

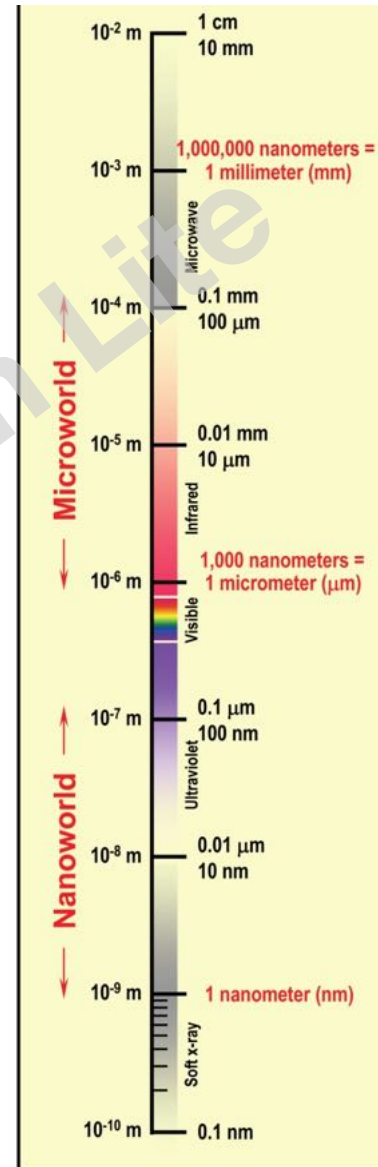
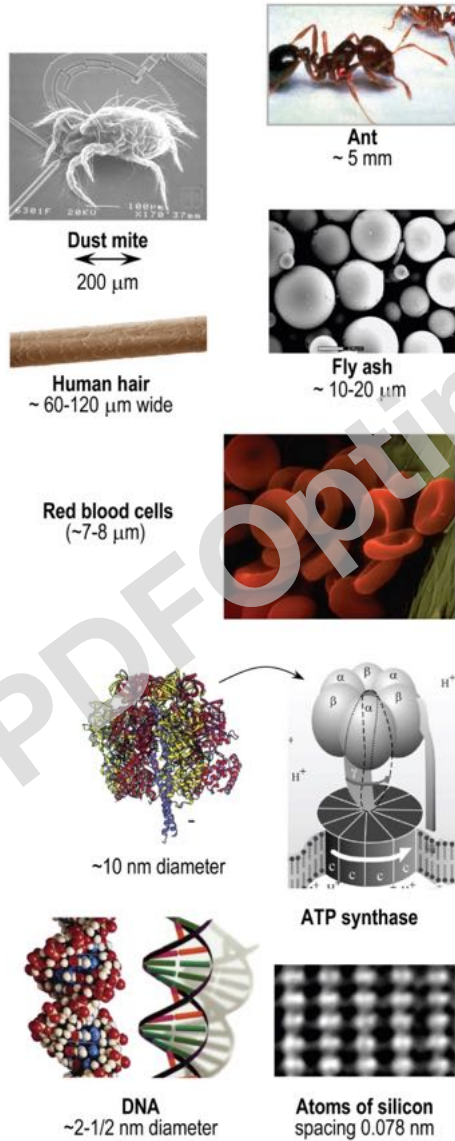
# New Microscopies:

*Single molecules Imaging & Superresolution microscopies*

Brahim Lounis  
*Institut d'Optique Graduate School  
CNRS, University of Bordeaux  
France*



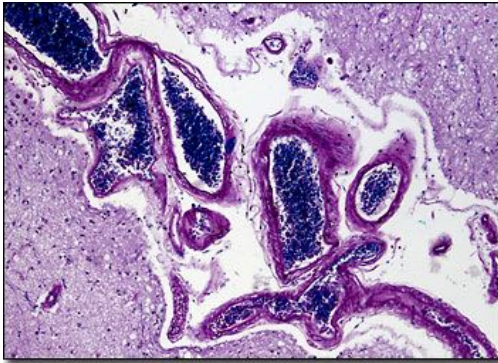
# The scale of things vs radiation wavelengths



# Common modalities of optical microscopy

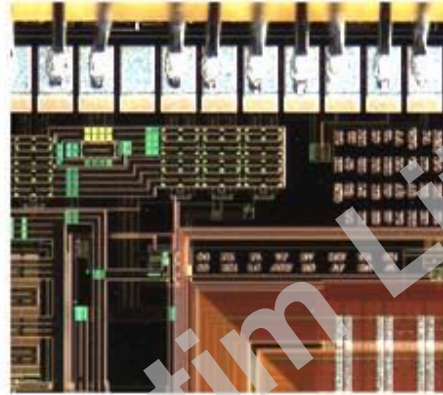
## Bright field microscopy

*Scattering, reflection, absorption*



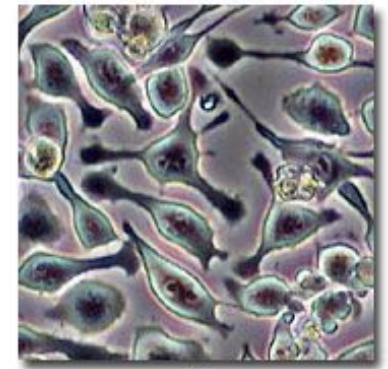
## Dark field

*Scattering*



## Phase contrast

*Phase*

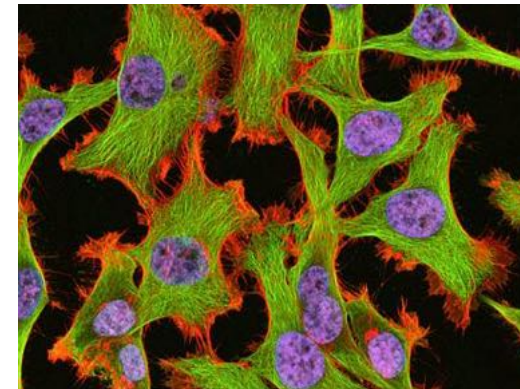


## Differential Interference contrast (Nomarsky) , *Phase gradients*



## Fluorescence microscopy

*Fluorescence*



# Single Molecule detection

## Why?

No ensemble averaging  
(distributions)

- inhomogeneous broadening free Spectroscopy
- Isolate a single quantum system
- Sub-wavelength localization possible
- Extreme sensitivity to local environment
- Time evolution, no synchronization needed

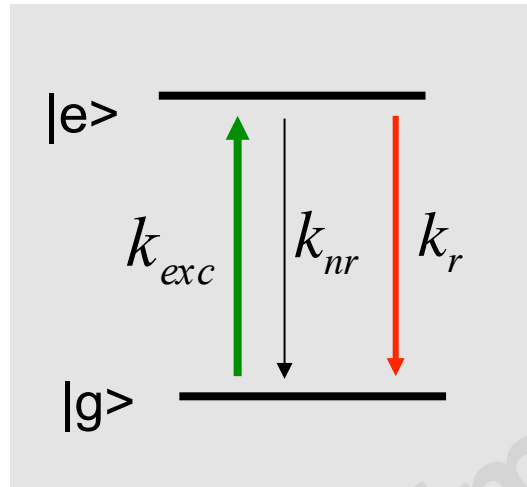
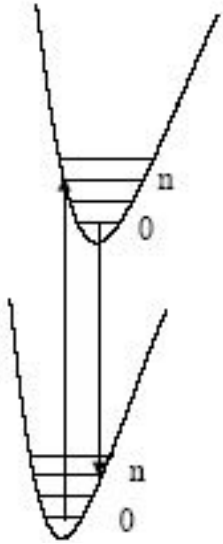
## How?

Far Field Optical Detection Techniques

Make sure that :

- only one nanoobject interacts with the laser in the excitation volume
- the signal from the nanoobject dominate all sources of background

# Fluorescent molecules as a two level system



$k_{exc}$  Excitation rate ( $s^{-1}$ )

$$k_{exc} = \sigma \frac{\lambda}{hc} I$$

$\sigma$ : absorption cross-section

Desexcitation rate ( $s^{-1}$ )

$$k_{des} = k_r + k_{nr}$$

non-radiative decay rate

$$k_{nr}$$

Radiative desexcitation rate

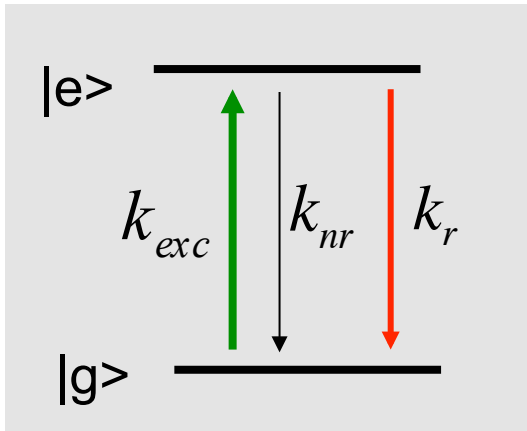
$T_{fluo}$  radiative lifetime

$$k_r = \frac{1}{T_{fluo}}$$

Fluorescence quantum yield

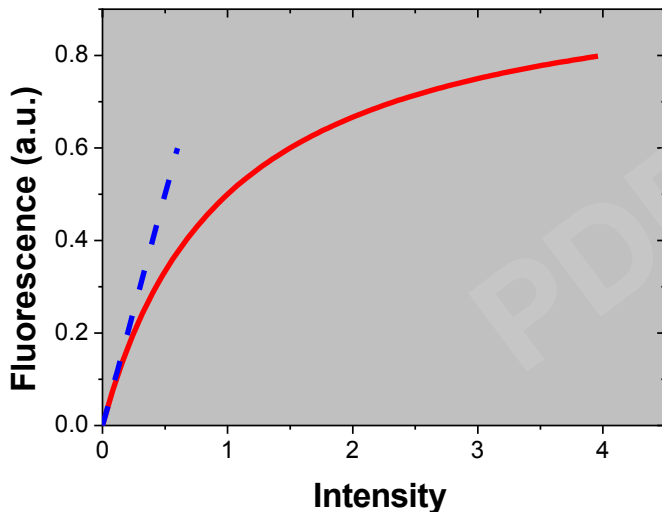
$$\eta = \frac{k_r}{k_r + k_{nr}}$$

# Fluorescence Emission rate



$$R_{fluo} = k_r P_e = \frac{1}{T_{fluo}} \frac{I/I_s}{1 + I/I_s} \text{ (fluorescence rate)}$$

$$I_s = (k_{nr} + k_r) \frac{hc}{\sigma\lambda} \text{ (saturation intensity)}$$



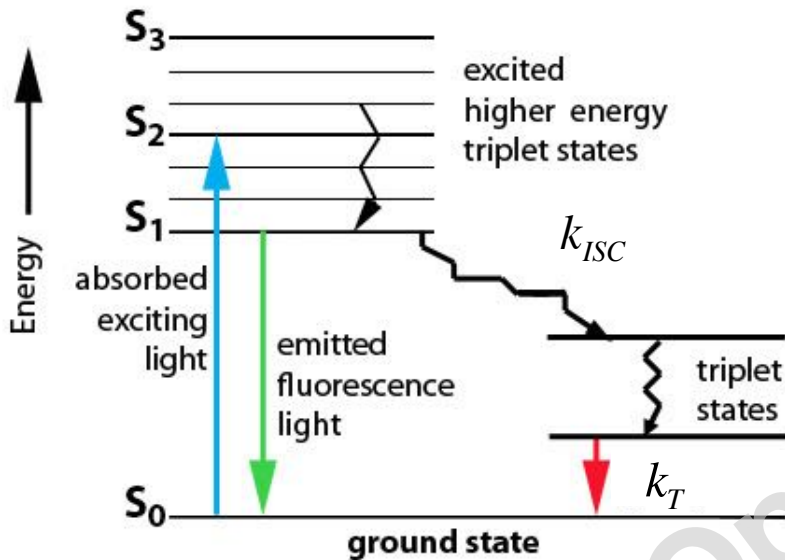
**At low excitation intensity: linear regime**

$$\text{For } I \ll I_s, \quad R_{fluo} \approx \eta \frac{\sigma\lambda}{hc} I$$

**At high intensity: saturation**

$$\text{For } I \gg I_s, \quad R_{fluo}^{\max} = k_r = \frac{1}{T_{fluo}}$$

# A good fluorophore for single molecule detection



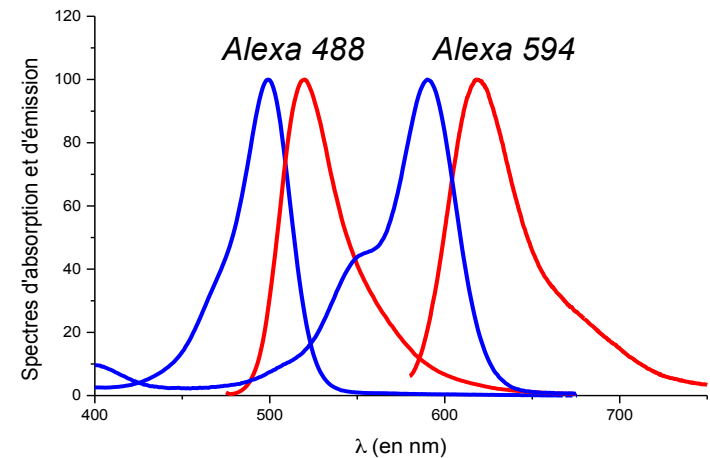
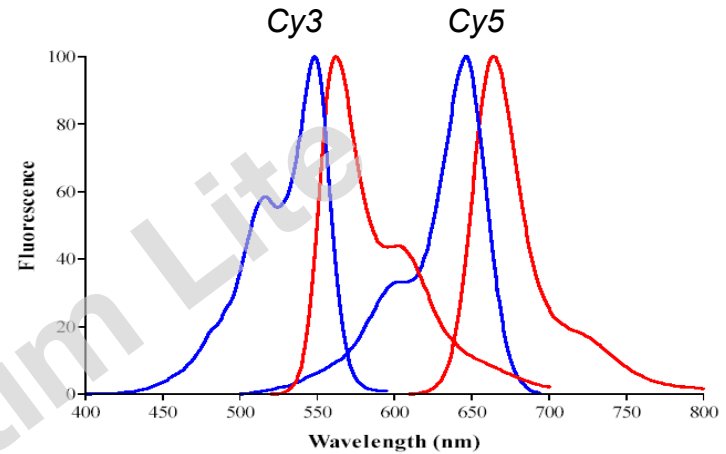
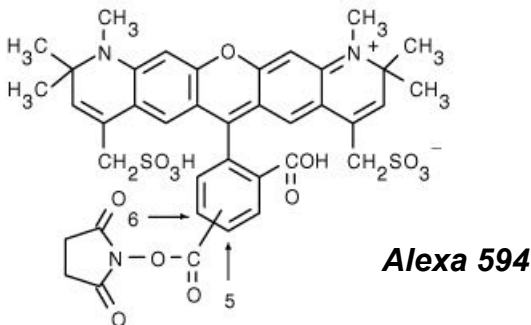
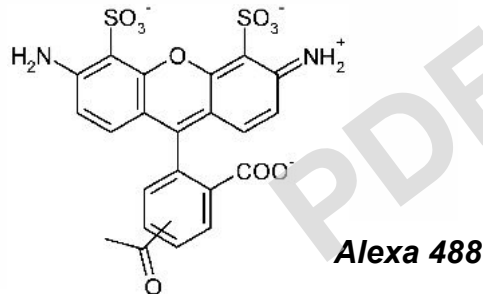
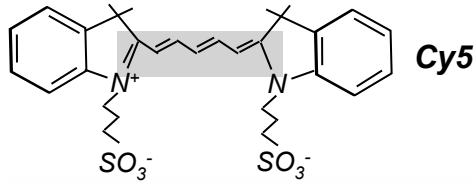
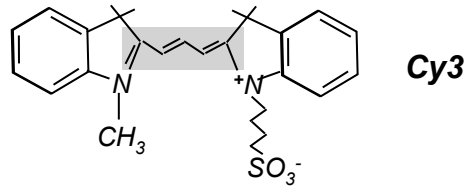
## Triplet State

$$R_{fluo}^{\max} = \frac{1}{T_{fluo}} \frac{1}{1 + k_{ISC}/k_T}$$

- large absorption cross section,  
low excitation intensities, less background  
@ Room T: few  $10^{-16}$   $\text{cm}^2$ , @ Low T:  $\sim 0.1$   $\mu\text{m}^2$
- large quantum yield and short excited state radiative lifetime ( $\sim$ few ns)
- low triplet yield, no bottleneck state
- good photostability (low photobleaching)

# Fluorescence labeling (1)

Dyes chemically attached to the proteins or to a ligand (e.g. nanobody)



Optical spectra given by the length of the double conjugated bounds



# Fluorescence labeling (1)

Fluorescent proteins, genetically fused to the protein of interest

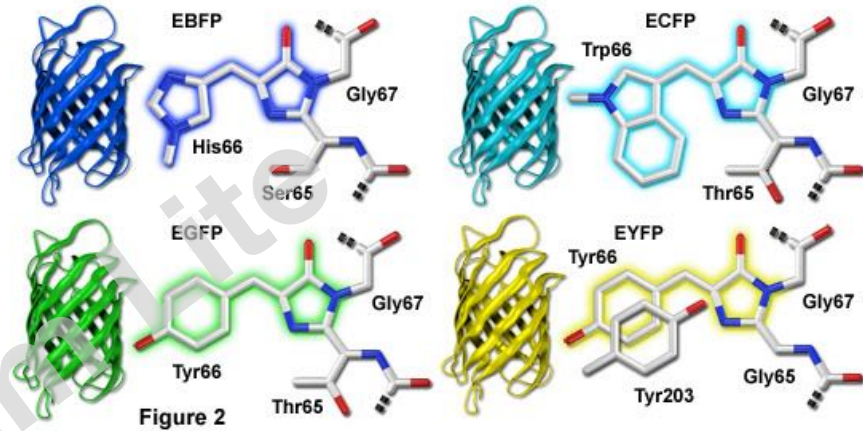
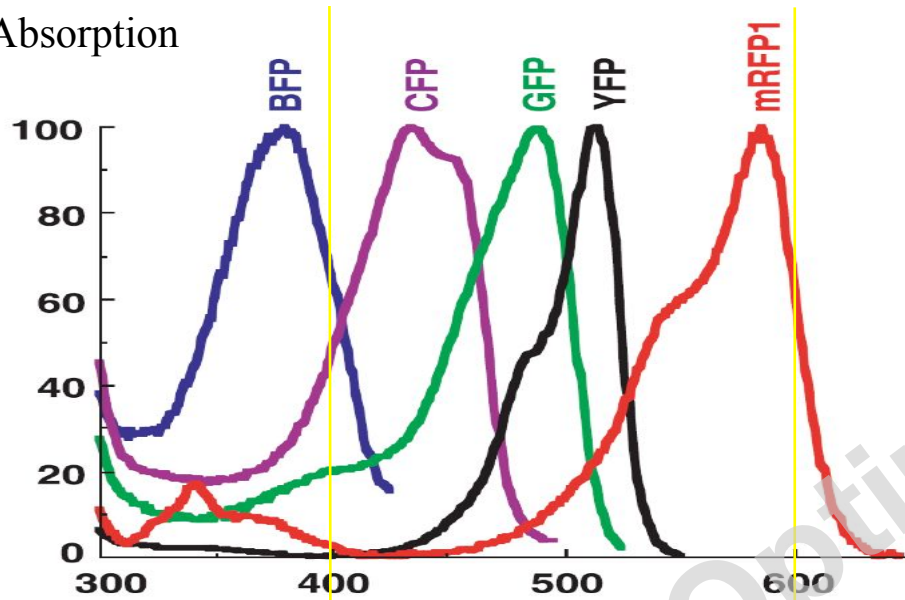


The jelly fish *Aequorea Victoria*

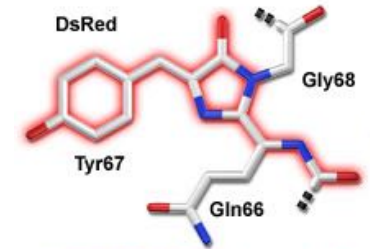
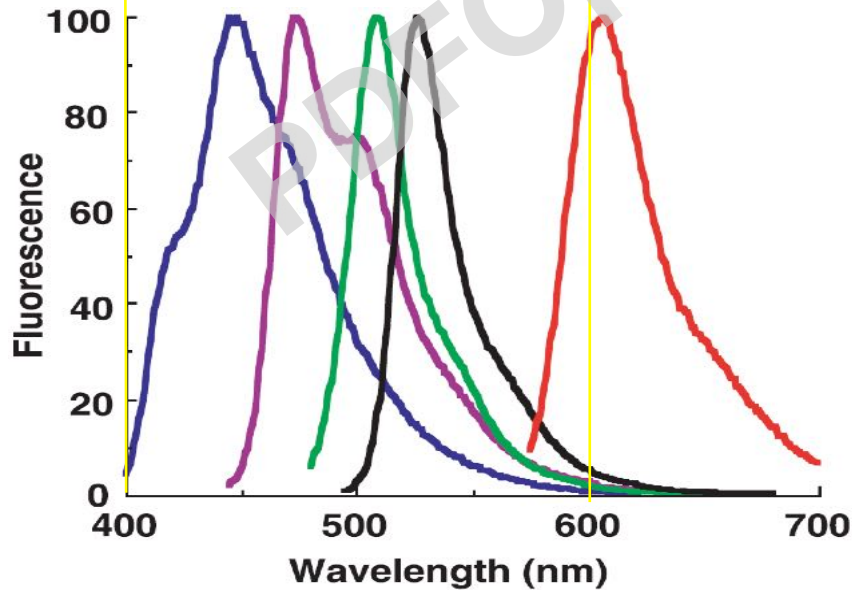


# A few mutants of the GFP

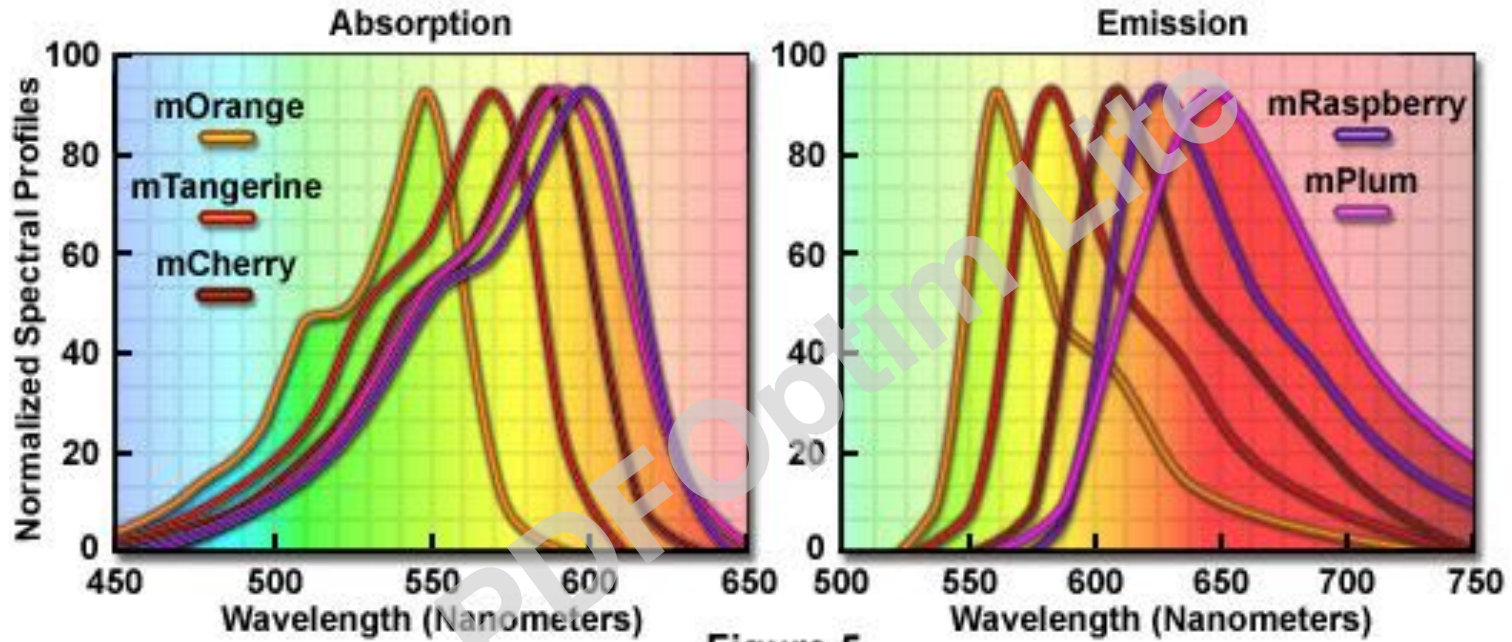
Absorption



Fluorescence



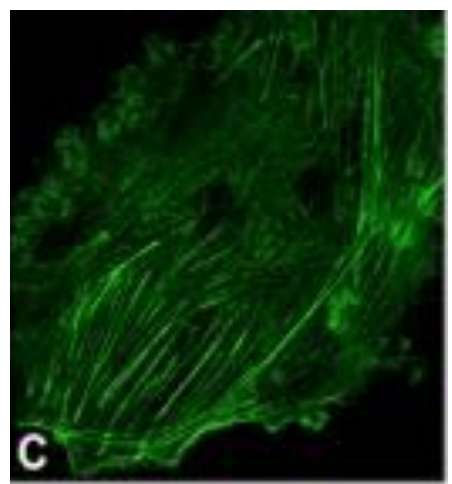
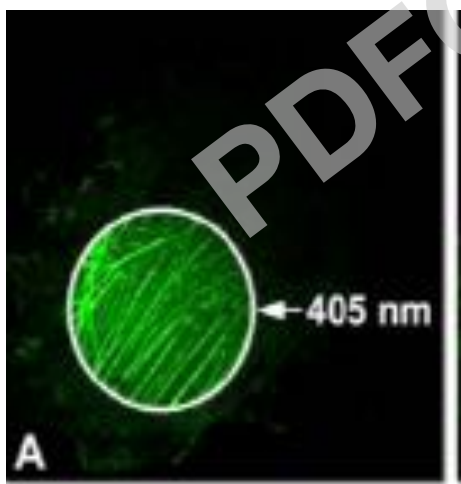
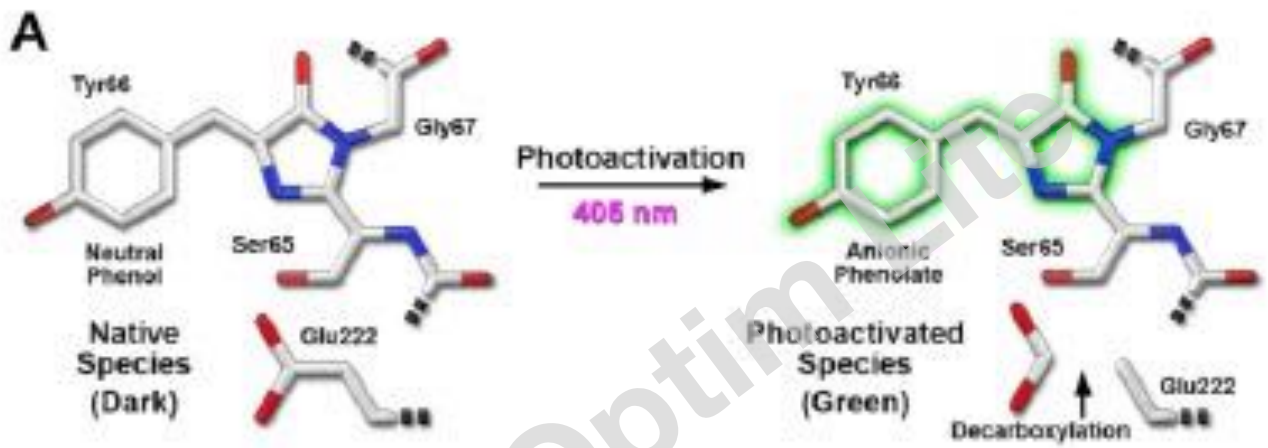
# Red and orange mutants



This rich photophysics can be used to engineer interesting nanoscale emitters in the cells...

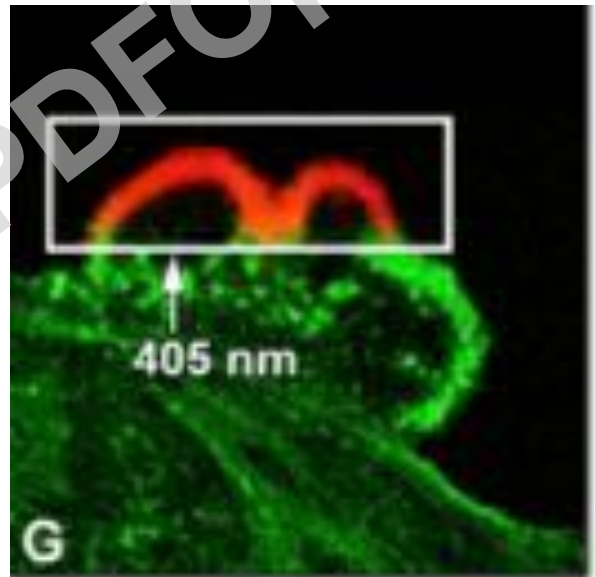
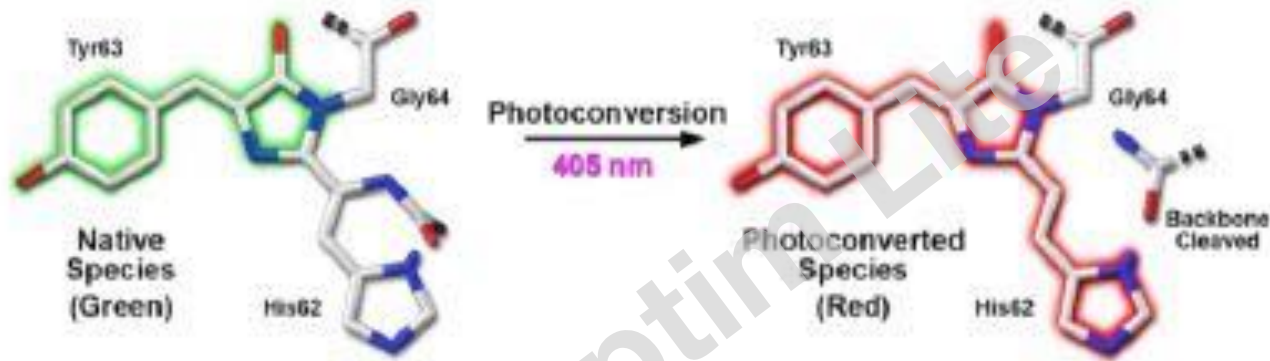
PDFOptim Lite

**Photoactivatable FPs** are dark and are irreversibly activated by irradiation. For example irradiation of PA-GFP with intense violet light results in a 100-fold increase in green fluorescence. It is presumed that the violet light causes the decarboxylation of Glu222, which aids in the formation of the anionic fluorescent form of the chromophore, see below.

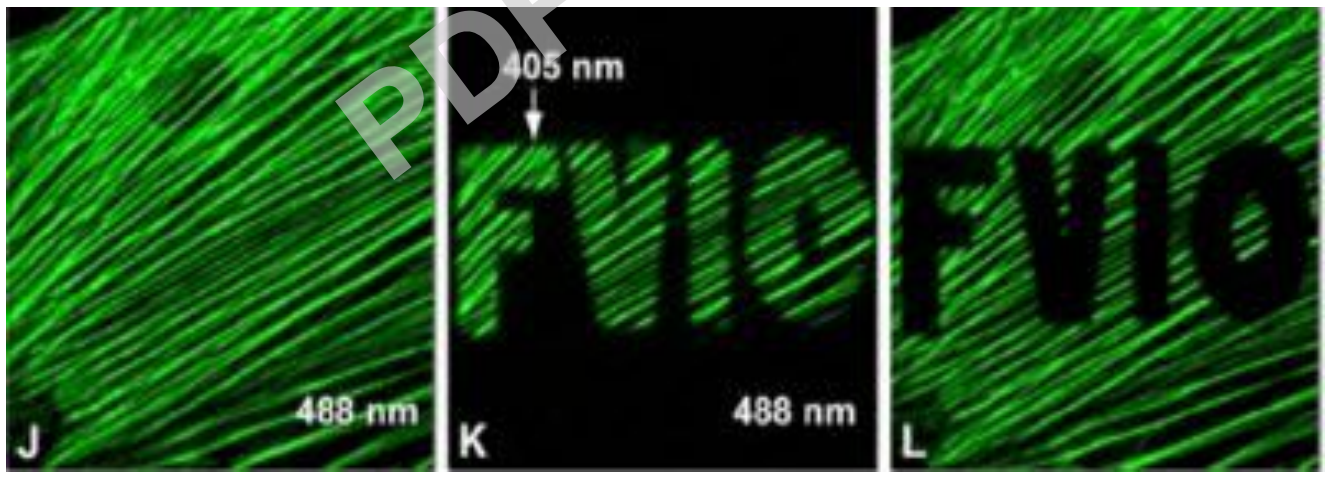


(*J. Cell Science* 2007,120, 4257)

**Photoconvertible FPs** can be irreversibly converted from a green fluorescent form to a red fluorescent form by violet or ultraviolet irradiation e.g. Kaede, KikGR, Dendra2 and Eos. The photoconversion is presumably associated with a cleavage occurring between the amide nitrogen and the alpha carbon of His62 that is followed by oxidation of the His62 sidechain.

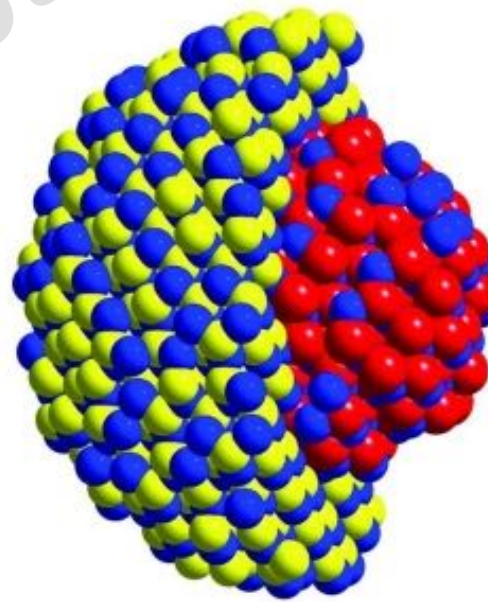
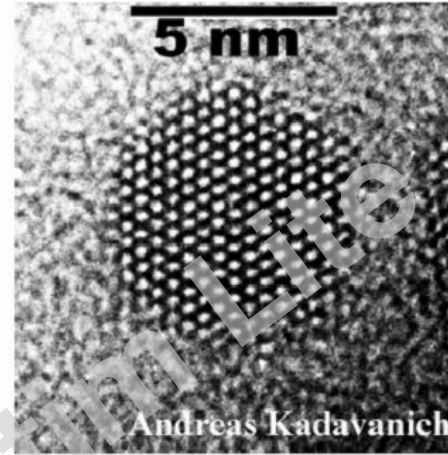
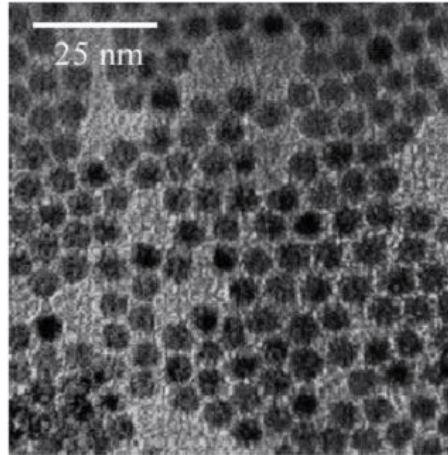


**Photoswitchable FPs** are dark and are reversibly activated by irradiation. Photoswitchable FPs such as Dronpa, mTFP0.7 and KFP switch between the dark E (or trans) state and the fluorescent Z (or cis) state, see below.



# Fluorescence labeling (3)

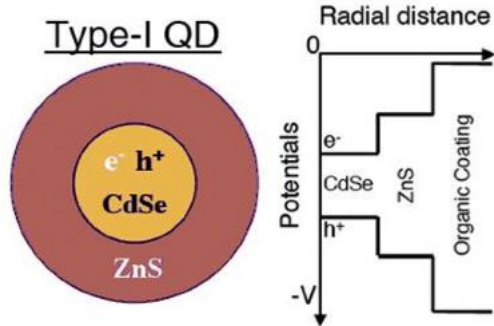
## Nanocrystals of Semiconductors



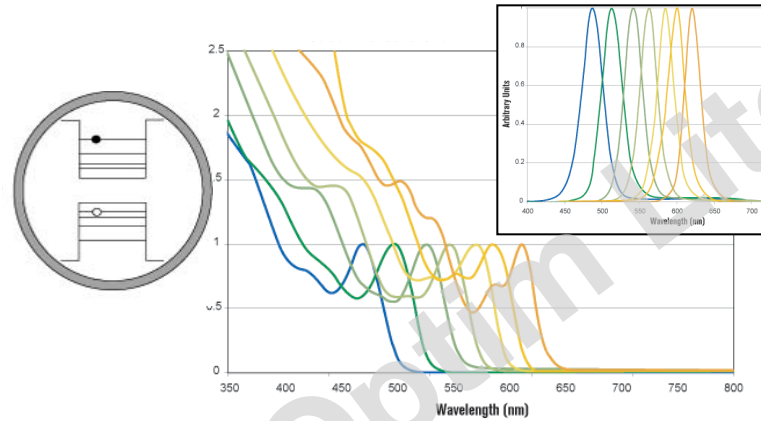


# Emission Properties (1)

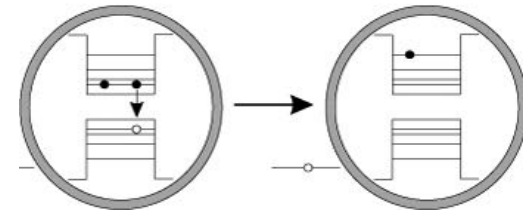
## Quantum Confinement



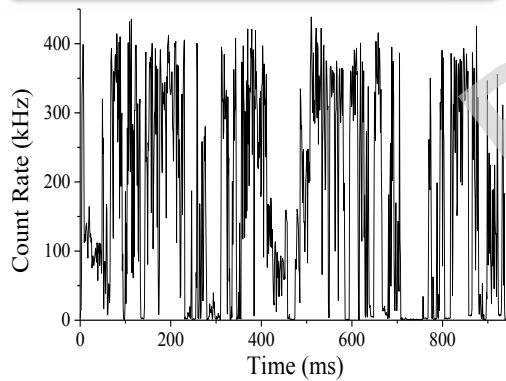
## Absorption & Emission



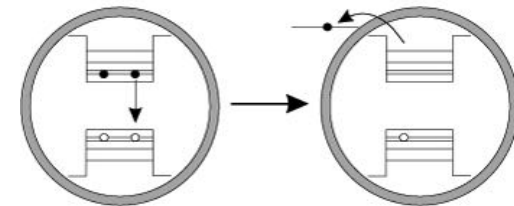
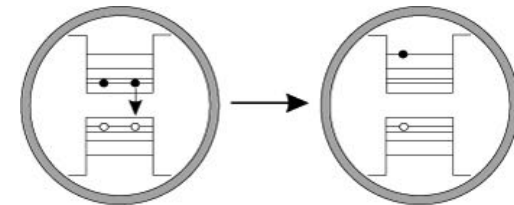
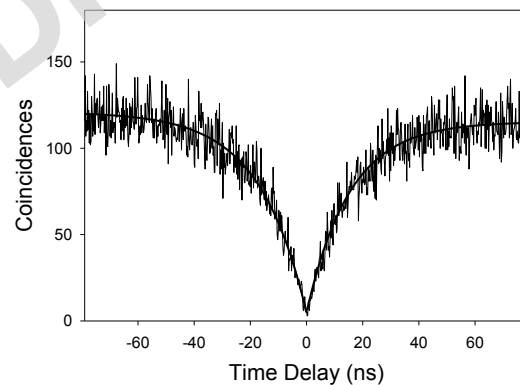
## Auger Process



## Luminescence Blinking

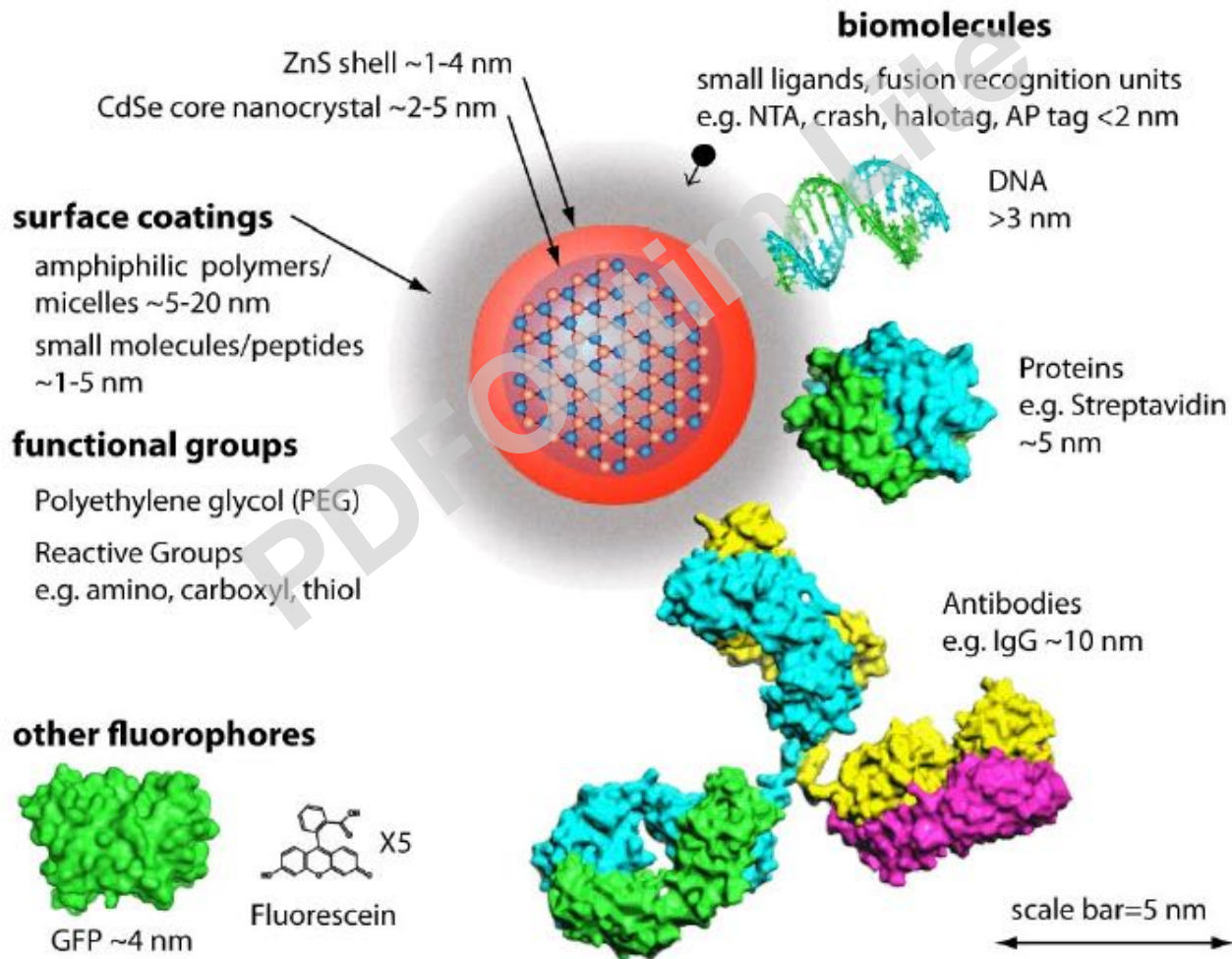


## Photons Antibunching

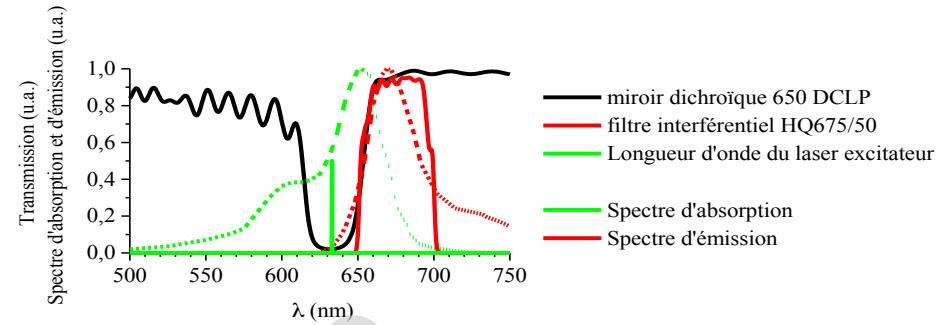
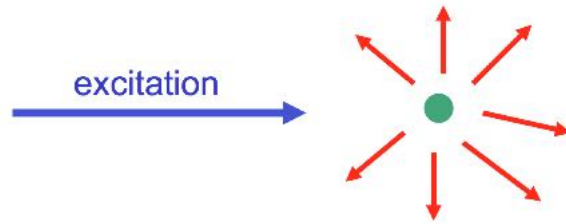


# Fluorescence labeling (3)

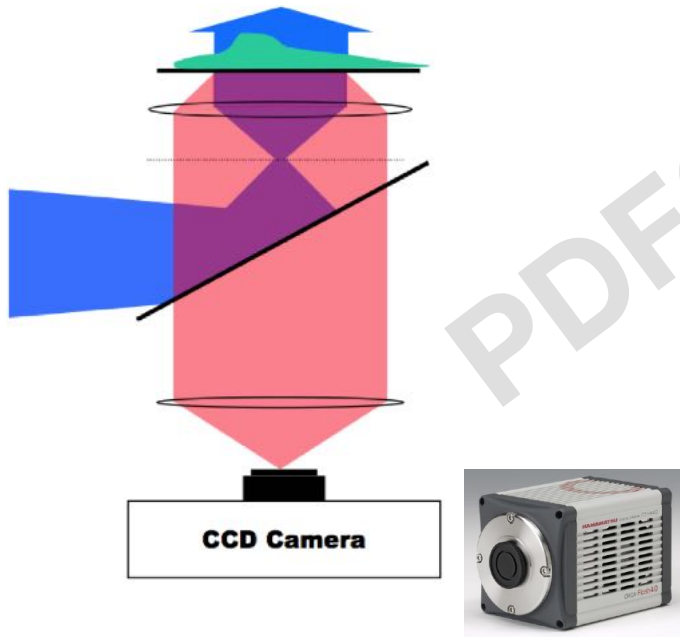
## Semiconductor quantum dots bioconjugation



# “Standard” fluorescence microscopy techniques

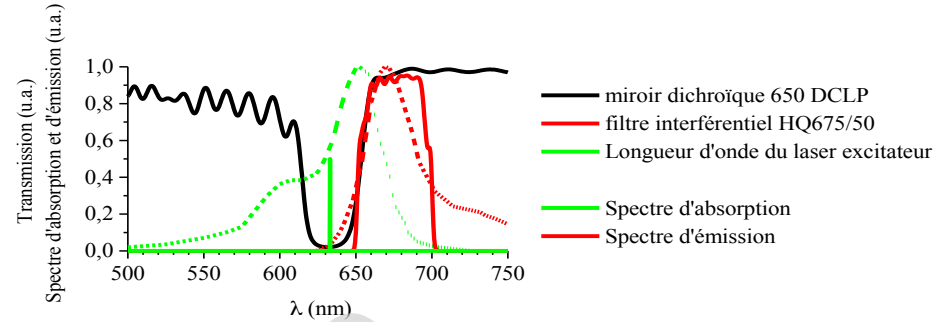
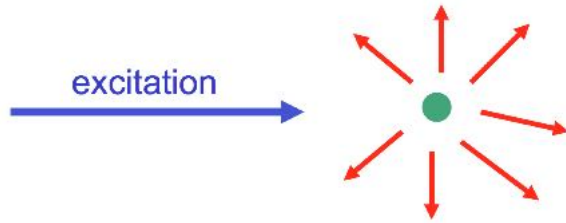


## Wide-field fluorescence microscopy



**Resolution  $1.22 \lambda / 2 NA$**

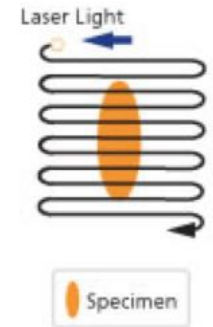
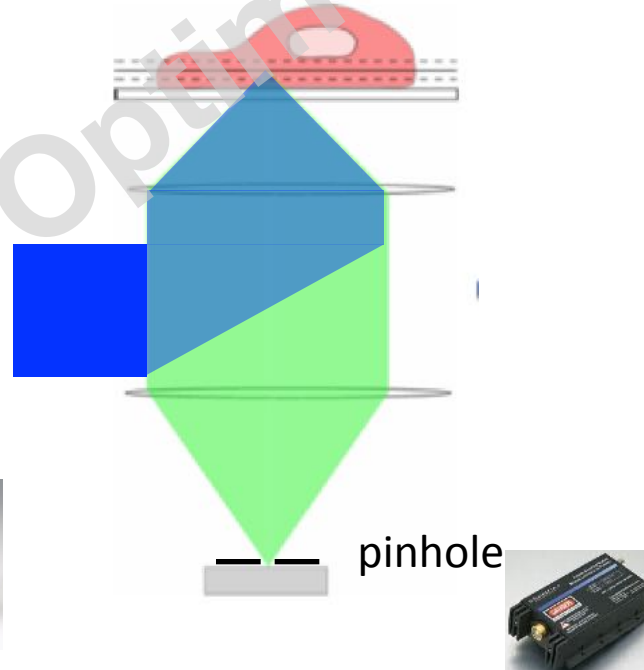
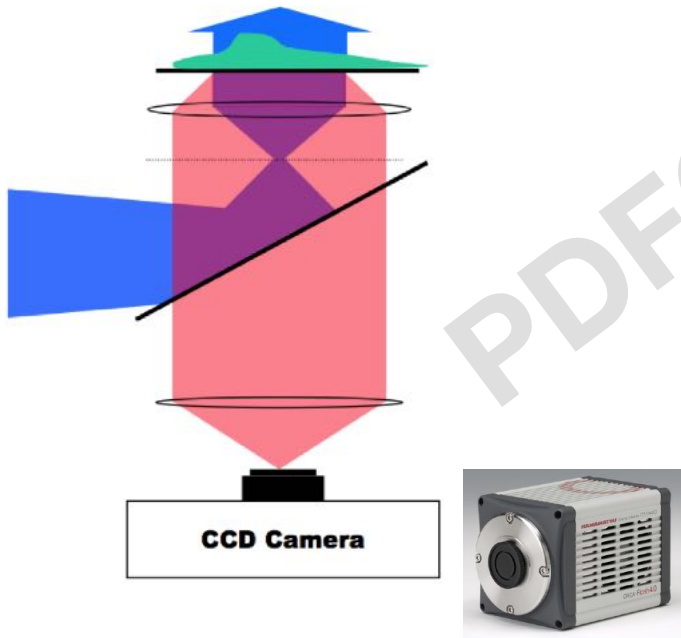
# “Standard” fluorescence microscopy techniques



## Wide-field fluorescence microscopy

## Confocal microscopy:

*localized excitation + spatially filtered detection*

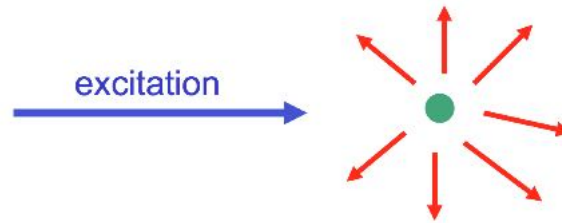


+ laser scanning

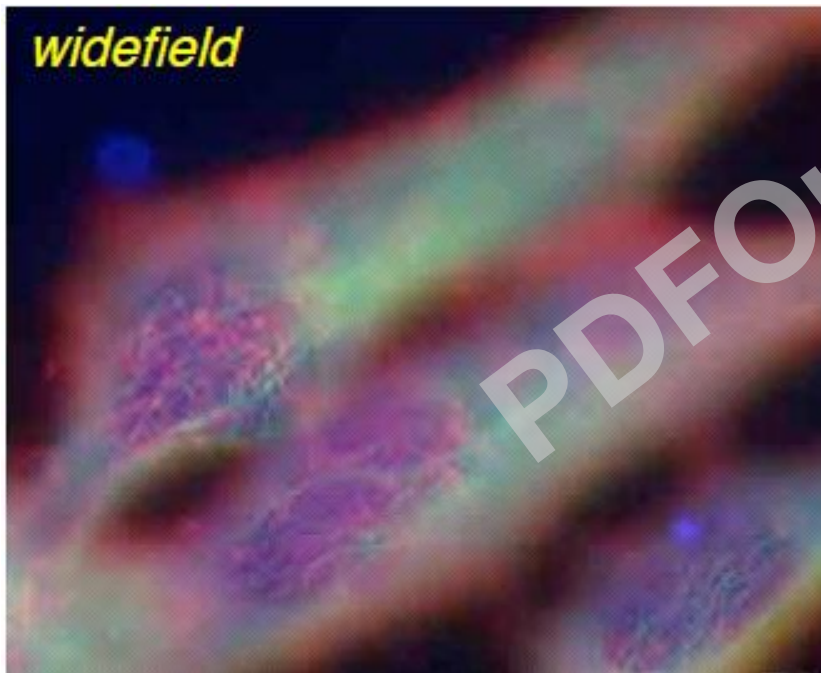
**Resolution  $1.22 \lambda / 2 NA$**

**Improved resolution  $0.86 \lambda / 2 NA$**

# “Standard” fluorescence microscopy techniques



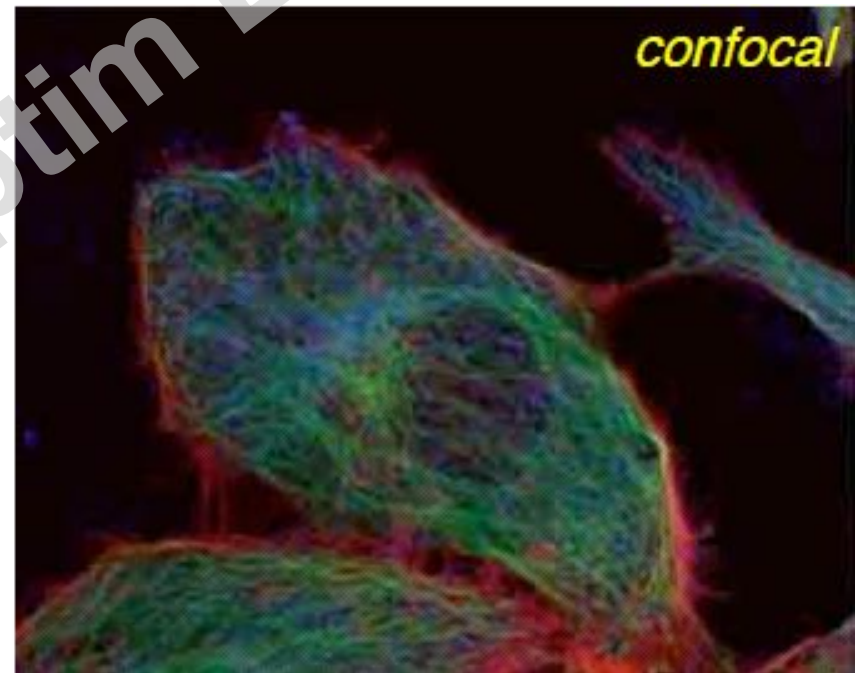
## Wide-field fluorescence microscopy



Resolution  $1.22 \lambda / 2 NA$

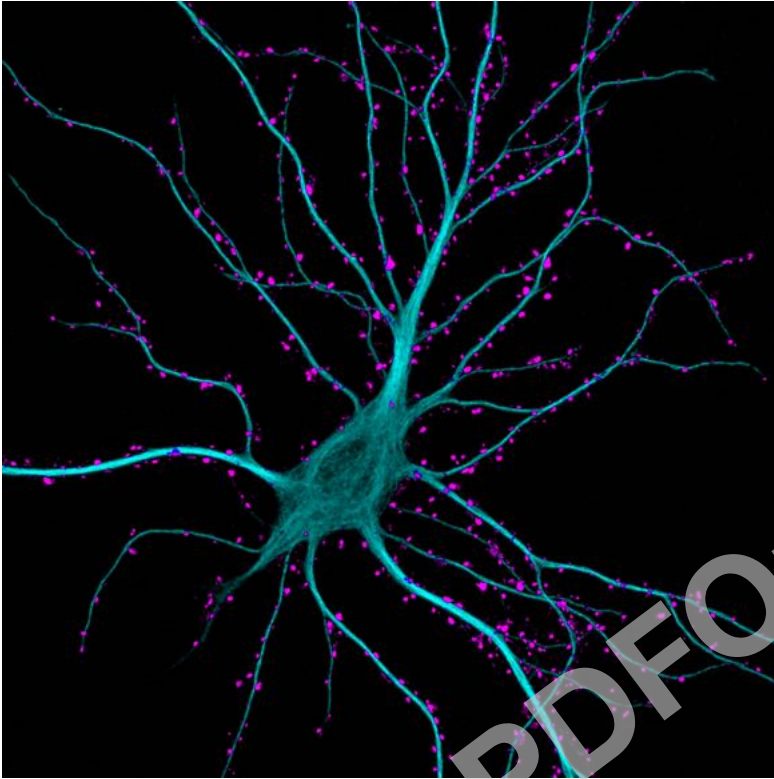
## Confocal microscopy:

*localized excitation + spatially filtered detection*



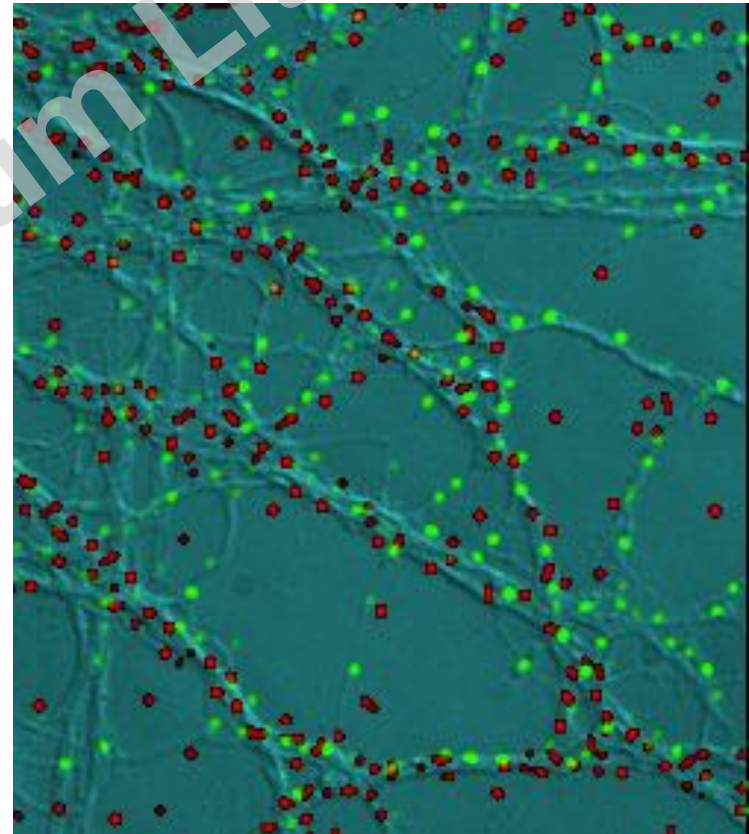
Improved resolution  $0.86 \lambda / 2 NA$   
+ Axial resolution

# Fluorescence microscopy

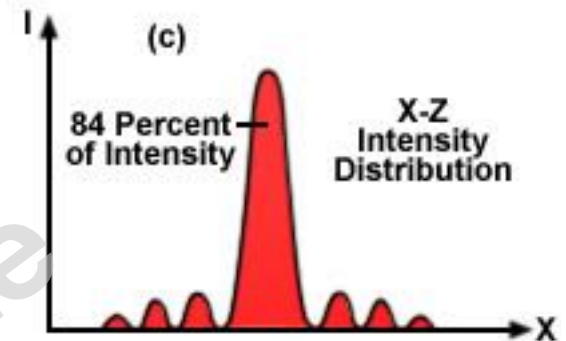
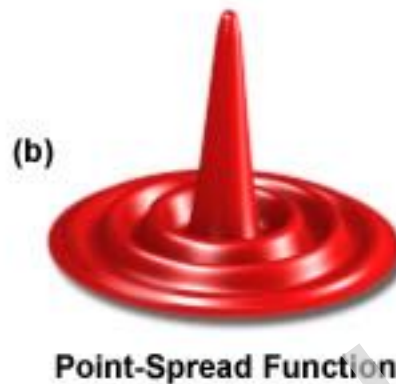
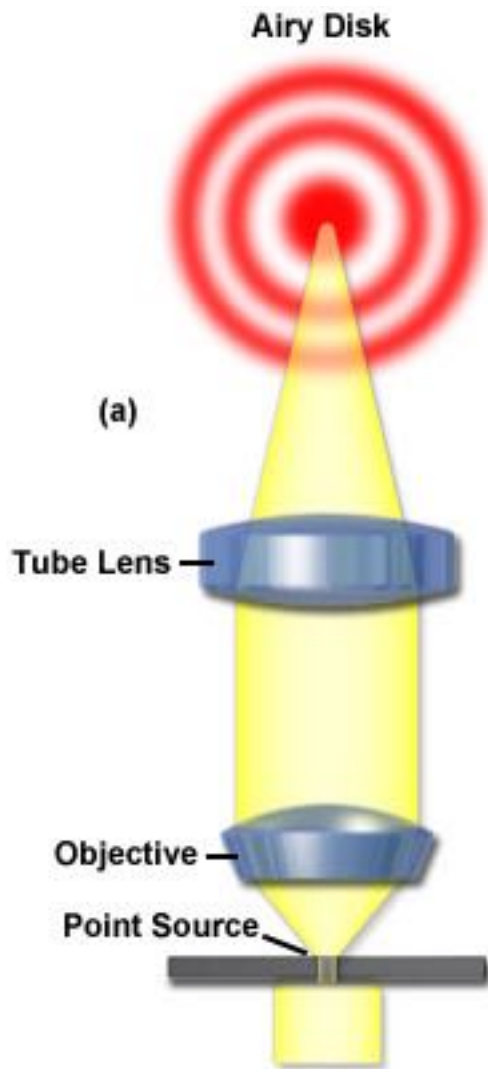


Fluorescence image of neuron

Live cell imaging



# Diffraction limit

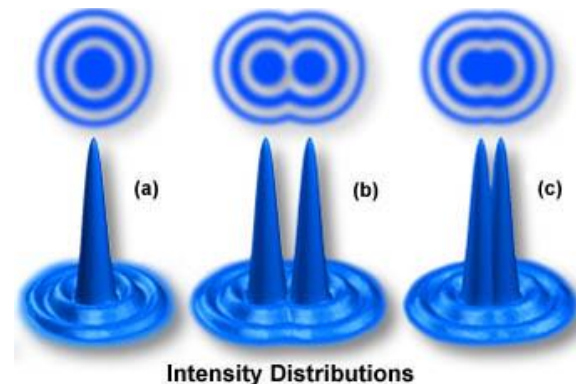


diffraction spot width

$$\Delta x = \frac{1.22\lambda}{2NA}$$

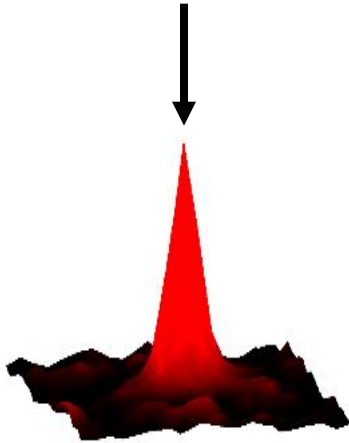
High N.A. = 1.49, oil immersion  
 $\Delta x = 214 \text{ nm}$  @  $\lambda = 500 \text{ nm}$ ,

Resolution :  
Rayleigh criterium



# Pointing accuracy

The pointing accuracy i.e. precision of the localization of the fluorophore is only limited by the signal to noise ratio



$$\langle (\Delta x)^2 \rangle = \frac{s^2 + p^2/12}{N} + \frac{8\pi s^4 B^2}{p^2 N^2}$$

N: number of the collected photons, s: PSF width,  
p: Pixel size B: Background signal

Typically , for a SNR of  $\sim 30$   
The pointing accuracy is  $\sim 40\text{nm}$

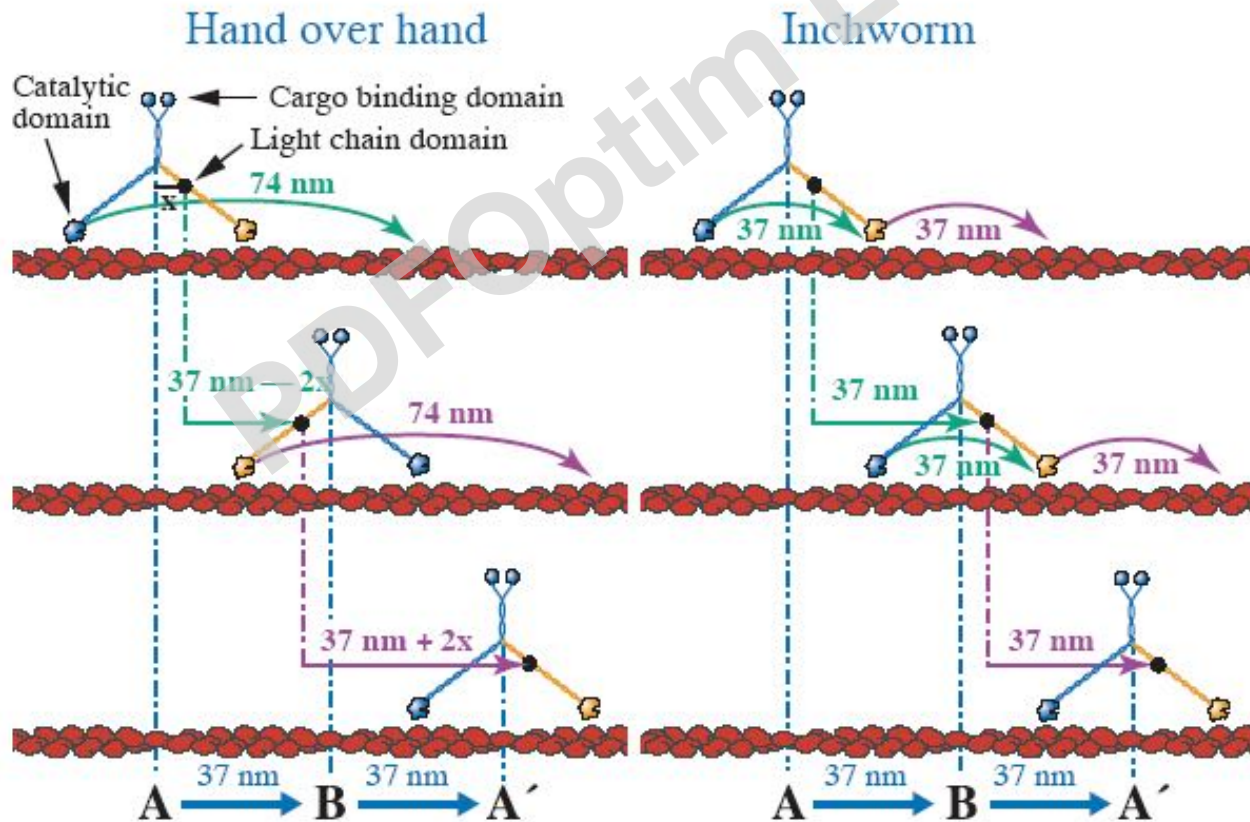
In the limit of a SNR limited by  
the photon number noise:

$$\langle (\Delta x)^2 \rangle \approx \frac{\lambda/2}{\sqrt{N}}$$

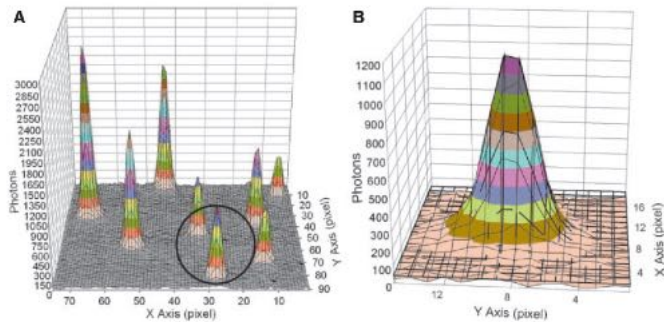


# Myosin V Motility

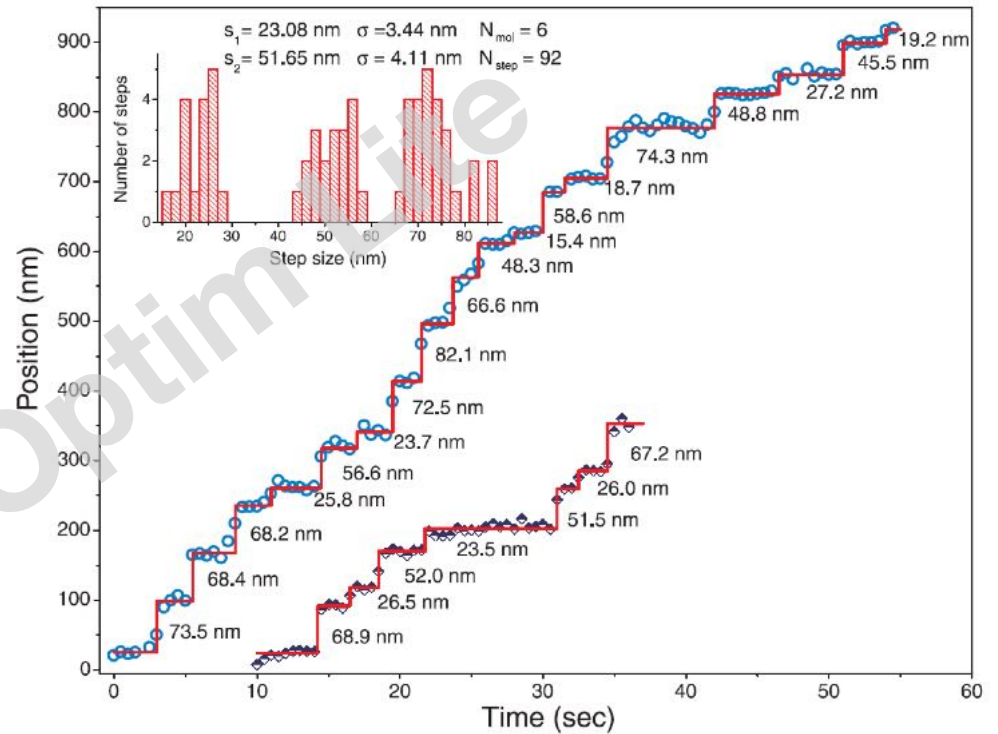
- Cargo carrying processive molecular motor
- 37 nm center of mass steps along the actin filament at each ATP hydrolysis
- two heads held together by coiled-coil stalk



# Myosin V Walks Hand-Over-Hand:



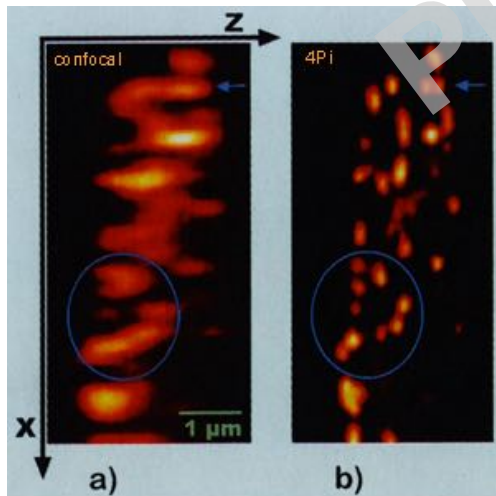
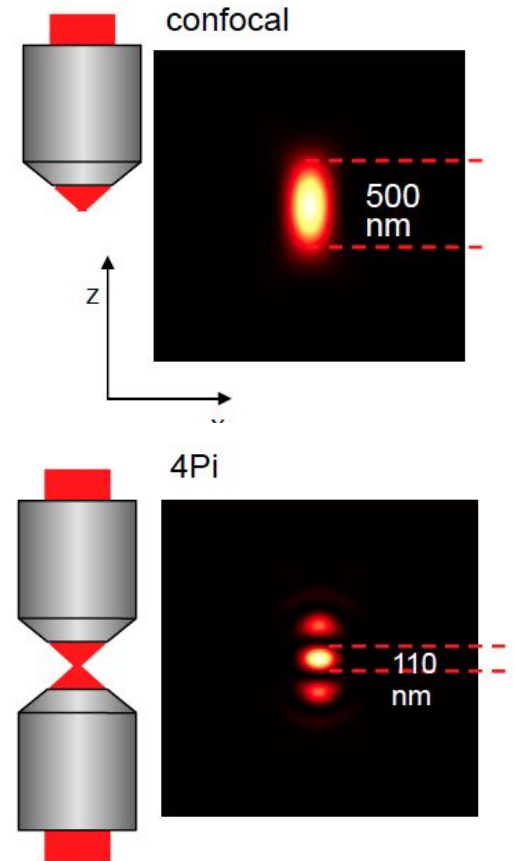
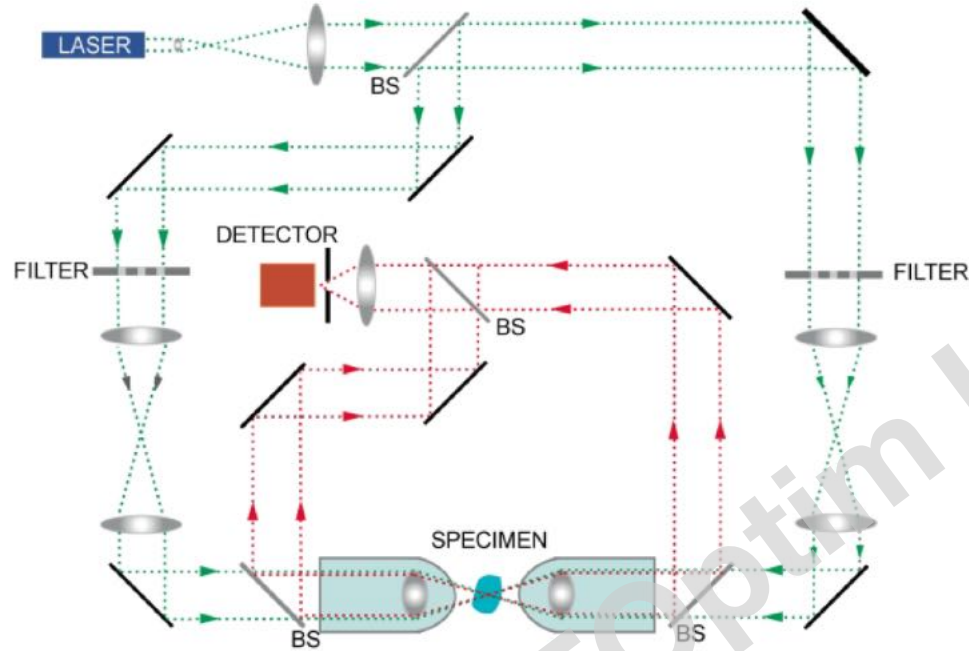
Single molecules detected  
with high S/N ratio  
Pointing accuracy < 5nm



**Fig. 4.** Stepping traces of two different BR-labeled myosin V molecules displaying alternating 52-23 steps, and histogram of a total of six myosin V's taking 92 steps. Due to the 0.5-s time resolution of measurements, some steps are missed and yield 74-nm apparent steps, the sum of two steps. On the basis of the alternating step size, we infer that the dye is 7 nm from the center of mass along the direction of motion.

Ahmet Yildiz,<sup>1</sup> Joseph N. Forkey,<sup>3</sup> Sean A. McKinney,<sup>1,2</sup>  
Taekjip Ha,<sup>1,2</sup> Yale E. Goldman,<sup>3</sup> Paul R. Selvin<sup>1,2\*</sup>

# 4 Pi confocal microscopy



improvement the axial resolution (z) of a Confocal Microscope

# Super-resolution microscopies

i.e. which provide images with resolution below the diffraction limit

- revolutionized imaging capabilities offered by far-field optical microscopy in complex environments
- development mainly driven by the need for improved resolutions to study biological processes in live samples.
- optical resolutions down to the scale of individual biomolecules in order to give access to nanoscale molecular organizations

based on:

controlling fluorescence emission volumes to highly localized regions, using structured illumination schemes or stochastic detection of single emitters

# Super-resolution microscopies

i.e. which provide images with resolution below the diffraction limit



The Nobel Prize in Chemistry 2014

Eric Betzig, Stefan W. Hell, William E. Moerner

Share this:      1.2K 

## The Nobel Prize in Chemistry 2014



Photo: Matt Staley/HHMI

**Eric Betzig**

Prize share: 1/3



© Bernd Schuller, Max-Planck-Institut

**Stefan W. Hell**

Prize share: 1/3



Photo: K. Lowder via Wikimedia Commons, CC-BY-SA-3.0

**William E. Moerner**

Prize share: 1/3

The Nobel Prize in Chemistry 2014 was awarded jointly to Eric Betzig, Stefan W. Hell and William E. Moerner *"for the development of super-resolved fluorescence microscopy"*.

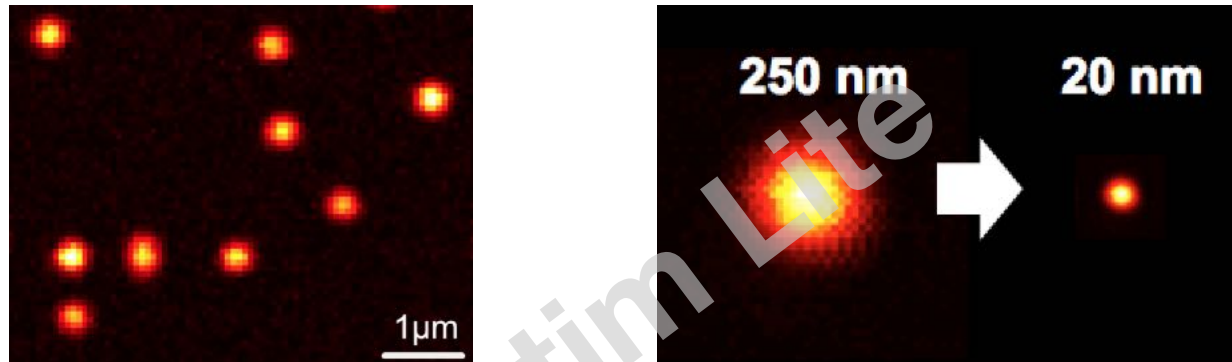
# Super-resolution microscopies

i.e. which provide images with resolution below the diffraction limit

- **based on single molecule detection: PALM, STORM, uPAINT etc...**
- based on controlled fluorescence emission volumes (STED, RESOLFT...)

PDFOptim Lite

# Single molecule detection allows localizing isolated emitters with nanometer resolutions

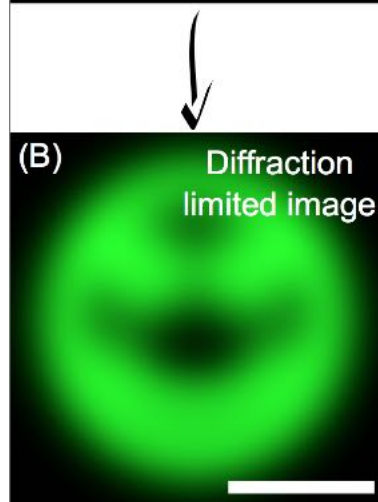
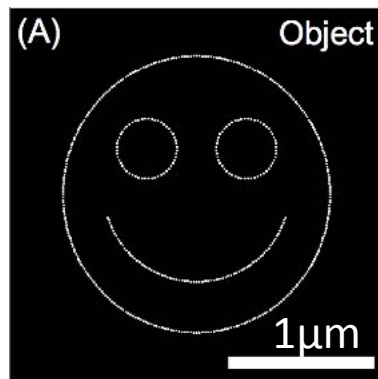


Every single molecule detection corresponds to a diffraction limited spot

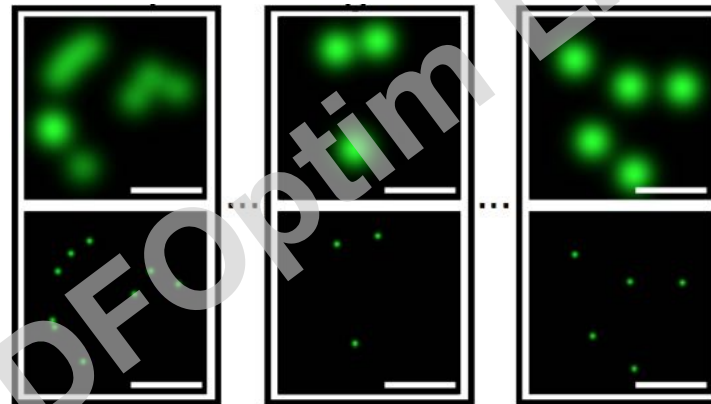
*With the pre-knowledge that each spot corresponds to a single molecule, determination of the center of each spot by 2D curve fitting provides the position of the emitting molecule with nanometer resolution (limited by signal to noise ratio).*

**Requirement : molecules are isolated so that their signal spatial distribution do not overlap**

# Super-resolution imaging methods based on single molecule detection (PALM, STORM, uPAINT ...)



The idea: Separate in space and time the detection of all molecules by acquiring movies where in each image, isolated molecules are detected so that their signal spatial distribution to not overlap. How? Stochastic photoactivation, binding etc...



Movie frames (1000's)

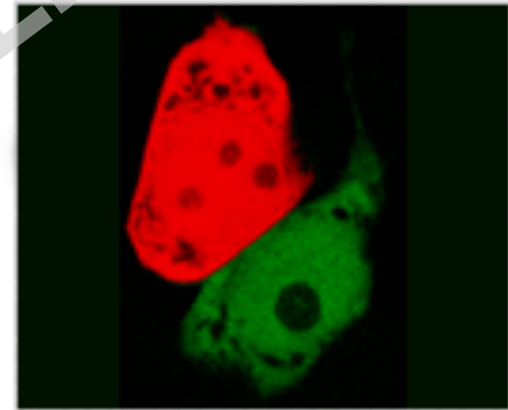
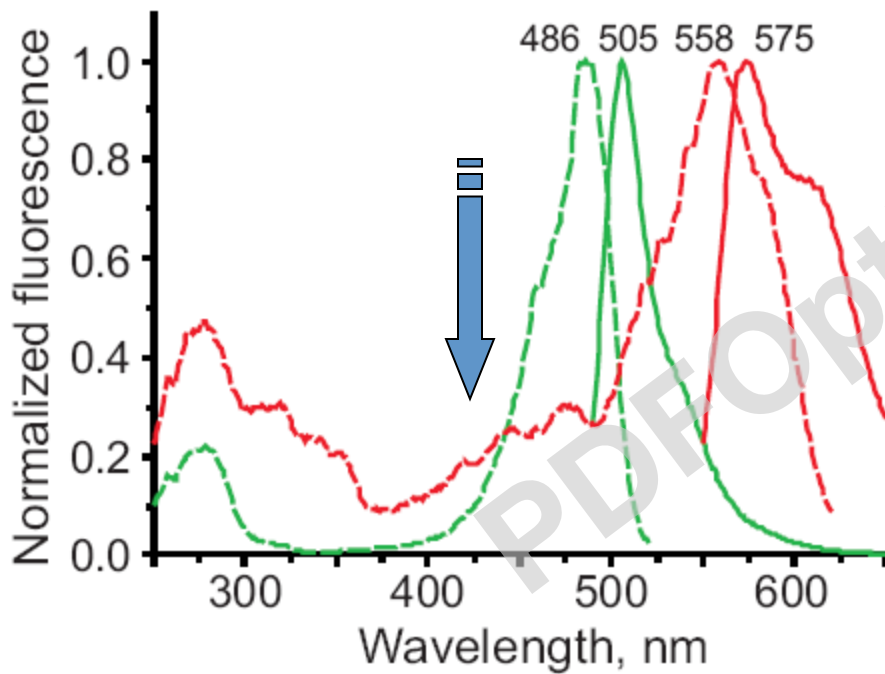
Single molecule positions after image analysis



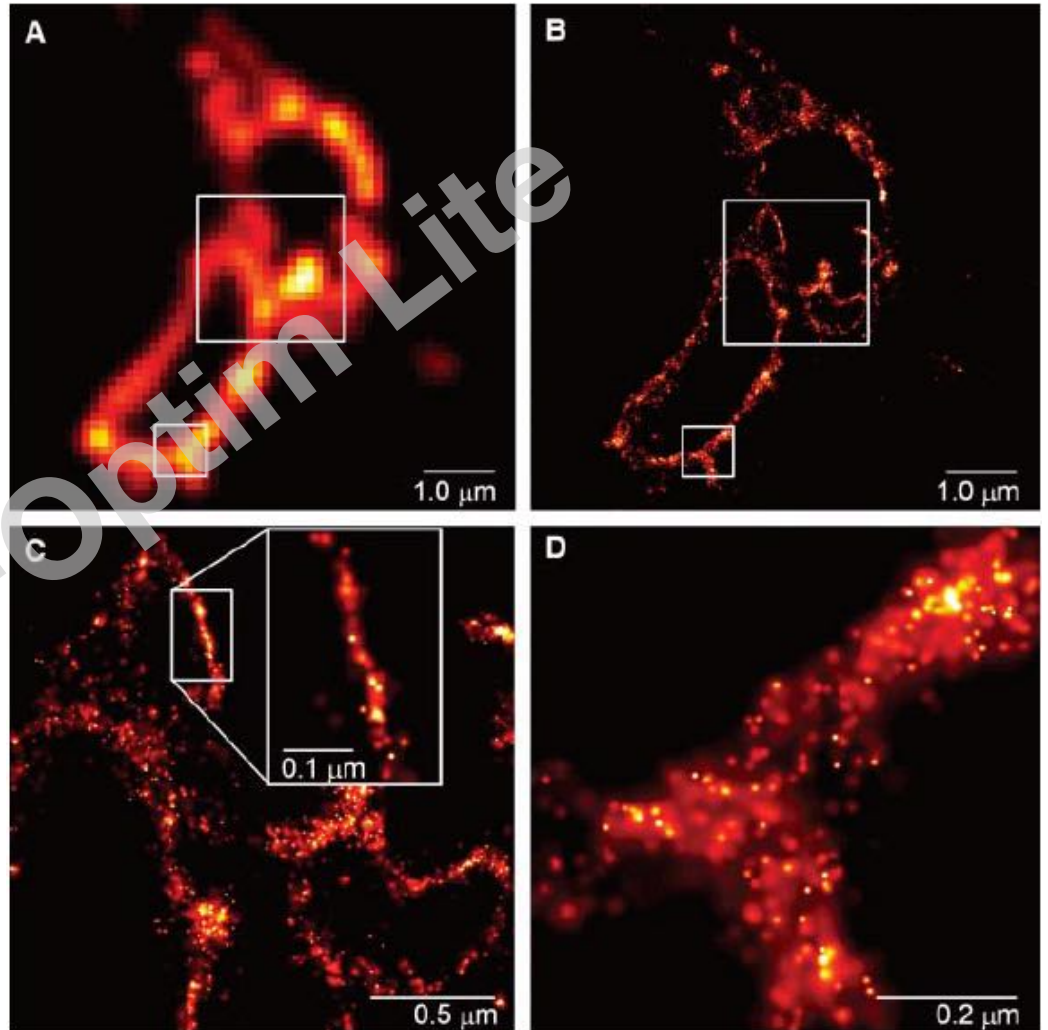
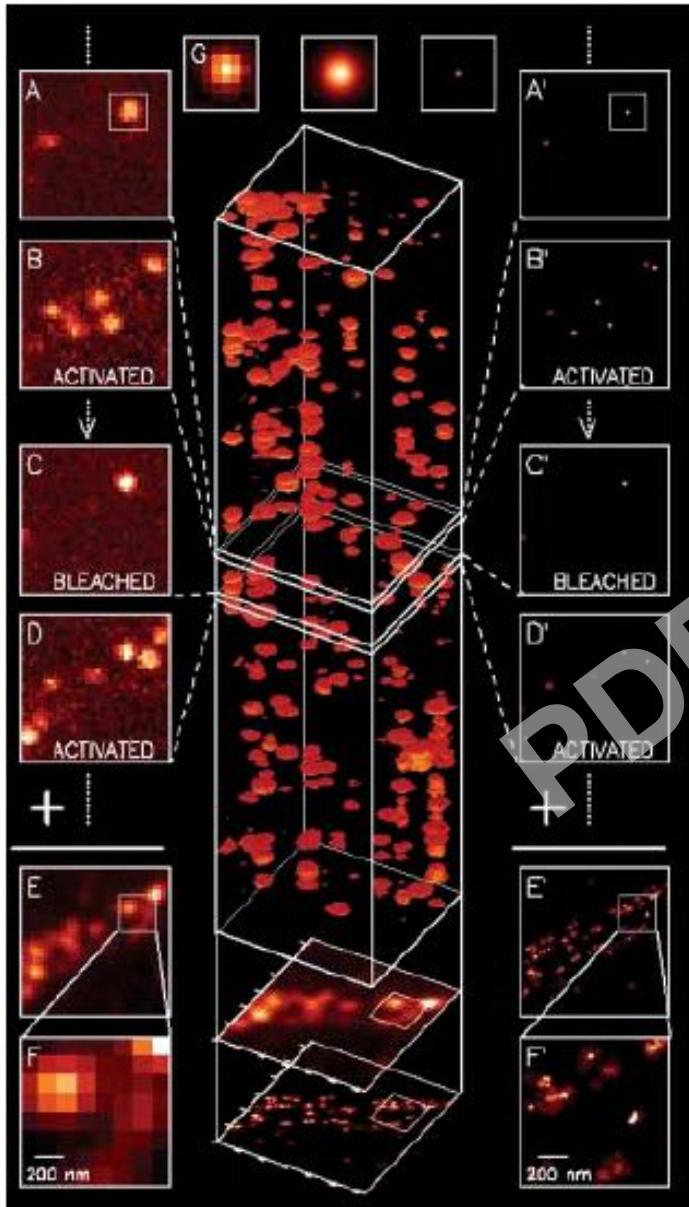
Super-resolved image (reconstructed!)



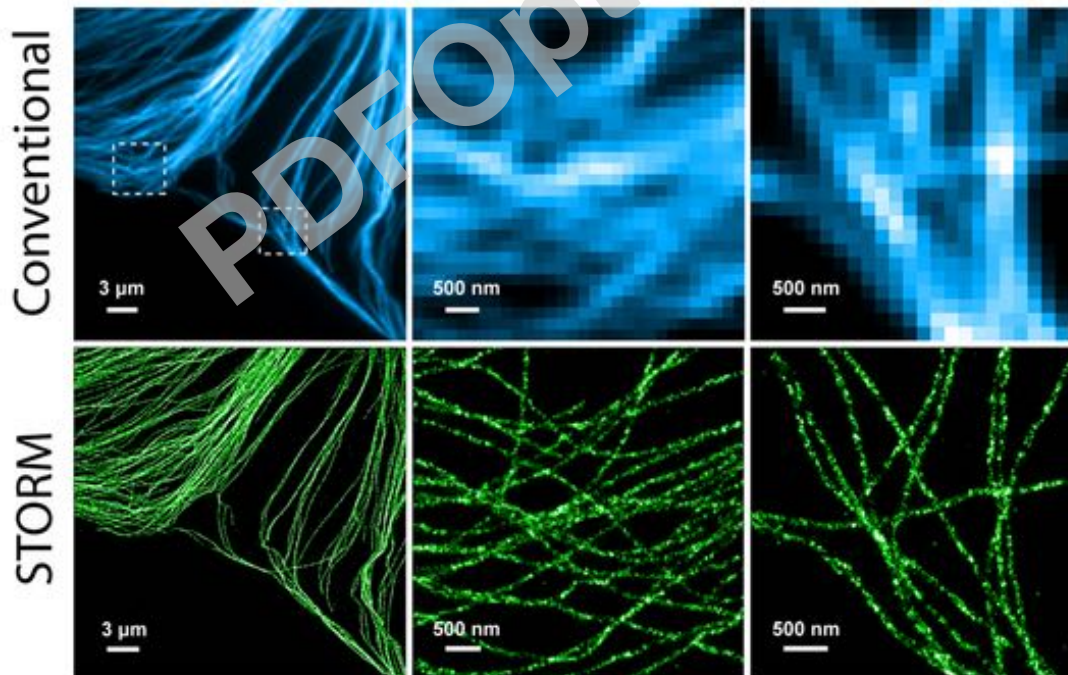
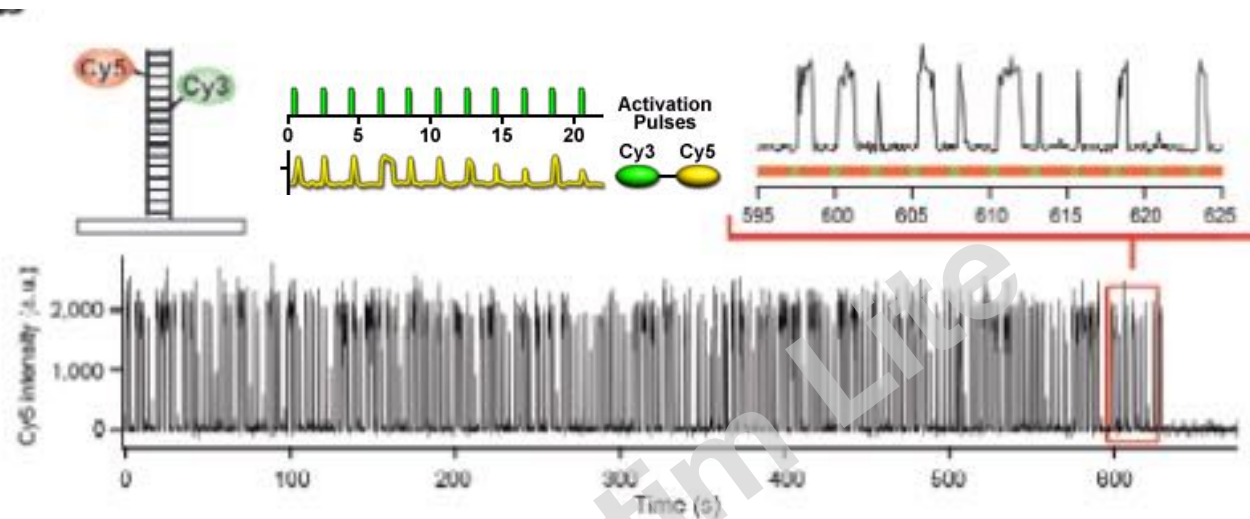
# Photo-switchable Fluorescent Protein



# PhotoActivable Light Microscopy (PALM)



# Stochastic optical reconstruction microscopy (STORM)

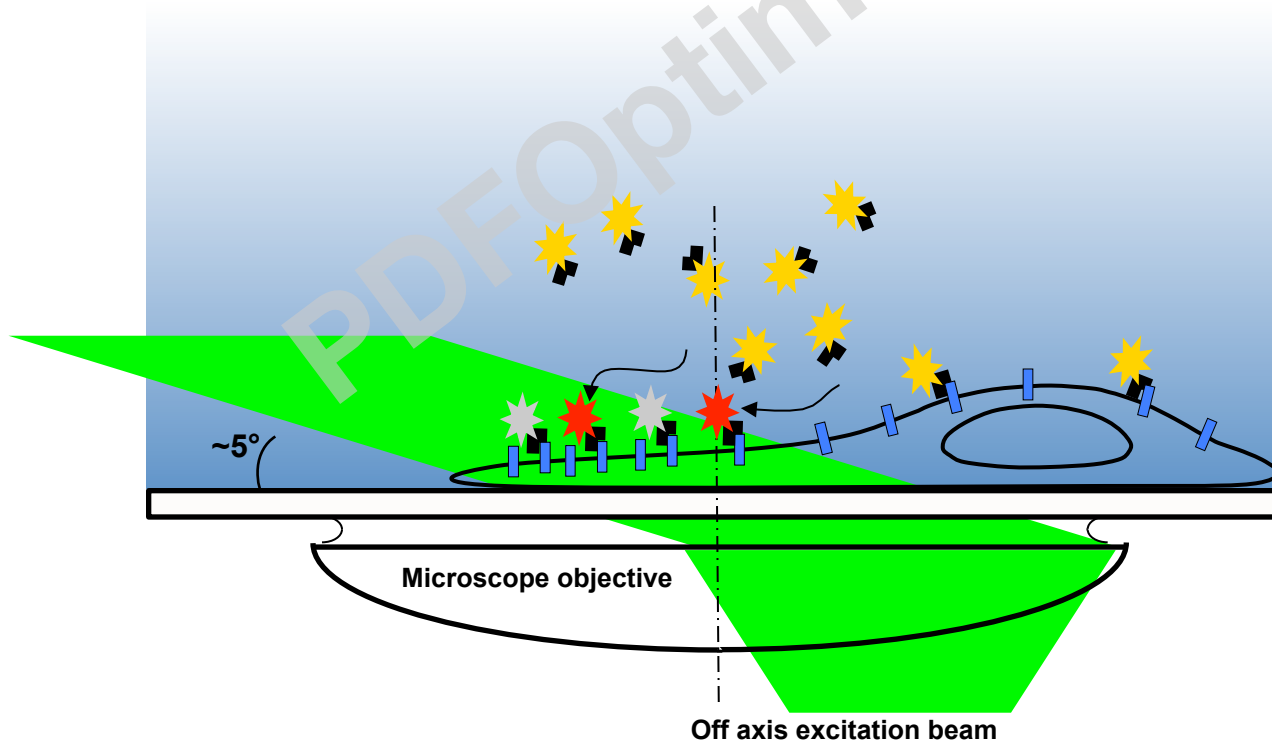


**Table 1 Photoswitchable fluorophores used in super-resolution fluorescence microscopy**

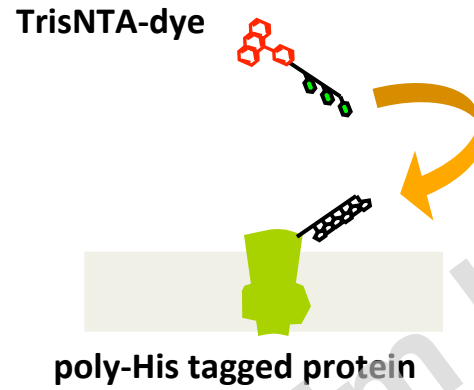
Fluorophore		Activation wavelength (nm)	Before activation		After activation		Reversible
			Ex <sup>a</sup> (nm)	Em (nm)	Ex (nm)	Em (nm)	
Cyan/dark-to-green FP	PA-GFP	405	400	517	504	517	No
	PS-CFP2		400	468	490	511	
Green-to-red FP	Kaede	405	508	518	572	582	No
	EosFP	405	505	516	569	581	
	Dendra2	405–488	490	507	553	573	
Dark-to-red FP	PAmCherry	405	NF		564	595	No
Reversible FP	Dronpa	405	NF		503	518	Yes
	Dronpa2				486	513	
	Dronpa3				487	514	
	rsFastLime				496	518	
	bsDronpa				460	504	
	EYFP				405	NF	
Caged dyes	Caged fluorescein	<405	NF		497	516	No
	Caged Q-rhodamine <sup>d</sup>				545	575	
Cyanine dyes	Cy5 & Alexa 647	350–570 <sup>e</sup>	NF		647	665	Yes
	Cy5.5				674	692	
	Cy7				746	773	
Photochromic rhodamine	SRA545	375	NF		Green	545	Yes <sup>f</sup>
	SRA552					552	
	SRA577					577	
	SRA617					617	

# universal Point Accumulation Imaging in the Nanoscale Topography (uPAINT)

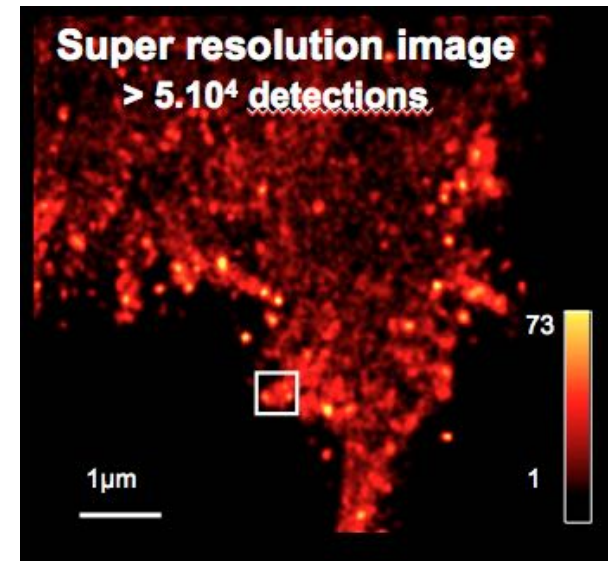
- do not need stochastic photoswitching of emitters
- captures real-time molecular interactions to control the density of fluorescent emitters
- can use any binding entity conjugated to fluorophores having high specificity toward a target molecule (e.g. ligand, antibody)
- allows to image and track endogenous receptors at high
- can combining single molecule FRET and dual-color uPAINT allow the specific super-resolution imaging and tracking of interacting receptors activated by their cognate ligand in live cells



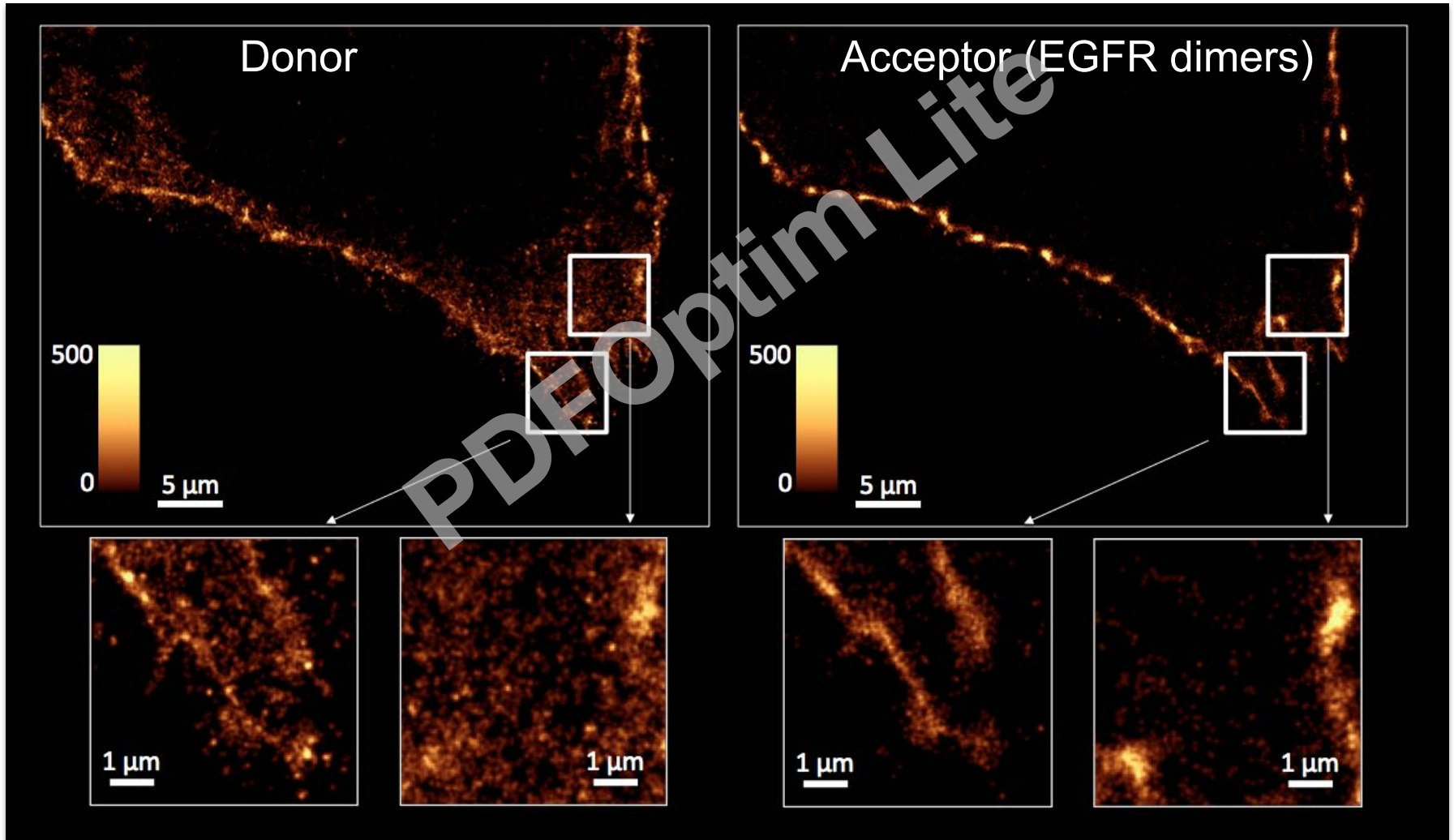
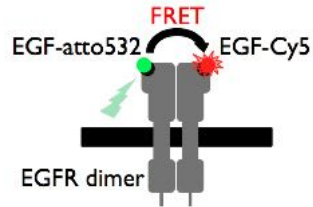
uPAINT Example : Unprocessed real time uPAINT images  
Model transmembrane protein on fibroblasts (Atto dyes)



Unprocessed real time uPAINT images



# uPAINT : Super-resolution imaging of endogenous EGFR dimers in live cells by smFRET



# Super-resolution en 3D (PALM / STORM / uPAINT etc...)

## Three-Dimensional Superresolution Imaging with STORM

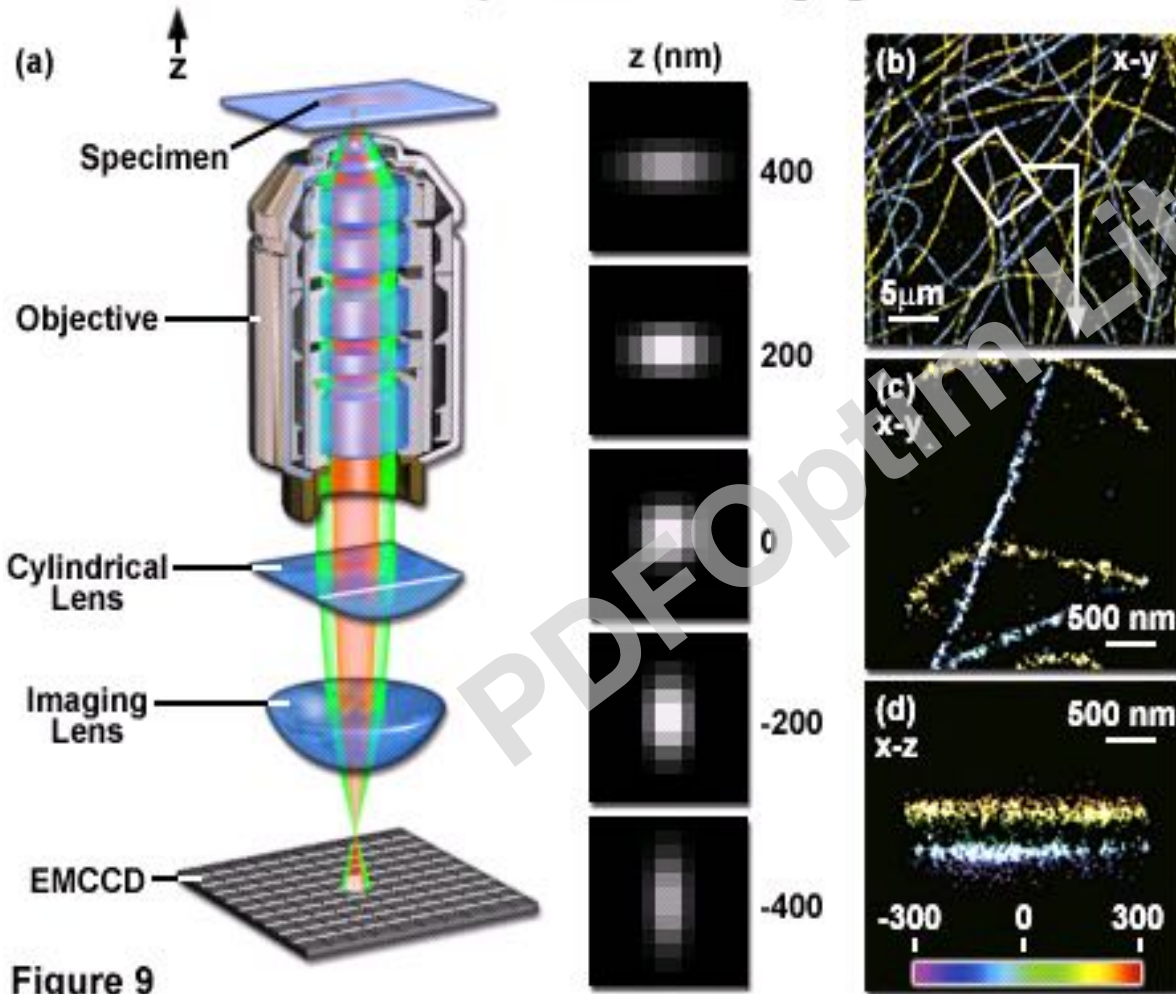
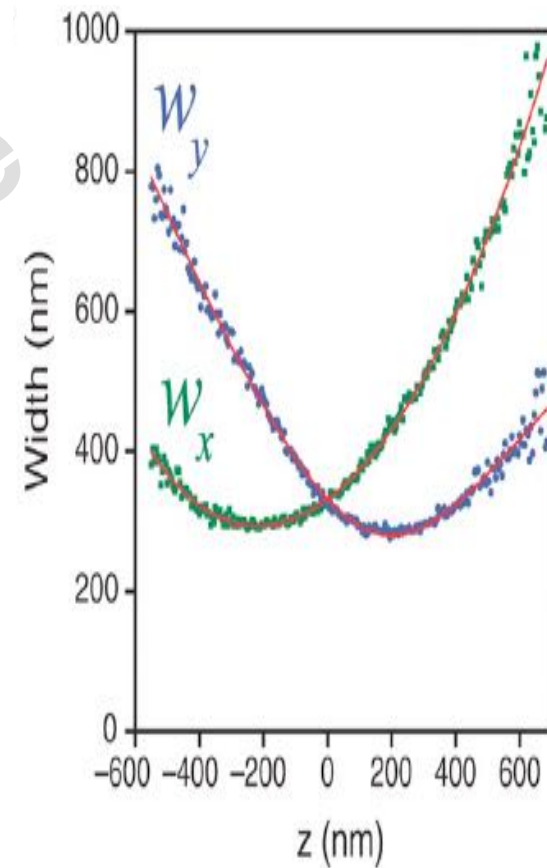


Figure 9





# Super-resolution microscopies

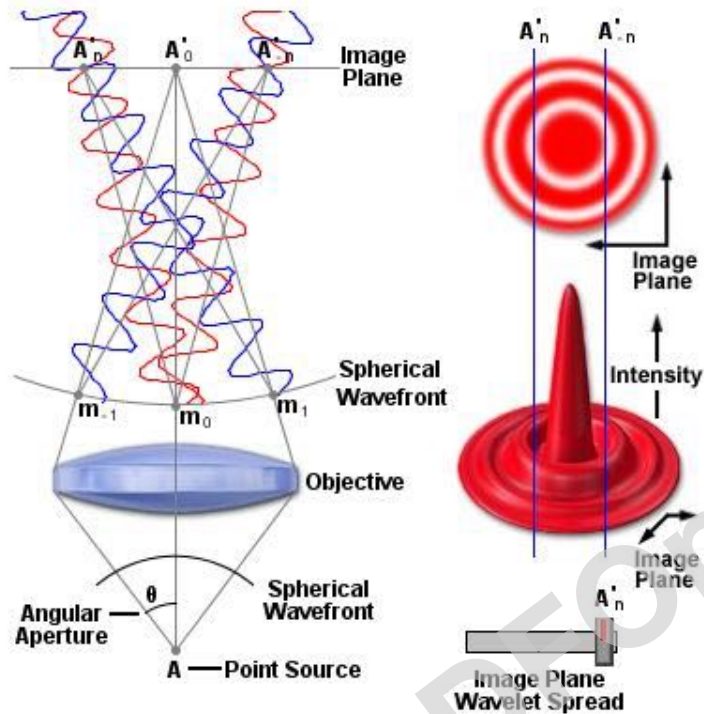
i.e. which provide images with resolution below the diffraction limit

- based on single molecule detection: PALM, STORM, uPAINT etc...

**- based on controlled fluorescence emission volumes (STED, RESOLFT...)**

PDFOptim Lite

# "confocal microscopy" beyond diffraction limit



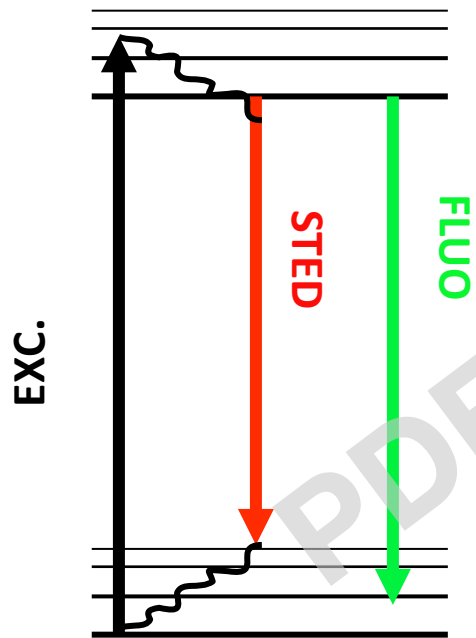
?????

Diffraction limit – distribution of light intensity

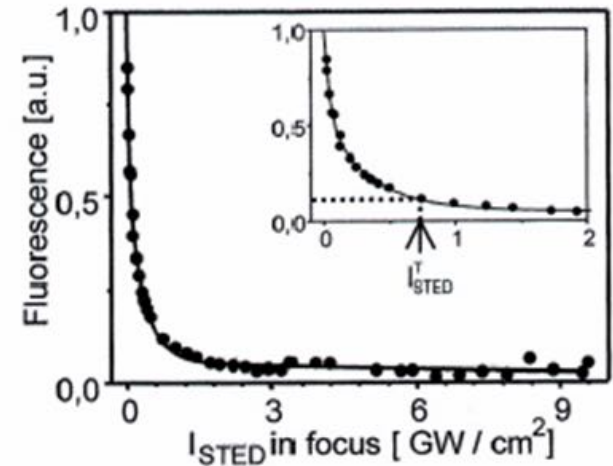
However, if the process is nonlinear function of intensity, then the localization is not limited by the wavelength

# STimulated Emission Depletion microscopy (STED)

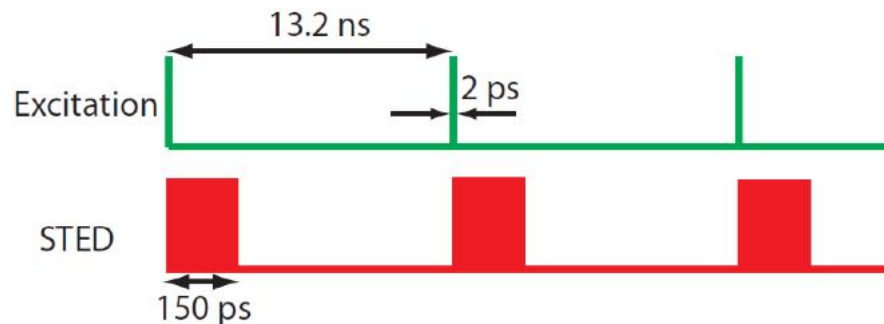
## Stimulated Emission



Experimental proof of the non-linear dependence of the excited state population with depletion beam intensity



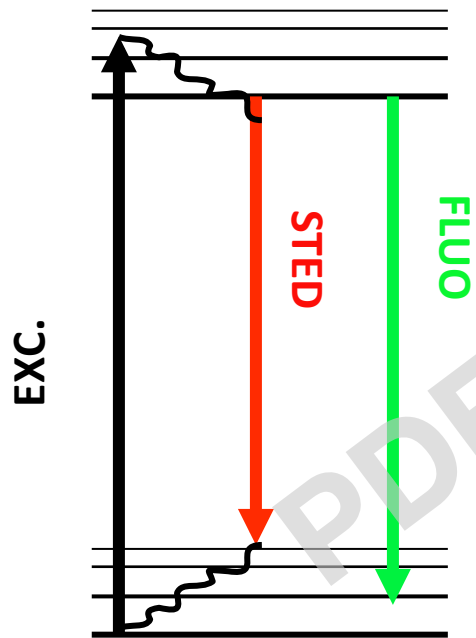
Exc: 561 nm, 2 ps  
Dep: 760 nm, 150 ps



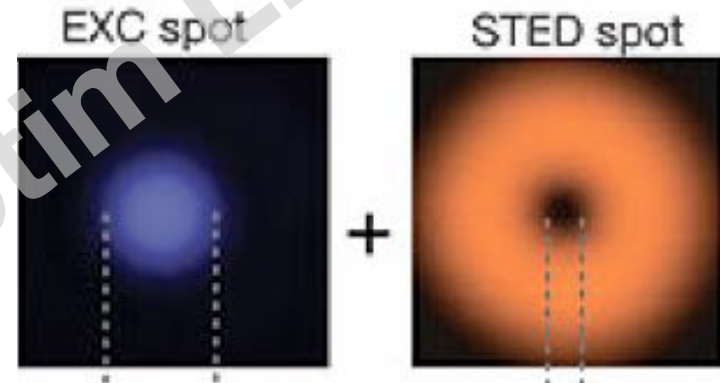
Hell, 1994

# STimulated Emission Depletion microscopy (STED)

Stimulated Emission

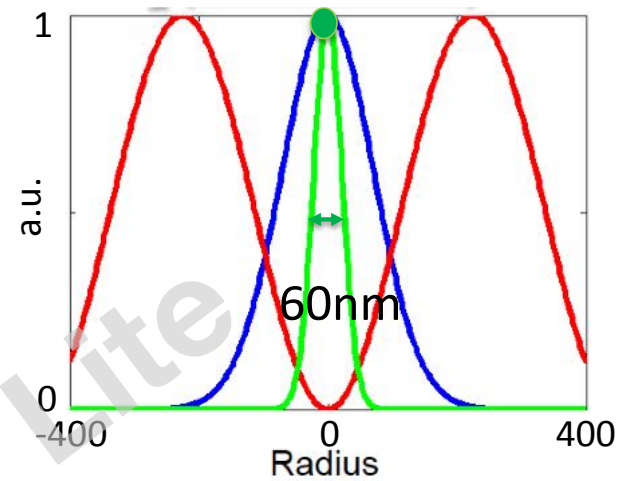
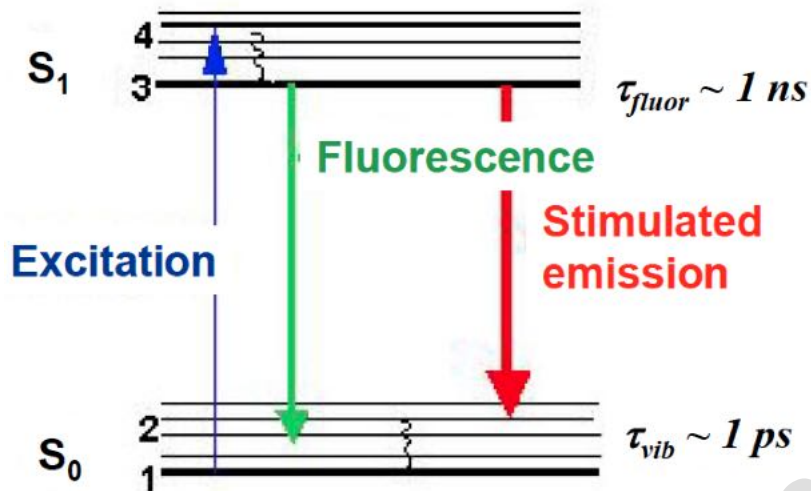


Structured illumination



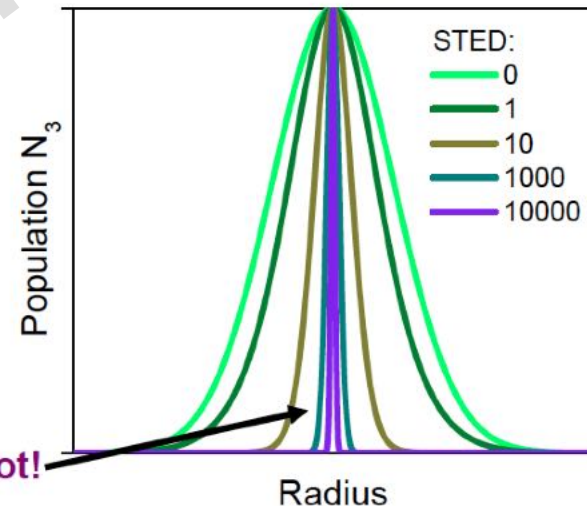
Hell, 1994

# Reduction of the fluorescence emission volume



$$N_3 = \sigma_{14} N_1 \tau_{vib} I_{Exc} e^{-I_{STED} \sigma_{23} t}$$

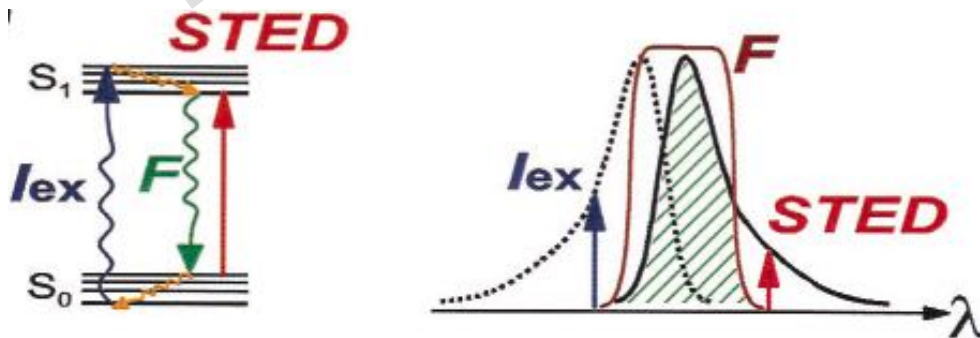
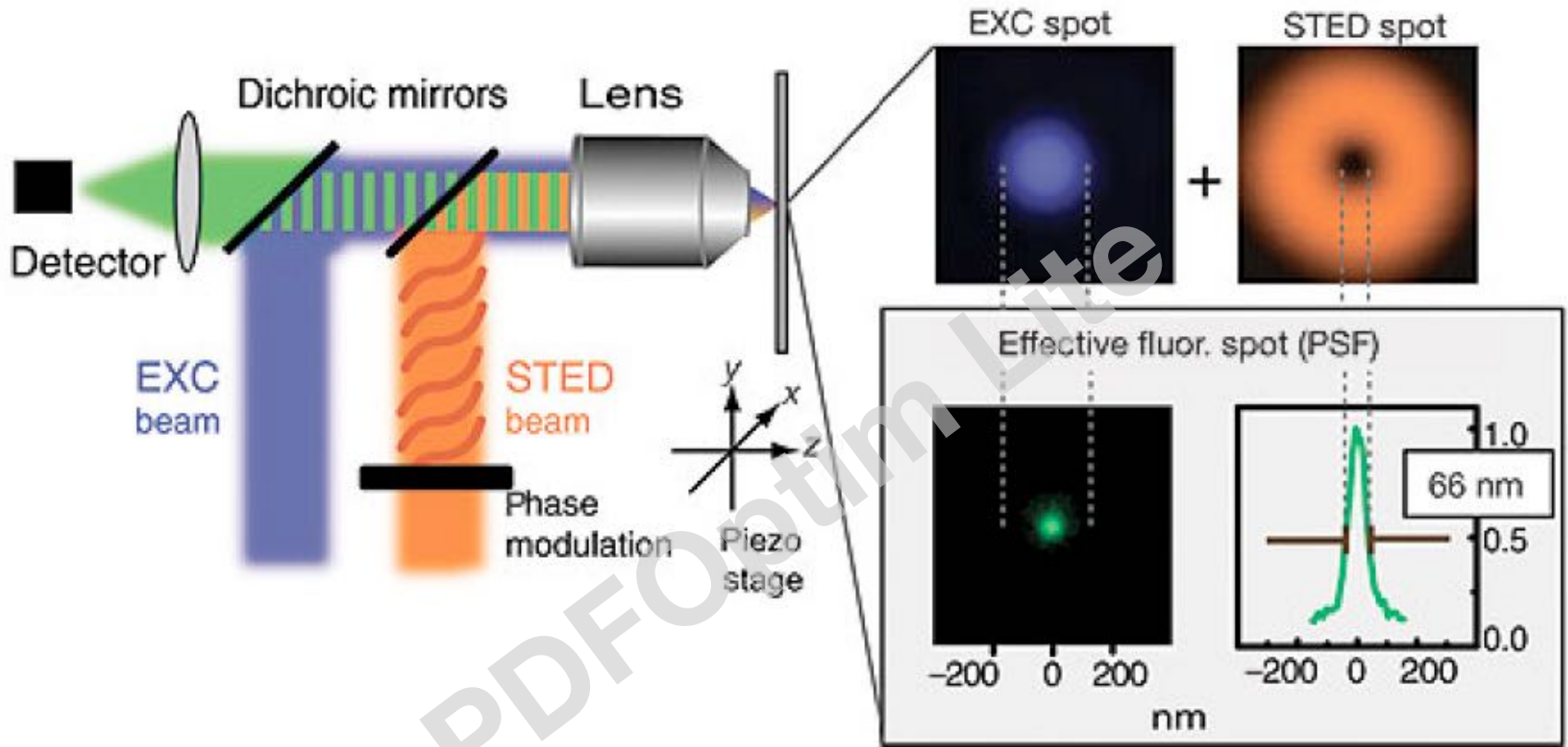
$$\text{STED resolution: } \Delta r \sim \frac{p}{\sqrt{I_{STED}}}$$



Fluorescence produces from a small spot!

In practice, one generally uses a depletion beam with a doughnut shape to deplete molecules excited around the center of the excitation beam

# Experimental setup

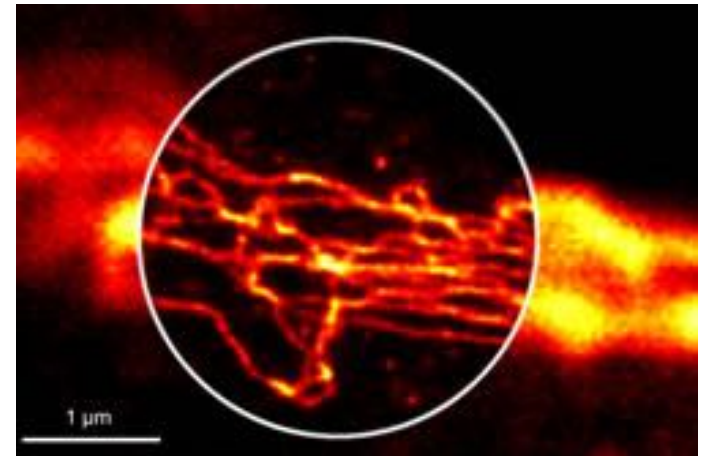
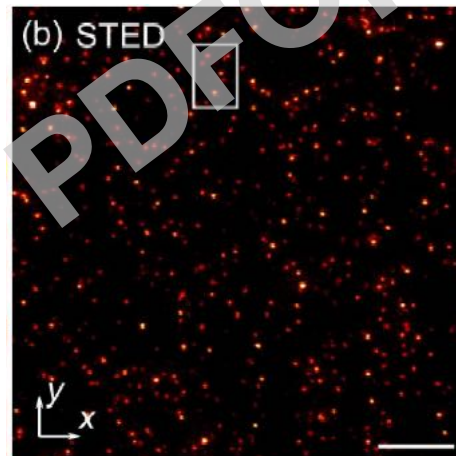
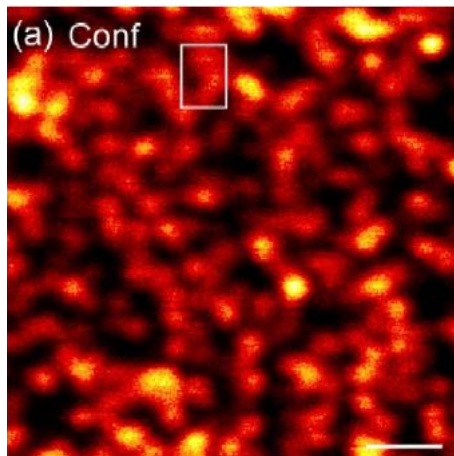
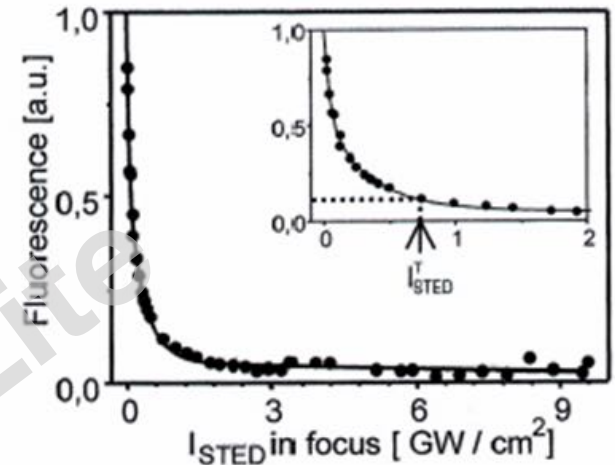


# Illustrations

Experimental proof of the non-linear dependence of the excited state population with depletion beam intensity

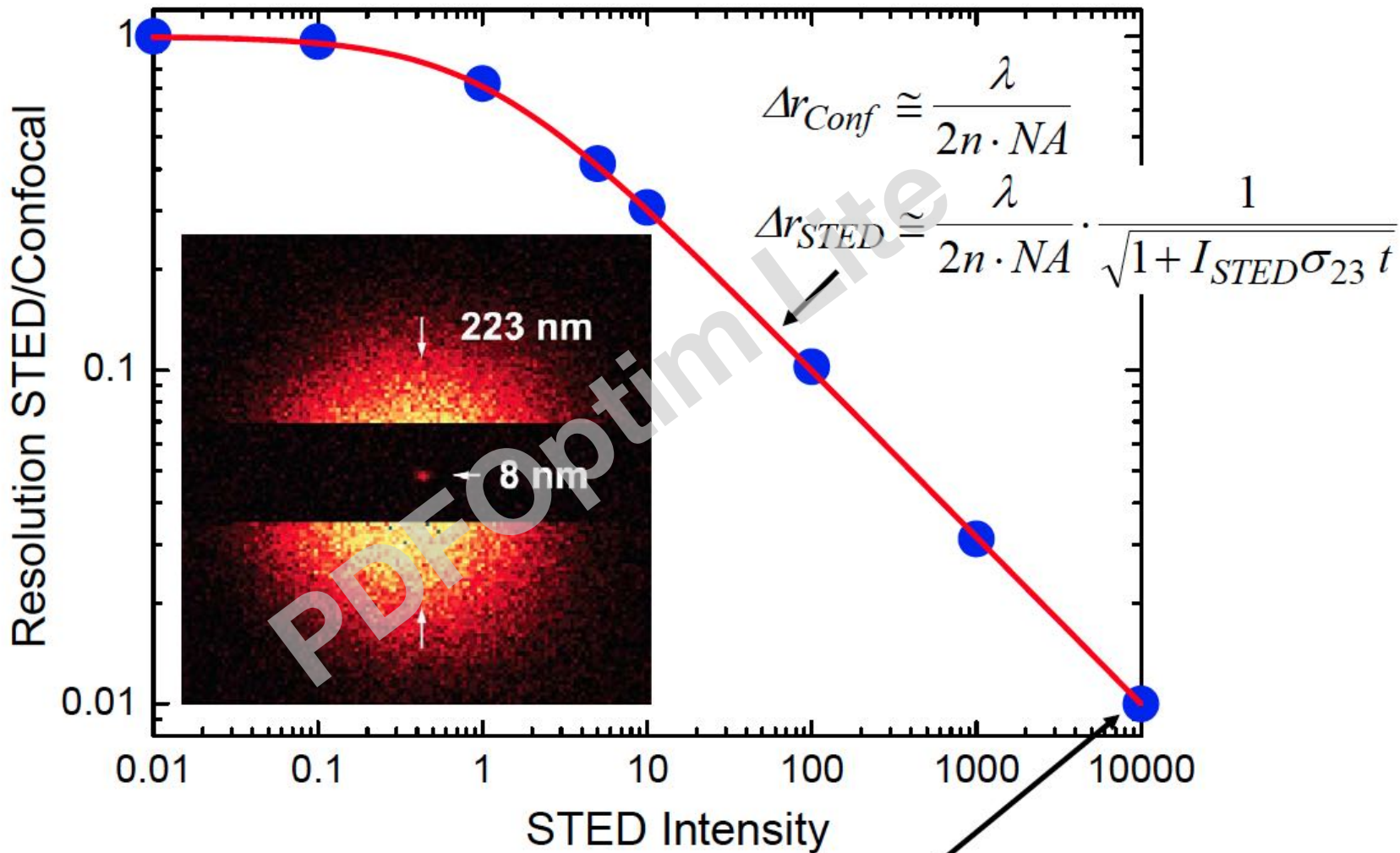
$$N_3 = \sigma_{14} N_1 \tau_{vib} I_{Exc} e^{-I_{STED} \sigma_{23} t}$$

The quality of the “zero” in the depletion beam is crucial



Images of 24nm fluorescent beads and of neuron from S. Hell Group

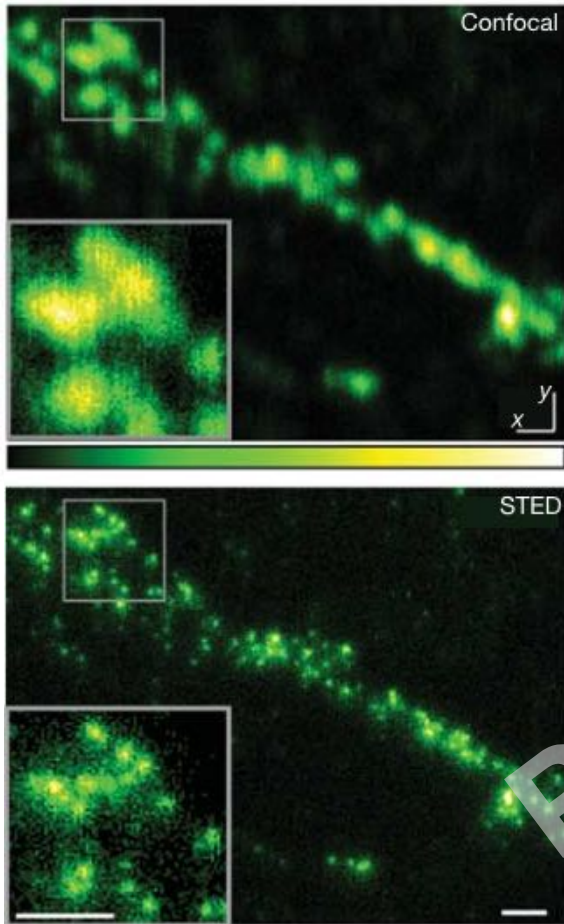
# Résolution du STED



**Better than confocal by a factor of 100 !**

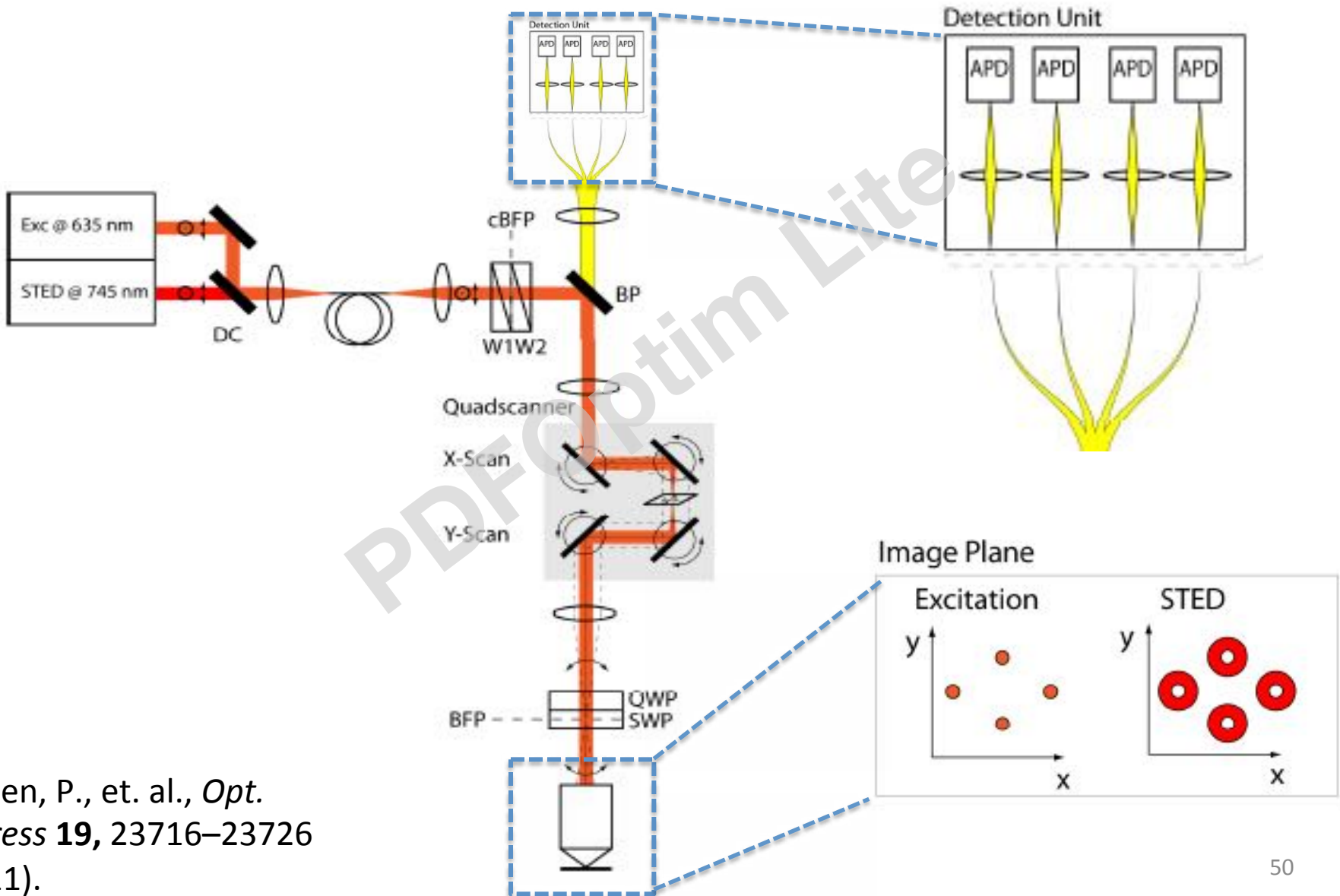


# STED Nanoscopy



- STED nanoscopy techniques are based on single point-scanning
- Gain in spatial resolution requires dense pixelation and hence long recording times
- This constitutes a drawback for fast wide field imaging
- need parallelization

# Multi-doughnut STED microscopy

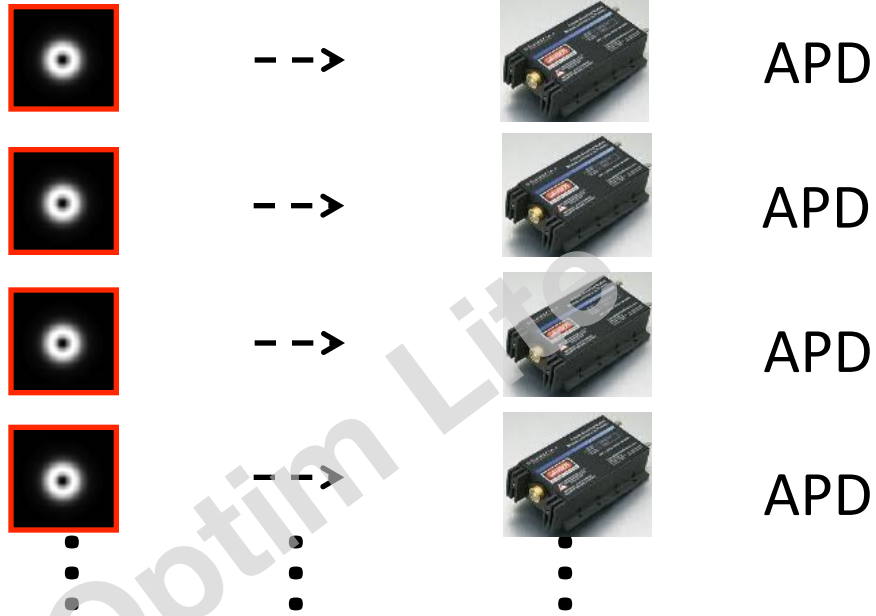


Bingen, P., et. al., *Opt. Express* **19**, 23716–23726 (2011).

# STED Parallelization

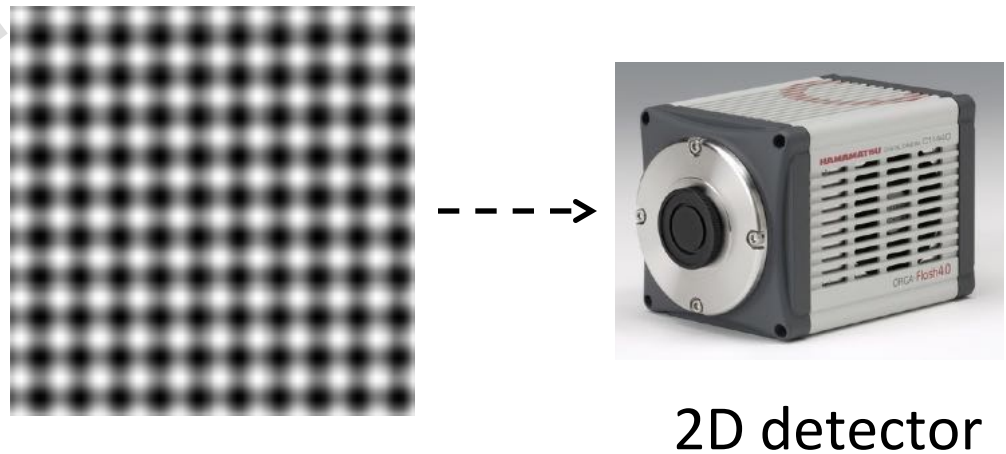
## Multi doughnuts configuration:

- Depletion power limit
- Experimentally Complicated



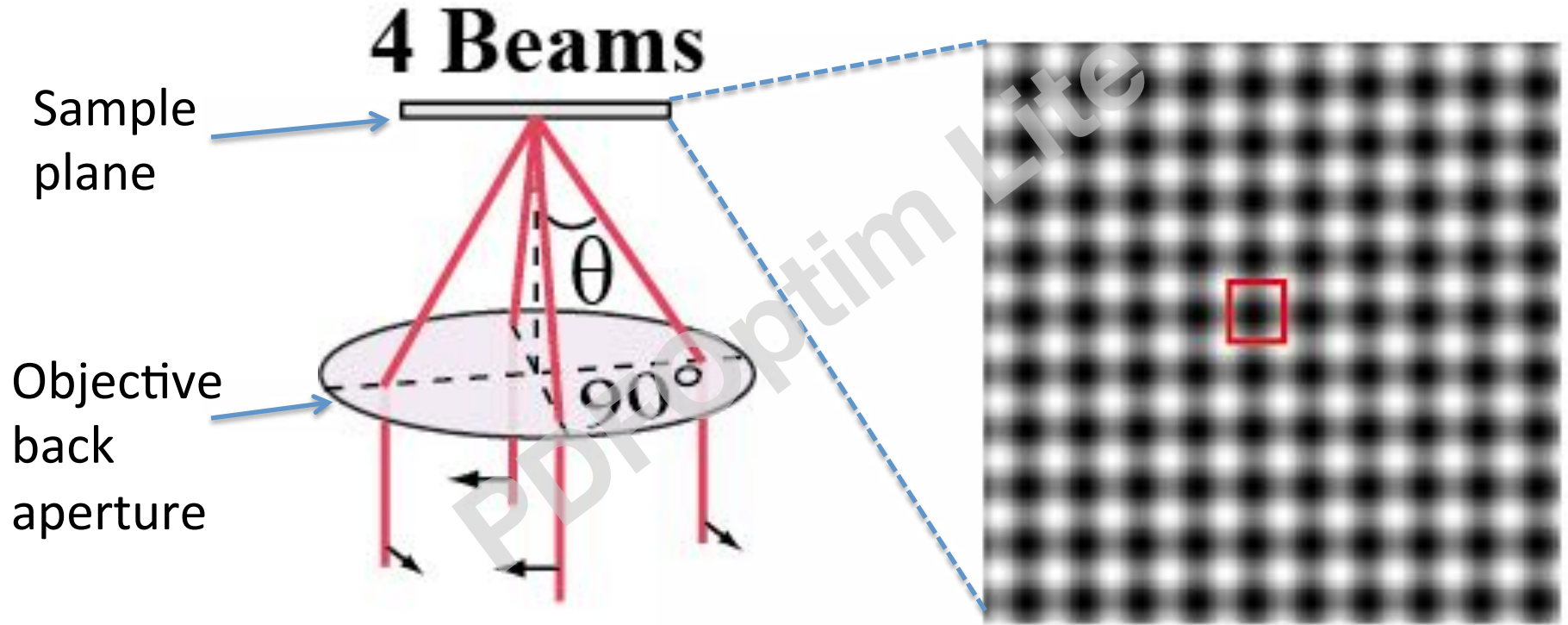
## Large STED parallelization:

- wide-field excitation
- optical lattices for depletion
- A fast camera for detection



2D detector

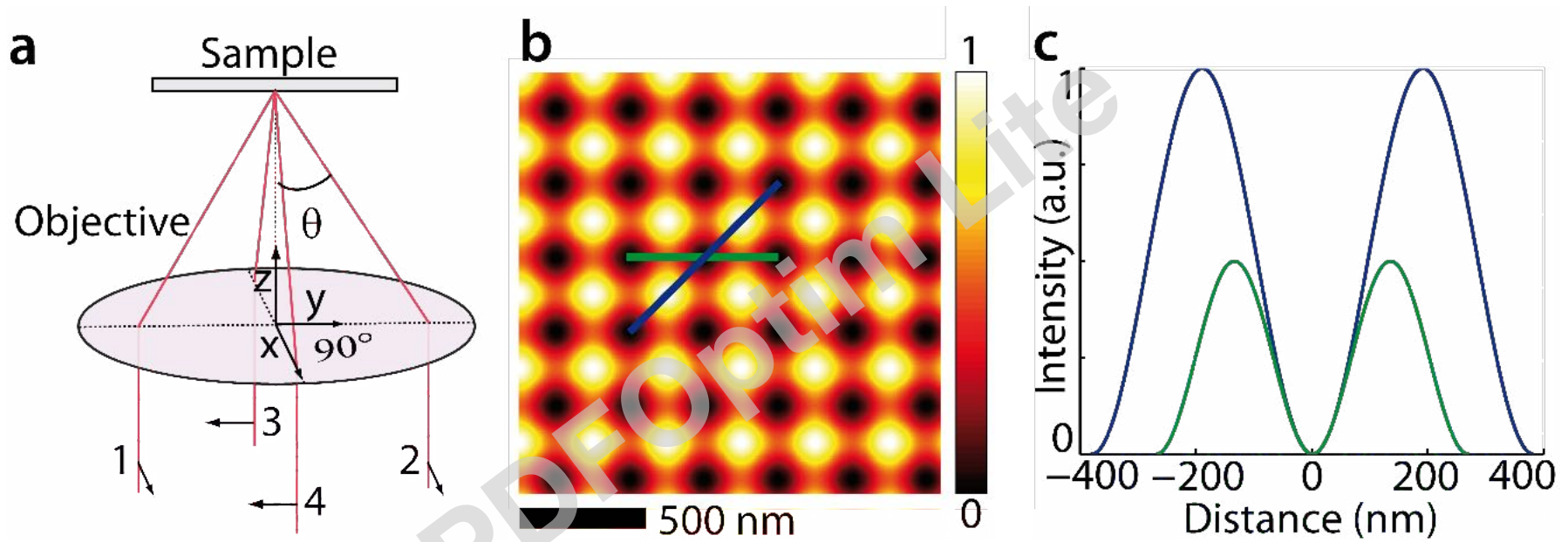
# Lattice-STED microscopy



Optical lattices

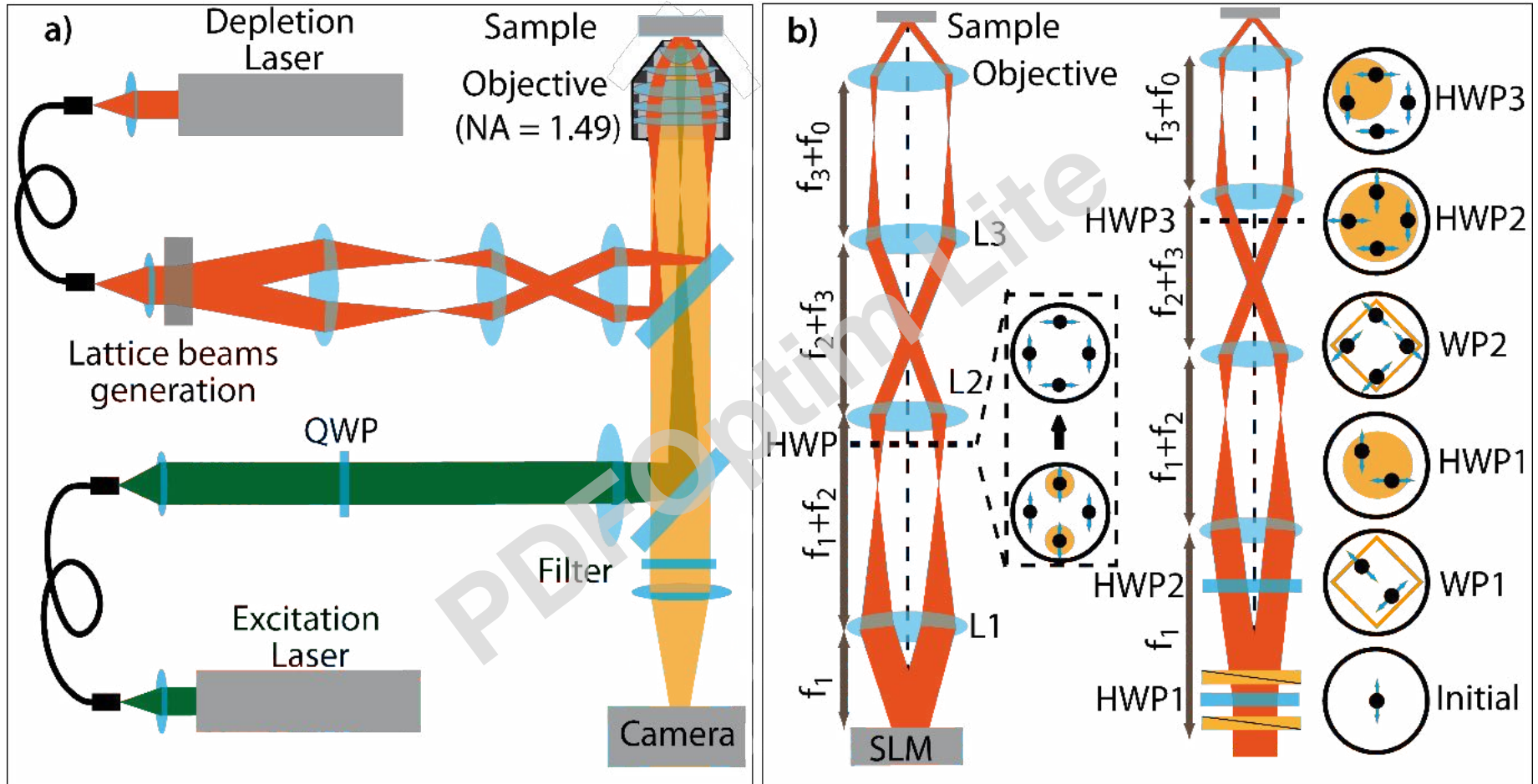
$$\text{Period: } p = \frac{\lambda}{2n \sin\theta}$$

# Lattice-STED microscopy



$$\text{Period: } p = \frac{\lambda}{2n \sin\theta}$$

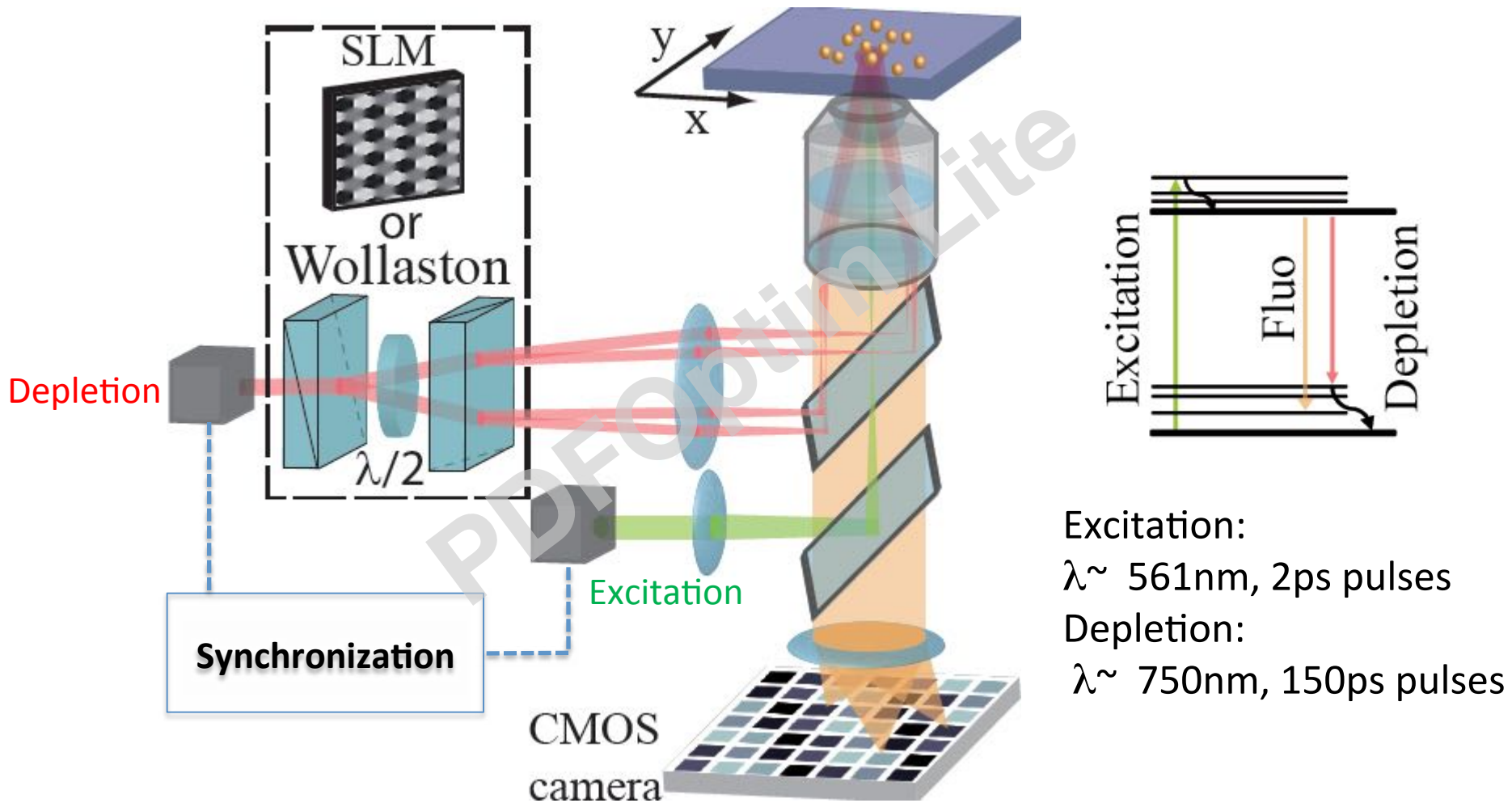
# Lattice-STED nanoscopy Setup



Excitation:  $\lambda \sim 561\text{nm}$ , 2ps pulses

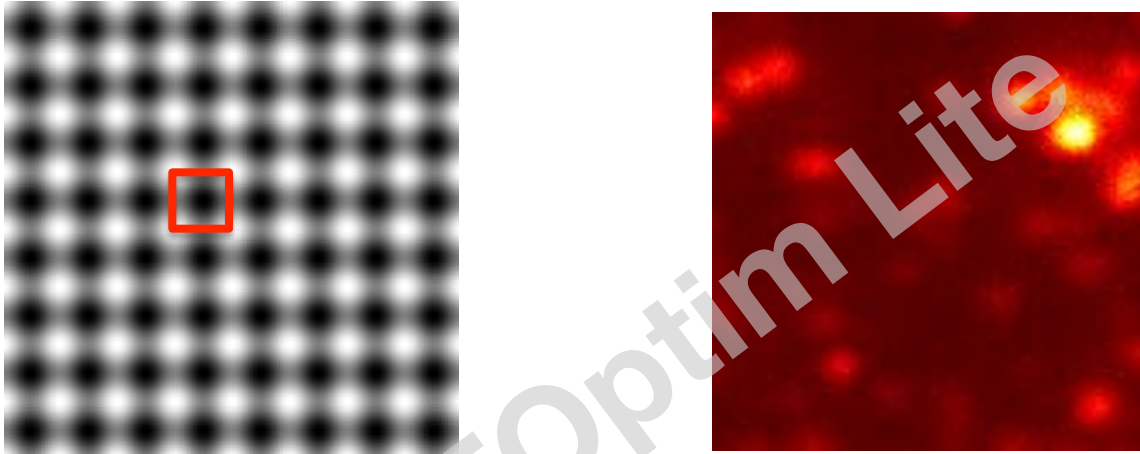
Depletion:  $\lambda \sim 750\text{nm}$ , 150ps pulses

# In-STED nanoscopy Setup



# Lattice-STED Images acquisition

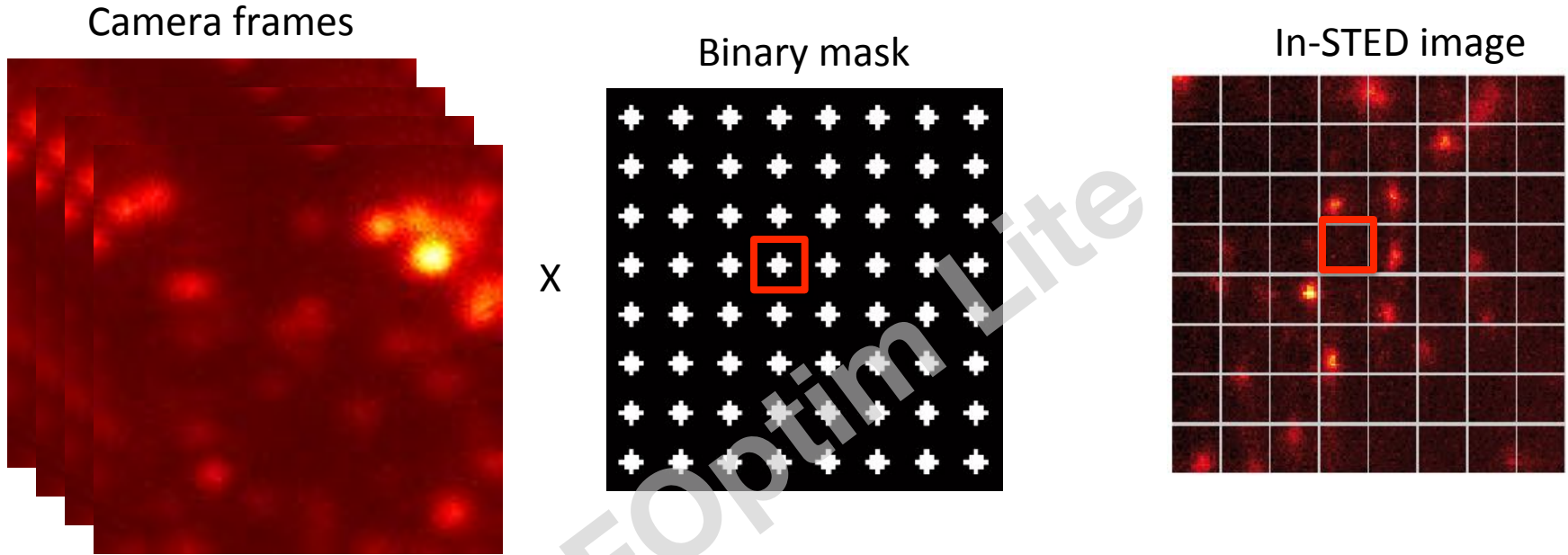
Depletion pattern



- **scan the sample over a unit cell** in the presence of the wide field excitation and the depletion pattern, while acquiring a fluorescence image for each scanning step
- A stack of camera frames is produced

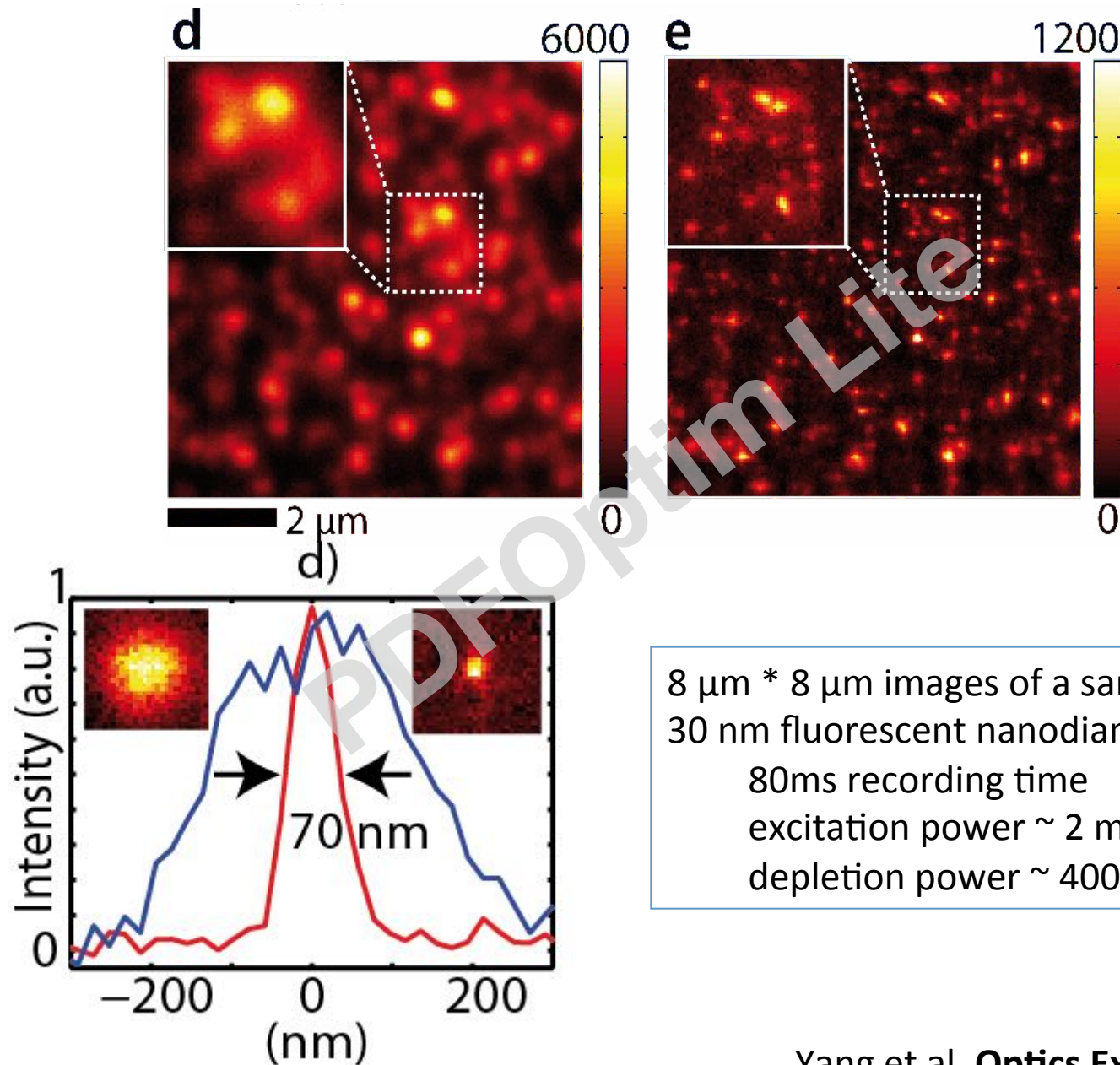


# Lattice-STED Images acquisition



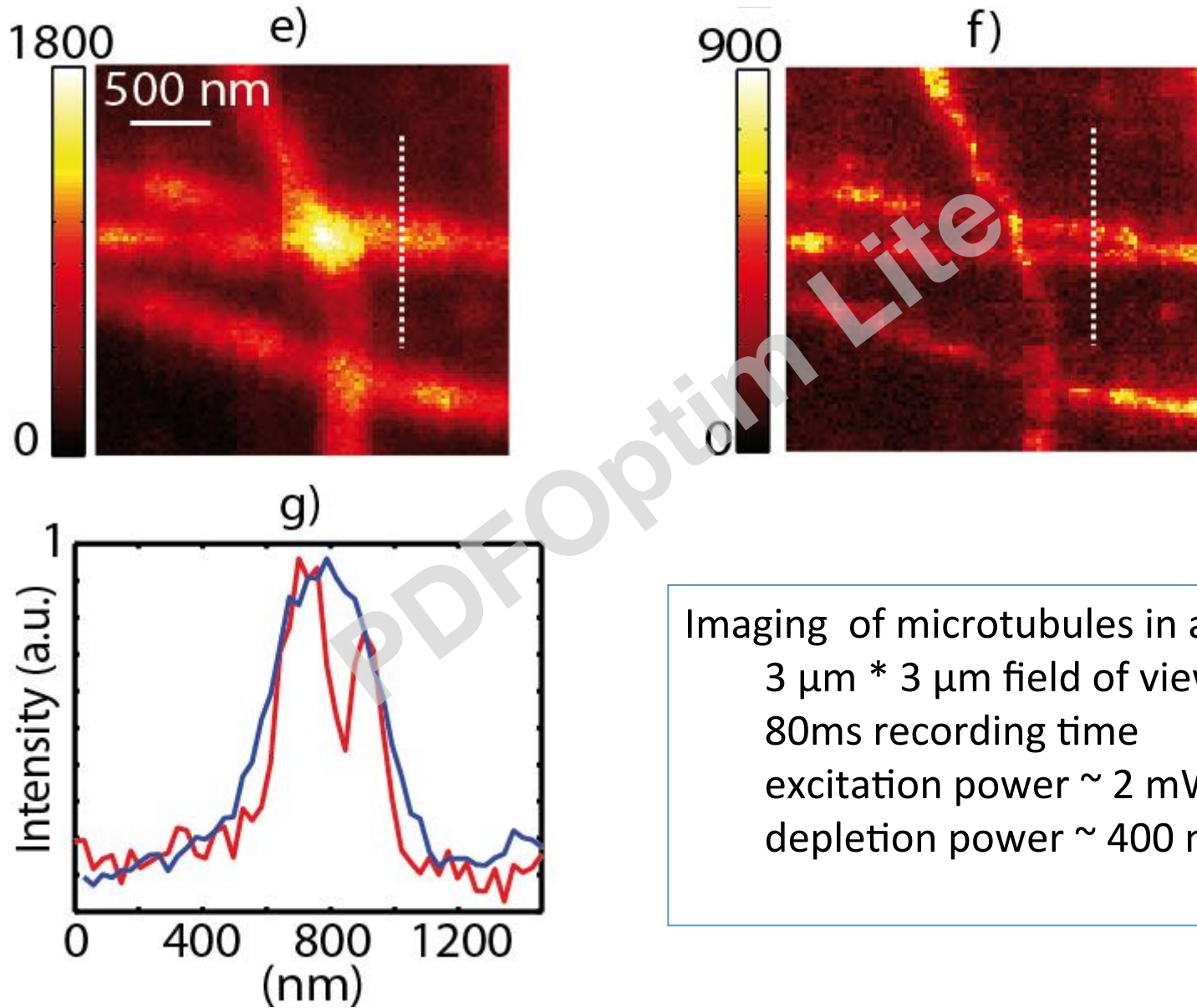
- Overlay a binary mask on the images, the transparent parts corresponding to the minima positions of the depletion pattern.
- CMOS camera + digital mask  $\rightarrow$  Array of parallelized “point detectors” recording an image of the size of the lattice unit cell.
- The In-STED image obtained by assembling all the unit cell images together.

# Lattice-STED images



8 μm \* 8 μm images of a sample containing  
30 nm fluorescent nanodiamonds  
80ms recording time  
excitation power ~ 2 mW  
depletion power ~ 400 mW

# Lattice-STED images

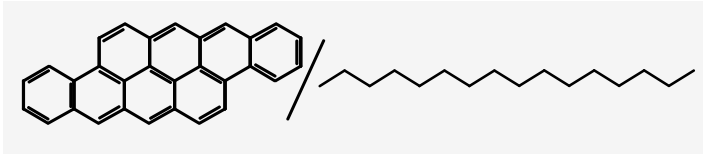


Cryogenic super-resolution microscopy  
by Excited State Saturation (ESSat)

Yang et al. (2015)

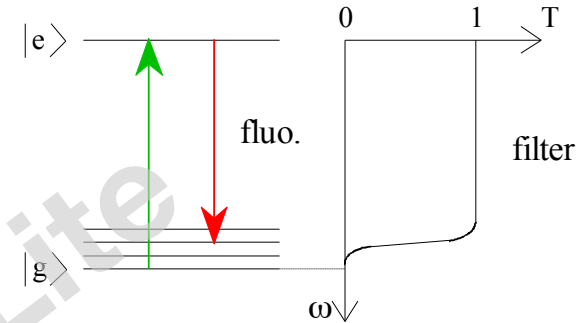
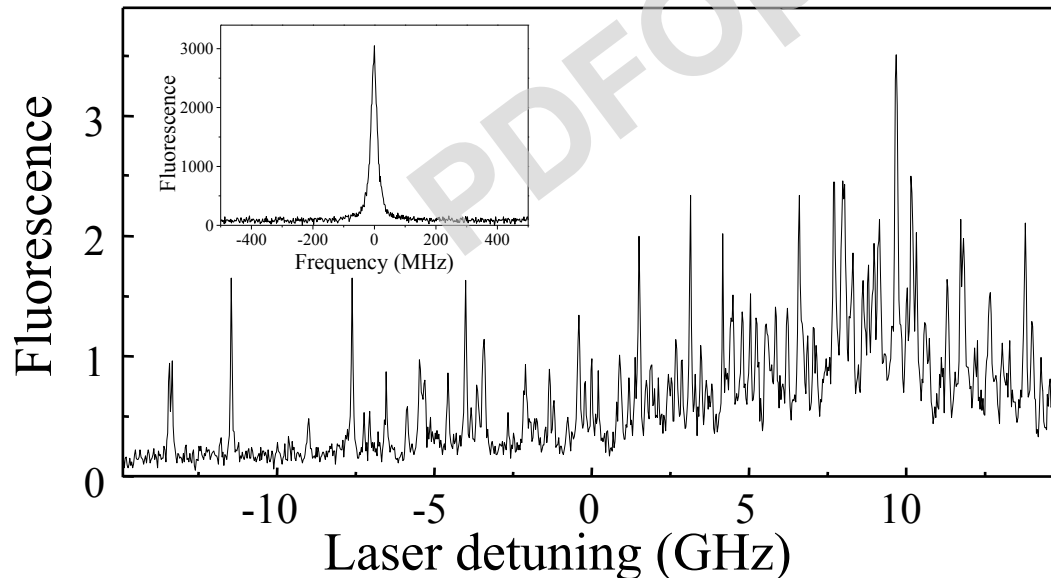
# Single Molecule Spectroscopy @ Low Temp.

## PAH molecules in Molecular Crystals



## Resonant Fluorescence Excitation spectra :

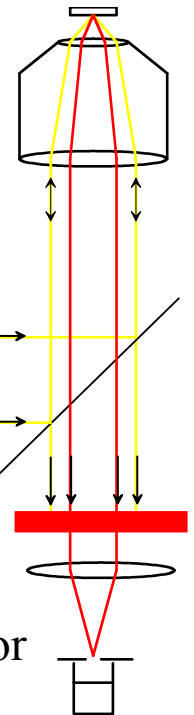
- Sharp Zero Phonon Lines ( $T_1$  limited)



Sample & objective in cryostat

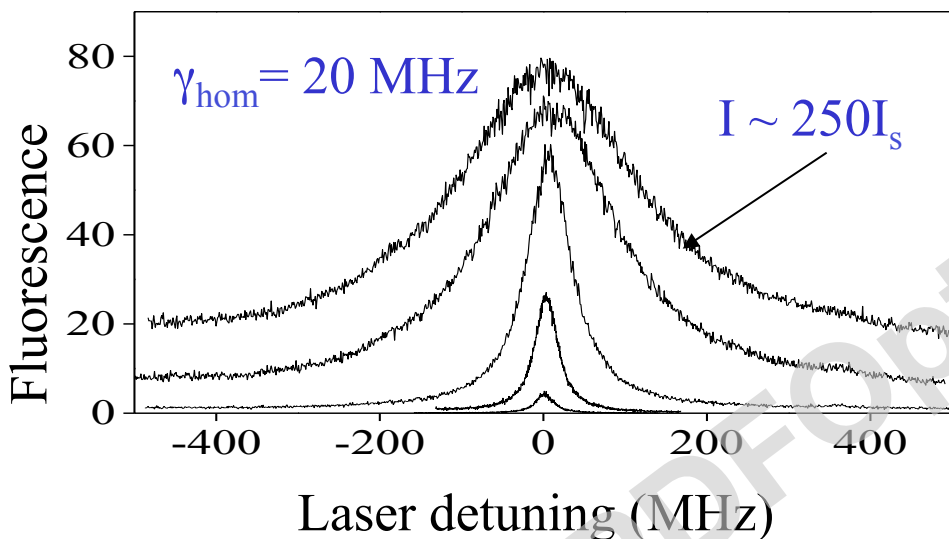
Tunable Single frequency Laser

Detector

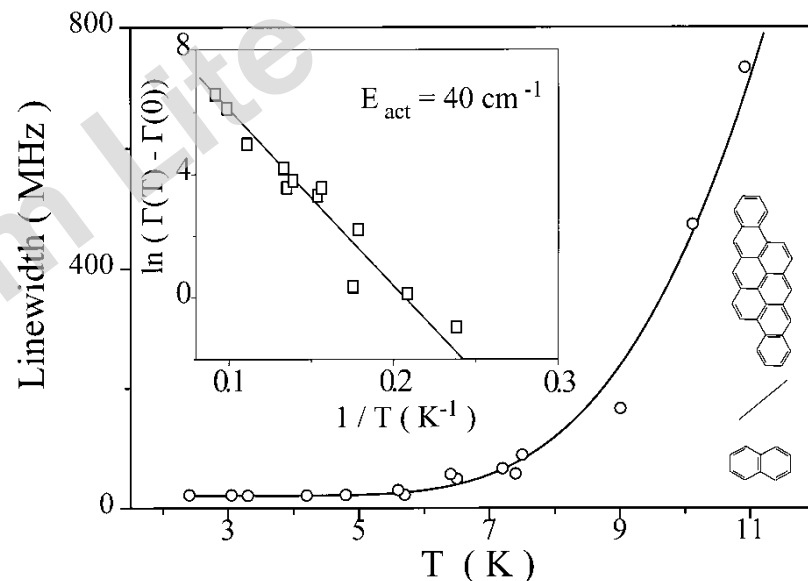


# Single Molecule Spectroscopy @ Low Temp.

## Intensity Saturation



## Temperature dependence



At low temperature and weak laser excitations  
Optical resonances with high quality factors (up to  $10^7$ - $10^8$ )  
Extremely stable lines: no spectral diffusion, no blinking

# Molecule excitation at linear regime

Image of a molecule excited with a Gaussian beam

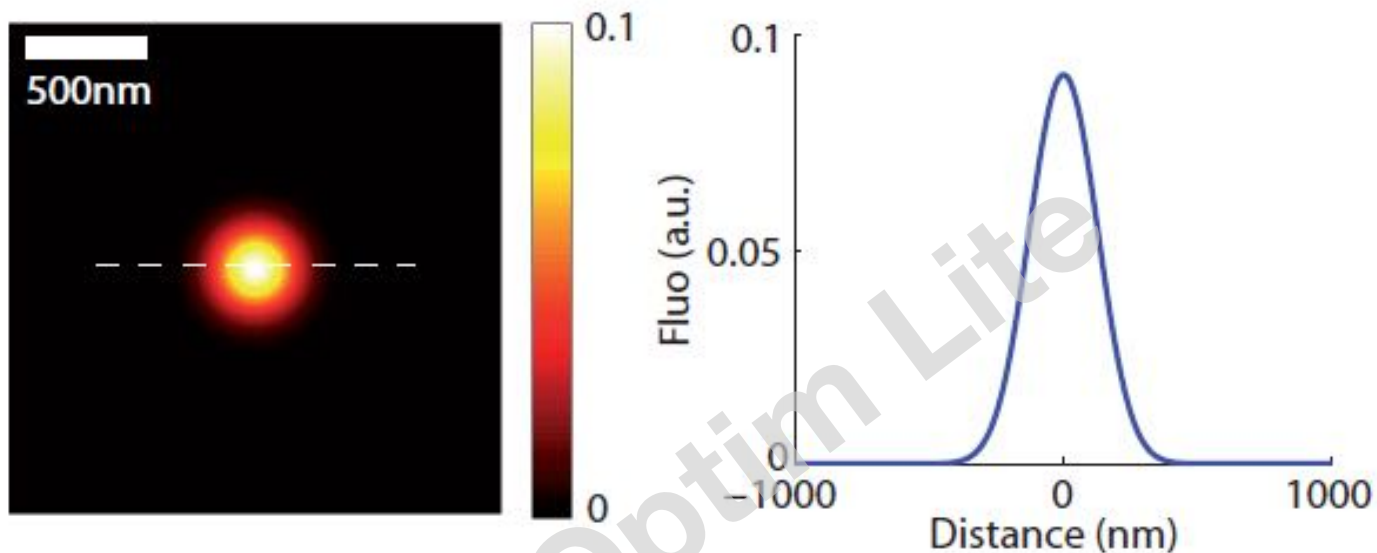
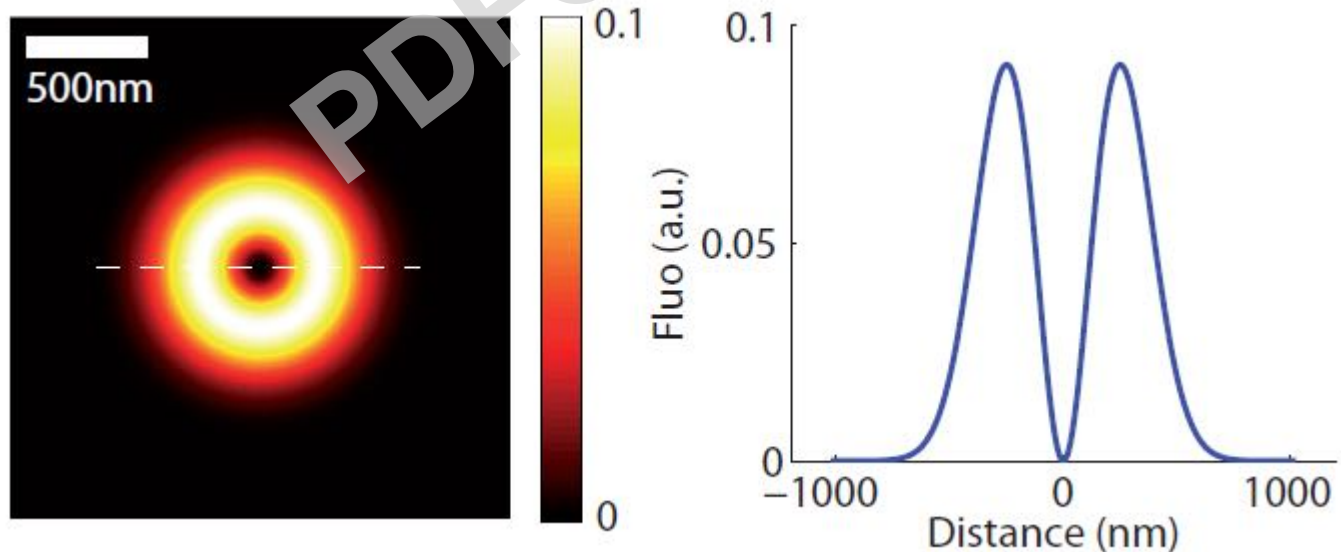
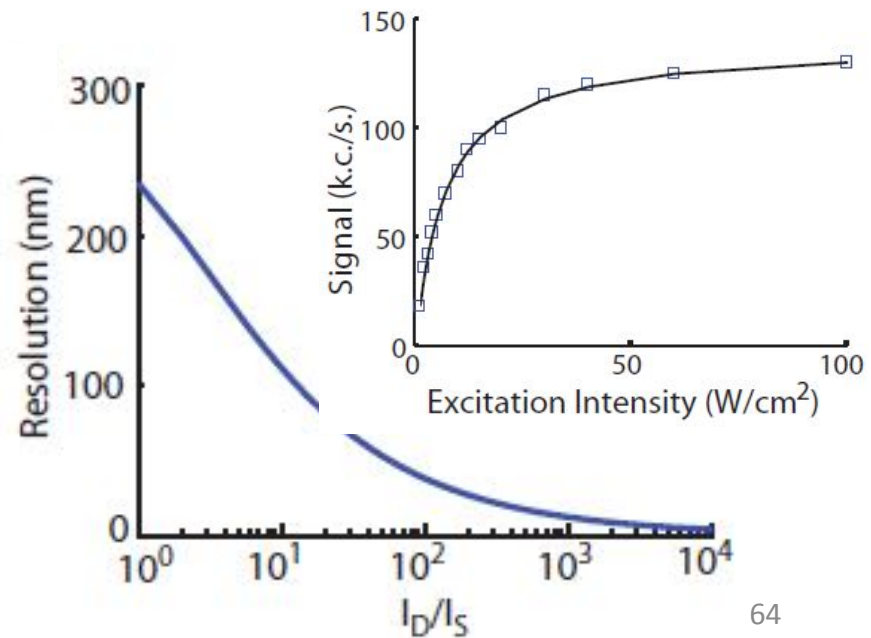
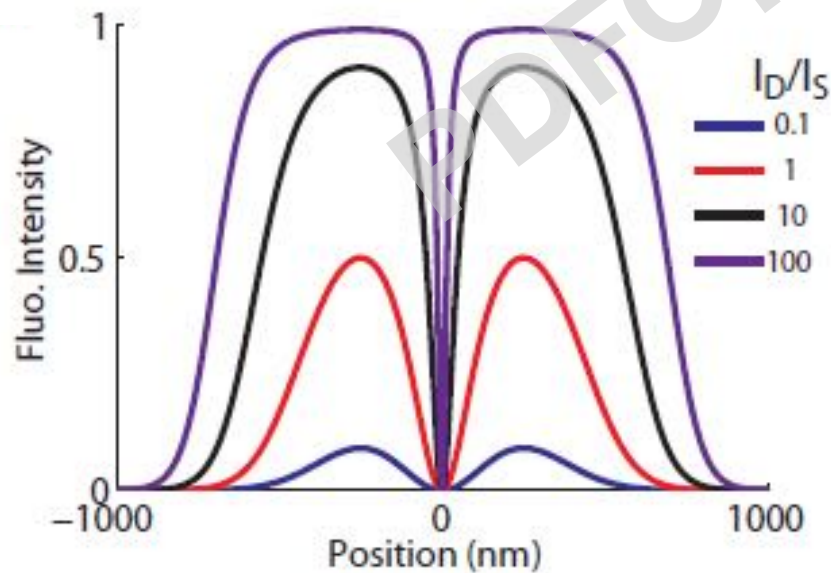
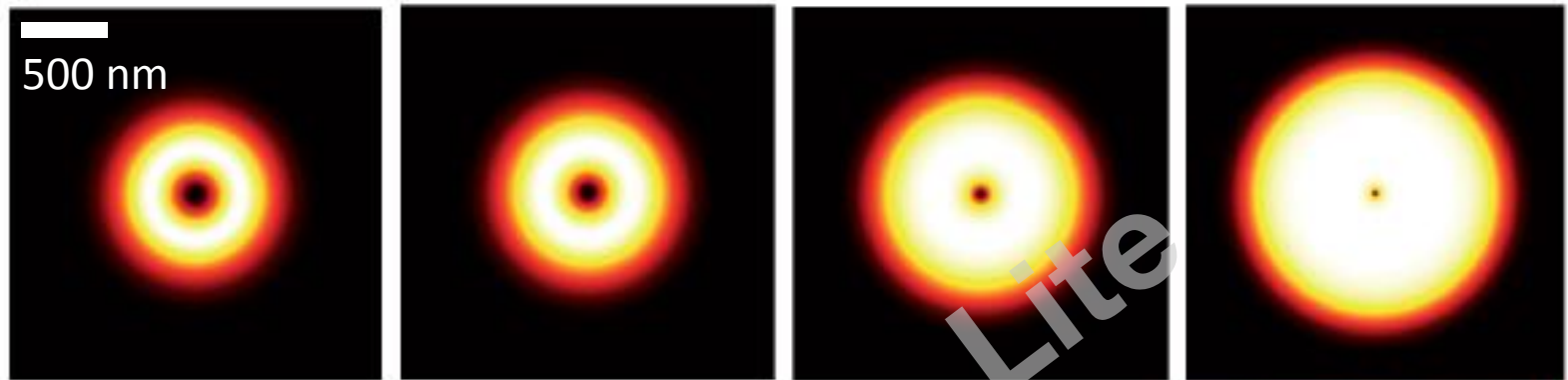


Image of a molecule excited with a doughnut beam



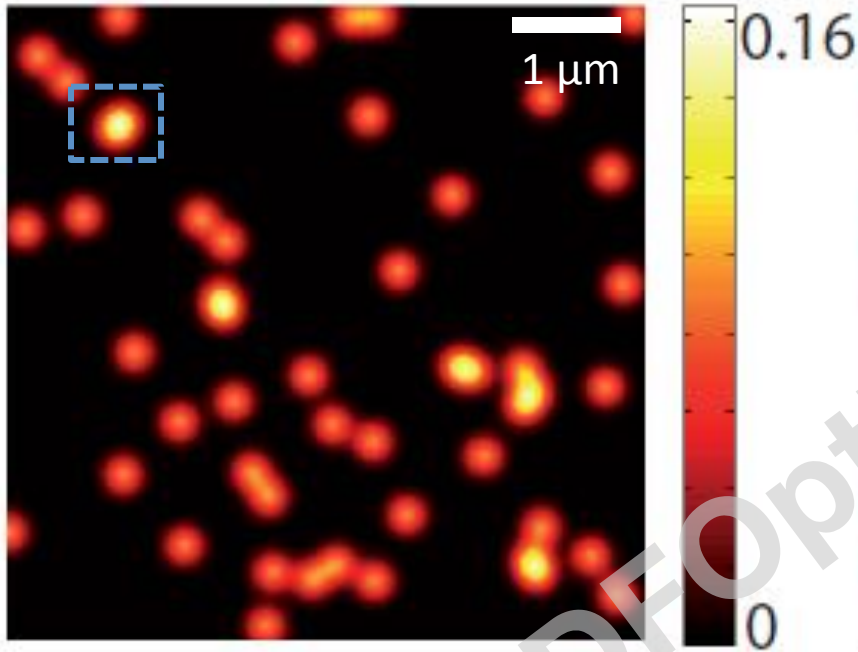
# Principle of ESSat microscopy



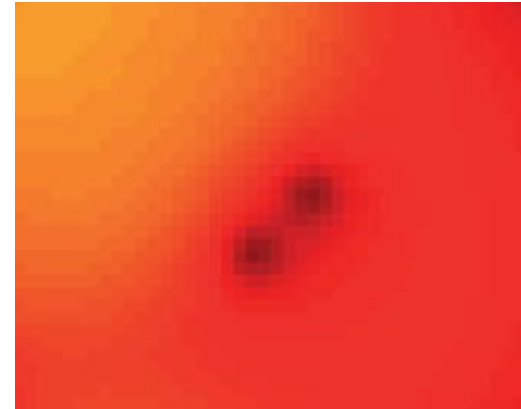
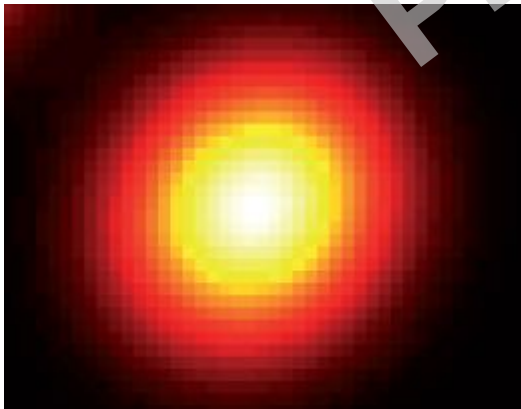
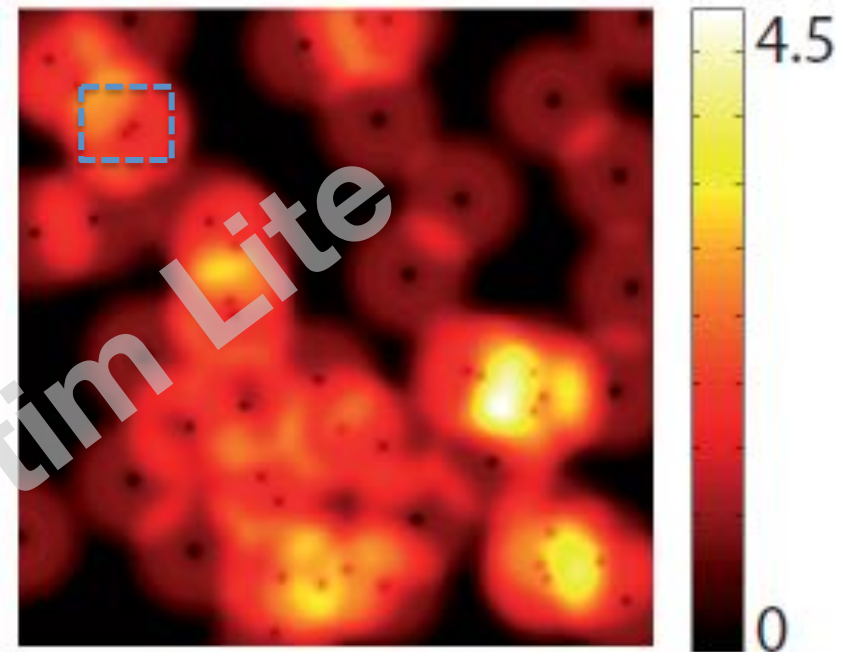


# Simulated confocal and ESSat images

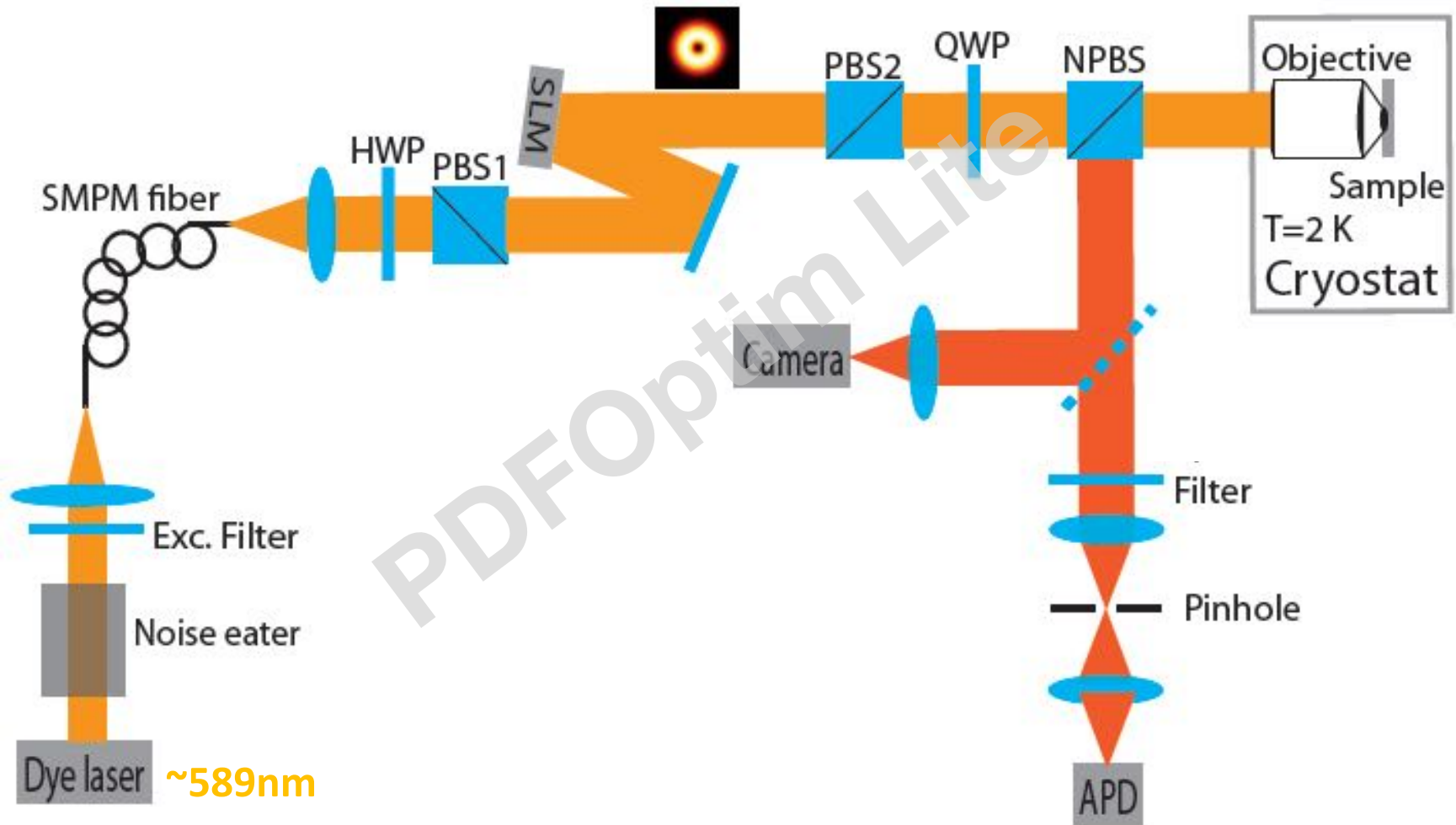
Confocal



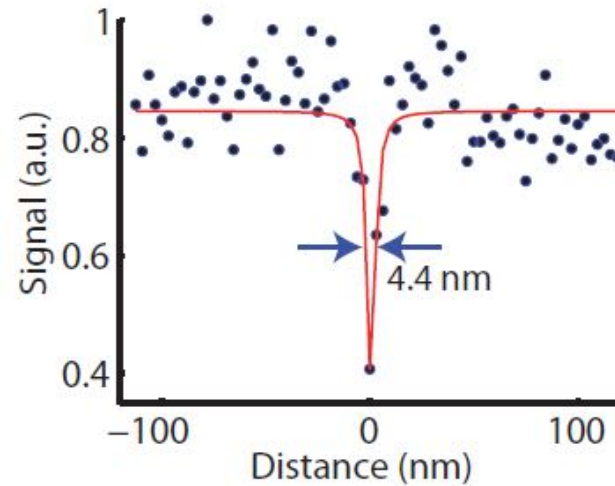
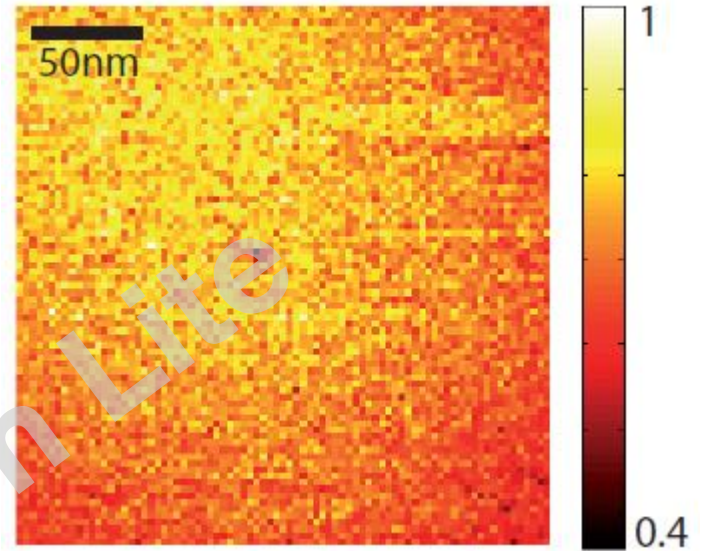
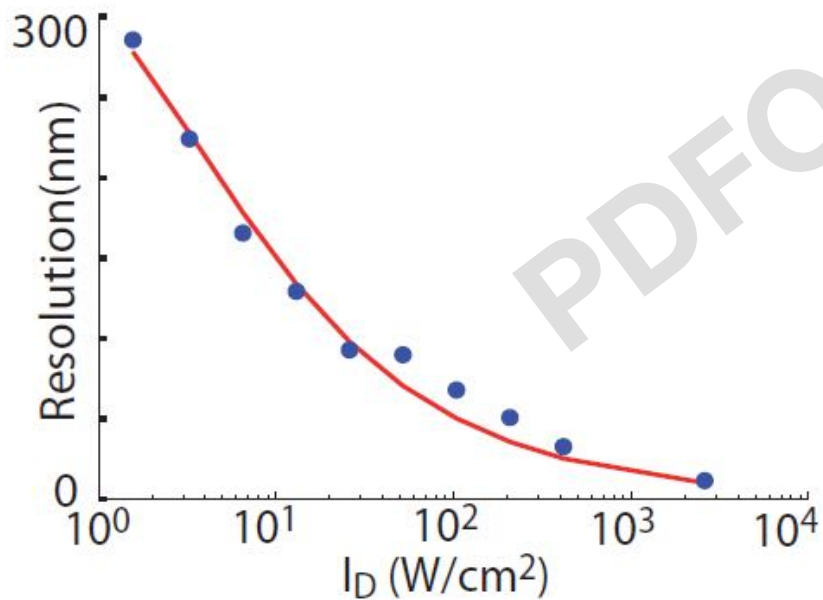
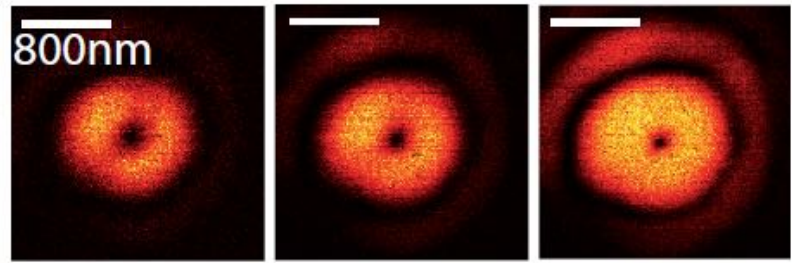
ESSat



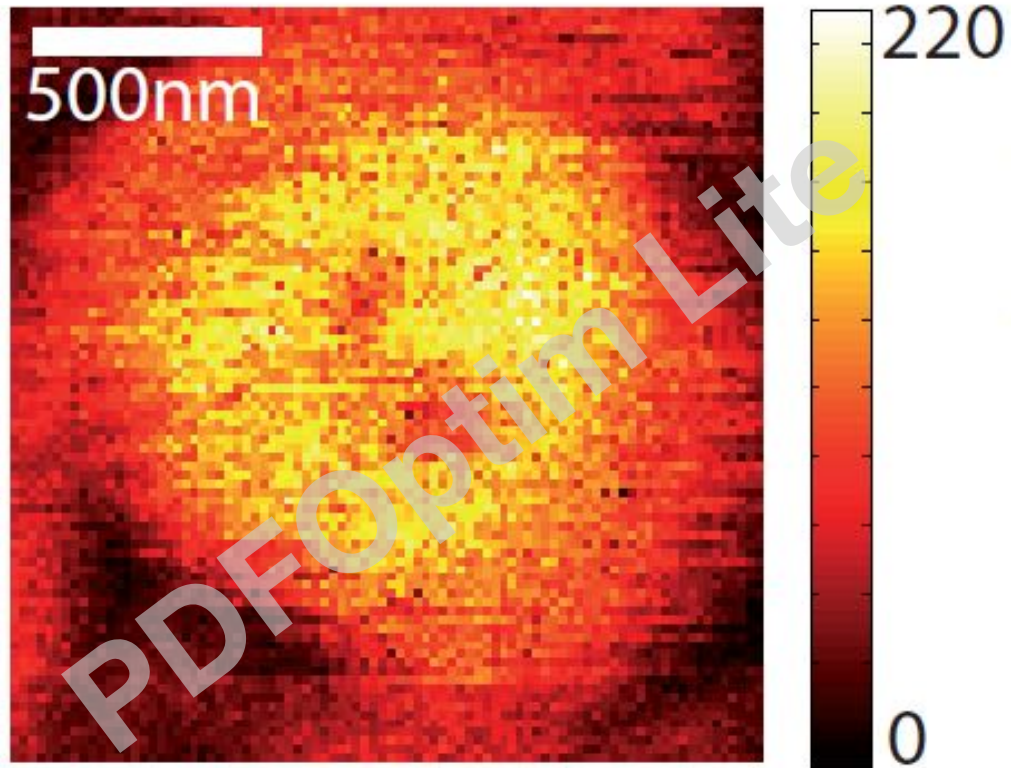
# Experimental setup of the ESSat microscope



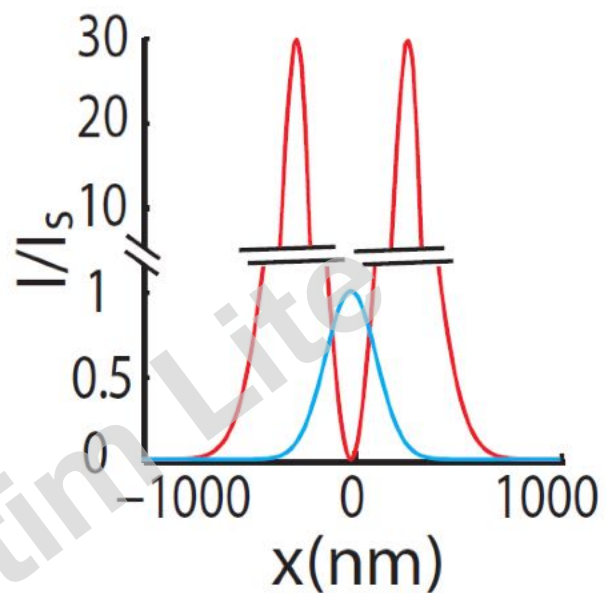
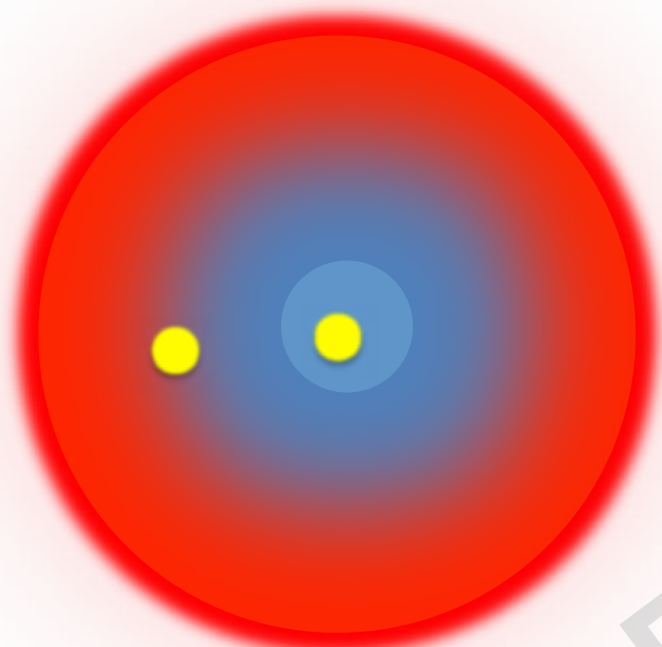
# Resolution of ESSat microscopy



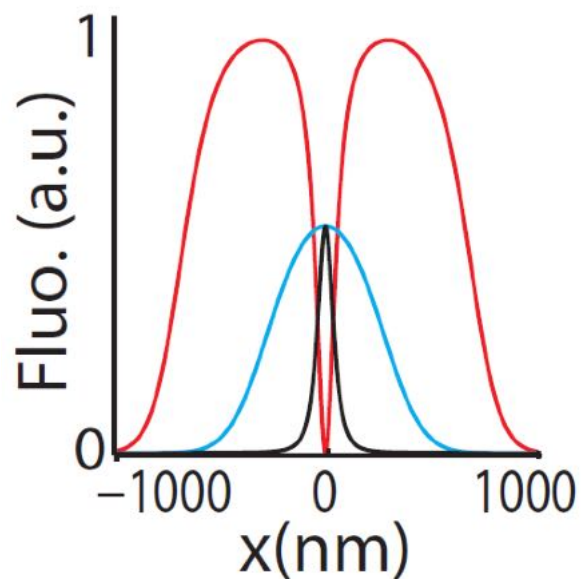
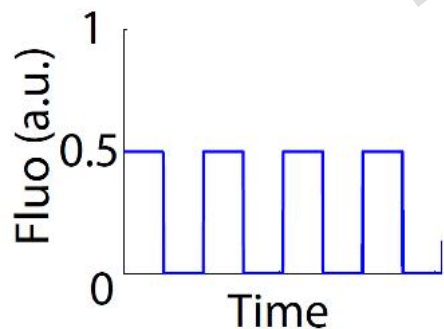
# Two super-resolved molecules



# Modulated-ESSat microscopy

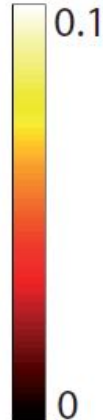
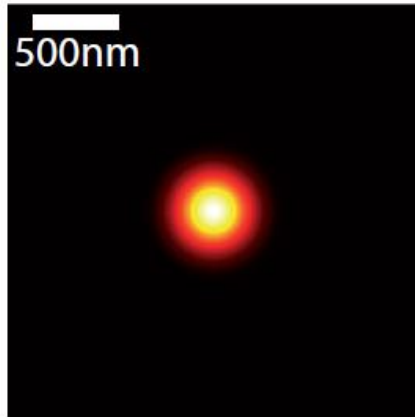


**Fluorescence signal**

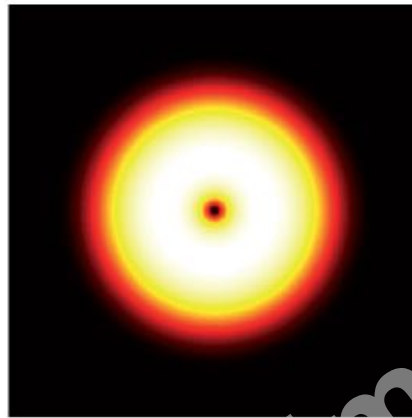


# Simulated images of single molecules

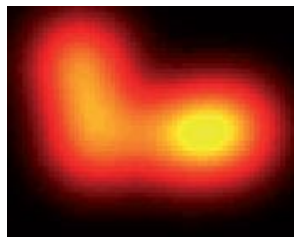
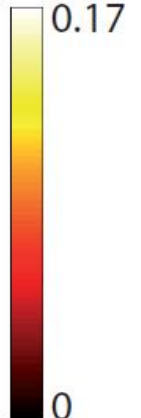
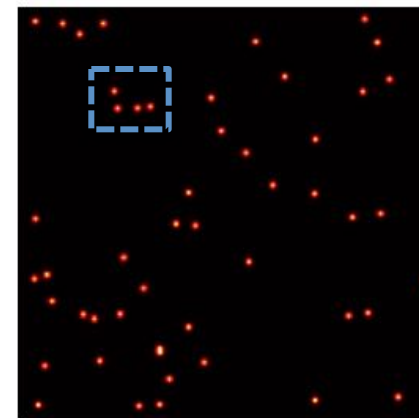
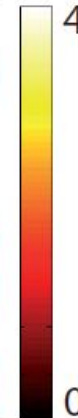
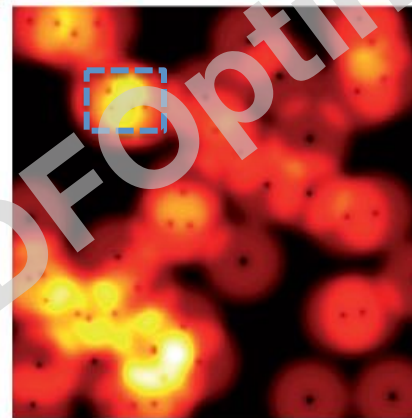
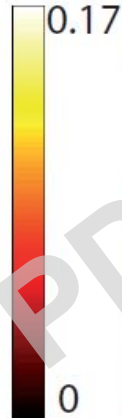
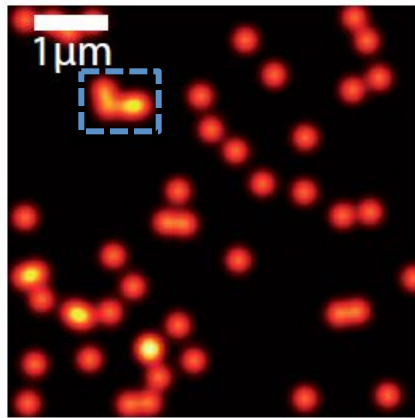
Confocal



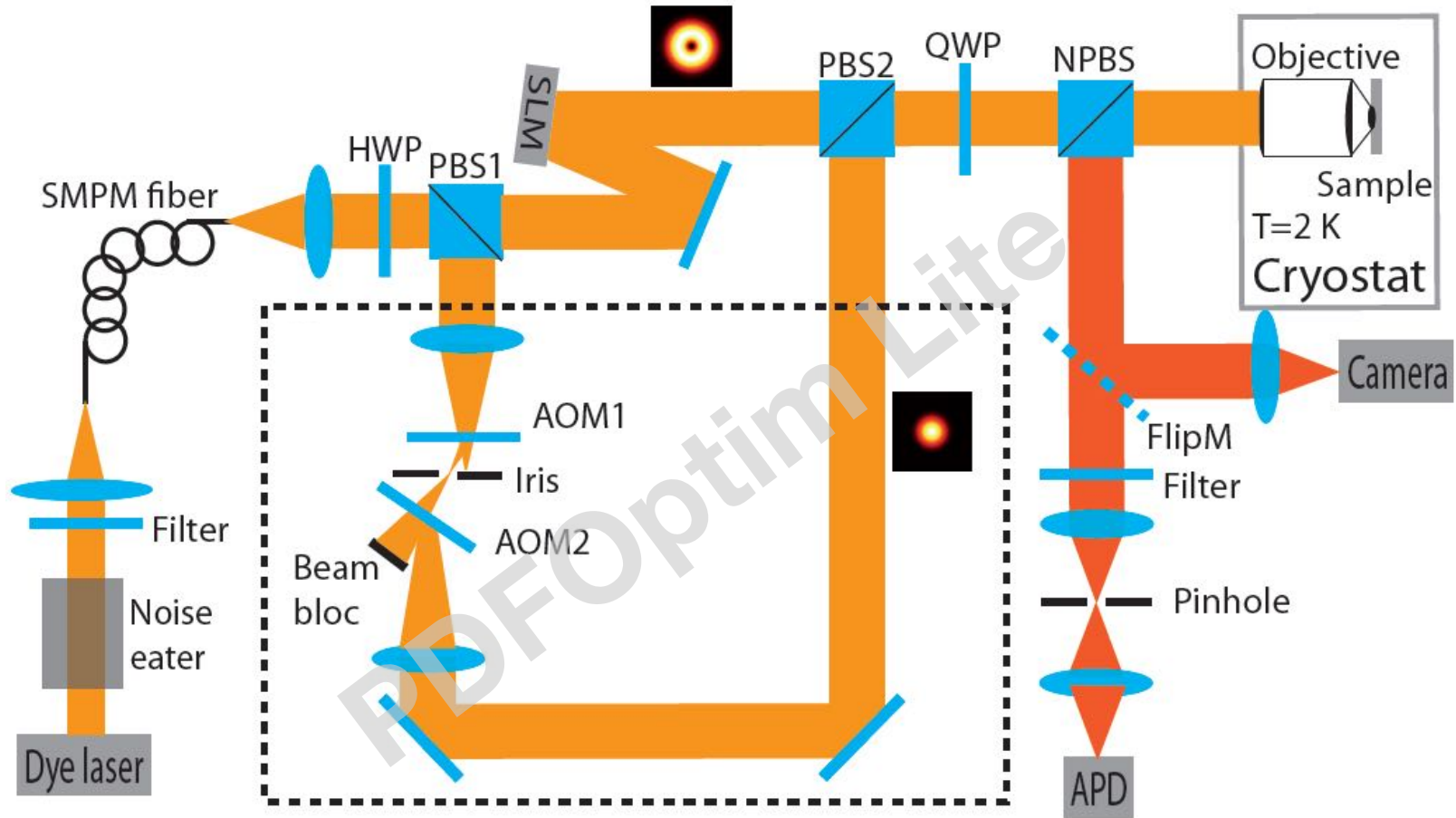
Direct-ESSat



Modulated-ESSat



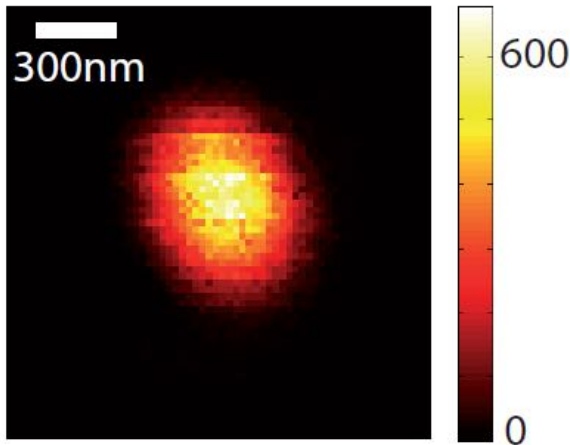
# Experimental setup of modulated-ESSat



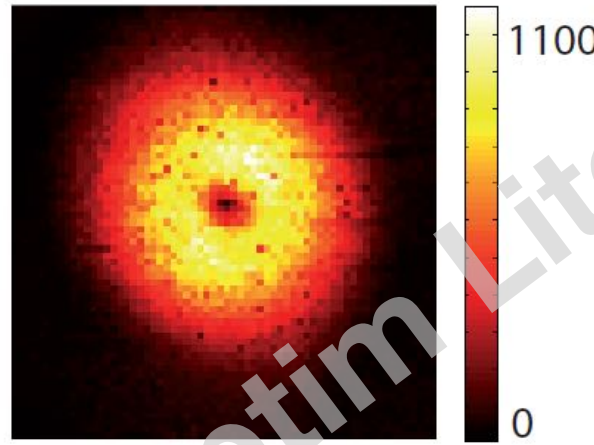
- ❑ Temporal modulation :  
1 kHz, 500  $\mu$ s “on” and 500  $\mu$ s “off”;
- ❑ Laser frequency shift:  $\sim$ 1 MHz

# Resolution of modulated-ESSat microscopy

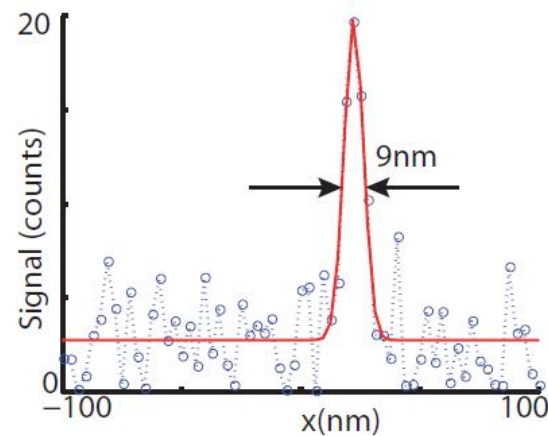
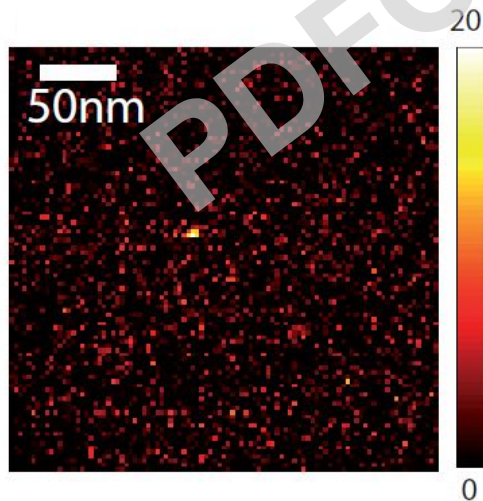
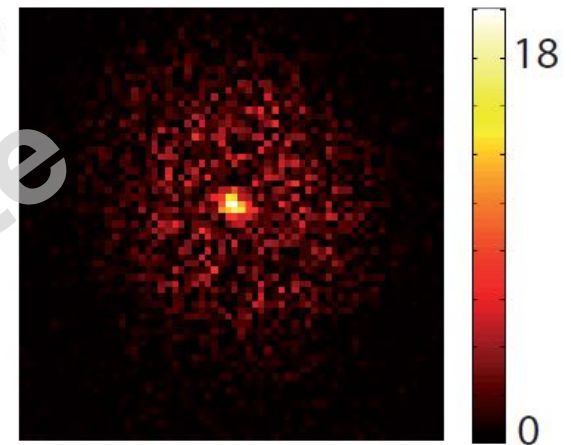
Confocal



Direct-ESSat



Modulated-ESSat

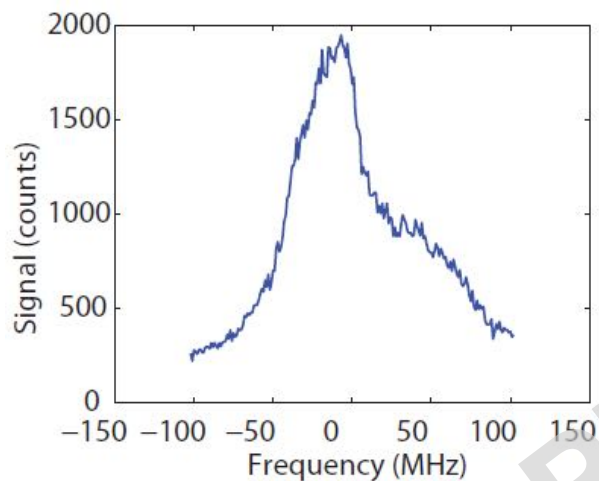




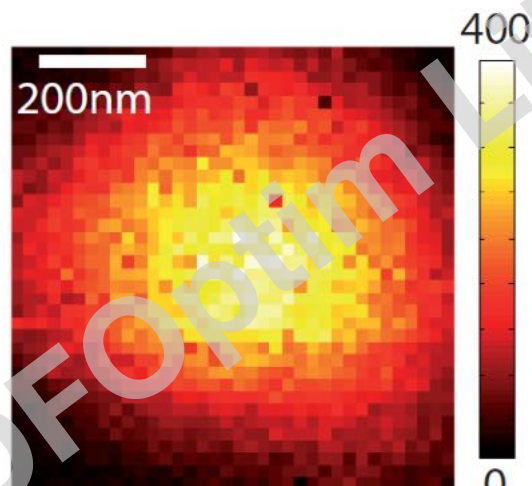
# Two molecules with overlapping resonances



Fluo. excitation spectrum



Confocal



Modulated-ESSat

