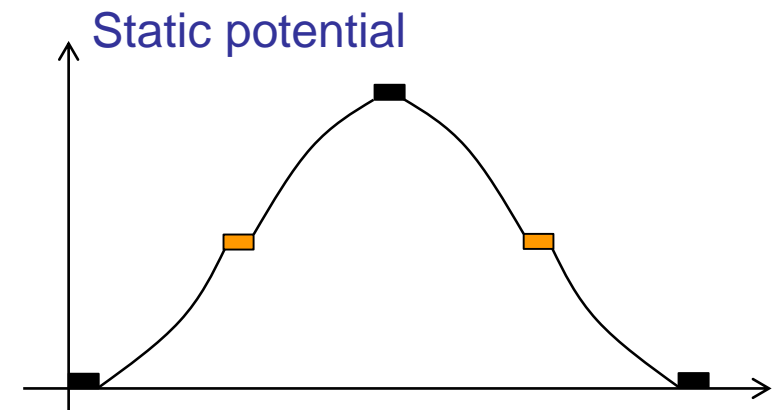
2002/2004 : Vertical Hall Device in the deep Nwell of HV-CMOS - (EPFL)

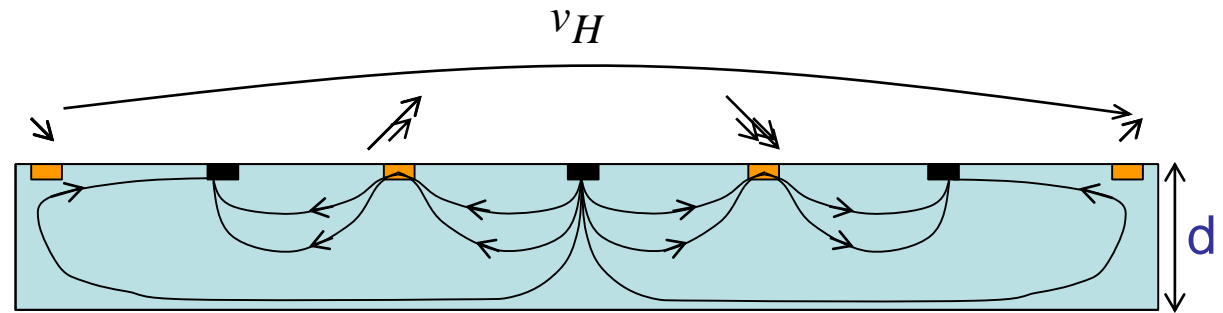
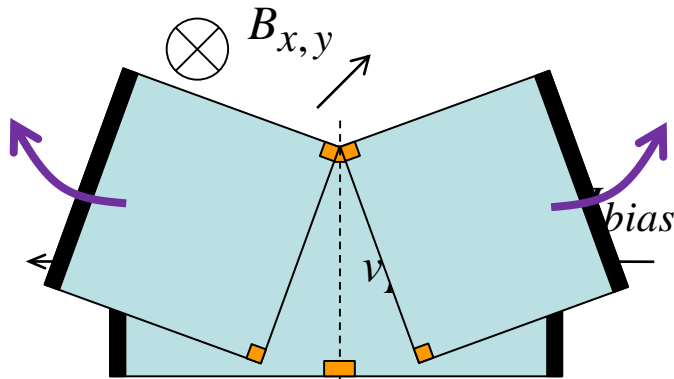
2008 : Vertical Hall Device in the shallow Nwell of LV-CMOS - (ICube)



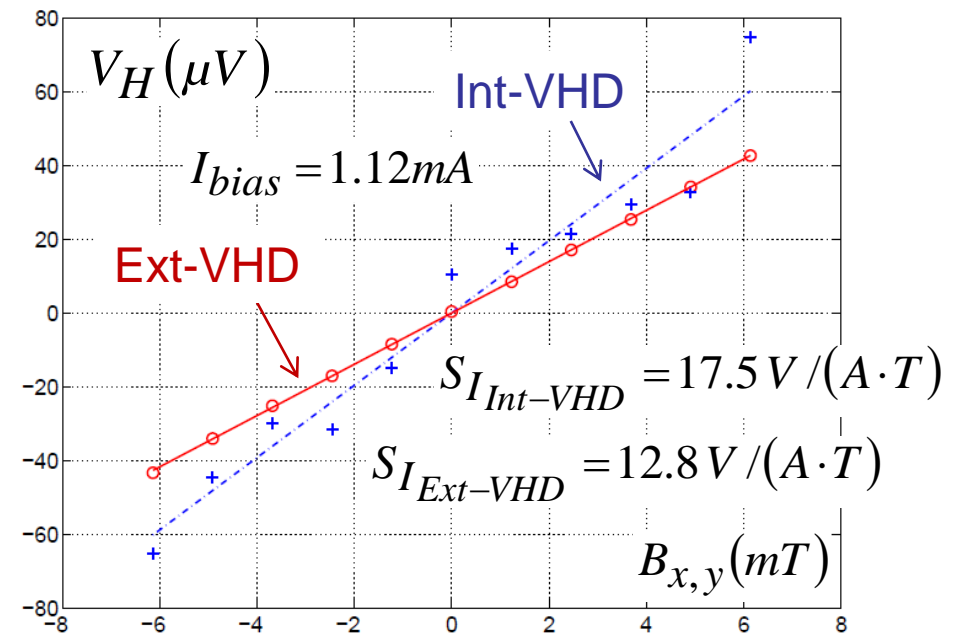
d has to be high to **avoid short-circuit by sensing contacts !**

- ➔ 1984 – 2002 : VHD were discrete devices
- ➔ 2002 First VHD in HV-CMOS ($d = 7\mu\text{m}$), but :
 - **Low sensitivity** (residual short-circuit)
 - **High offset** → amplifier saturation
 - **High $1/f$ noise** → 1mT resolution

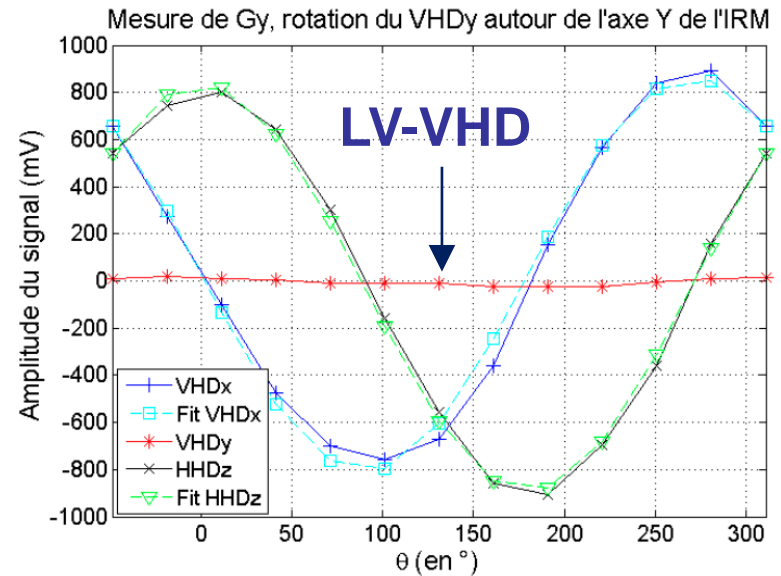
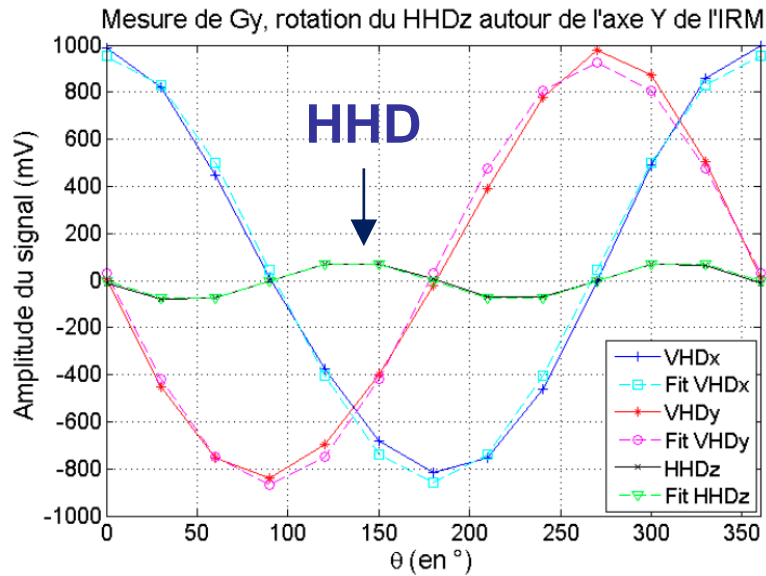
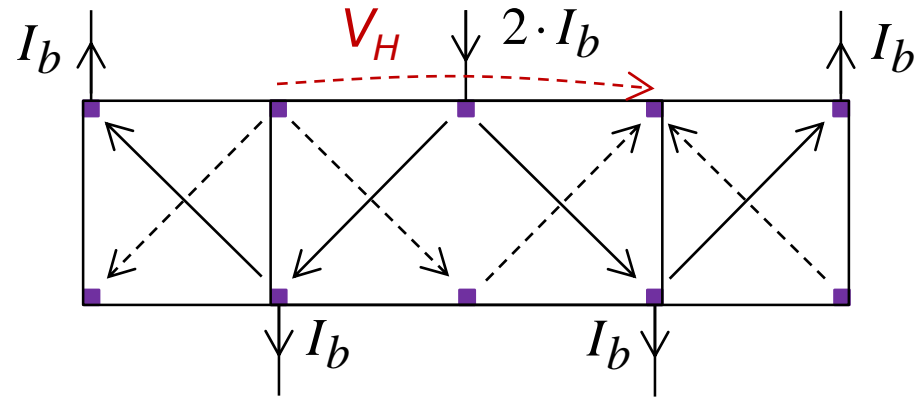




The Ext-VHD resolution of $80 \mu\text{T}$ over 1.6 kHz without any electronics while it is of $800 \mu\text{T}$ for the Int-VHD

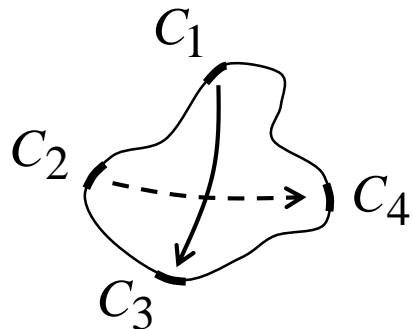


HV-VHD



➔ The only way to remove the $1/f$ noise, as well as PHE, and offset

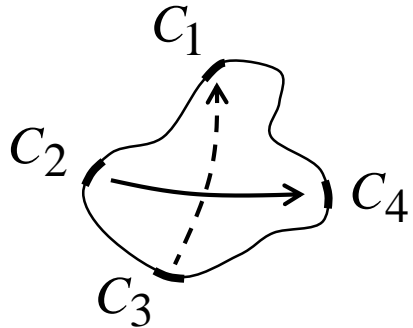
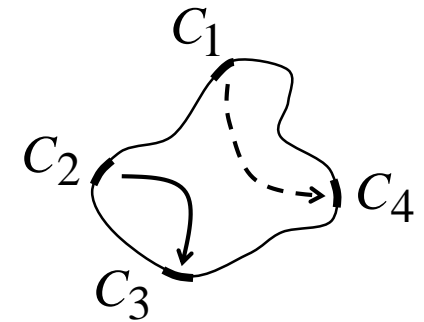
From the Reverse Magnetic Field Reciprocity theorem, i.e. $\sigma(\mathbf{r}, \mathbf{B}) = \sigma^t(\mathbf{r}, -\mathbf{B})$, it can be shown that in a linear material :



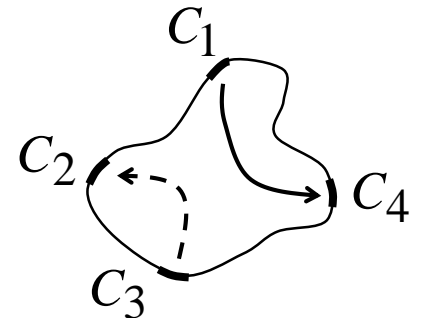
$$V_{out1} = V_H + V_{off} + V_{1/f} + V_{PHE}$$

—————→ I_B

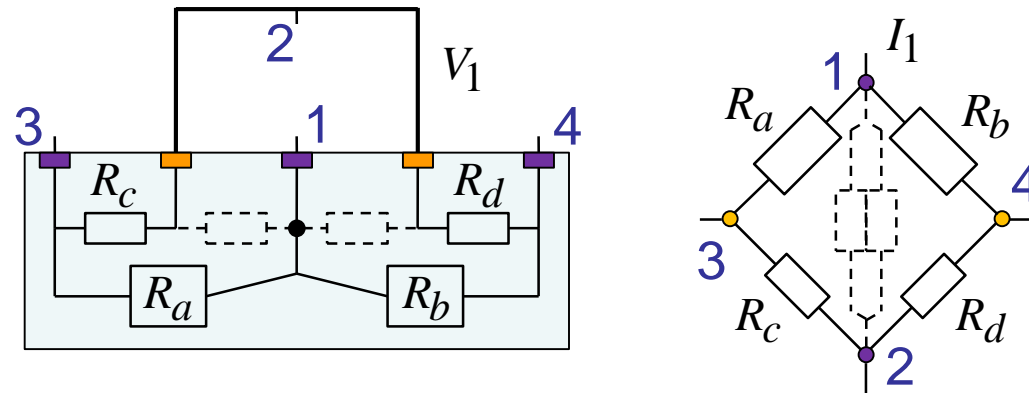
-----→ V_{out}



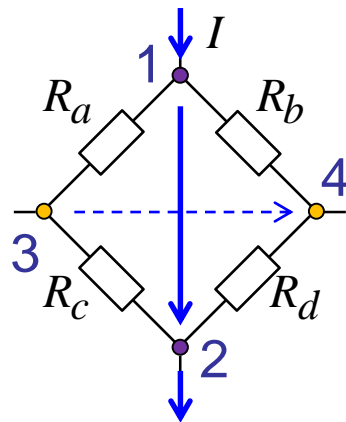
$$V_{out2} = V_H - V_{off} - V_{1/f} - V_{PHE}$$



➔ You need to make the 5-contact LV-VHD a 4-contact sensor



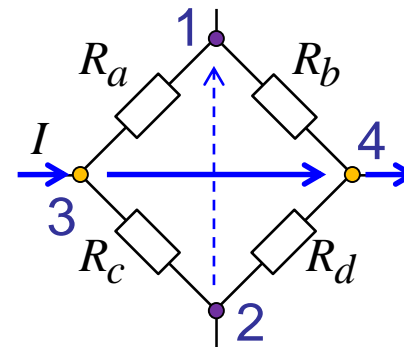
... and to exchange the biasing and sensing contacts periodically



Phi1

$$V_1 = V_{off}$$

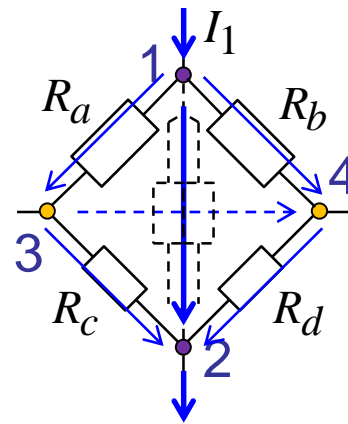
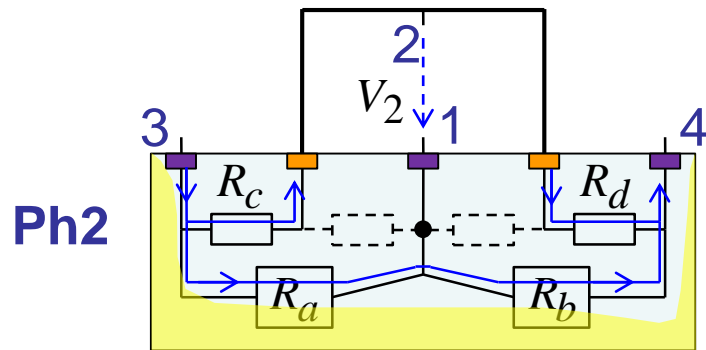
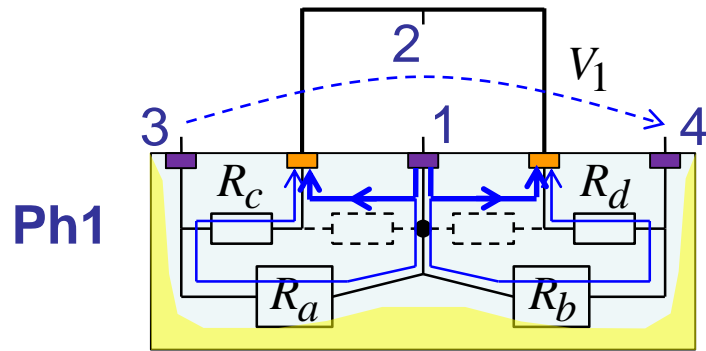
$$= \frac{R_a \cdot R_d - R_b \cdot R_c}{R_a + R_b + R_c + R_d} \cdot I$$



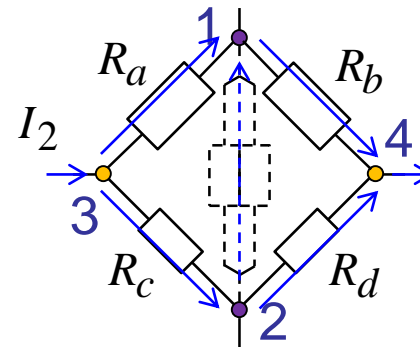
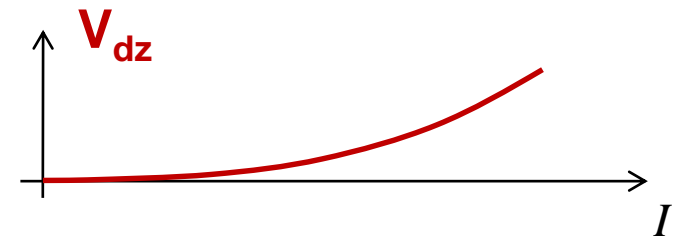
Phi2

$$V_2 = -V_{off}$$

$$= \frac{R_b \cdot R_c - R_a \cdot R_d}{R_a + R_b + R_c + R_d} \cdot I$$

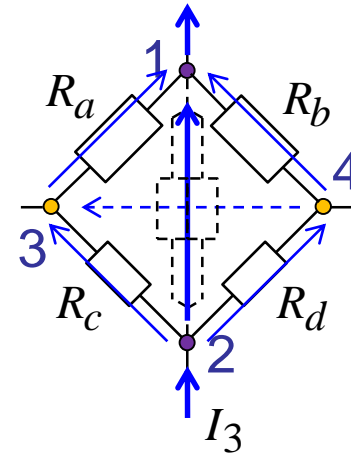
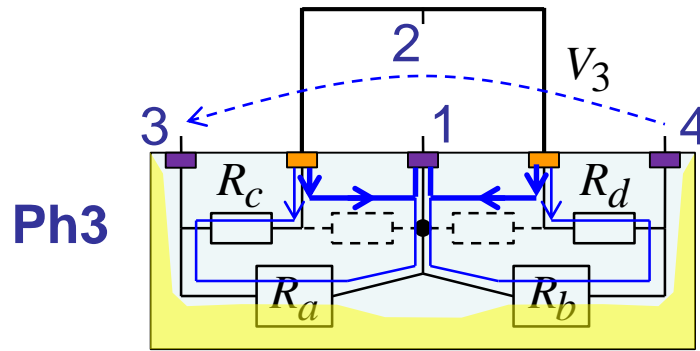


$V_{off} + 0$

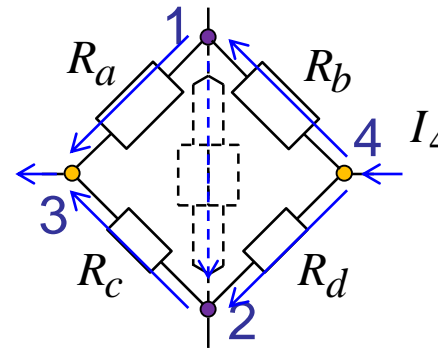
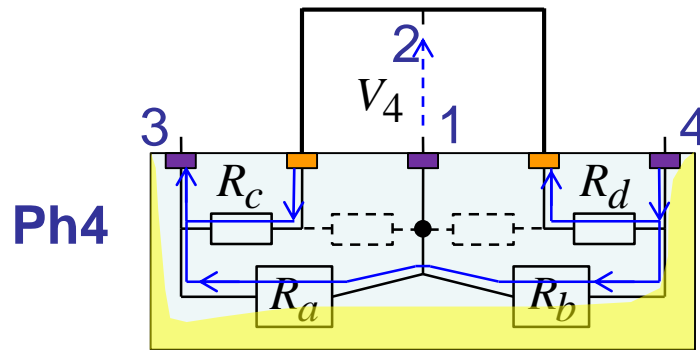


$-V_{off} + V_{dz}$

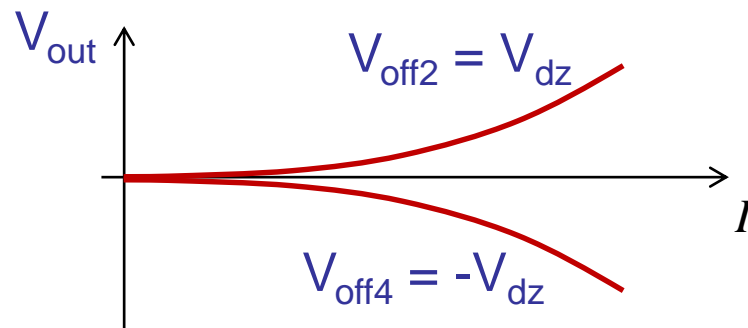
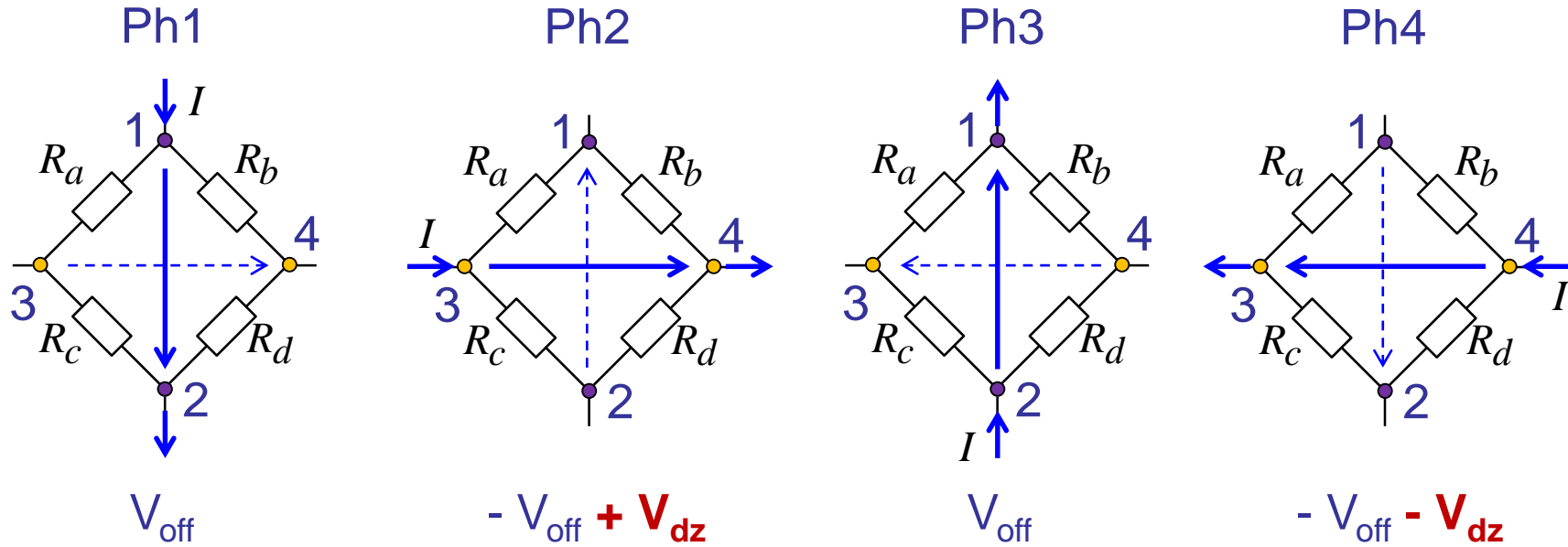
$$I_{1max} > I_{2max} \Rightarrow I = I_1 = I_{2max}$$



$V_{\text{off}} + 0$



$-V_{\text{off}} - V_{\text{dz}}$



We need a 4-Ph Spinning-current in VHD to remove the offset

$$I_{1\max} = I_{3\max} > I_{2\max} = I_{4\max} \quad \Rightarrow \quad I_B \text{ (conventional SC)} = I_{2\max}$$

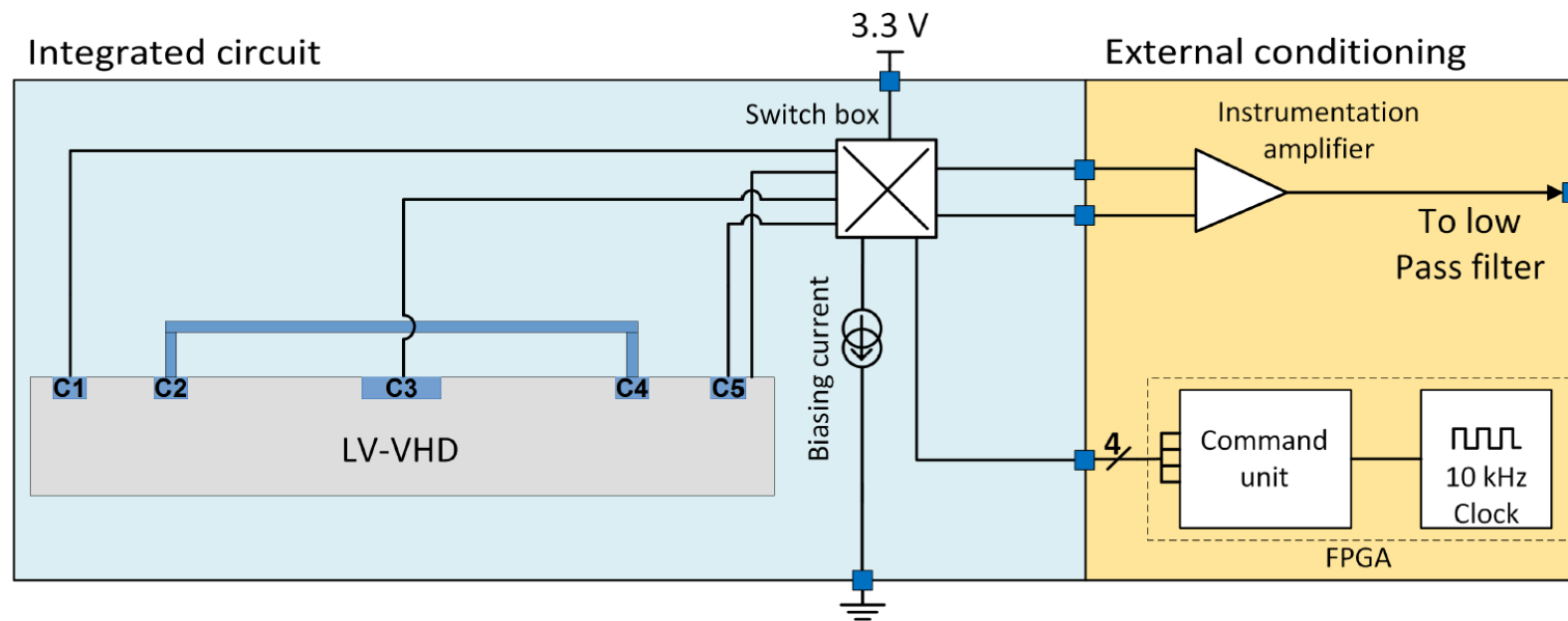
However, offset, $1/f$ noise and PHE are proportional to I_B !

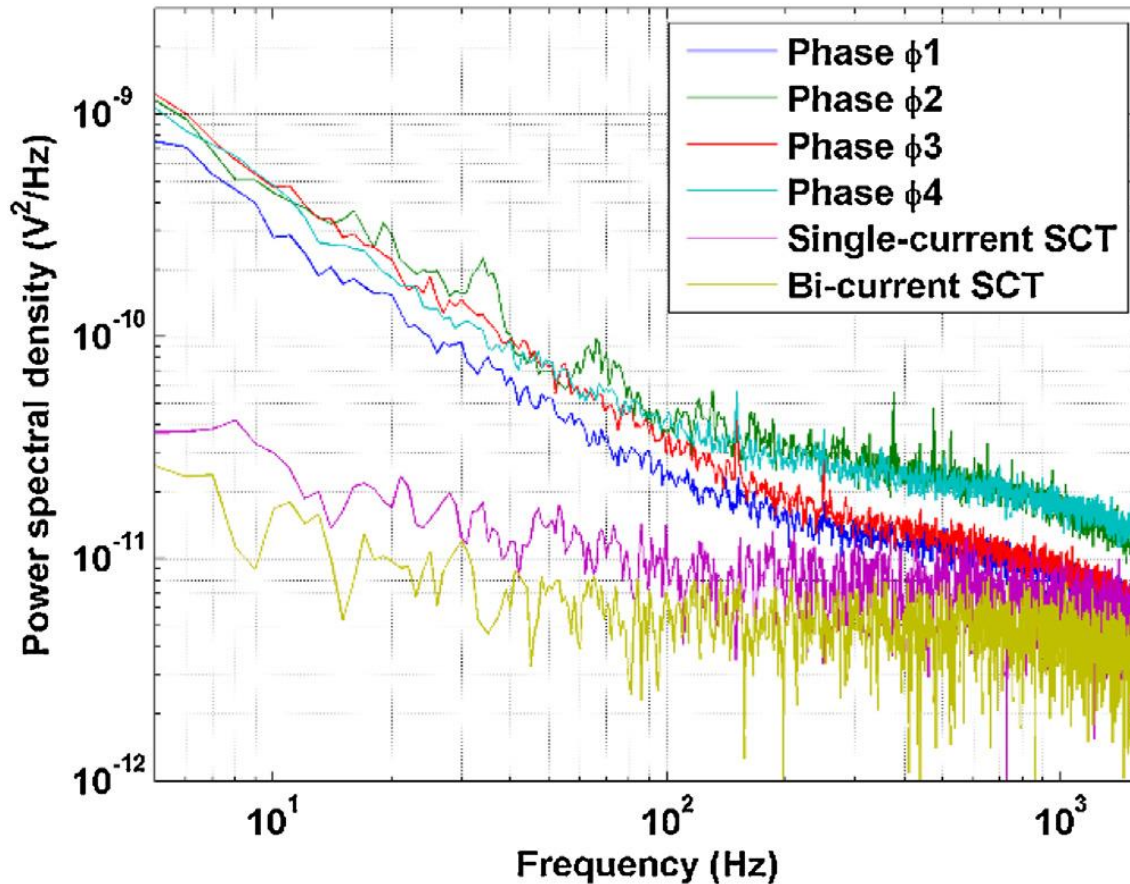
Using the maximum current on each phase $\Rightarrow V_{off1} = -\frac{I_{1\max}}{I_{2\max}} \cdot V_{off2}$

4-phase bi-current Spinning-current

- ⇒ { Maximum current on each phase
- Amplify V_2 and V_4 by $I_{1\max}/I_{2\max}$
- Take the average

3 μm wide, 25 μm long and 2 μm deep
LV-VHD with external SC conditioning





$$I_{1\max} = 1100 \mu\text{A}$$

$$I_{2\max} = 550 \mu\text{A}$$

Over 1.6 kHz bandwidth

$$R(1-I_B \text{ SC}) = 64 \mu\text{T}$$

$$R(2-I_B \text{ SC}) = 51 \mu\text{T}$$

**51 μT with an average
 I_B of 825 μA**

Better results expected with Bi-current 4-Phase spinning-current **integrated on chip**

Most commercial Hall Devices are 1D HD switches, or 1D HDD for B measurement

A few 3D magnetometers are available commercially :

ST : LSM303D → based on AMR and a multi-chips package (with a 3D accelerometer)

2009

Melexis : MLX 90393 → based on HDD with Integrated Magnetic Concentrators (*Sentron acquired by Melexis on 2004*)

2005

Metrolab : MagVector MV2 → based on a HDD and two HV-VHD (*from Sensima founded in 2008 and delivered by Metrolab*)

2015

Allegro : ALS31300 → 3D Hall (3x3x0.8mm³ DFN pack. $\pm 200\text{mT}/100\mu\text{T}$)

2017

AKM : AK09970N → 3D Hall (3x3x0.75mm³ QFN pack. $\pm 36\text{mT}/3\mu\text{T}$)

2017



Advantages of MRI scanner :

- High tissue contrast
- Free imaging plane positioning
- No ionising radiation



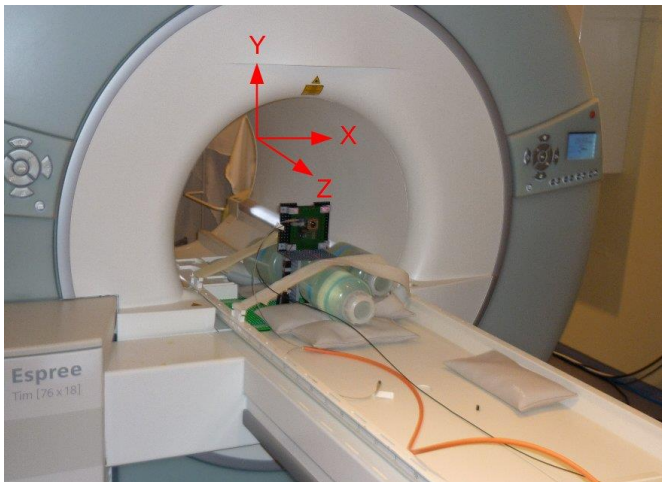
MRI for minimally-invasive surgery



Need for fast tracking systems for MRI scanner

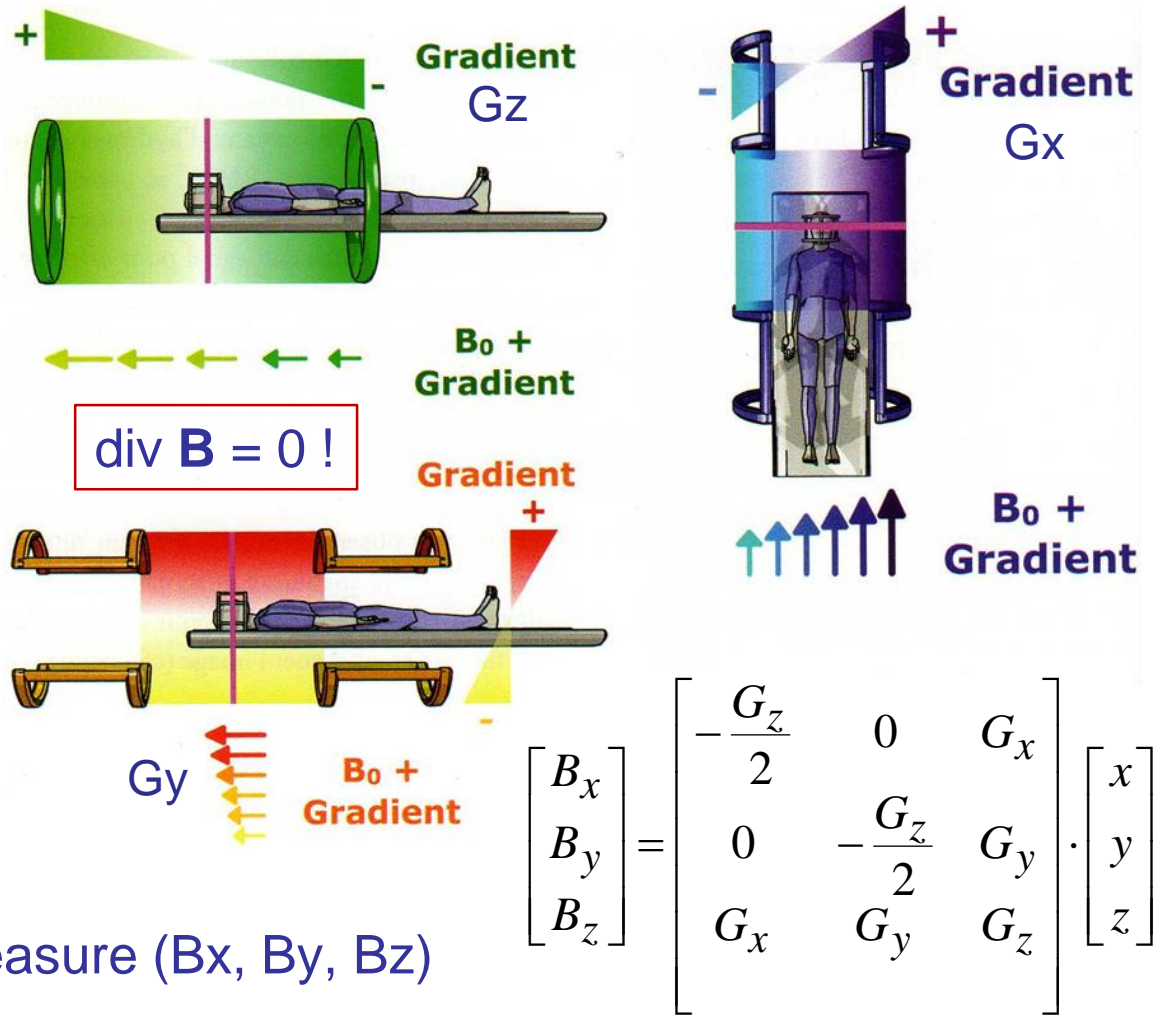


Magnetic localization device

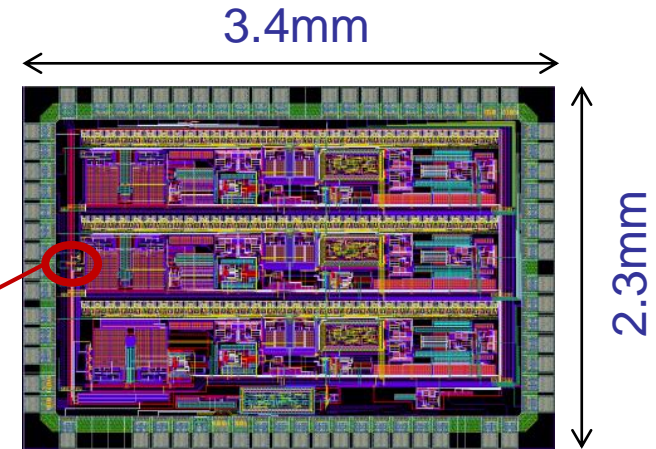
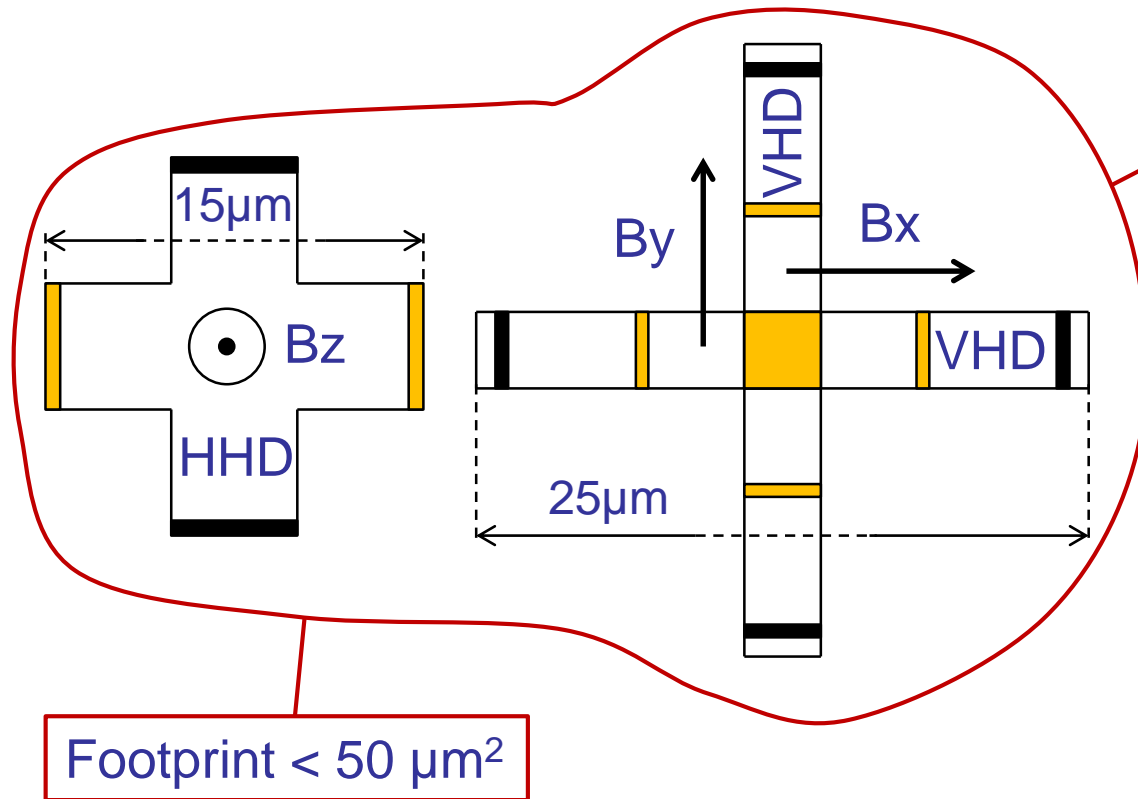


(G_x, G_y, G_z) stand for a space graduation.

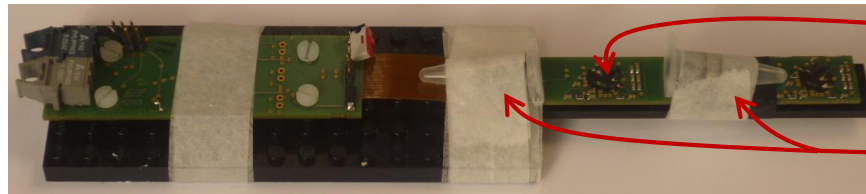
↳ 3D Hall probe to measure (B_x, B_y, B_z)



J.-B. Schell, and al., « Hall effect magnetic tracking device for Magnetic Resonance Imaging », *IEEE Sensors Conference, Baltimore, Maryland-USA, Nov. 4-6, 2013, pp. 1382-1385*



- 0.35 μm AMS LV-CMOS
- B_0 removing
- B_x , B_y , B_z measured in 1ms
- 1.5T or 3T MRI scanner



Used 3D Hall probe

Markers with gadolinium + a coil

Spoiled gradient echo sequence

780ms for one image

4.1ms /line + 1ms G pulse : G0
Gx
G0
Gy
G0
Gz
⋮ 154 lines ⋮

12 measurements averaged → 367ms

+

240ms for position computation

+

400ms at least for image adjustment by the scanner

↓

Total = 1s

adjustment...





Fluxgate → the best resolution, but macroscopic device (a few cm³)

Micro-fluxgate → in the future ?

Magnetoresistances : a few nT to a few mT, resolution around 1 nT

Magnetoresistance are CMOS compatible, but multi-chip design remain the state-of-the art

Hall devices remain the state-of-the-art magnetometer for co-integration on CMOS

3D magnetometers now available in LV as well as HV-CMOS

Hall effect in silicon → a few μT to tens of Tesla

Hall device resolution : a few μT over a few kHz of BW

~ 10pT

~ 10nT

~ 10μT



New applications expected with 3D Hall devices



Thanks to my colleagues

J.-B. Schell, J. Pascal,

V. Frick, J.-B. Kammerer, M. Madec

Thanks for your attention