

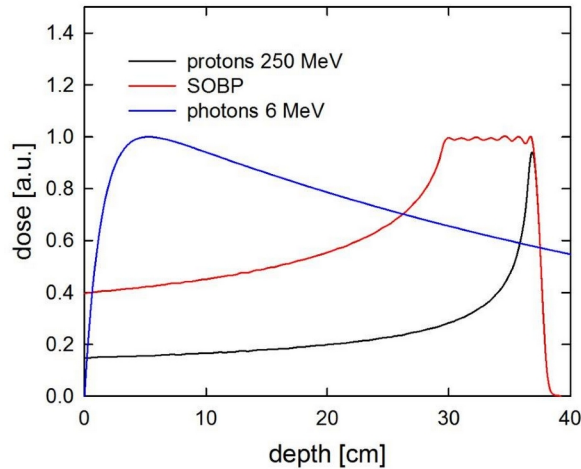


J-PET for range monitoring in proton therapy: a feasibility study using GATE

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And on behalf of the J-PET collaboration

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PET for range monitoring in proton therapy

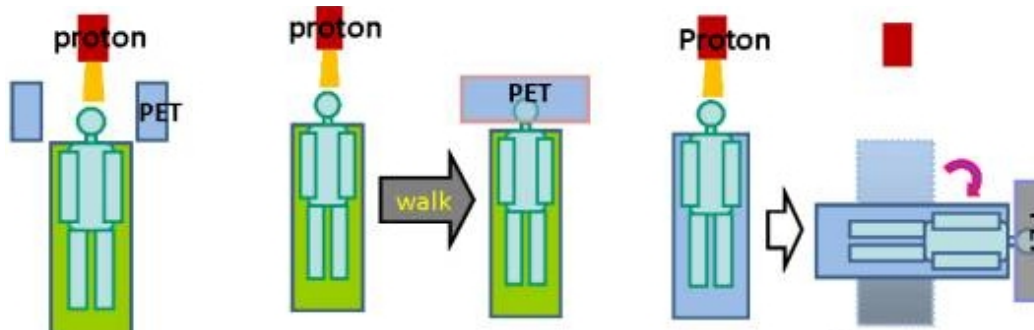


Protons therapy:

- Less dose to normal tissue
 - Tumor dose escalation
 - Organ at risk (OAR) dose reduction
- More sensitive to deviations
 - Ion range uncertainties
 - Day-to-day variations in patient position
 - Anatomical changes in the patient
- *In vivo* range verification
 - Positron emission tomography (PET)

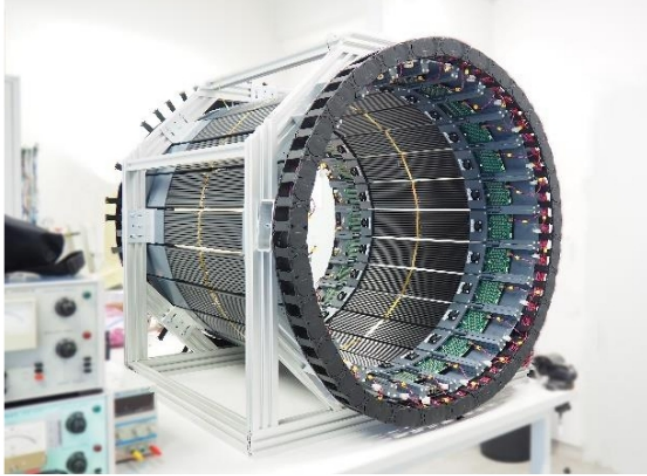
Main PET nuclei produced in patient tissue by the proton beam

nucleus	$T_{1/2}$	$E_{\max}^{\beta}$ (MeV)	reaction
^{15}O	2.04 min	1.73	$^{16}\text{O}(p,pn)^{15}\text{O}$
^{14}O	70.6 sec	1.8	$^{16}\text{O}(p,p2n)^{14}\text{O}$
^{13}N	9.97 min	1.2	$^{16}\text{O}(p,\alpha)^{13}\text{N}$
			$^{16}\text{O}(p,2p2n)^{13}\text{N}$
			$^{14}\text{N}(p,pn)^{13}\text{N}$
^{11}C	20.4 min	0.96	$^{12}\text{C}(p,pn)^{11}\text{C}$
			$^{14}\text{N}(p,\alpha)^{11}\text{C}$
			$^{14}\text{N}(p,2p2n)^{11}\text{C}$
			$^{16}\text{O}(p,\alpha pn)^{11}\text{C}$
			$^{16}\text{O}(p,3p3n)^{11}\text{C}$
^{10}C	19.3 sec	1.9	$^{12}\text{C}(p,p2n)^{10}\text{C}$
^{30}P	2.5 min	3.21	$^{31}\text{P}(p,pn)^{30}\text{P}$
^{38g}K	7.64 min	2.72	$^{40}\text{Ca}(p,2pn)^{38g}\text{K}$



J-PET for range monitoring in proton therapy

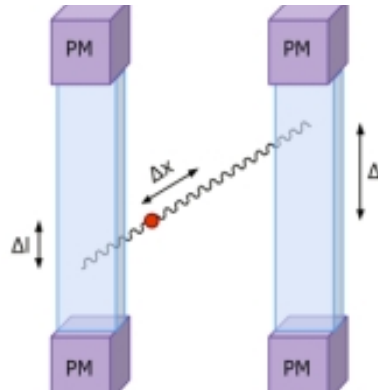
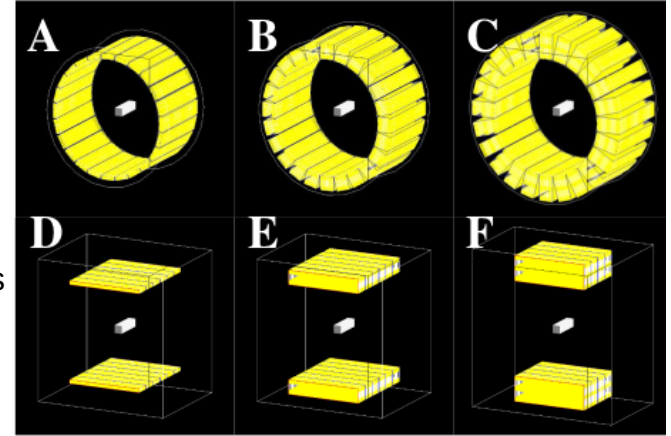
PET based on plastic scintillators



- Cheap, light, portable, easy to reconfigure
- 24 modules
- Each with 13 single plastic strips ($5 \times 24 \times 500 \text{ mm}^3$)
- Compton instead of photoelectric absorption



- A. Single layer barrel – 24 modules
B. Double layer barrel – 48 modules
C. Triple layer barrel – 72 modules
D. Single layer dual-head – 12 modules
E. Double layer dual-head – 24 modules
F. Triple layer dual-head – 24 modules

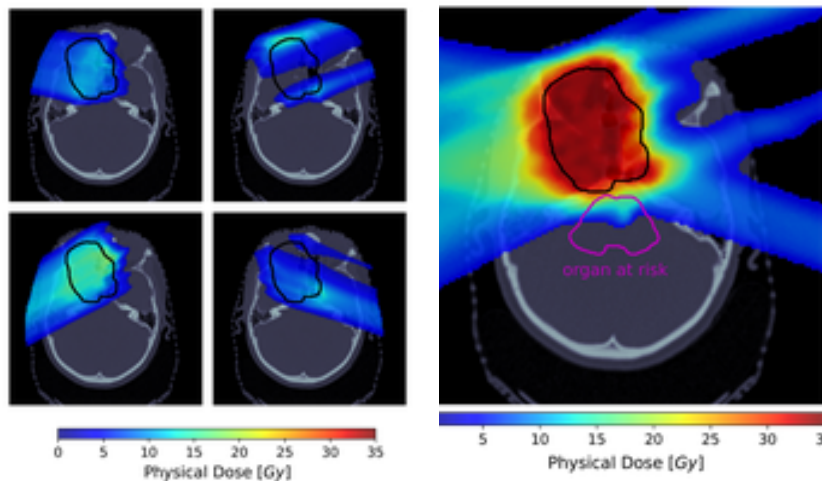
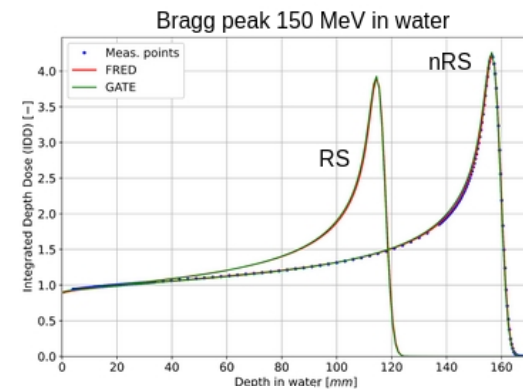
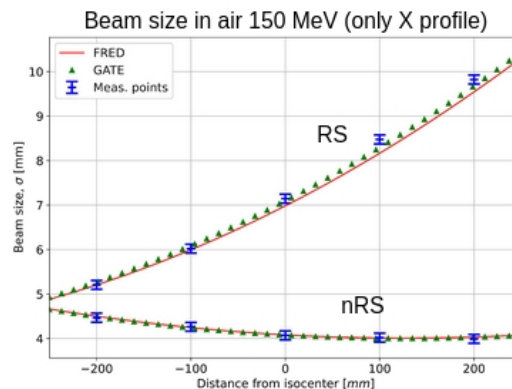


TOF for z position in strip



Patient data and beam model from CCB proton facility

- Validated beam model in GATE
- Patient database with a range tumor sites and volumes
 - 95 head & neck + brain patients treated at CCB with IMPT
 - 2 - 6 fields per patient
 - Target volumes: 10-1000 cm³
 - From 300 to 12000 pencil beams per field
 - From 2E9 to 7.5E10 primary protons per field
 - Treatment plans
 - CT 3D images



2-stage GATE simulations using patient data

1st stage

Patient irradiation and β^+ production

- ^{15}O , ^{14}O , ^{10}C , ^{11}C , ^{30}P , ^{13}N , ^{38}gK
- Treatment plans (multiple fields)
- Phantom from CT
 - Cropped & rebinned to 2.5mm
 - HU to material definitions
- Introduce shifts of HU ($\pm 2\%$) and patient position ($\pm 2,4$ mm) in x, y, z
- Output: production maps of positron-emitting isotopes

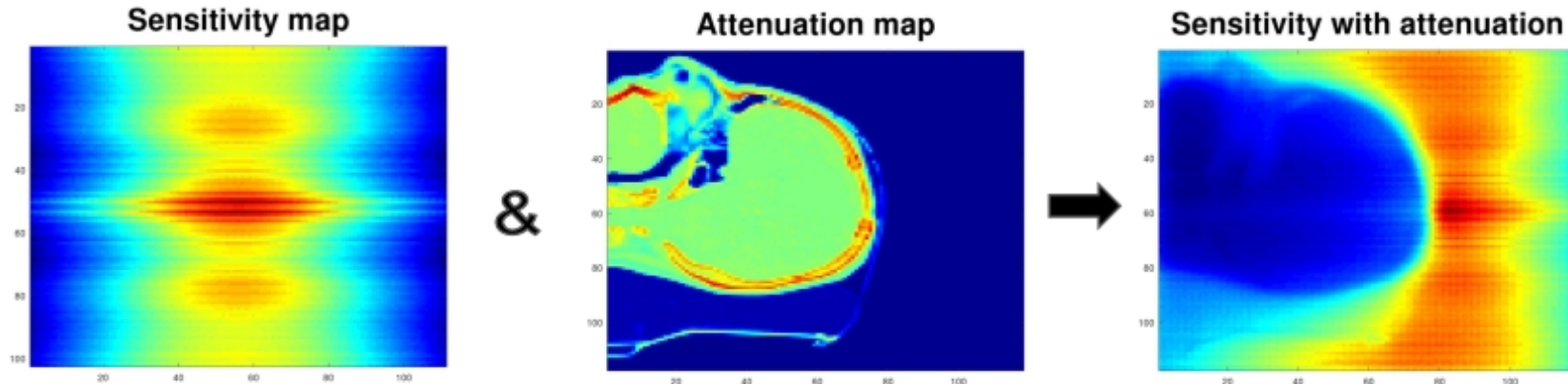
2nd stage

PET acquisition

- J-PET geometries
- Phantom from CT
- Treatment isocentre z-component to scanner axial centre
- Activity source calculated from production maps of positron-emitting isotopes
- Positron energy spectra defined for each isotope

Image reconstruction

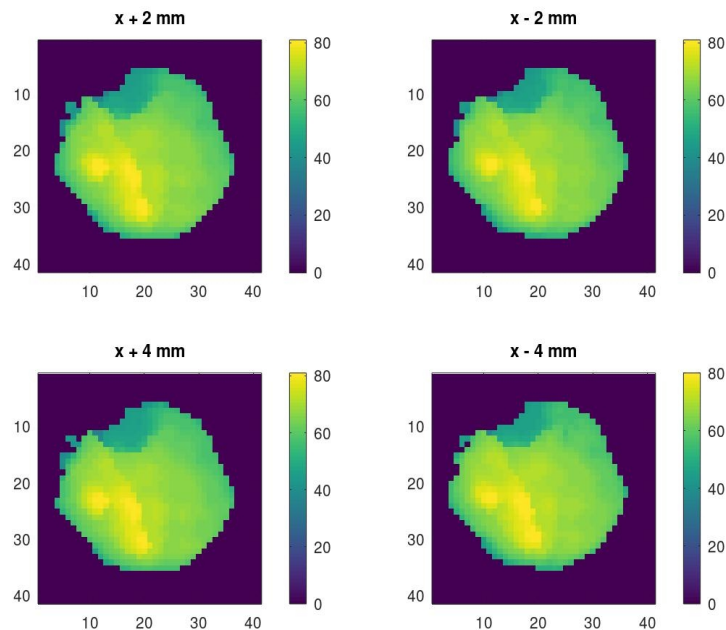
- Iterative methods implemented in CASToR
- Sensitivity map with patient attenuation included
 1. Simulation of homogeneous activity filling the PET FOV
 2. Calculation of attenuation map from CT and position at z-isocentre
 3. Backprojection of acquired coincidence data through attenuation map
- Post-reconstruction smoothing (Gaussian with sigma = 1 voxel)
- Stopping criteria: Iteration minimizing NRMSD with emission map



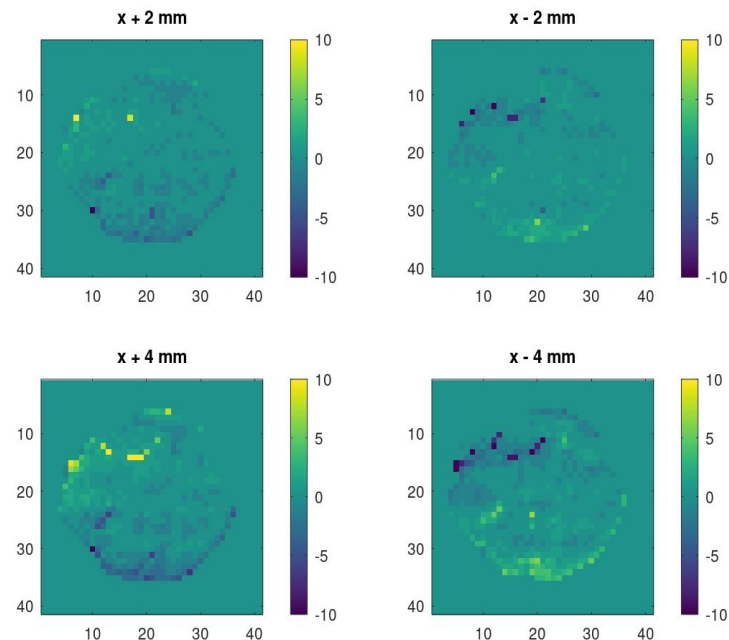
Range measurements

Difficult due to activity from overlapping fields → concentrate on last field

- Compare beam's-eye-view 2D maps of range shifts in **dose** and **PET activity** distributions (PET images). Is a shift in **dose** reflected the **PET images**?



Dose range map in BEV (at 70-80% of max)



Dose range shift map in BEV

Implementation

- Workflow is scripted automatized
- Run split Gate simulation using SLURM queue system
- Computer cluster “Ziemowit” (Silesian Univ. of Technology, Gliwice)
www.ziemowit.hpc.polsl.pl
 - 80 ibm nodes (12cores/node, min. 36GB RAM) - old CPU (intel x5650) - in total 960 cores
 - 28 quanta nodes (20cores/node, 256GB RAM) - newer CPU (intel E5-2660v3) - in total 560 cores
- 1st stage simulations
 - Ibm node performance : ~ 355 Primary per sec (PPS)
 - Quanta node performance : ~650 PPS (no HT)
 - One field from one patient takes several hours (quite slow)
 - May transition to FRED

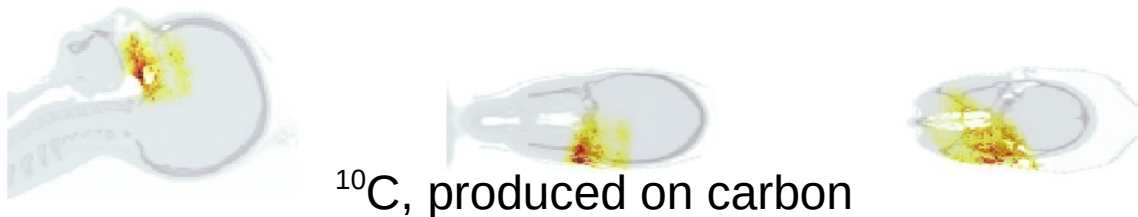


Acknowledgments

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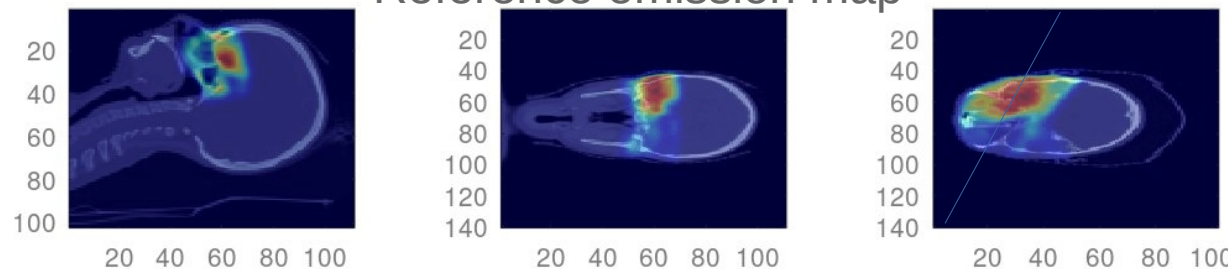
^{15}O , produced on oxygen ^{30}P , produced on phosphorus ^{10}C , produced on carbon

Stacked bar chart showing the number of β^+ emissions during a 120 s scan for three different times before the scan: 0, 60, and 120 seconds. The y-axis represents the number of β^+ emissions, ranging from 0 to 8×10^7 . The x-axis represents the time before the scan in seconds. The legend identifies the isotopes contributing to the emissions: ^{15}O (dark blue), ^{14}O (blue), ^{10}C (cyan), ^{11}C (light green), ^{30}P (yellow), ^{13}N (red), and ^{38}K (dark red).

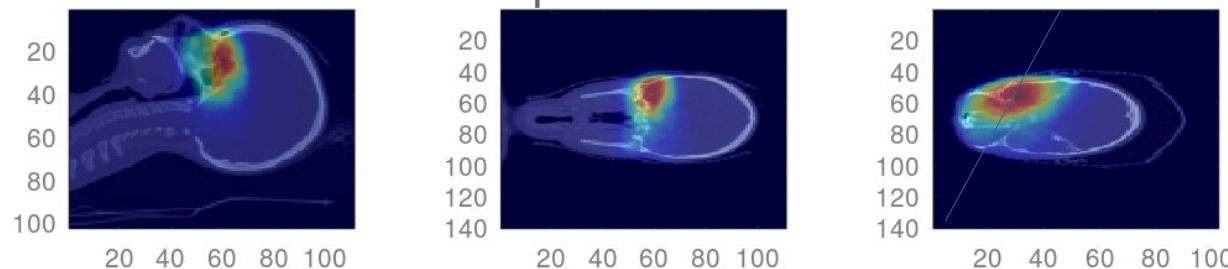
Time before scan (s)	^{15}O	^{14}O	^{10}C	^{11}C	^{30}P	^{13}N	^{38}K
0	$\approx 6.0 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.5 \times 10^7$
60	$\approx 4.2 \times 10^7$	$\approx 0.3 \times 10^7$	$\approx 0.1 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.3 \times 10^7$	$\approx 0.3 \times 10^7$	$\approx 0.3 \times 10^7$
120	$\approx 3.1 \times 10^7$	$\approx 0.2 \times 10^7$	$\approx 0.1 \times 10^7$	$\approx 0.5 \times 10^7$	$\approx 0.2 \times 10^7$	$\approx 0.3 \times 10^7$	$\approx 0.2 \times 10^7$

Preliminary results for HU variation

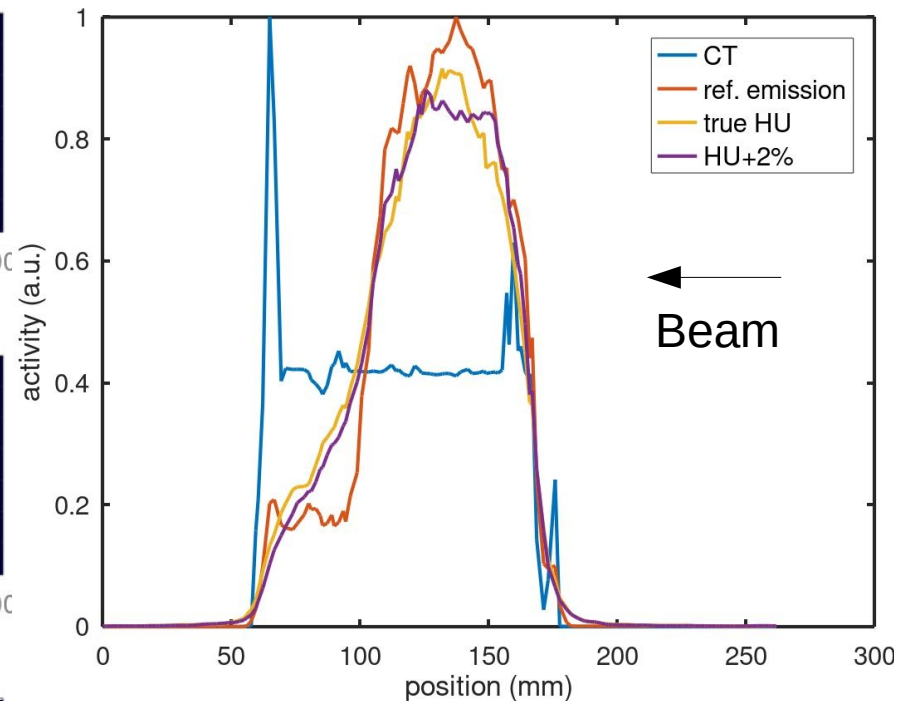
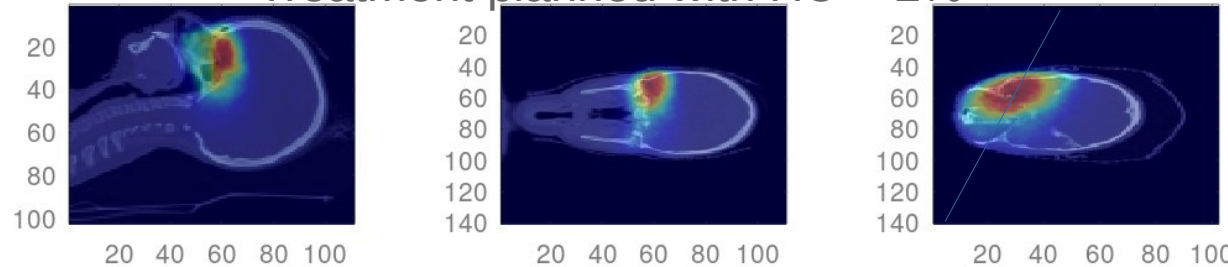
Reference emission map



Treatment planned with true HU



Treatment planned with HU - 2%



Next step: Quantify range shift over all patients, protocols and shifts