

# Monte Carlo track structure simulations and the biophysical model NanOx in targeted radionuclide therapy

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# TRT with Auger electron and $\alpha$ -particle emitters

- TRT using Auger electrons (AEs) and  $\alpha$ -particles has generated much interest in the last decades
- AEs and  $\alpha$ -particles are high linear energy transfer (LET) radiations able to deliver cytotoxic radiation doses to tumors while sparing the healthy tissue, in contrast to  $\beta^-$ -particles and X-rays
- Computer simulations may be used for pre-clinical dosimetry of promising AE and  $\alpha$ -particle emitters

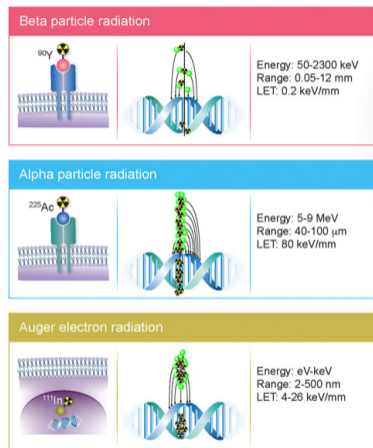


Figure 1: Comparison of radioactive particles for TRT [1]

# The role of Monte Carlo track structure (MCTS) simulations in TRT

- MC codes have a long history in radiation physics and radiation biology ("gold standard")
- Track structure simulations follow radiations on an event-by-event basis
- Very time-consuming, but ideal for subcellular volumes, low-energy radiations and DNA damage studies
- Features make MCTS simulations interesting for accurate radiation dosimetry in TRT

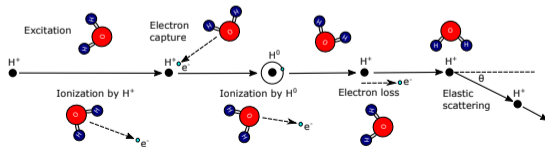


Figure 2: Illustration of the event-by-event approach for protons in water

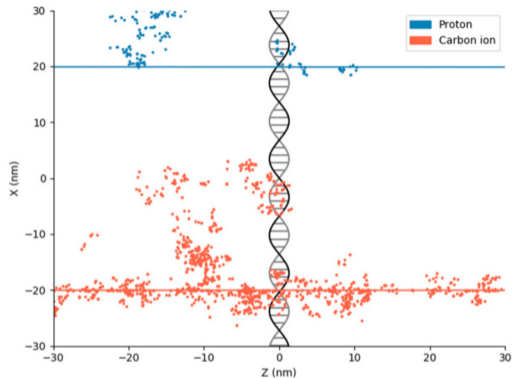


Figure 3: Illustration of the track structure of a 10 MeV proton and 200 MeV carbon ions [2]

# Cellular dosimetry with CELLDOSE

CELLDOSE [3] simulations for evaluating radionuclides for TRT:

- $\beta^-$ -emitters:  $^{90}\text{Y}$ ,  $^{131}\text{I}$ ,  $^{177}\text{Lu}$ ,  $^{161}\text{Tb}$
- **AE-emitters**:  $^{71}\text{Ge}$ ,  $^{103\text{m}}\text{Rh}$ ,  $^{119}\text{Sb}$ ,  $^{125}\text{I}$ ,  $^{161}\text{Ho}$ ,  $^{189\text{m}}\text{Os}$ ,  $^{193\text{m}}\text{Pt}$ ,  $^{195\text{m}}\text{Pt}$
- $\alpha$ -emitters:  $^{211}\text{At}$ ,  $^{212}\text{Pb}/^{212}\text{Bi}$ ,  $^{213}\text{Bi}$ ,  $^{223}\text{Ra}$ ,  $^{225}\text{Ac}$  and  $^{227}\text{Th}$
- Calculation of S-values ( $\text{Gy}\cdot\text{Bq}^{-1}\cdot\text{s}^{-1}$ ) and normalized absorbed doses assuming **cell nucleus** as critical target

- Case of a **single cell** and a **small cell cluster**

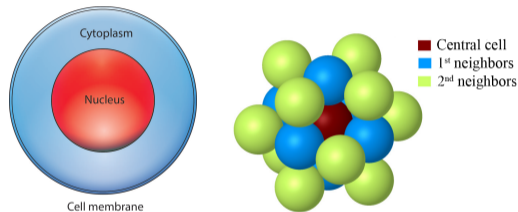


Figure 4: Left: single cell with spherical geometry ( $R_C = 7 \mu\text{m}$ ,  $R_N = 5 \mu\text{m}$ ); right: cell cluster (19 cells)

- **Different radionuclide distributions**: cell surface, intracytoplasmic, intranuclear and whole cell

# Cellular dosimetry with CELLDOSE

## Single cell

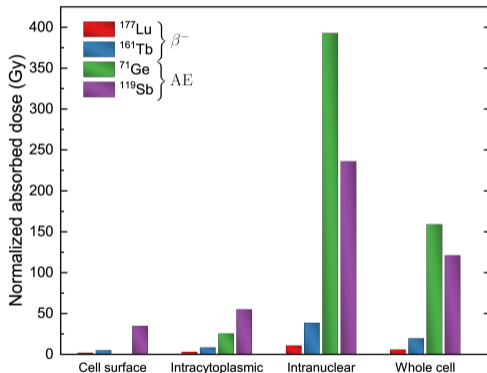


Figure 5: Normalized absorbed doses to the **nucleus of a single cell** for different distributions of selected  $\beta^-$ -particle and AE emitters

## Cell cluster

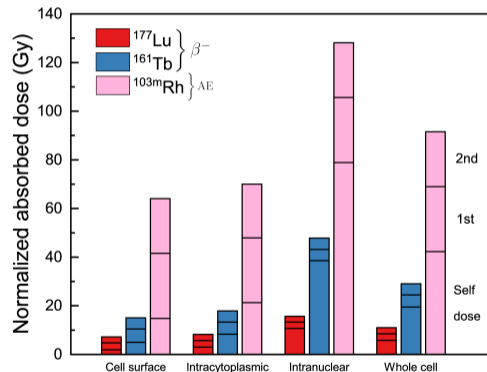


Figure 6: Normalized absorbed doses to the **nucleus of the central cell in a cluster** for different distributions of selected  $\beta^-$ -particle and AE emitters

# Towards more comprehensive approaches

Some limitations in the previous studies include:

- Energy deposition events described exclusively during the physical stage.  
→ Need of accounting for processes occurring in later stages of radiation action (Fig. 7)
- Need of modeling realistic cell geometries and complex multicellular systems

Other simulation tools and biophysical models may be applied for reaching more clinically relevant endpoints, e.g. the **biological dose** for ion irradiations

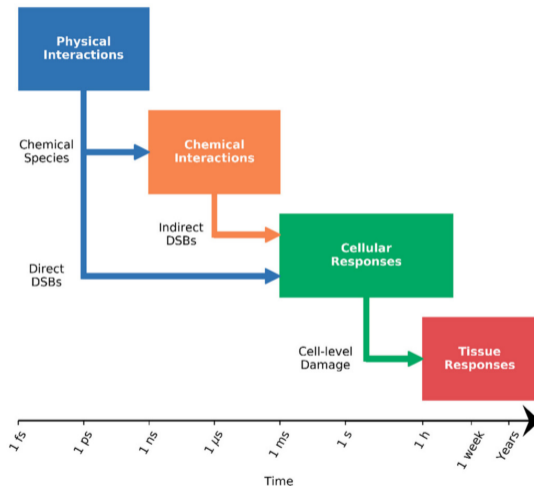


Figure 7: Stages of radiation action [2]

# Planning Innovative Cancer Therapies Using RadioElements

The **PICTURE** project focus on the optimization of dosimetry calculations for targeted alpha therapy (TAT) and boron neutron capture therapy (BNCT), considering:

- **Biological dose** modeling: **NanOx** + Geant4-DNA
- The impact of different **radionuclide distributions** in cells, including heterogeneities
- The role of **nuclear** and **extra-nuclear** sensitive sites in radiation-induced cell death

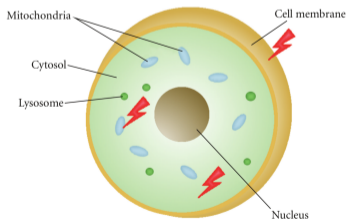


Figure 8: Potentially important extra-nuclear sites in a cell [6]

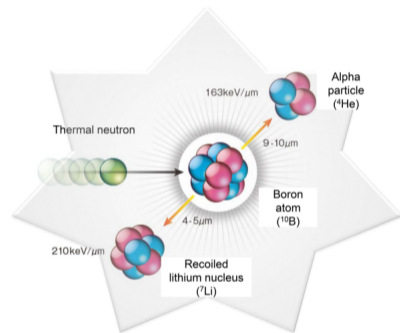


Figure 9: Principle of boron neutron capture therapy (BNCT) [7]

# The PICTURE project

- Creation of a database of **realistic 3D cell geometries** based on confocal microscopy
- Experimental studies with different cell lines (CHO-K1, SQ20B and U87) irradiated in conditions of full (FCT) and partial cell transversal (PCT)

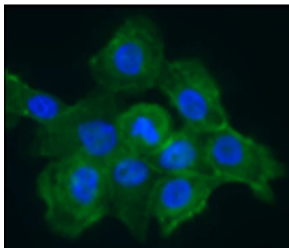


Figure 10: Micrograph of SQ20B cells [8]

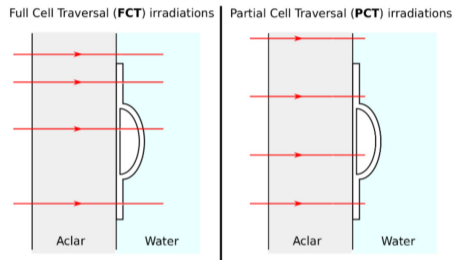


Figure 11: Cell irradiation conditions with broad ion beams



# The NanOx biophysical model

- Prediction of cell survival for ion irradiations
- Considers stochastic nature of radiation at different scales. Two types of biological events: **local lethal events (LLE)** and **global events (GE)**:

**LLE** → inactivation of **nanometric targets**

**GE** → accumulation of sublethal lesions including physico-chemical processes (**micrometric scale**)

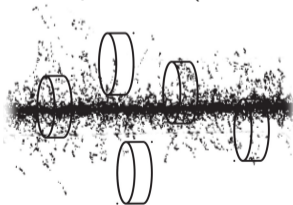


Figure 13: Irradiation of cells by a given radiation impact [9]

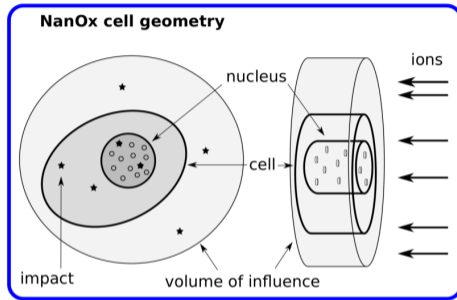


Figure 12: Current cell geometry in NanOx simulations

$$S = S_{LLE} \times S_{GE} \quad (1)$$

# The NanOx biophysical model

- 5 parameters derived from experimental data:
  - **Sensitive volume radius**
  - 3 parameters characterizing the **effective local lethal function**, used for calculating the survival to LLE (Fig. 14)

$$F(z) = \frac{h}{2} \left[ 1 + \operatorname{erf} \left( \frac{z - z_0}{\sigma} \right) \right] \quad (2)$$

- **Quadratic coefficient**  $\beta_r$  for reference (photon) irradiation

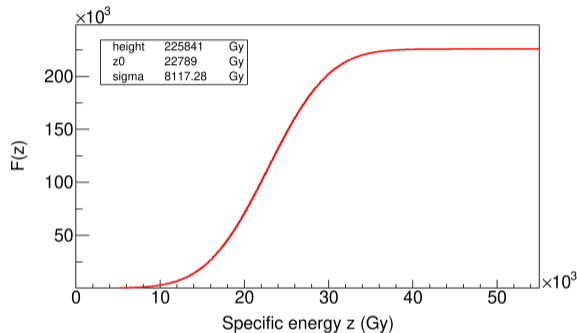


Figure 14: Effective local lethal function for the V79 cell line

# The NanOx biophysical model

- NanOx has been applied to study the radiation response of several cell lines in the context of hadrontherapy [10]
- $\alpha$  and  $\beta$  coefficients can be obtained from a LQ fit to NanOx results (Fig. 16)

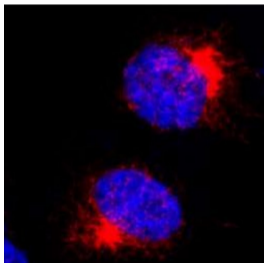


Figure 15: Image of HSG cells [11]

- **NanOx predictions are more accurate than the ones of other biophysical models**

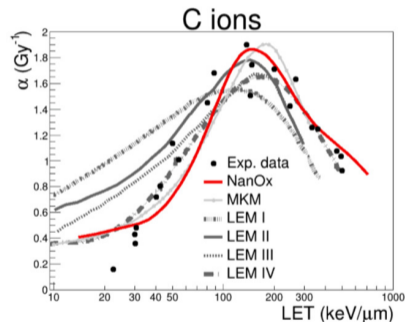


Figure 16:  $\alpha$  values of HSG cells for carbon ions. The graph shows experimental data as well as the predictions of several biophysical models, including NanOx [12]

# Conclusions

- MCTS codes remain the best computational tools for investigating ionizing radiation interactions at the subcellular level, including preclinical studies for TRT
- Current challenges for realistic simulations of TRT treatments include the consideration of complex cell geometries, heterogeneous distributions of radiation sources in the cells and extra-nuclear sensitive sites
- The ongoing PICTURE project is expected to improve the biological dose estimation for innovative radiation therapies, especially TAT and BNCT
- **Need of experimental data regarding the 4D biodistribution of radionuclides with subcellular resolution**

*Thank you for your attention*

*Merci pour votre attention*

# References

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# Appendix: Physical properties of some $\beta^-$ -emitters

Radionuclide	$^{131}\text{I}$	$^{90}\text{Y}$	$^{177}\text{Lu}$	$^{161}\text{Tb}$
Half-life (day)	8.02	2.67	6.647	6.906
$\beta^-$ -particles mean energy (keV)	182	932.9	133.3	154.3
Daughter nucleus	$^{131}\text{Xe}$ (stable)	$^{90}\text{Zr}$ (stable)	$^{177}\text{Hf}$ (stable)	$^{161}\text{Dy}$ (stable)
CE (intensity per decay)	6.46%	0.01%	15.47%	142%
CE (energy per decay in keV)	9.57	0.2	13.52	39.28
CE energy range in keV <sup>†</sup>	45.6 – 602.4	1742.7	6.2 – 206.3	3.3 – 98.3
AE (intensity per decay)	69.75%	0.13%	111.65%	1096.4%
AE (energy per decay in keV)	0.41	0.0007	1.13	8.94
AE energy range in keV	0.026 – 32.9	0.022 – 1.8	0.01 – 61.7	0.018 – 50.9
Total electron energy per decay (keV)	191.8	933.1	147.9	202.5
$\gamma$ or X-ray radiation useful for imaging (energy in keV and % abundance)*	364.5 (81.7%)			
	330 (1.6%)	–	208 (11%)	75 (10.2%)
	284.3 (6.1%)		113 (6.4%)	
	80.2 (2.6%)			
Photons (energy per decay in keV)	382.7	–	35.1	36.35
Total energy per decay in keV (photons + electrons)	574.5	933.1	183	238.9
% of energy emitted as electrons	33.4%	~100%	80.8%	84.8%
% of energy emitted as photons	66.6%	~0%	19.2%	15.2%

# Appendix: Physical properties of some AE-emitters

Radionuclide	<sup>71</sup> Ge	<sup>103m</sup> Rh	<sup>119</sup> Sb	<sup>125</sup> I
Half-life (day)	11.43	0.039	1.591	59.4
Type of decay (%)	EC (100%)	IT (100%)	EC (100%)	EC (100%)
Daughter nucleus	<sup>71</sup> Ga (stable)	<sup>103</sup> Rh (stable)	<sup>119</sup> Sn (stable)	<sup>125</sup> Te (stable)
CE (intensity per decay)	–	99.06%	83.97%	94.47%
CE (energy per decay in keV)	–	34.97	16.97	7.28
CE energy range in keV <sup>†</sup>	–	16.56 – 39.76	19.4 – 23.9	3.7 – 35.5
AE (intensity per decay)	520.5%	587.94%	2368%	2300%
AE (energy per decay in keV)	5.01	2.72	8.86	11.96
AE energy range in keV	0.012 – 10.1	0.034 – 22.28	0.011 – 27.9	0.023 – 30.3
Total electron energy per decay (keV)	5.01	37.69	25.83	19.24
γ or X-ray radiation useful for imaging (energy in keV and % abundance)*	–	–	–	–
Photons (energy per decay in keV)	4.07	1.65	23.14	42.5
Total energy per decay in keV (photons + electrons)	9.08	39.34	48.97	61.74
% of energy emitted as electrons	55.2%	95.8%	52.8%	31.2%
% of energy emitted as photons	44.8%	4.2%	47.2%	68.8%
photon-to-electron energy ratio (p/e)	0.81	0.04	0.90	2.21